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## ROADMAP

## Roadmap for optical tweezers

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## Abstract

Optical tweezers are tools made of light that enable contactless pushing, trapping, and manipulation of objects, ranging from atoms to space light sails. Since the pioneering work by Arthur Ashkin in the 1970s, optical tweezers have evolved into sophisticated instruments and have been employed in a broad range of applications in the life sciences, physics, and engineering. These include accurate force and torque measurement at the femtonewton level, microrheology of complex fluids, single micro- and nano-particle spectroscopy, single-cell analysis, and statistical-physics experiments. This roadmap provides insights into current investigations involving optical forces and optical tweezers from their theoretical foundations to designs and setups. It also offers perspectives for applications to a wide range of research fields, from biophysics to space exploration.

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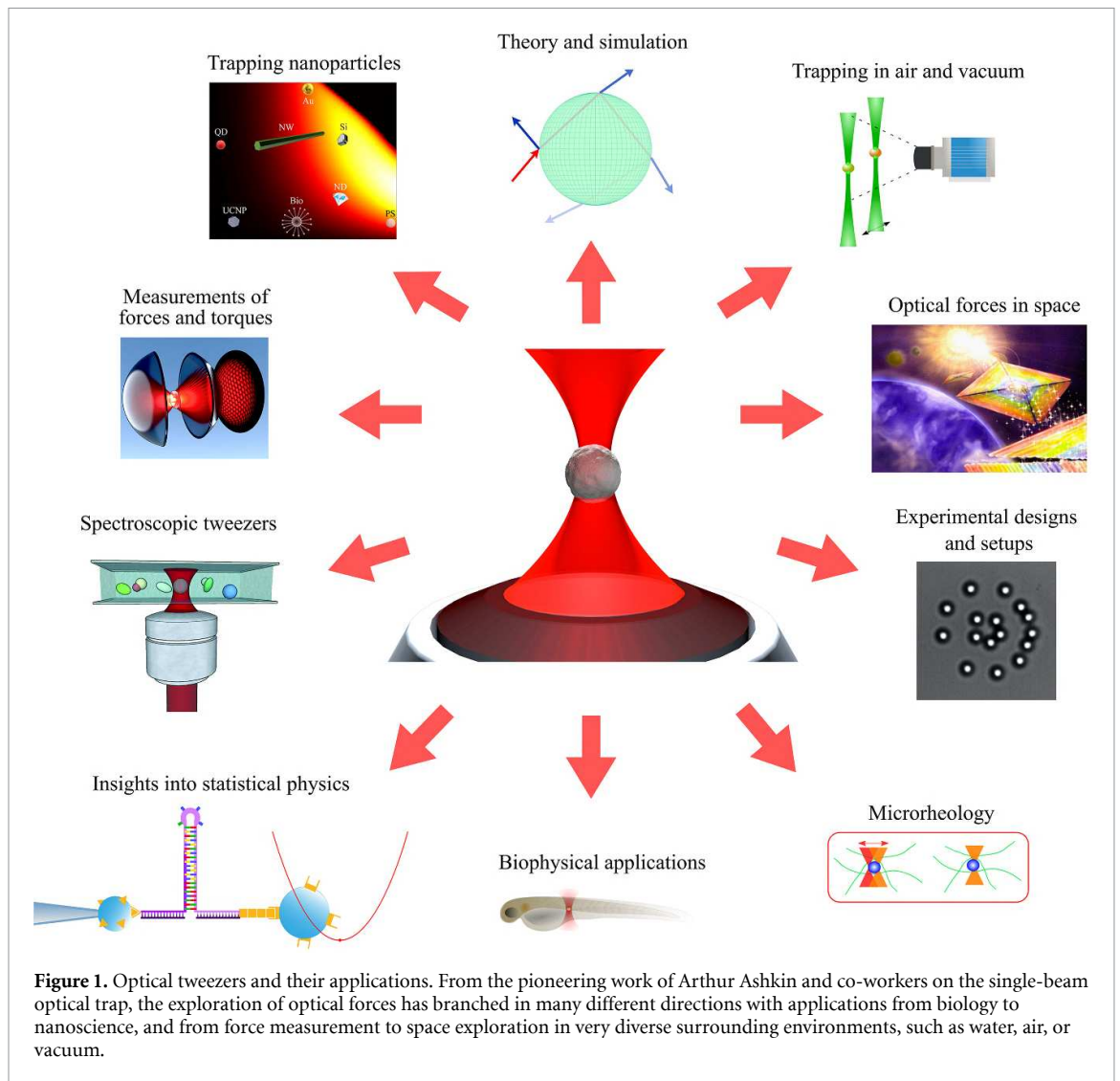
## Introduction

Optical forces emerge from momentum exchange between light and matter [1]. Despite their minuteness, they yield macroscopic consequences in extraterrestrial affairs. For example, in the 17th century, Kepler had already recognized that the tails of comets are a consequence of the light pressure produced by the Sun's light [2].<sup>56</sup> More recently, radiation pressure has been shown to be a key factor to ensure the stability of a star against gravitational collapse [3]. However, their role in laboratory experiments on Earth was elusive for many years [4, 5]. The turning point came with the advent of the laser age that offered intense and coherent light sources [6]. These were used by Arthur Ashkin [7] and co-workers in a series of pioneering experiments to trap and manipulate particles [8, 9], atoms [10–12], and biological matter [13, 14].

In their simplest configuration, optical tweezers are created by a single laser beam focused down to its diffraction limit, which creates the light intensity gradients needed to hold particles in three dimensions. Today, optical tweezers have become sophisticated and versatile instruments that can hold, guide, push, stretch, poke, probe, and sort particles, ranging from single atoms to microparticles, to cells and bacteria in a variety of environments, such as liquids, gases, or vacuum (figure 1).

In this Roadmap, we collected a series of perspectives that give an overview of the different research areas where optical tweezers have found application and have advanced the science of light–matter interactions further. We also look at current and future challenges in the field and provide insights into what are the possible future directions for the field. This Roadmap is organized as follows. We start by presenting information on experimental designs and setups, from the standard single-beam configuration to more complex designs, including recent developments employing intracavity feedback and metamaterials to generate optical forces. Then, we explore some fundamental aspects of theory and simulations that are crucial for a deeper understanding of experiments. Subsequently, we highlight some key applications for the accurate measurement of forces and torques. We show how the tweezers can be used for the characterization of the microrheological properties of fluids, the control and manipulation of nanoparticles, the trapping of particles in gas and vacuum, the exploration of statistical physics and nanothermodynamics, their combination with spectroscopy, their use for the study of biological matter from biomolecules to cells, and the use of optical forces in space applications. This Roadmap provides both an overview of the current state of the art in optical tweezers research and a guidance towards its future.

<sup>56</sup> The first mentioning of radiation pressure by Kepler was published in Kepler Johannes 1608 “Ausführlicher Bericht von dem 1607 erschienenen Haarstern” (Halle in Sachsen). The later publication of 1619, Ref. 2, contains a latin translation of this earlier publication.



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We wish to dedicate this Roadmap to the memory of Arthur Ashkin, Ferdinando Borghese, Michael Mishchenko, and Juan José Sáenz. These pages are part of their scientific legacy made of visionary and pioneering ideas that led to novel interdisciplinary research fields and applications.

## Experimental designs and setups

### 1. Optical tweezers setups

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#### Status

In 1986, Arthur Ashkin and colleagues successfully trapped, in 3D, micrometre- and nanometre-sized particles, dispersed in water, with a laser beam focused by a high-numerical-aperture objective lens [9] (figure 2). This is how the amazing and powerful world of optical manipulation began. Since then, optical manipulation has been used in a myriad of experiments across different fields: biology, statistical mechanics, rheology, opto- and bio-fluidics, and plasmonics are only a few examples of research fields where optical tweezers (OTs) played a key role. The ability to manipulate microscopic objects in a contactless manner was rapidly overcome by more quantitative experiments. OTs are not just simple ‘tweezers’: they are force transducers, as they can exert and measure forces, very tiny forces. The available range spans a very interesting scale: from few piconewtons (pN) down to few femtonewtons (fN). In fact, OTs expanded this range, until then dominated, but also limited, by atomic force microscopy. This force range is extremely interesting since it comprises many biological, chemical and, more in general, condensed matter interactions. The typical trapping stiffness for  $1\text{--}2\text{ }\mu\text{m}$  particles is of the order of  $1\text{ pN }\mu\text{m}^{-1}$  that corresponds to energies of few  $k_{\text{B}}T$ , i.e. energies comparable to those of thermal baths. Specifically, the dynamics of trapped particles can be used to understand the thermodynamics properties of the medium in which the particles are dispersed. Thus, OTs were immediately employed in statistical mechanics as well as in microrheology [1].

The need to unveil so many different phenomena stimulated researchers to develop new setup schemes and novel trapping techniques [15, 16]. The single-laser-beam OT immediately turned into OTs with two or more laser beams, first dividing the beam with beam splitters then using acousto-optical deflectors to obtain time-shared traps. Later, very versatile devices, like spatial light modulators, allowed researchers to explore other directions far away from simple trapping and manipulation. With these devices the light wavefront can be modified and engineered on demand: initially, multiple trapping, optical lattices, and sieves demonstrated the power of this new technique, but it did not take long to see experiments where the angular momentum of light played a key role.

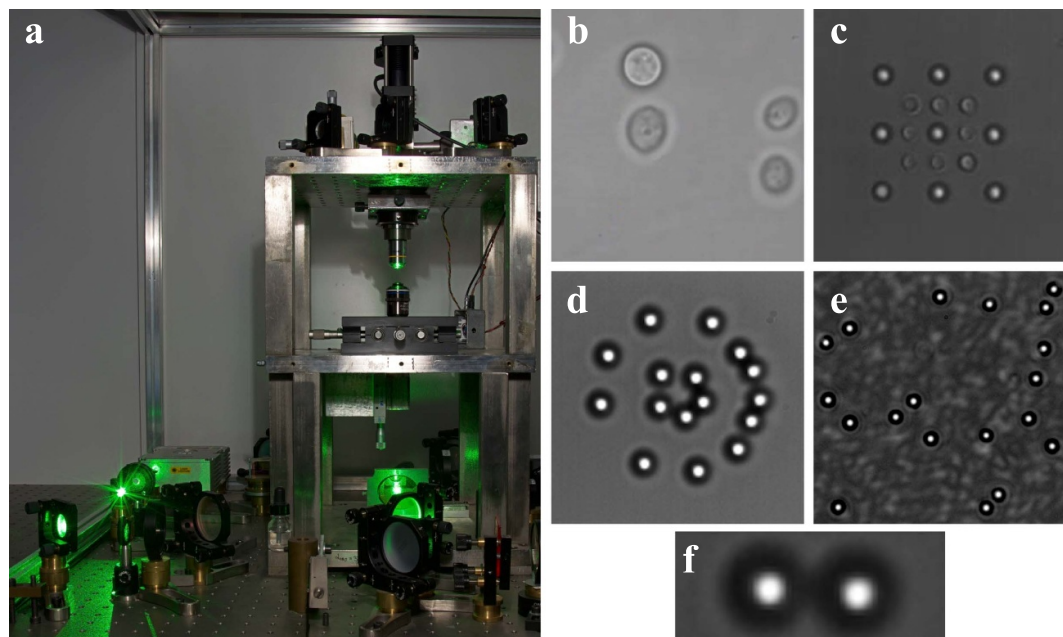
Despite its nearly 40 year history, optical trapping and manipulation is still an active research field. The recent advances in the trapping of nanoparticles in vacuum have opened up new challenges on testing fundamental physics, and quantum information science, many-body physics, metrology, quantum optics and ultracold chemistry.

#### Current and future challenges

In biological applications, OTs have contributed to the achievement of exceptional results. Nevertheless, one of their main limitations still needs to be resolved. To exert reasonable forces on biological samples, OTs use several milliwatts of light power that, even if at infrared wavelengths where the absorption is reduced, could damage the sample. Several attempts have been made to solve this issue, mainly using handles (beads or structures made with appropriate shapes) that once trapped can be used to manipulate cells and avoid heating due to incident light. Solving this issue is of fundamental importance to boost the usefulness of OTs in biomedical applications, especially for *in vivo* scenarios [17].

Another aspect that currently hampers OT applicability, limiting it prevalently to fundamental research only, is the size and cost of setups. Turnkey systems, provided by some companies, have quite high prices, because of the costs of optical components and those related to the development of stable systems. In fact, they are expected to provide easy and reliable operation.

OTs require microscope objectives to obtain gradient forces high enough to reach the trapping conditions, otherwise two counter-propagating beams can be used to cancel the scattering force; this represents a great limit in setup development. Home-made systems can be less expensive, but are often too sophisticated and very large in size to be handled by inexperienced personnel and in routine applications, even if built with commercial microscopes. Moreover, they comprise microscope objectives, whose price is in the order of thousands of euros. Alternative solutions to microscope objectives are based on the use of optics fibres, which can be arranged in counter-propagating beams or by creating a lens at their tip that is able to strongly focus the laser light and obtain trapping conditions. Microfluidics and fibre optics have greatly helped to move towards automatization and compactness, but a stand-alone trapping chip device is far from being realized.



**Figure 2.** A typical optical tweezers setup realized with a home-made microscope that allows great flexibility to adapt different techniques. The insets show some examples of various applications: (a) A yeast cell trapped by single-beam optical tweezers; (b) multiple trapping with a spatial light modulator; (c) wavefront engineering with a spatial light modulator; (d) speckle optical tweezers; and (e) time-sharing traps with an acousto-optic deflector (AOD).

Very recently, research in optical manipulation has shown a renewed interest in trapping in air and in vacuum. In vacuum the motion of an optically levitated dielectric nanosphere is well isolated from the environment and, with appropriate techniques, it is possible to cool down the motional energy of a trapped particle to demonstrate the quantum behaviour of a macroscopic object at room temperature. Consequently, setups are becoming increasingly sophisticated and new technical challenges must be faced [16].

#### Advances in science and technology to meet challenges

To overcome the issue of thermal damage to biological samples caused by laser power, several approaches can be pursued. A possibility is to develop new trapping schemes that use higher trapping efficiency. Very recently, a new idea based on intracavity trapping has been proposed and demonstrated [18]. Trapping occurs inside a laser cavity instead of the usual practice of using its output laser beam. The trapped object increases the power losses when it is at the beam waist centre so that the power is low: as it moves out, losses decrease and the power increases, pulling the object towards the centre and the power decreases again.

Other possibilities rely on developing special handles so that the parts in contact with the cells are not held directly by the laser beam. This is quite simple to do, and it is already widely used, but is limited to manipulation only. If quantitative measurements are required, it is necessary to explore new ideas. Other physical effects can also be used. Li and colleagues proposed an interesting solution, where the laser beam cools down a small volume of appropriate material and samples are trapped by thermophoresis [19].

However, the main issue, especially when looking at the establishment of OTs as a routine technique, remains the cost and the size of the setup. OTs are strictly bonded to microscope objectives. Efforts should be made to develop new technologies that are able to produce smaller and less expensive lenses with the same focusing properties. Metamaterials have been successfully used to create a very tiny meta-lens using nanopillars on a glass coverslip [20, 21]. This still has some limitations in terms of flexibility and applicability, since the lens is fabricated on the substrate, and its position and trapping depth are fixed or very limited; nevertheless, this may pave the way towards new and interesting directions.

#### Concluding remarks

The ability to manipulate small objects with focused laser beams opened up a broad spectrum of opportunities in fundamental and applied studies, such as biosciences, sorting, guiding, and analysis of materials. These experiments require precise control over mechanical paths and high stability. OT setups are cumbersome and are limited by a lack of flexibility and integrability. The cost of optical components is another key point that restricts the diffusion of trapping and manipulations setups. Since their beginning, about 40 years ago, OTs have shown a constant tendency to evolve by exploiting new research quests which are only limited by the advances in technology.

## 2. Structured light for the tuning of light–matter interactions

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### Status

The use of structured light permits one to alter on demand the properties of optical tweezers by altering the properties of the wavefront that generates it. Thus, optical tweezers that employ structured light can be used to more finely manipulate trapped objects, and they have been applied to gain a deep understanding of several complex biological and physical systems [22]. Light can be structured/sculpted by modifying its intensity distribution, phase, and polarization states using various spatial light modulator (SLM) technologies. Two common SLM technologies that are used to create structured light are derived from liquid crystals and digital micromirror devices. These devices enable manipulation of the intensity and phase of the light as well as polarization states. Structured light enables unprecedented control over light–matter interactions. The historical killer application of beam shaping using these devices has tended to be the multiple independent control of focused Gaussian spots or the introduction of angular momentum through azimuthal phase ramps in the Fourier plane [22, 23]. The operational effect is the transfer of momentum to particles with refractive index contrast to the surrounding medium through refraction and interference. More recently, the spatially varying phase, amplitude, and polarization have been developed to enhance control of light–matter interactions, such as the transfer of the exotic transverse angular momentum [24] (also figure 3), or the multiple independent control of radial, linear, or azimuthally polarized laser beam traps [25, 26]. An opportunity for the development of a powerful new technique based on the theory of the optimal control of light–matter interaction to precisely control not merely linear, but also angular transfers of momentum, exist. Demonstrations of exceptional change in linear momentum have been demonstrated using carefully structured light [27, 28], and the modification of particle properties [28, 29].

### Current and future challenges

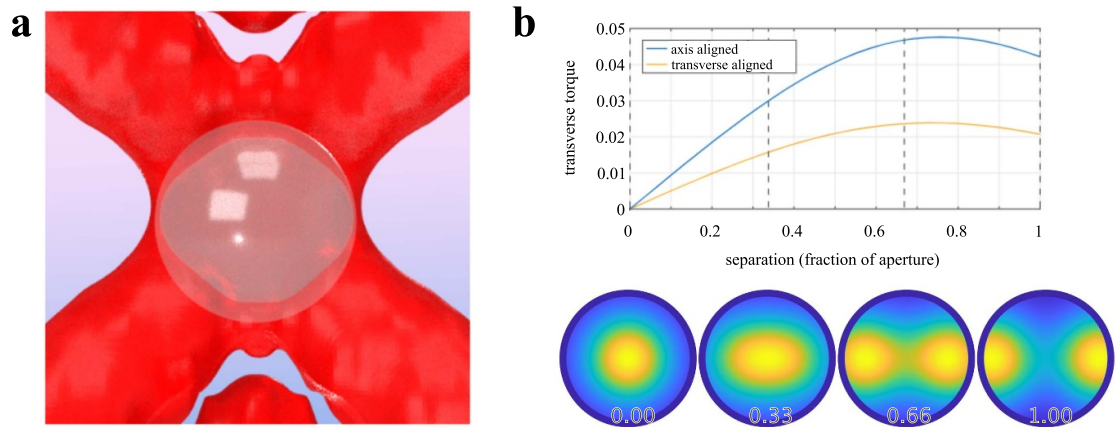
The idea of controlling the electromagnetic coupling between the incident and scattered components of light scattered by a particular particle is well established [27, 30] but it is limited by a set of challenges.

Ordinarily, optical tweezers act on spherical particles with simple structured laser beams. Simple and not necessarily complementary transfers of linear and angular momentum occur. For example, Laguerre–Gaussian type beam modes with a large azimuthal number are notoriously poor at confining small particles to the focus of a beam in 3D, but contain large quantities of orbital angular momentum. Simultaneous control of stable linear and angular momentum transfer to matter is elusive. Partly, this is due to the homogeneity of the plastic and glass particles commonly used in optical tweezers. Strongly anisotropic particles, such as those with shape and material birefringence, trirefringence, or exceptionally high-refractive-index objects [29], have much richer interactions with the electromagnetic field. Exotic particles can have capabilities beyond those of ordinary materials [28, 29], such as forces on the nano-newton scale and the transfer of spin or orbital angular momentum. To precisely control these exotic particles, we have to understand what the best arrangement of modes is to do so. Gaussian and higher-order Laguerre– or Hermite–Gaussian modes are not good candidates to control these particles as their optimal interactions are influenced by interference and emergent dielectric resonances [30].

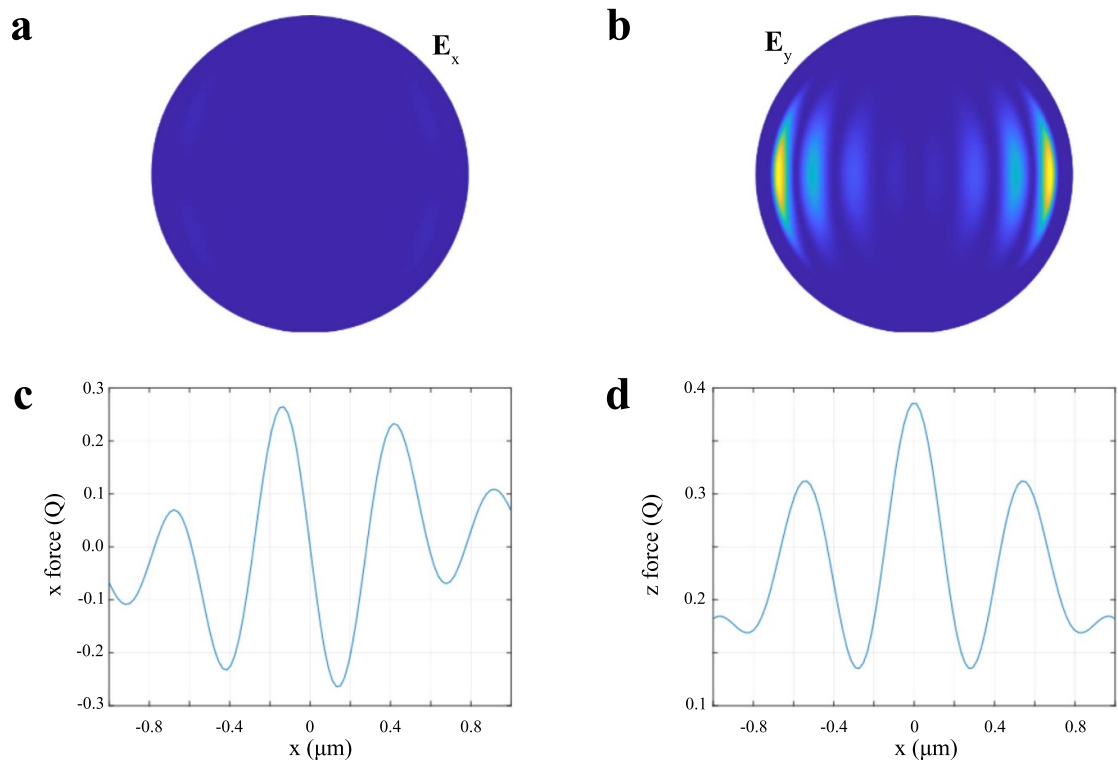
Optimized light fields have been experimentally realized for a range of different momentum operators in 2D [30]. The extension to 3D is possible. However, there are challenges with these approaches: namely, interactions are generally derived from the eigenspectrum of the effective measurement of momentum. Two problems arise that need to be addressed: (1) not all fields are realisable, particularly in optical tweezers where light moves through an aperture, and (2) optimization of one parameter, such as spin angular momentum transfer or stiffness in one dimension, will not necessarily yield a field in which a particle can be either levitated or three dimensionally trapped (figure 4). There are some strategies that can address this, ranging from modification of the theories to allow more stable configurations of less optimal transfers of momentum, to increasing the number of manipulated states, and to using a specially designed structure: for example, self-stabilizing levitation of a surface in low pressures [31].

The technical problems associated with producing a stable configuration and thus allowing for less optimal transfers of momentum run deep as there are a large number of ways that a momentum transfer may be made suboptimal but very few that will sufficiently improve stability. Subtle differences in the dimension and shape of particles are known to influence measurements in ordinary optical trapping experiments. In these circumstances, it will also prevent the achievement of both optimal interactions and the correction for trapping stability.





**Figure 3.** (left) A 3D model of a structured light field transferring transverse spin angular momentum to a spherical birefringent particle. (right) Transverse torque with birefringent axis light with and orthogonal to the direction of beam propagation as a function of the separation at the back aperture of a high-numerical-aperture lens between two orthogonally circular polarized Gaussian beams.



**Figure 4.** Far-field light distribution for two polarization channels and the forces generated when optimizing stiffness for a Titania particle. (a)  $E_x$  field component. (b)  $E_y$  field component. (c) Force for the stiffness optimized component. (d) Axial force. Titania particles are difficult to trap but interact strongly. High stiffness traps are generated but the particle must be levitated at this height for the optimization to succeed.

Vectorial beam shaping techniques can be used to increase the number of states in the light–particle interaction. The challenge with implementation will be ensuring good beam quality, stability (reliability), and alignment of the different polarization channels and will remain an ongoing battle [26].

Specially designed surfaces are an interesting approach. The challenge here is to design materials/structure that also allow for further enhancement of the light–matter interaction with the structured light that may be needed for a particular type of momentum transfer.

#### Advances in science and technology to meet challenges

Marrying exotic particles with beam shaping could prove to be a powerful technique that has applications not only in trapping in water, but the examination of macroscopic levitated quantum states. There have been

impressive and interesting developments in this area [32, 33] that have developed subtle control and sensitive detection of particles that may be more generally usable for fluid environments.

The power of optimized structured light and materials lies in the ability to precisely tune the light–matter interaction: for example, to enable new high-precision measurements of position and momentum, or extend trapping to low or negative refractive index contrasts, or to self-contained lab-on-a-chip devices. Recent developments in the consistent and rapid measurement of viscosity at ballistic timescales [34] would be enhanced through the inclusion of shaped particles and optimized/shaped trapping fields.

Addressing the stable configuration challenge may be the hardest of those listed here. The solution requires a clearly laid out problem, where an optimization can be performed that also preserves the desired properties of the optical trap, for example, a stable trapping position, or a consistent transverse of torque with rotation (see the left panel of figure 3, where two alignments of the optical axis have different levels of torque transfer). Perhaps moving away from the optimization using an effective momentum measurement operator is a good idea as it cannot, by its very construction, have a good solution with these constraints.

The preferred solution for vectorial beam shaping would be the production of Huygens' style sources of on-demand beams with spatially varying polarization. The use of polarized light shaping is growing and this may be a product that becomes available in the near future. Otherwise, better designs of the polarization shifting interferometers will be needed to increase stability and allow optimal light–matter interactions.

As fabrication technology continually advances, new and structured materials will become available over time. There are two levels of the complexity of the design of these materials. The first is where simple beams and plane waves supply the momentum to control them. The situation where structured illumination is used is much less certain. It provides an opportunity to investigate various forms of iterative design, where a light field and its target object can be subject to individual constraints, such as uniform polarization, pulse mode operation, and feature size. It provides one of the most flexible approaches to the problem of enhancing optical trapping in multiple translational and rotational degrees of freedom.

### Concluding remarks

Unprecedented versatility and superb control of light–matter interaction at the nano- and micro-scale has been enabled with optical beam shaping. The progress made to date is extremely encouraging. However, there are still outstanding challenges in applying these methods to a wide variety of systems. There are remaining questions on how to tune light–matter interactions for versatile uses in an arbitrary system. The availability of well-defined and dynamic structured light fields could enable novel studies in complex biological systems where there may be limitations in knowledge about the scattering properties in the surrounding environment. New shaped fields could open up investigations and further exciting studies in the interface of classical and quantum mechanics by allowing more precise tuning of the momentum transferred to and from a target system, allowing a better understanding of phenomena, such as the cooling to the ground state of systems over a large size range, studies of quantum behaviour at these scales, and out-of-equilibrium phenomena. The combination of optical tweezers using highly structured light fields with other imaging and spectroscopic techniques could enable insights into the burgeoning fields of quantum biotechnology and continue its contribution to the understanding of mechanobiology, physics, and chemistry on microscopic size scales.

### Acknowledgments

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### 3. Speckle optical tweezers

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#### Status

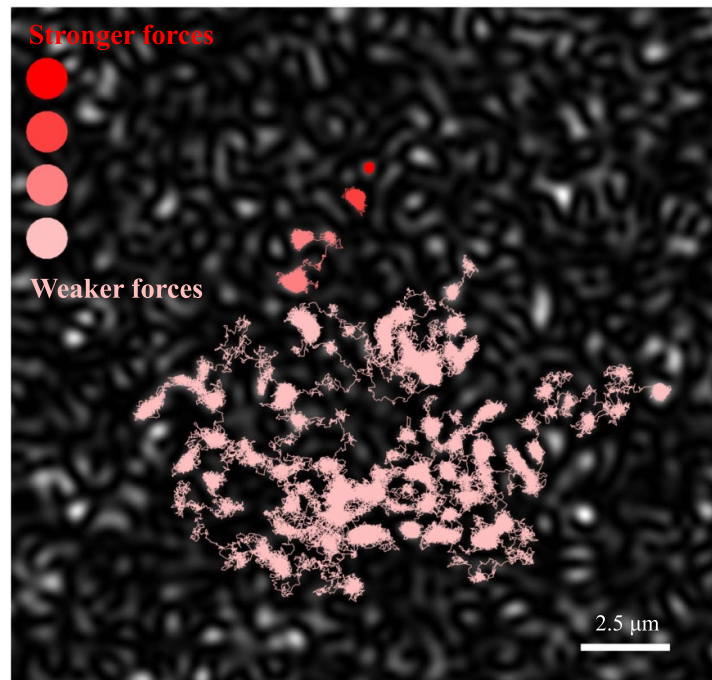
Speckle optical tweezers are an optical manipulation technique that relies on disordered light fields to exert optical forces on micro- and nano-particles [35] (figure 5). They are named after optical speckle patterns, which are light fields with a random appearance but with universal statistical properties [36]. These optical patterns result from the interference of several optical waves with random phases. For a long time, the field of optical trapping and manipulation has considered these light patterns as an undesirable consequence of the propagation of coherent light through optically complex media, such as diffusers, multimode optical fibres, colloidal dispersions, turbid liquids, and biological tissue. In contrast to most optical manipulation techniques, where disorder is an issue to be minimized, speckle optical tweezers take advantage of the random nature of these light fields to address fundamental physical questions and for applications in microfluidics [35–37]. Historically, the atom-cooling community was the first to adopt speckle light fields to trap small particles [38]. The last decade has experienced a revival of the technique to tackle questions in mesoscopic physics, where both static and time-varying speckle optical potentials have been used to study the emergence of anomalous diffusion (from subdiffusion to superdiffusion) in colloidal dispersions [36, 39–42], to tune effective dispersion forces between small colloidal particles [43], to perform standard microfluidic operations, such as particle guiding and sorting [35], to assemble 2D crystal-like and glassy colloidal materials [44], to control collective behaviour in active matter [45], and to reproduce first-passage statistics [46].

The future appeal of the technique (subject to further technical advances) is both fundamental and applied. On a more fundamental side, speckle optical tweezers can be further developed into a fully controllable proxy for many natural phenomena where particles move within potentials in the presence of disorder. Examples range from the emergence and propagation of defects in materials to the motility of molecules and organelles in cells, from the individual and collective motility of groups of animals to the diffusion of stars within a galaxy. The desirable feature in this model system would be that all variables and degrees of freedom of interest can, in principle, be controlled at the touch of a knob, i.e. light. On a more applied note, speckle optical tweezers can outperform standard optical manipulation techniques in instances (e.g. in microfluidic and biomedical applications), where simplicity of operation and robustness to environmental noise are key.

#### Current and future challenges

The main research challenge behind further advancements in speckle optical tweezers is intimately connected with the nature of optical disorder and its control. As the statistical properties of standard optical speckle patterns (i.e. their intensity distribution and correlation function) are universal [36], advancements in the field will go hand in hand with advancements in our capabilities to engineer disordered optical potentials in space and time:

- **Structured speckle tweezers.** Despite their random appearance, the universal properties of speckle fields have been harnessed to influence the translational diffusion of microscopic particles [36, 39–41]. Customizing speckle properties by modulating the amplitude, phase, and polarization of the light field can enable the implementation of more complex speckle patterns with, e.g. tailored intensity distributions and correlations. Speckle optical tweezers could therefore be applied to perform complex optical manipulation tasks based on controlling both the translational and rotational diffusion of microparticles, such as by introducing short-, mid-, and long-range correlations in the particles' motion or by generating torques with advanced disordered non-conservative force fields.
- **Three-dimensional speckle tweezers.** A key feature of many optical manipulation techniques is the ability to trap and guide particles in 3D space using single or multiple laser beams. A downside of most current speckle tweezers setups is that they can be operated primarily near a surface or at an interface. Indeed, the diffraction processes typically used to generate speckle patterns lead to out-of-plane divergence and longitudinal speckle grain elongation. Both aspects hamper non-trivial 3D manipulation tasks with speckle optical potentials. Controlling the statistics of optical disorder over a volume (i.e. along the direction of light propagation as well as along the transverse plane) could enable the systematic extension of the technique to the third dimension [37].



**Figure 5.** Speckle optical tweezers at work. The trajectories of a Brownian microsphere become increasingly confined the stronger the average force exerted by the bright spots of a speckle pattern (black and white background). The trajectories are colour-coded (legend) for the average force experienced by the particle.

- Near-field speckle tweezers. While trapping with random plasmonic islands has been demonstrated [47], using the localized fields generated by random metallic or dielectric nanostructures to manipulate small particles has an untapped potential for scaling speckle tweezers down towards the molecular level and for embedding them with molecular spectroscopy and sensing capabilities.
- *In vivo* speckle tweezers. Finally, particularly alluring is the possibility of using speckle optical tweezers to directly manipulate matter *in vivo*, where the exploitation of other non-invasive optical manipulation techniques is compromised by the natural optical turbidity of biological tissue. Nonetheless, for this to happen, optical methods need to be able to penetrate deeper into tissue and guarantee that adequate levels of power and imaging capabilities are met simultaneously.

#### Advances in science and technology to meet challenges

As speckle optical tweezers operate by exploiting complex optical potentials, developments in the field will benefit greatly from further scientific and technological advances in the fields of structured light and complex photonics. The possibility of structuring disordered optical potentials in three dimensions is intimately connected with our technical capabilities to control a large number of optical modes as well as all three components of the electric field simultaneously. Current wavefront shaping devices, such as spatial light modulators and digital micromirror devices, have driven significant scientific progress so far in these fields. Further development of these technologies (in terms of, e.g. efficiency, number of pixels, spatial homogeneity, pixel crosstalks, spectral bandwidth and speed) together with the advent of novel devices capable of independently controlling all classical degrees of freedom of light at once will also undoubtedly expand the range of applications for speckle optical tweezers. Similarly, the realization and adoption of turnkey laser systems, capable of supplying light beams with tailored structures, would enable the straightforward generation of a great variety of high-power complex optical potentials for optical manipulation purposes. Alternatively, the fabrication of disordered plasmonic and dielectric surfaces and metasurfaces for the generation of structured light within optofluidic chips or at the distal end of an optical fibre can help the miniaturization of speckle optical tweezers, their extension to trapping applications on the nanoscale, and their use for *in vivo* optical manipulation tasks. This possibility, while alluring, places high strains on current nanofabrication methods and modelling techniques. Moreover, non-invasive *in vivo* applications of speckle optical tweezers require light-shaping methods to guarantee higher efficiencies in terms of enhancing and stabilizing trapping potentials deep within tissue. Improvements in deep-tissue imaging techniques (e.g. based on acoustic guiding), fast data handling and machine learning methods will also be a welcome development for the *in vivo* implementation of speckle optical tweezers. Finally, from a

more pragmatic point of view, simplicity of operation, robustness to environmental noise, and low cost are major selling points for current speckle optical tweezer setups. Thus, any technical development that extends the range of operability of this technique will need to be affordable and easily available to the broader scientific and engineering community. To date, affordability remains a major practical challenge to the integration of novel technology in speckle optical tweezer setups.

### Concluding remarks

In conclusions, despite the random appearance of optical speckle fields, their statistical properties have been exploited to control and manipulate the diffusion properties of small particles. Although carefully engineered periodic potentials can perform better in specific optical manipulation applications, speckle optical tweezers offer additional advantages as they are intrinsically simple to operate, low cost, widefield, and robust to aberrations from the optics and the surrounding environment. Beyond their applied interest for microfluidic, biomedical, and *in vivo* applications, speckle optical tweezers are an ideal tool in the hands of researchers to tackle fundamental scientific questions in both equilibrium and nonequilibrium statistical physics and materials science. To expand the applicability of this tool further, the possibility of structuring optical disorder in two and three dimensions in space and over time is an attractive avenue to directly engineer new light–matter interactions in random optical potentials. Nonetheless, to maintain the broad appeal of speckle optical tweezers, it is key that the integration of novel technologies does not alter the fundamental character of the method, i.e. its accessibility to an extended scientific and technical audience.

### Acknowledgments

I would like to acknowledge Sylvain Gigan and Giovanni Volpe for critical reading and fruitful discussions on the future of the technique.

## 4. Optical trapping and manipulation mediated by optical nanofibres

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### Status

Optical nanofibres (ONFs) are waveguides produced by controlled drawing of a transparent material (most commonly glass softened by local heating), a technology largely developed over the last two decades [48]. The thinnest region or ‘waist’ of an ONF has a diameter comparable to the working wavelength. Strong transverse confinement of the guided light at the waist leads to a significant evanescent field near the fibre surface and to radical restrictions of the allowed guided modes. In particular, if an ONF is sufficiently thin, it operates in the single-mode regime, where the internal and external field profiles are the most predictable.

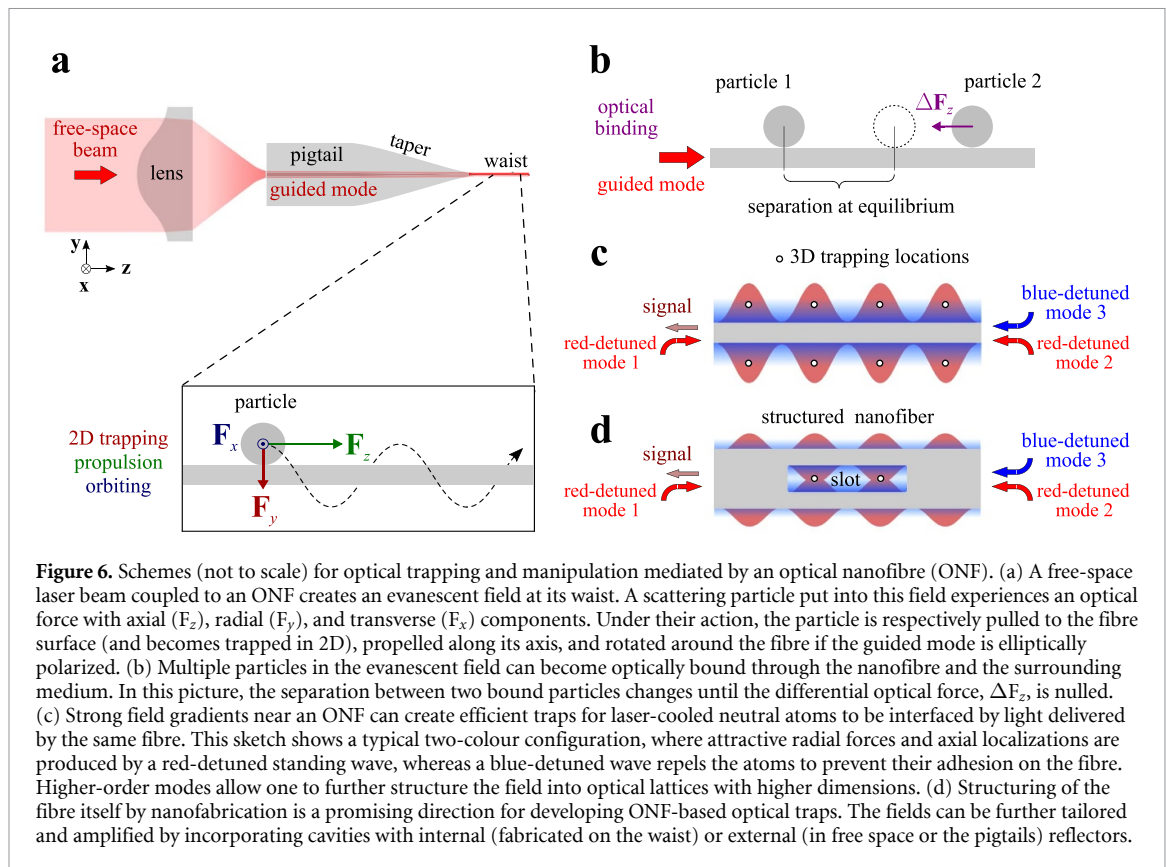
ONFs have many attractive features, which explain their broad range of applications. Here, we focus on optomechanical ones, where material objects can be trapped or acquire forces and torques by interactions with ONF evanescent fields (see the overview in figure 6). The large gradients and intensities of these fields are comparable to those of standard optical tweezers. Therefore, much like a tightly focussed laser beam, an ONF can stably trap dielectric particles in 2D by gradient optical forces. However, unlike a free-space beam, a single guided mode of an ONF has no restrictions in the axial direction, and the captured particle is optically propelled along the fibre [49]. When an ONF simultaneously captures multiple particles, they become optically bound to each other through the waveguide and the surrounding medium [50]. A recent study has demonstrated that ONFs show great potential for optical manipulation of composite metallo-dielectric particles [51], which are notoriously difficult to handle with free-space optical fields. Besides linear manipulation (trapping, propulsion, binding), ONFs can mediate light-induced rotation of material objects [52]. Free-space fields are often structured for spatial filtering and advanced optical manipulation and, similarly, the ONF-guided light can be made highly inhomogeneous in intensity or polarization by using interfering fundamental modes or higher-order modes [53]. One of the unique features of ONF technology is the possibility to structure the fibre itself by nanomachining [54] to incorporate cavities or metastructures, an option largely unexplored within the context of optical trapping and manipulation. A major and arguably the most promising area of research involving ONFs concerns optical trapping and interfacing of laser-cooled atoms and other quantum emitters [55]. Note that such a radical downsizing of the manipulated object brings extra complexity to the ONF-based trapping; for instance, the scheme with two-coloured (attractive and repulsive) near-resonant modes is the standard approach for neutral atoms [56].

### Current and future challenges

Overall, ONF-based photonics and optomechanics are in their early development stages, with many challenges remaining on the route to realization of the full application potential of this technology. By the nature of their applications, ONFs must have low losses and highly predictable geometrical parameters of the waist region. Losses are especially important in experiments with quantum emitters, where the signal-to-noise ratio is critical and ONFs are held in ultrahigh vacuum making heat dissipation very difficult. Obviously, heating increases the noise and severely lowers the optical damage threshold for the fibre. The existing fabrication techniques allow one to produce low-loss ONFs with the needed parameters, but currently there are no industry-standard implementations of an ONF-drawing rig. As a result, the fabrication quality varies greatly between custom-built systems, strongly depending on the operator’s ability to calibrate and maintain the equipment, and even to handle the fibres. Moreover, the existing methods for precise characterization require near-field scanning, which renders the probed nanofibre unusable for most applications. Therefore, improvement of the fabrication repeatability remains one of the major challenges for ONF technology.

In theory, unstructured ONFs are cylindrically symmetric and therefore do not alter the guided mode during propagation. However, experiments show that the symmetry is broken even in single-mode ONFs, where uncontrolled stress birefringence transforms the polarization of guided light. While for an adiabatic single-mode ONF, these transformations can be undone using the Poincaré-sphere representation of the polarization states at the waist [52], reliable control of higher-order modes in ONFs still evades experimentalists. This practical issue limits the use of ONFs to the single-mode regime and theoretical predictions involving vectorial evanescent fields [53] remain unrealized.

Another big challenge with ONF-based systems is scalability. To date, they are built around a single ONF waist, which is used for optical manipulation or interfacing of colloidal particles or quantum emitters. While high-throughput lab-on-a-chip devices for handling colloidal particles with multiple ONFs are relatively easy to imagine, multiplexing for quantum ONF-based applications is much more challenging. One very promising solution involves Rydberg atoms coupled to an ONF; however, it is not clear whether such atoms



can be arranged in a chain and addressed independently to work as a quantum simulator [57]. It is feasible that multiple ONFs coupled to quantum emitters and linked to each other could form a functional quantum network, or the system could gain a higher dimensionality by the use of structured ONFs with a series of nanoscale cavities each representing a node in the network. These and similar ideas still lack proof-of-concept experimental demonstrations, not to mention implementations in actual photonic devices.

### Advances in science and technology to meet challenges

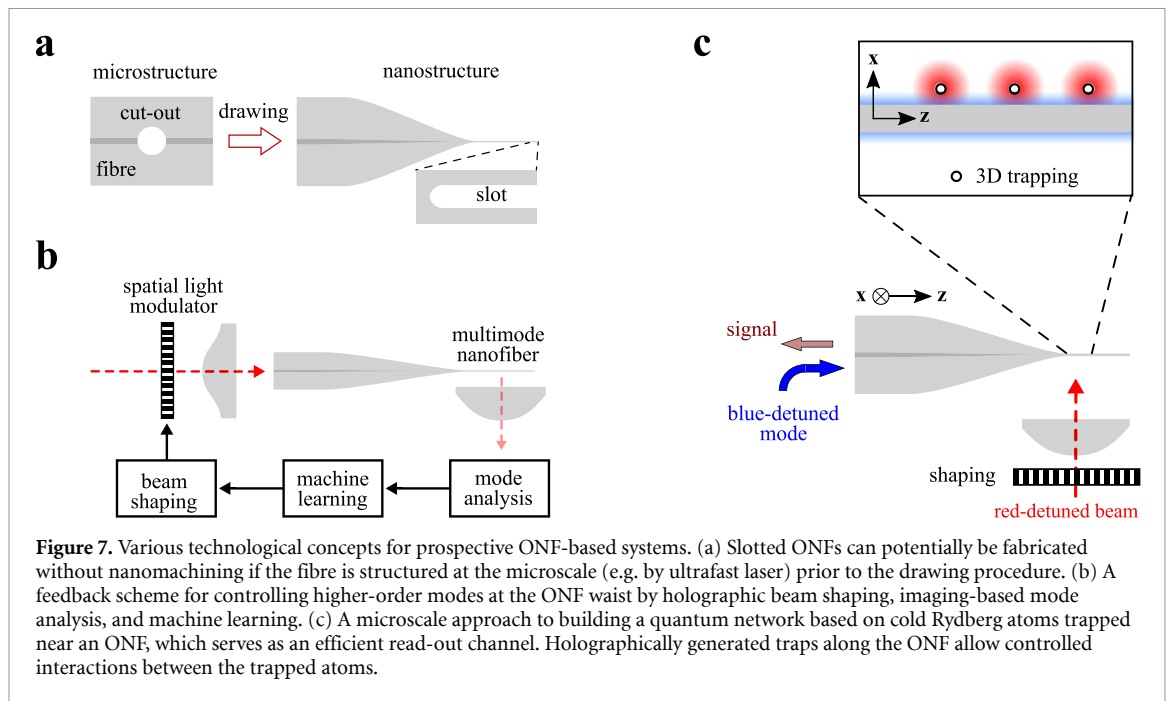
Repeatability of ONF fabrication should be improved by standardization and automation of the drawing process. Commercial fusion splicers solve the analogous problem related to joining telecom optical fibres; similarly, one could imagine an automated machine that allows the operator to reliably produce ONFs with desired parameters that are verifiable by *in situ* probing. On a larger scale, major engineering advances are needed for consolidation of the ONF-drawing technology with integrated photonics based on lithographic printing. Perhaps nanowaveguides similar in quality to ONFs could be produced by reflowing of printed structures, as is often done with on-chip whispering-gallery microcavities. Thus, the need for precise mechanical manipulation associated with drawing could be eliminated.

State-of-the-art methods for structuring ONFs are based on nanomachining the fibre with a focussed beam of ions (gallium is more common, while helium offers contamination-free milling and a 10-fold higher resolution reaching 1 nm). These methods are expensive, low-throughput, and time-consuming, especially with the high chances of damage to the nanofibres during the process. A promising alternative could be to use micromachining (such as femtosecond laser writing, which has a wavelength-scale resolution) of the fibre and then to downsize the structured region in the radial direction by drawing (figure 7(a)), as is common for fabrication of photonic crystal fibres.

To improve heat dissipation of vacuum-clad ONFs, it is worth researching atomic-scale coatings. Carbon, with 1000-fold higher thermal conductivity compared to silica, is one excellent candidate. ONFs wrapped in graphene (e.g. via the Langmuir–Blodgett technique) would be a powerful tool for photonic and optoelectronic applications.

To control the guided modes in ONFs, one can structure the input beam, for which purpose the mode content at the waist region must be analyzed. This task is very challenging but feasible, for instance by spatial spectroscopy of beating modes [58]. We expect reliable mode control for ONFs to be achieved by merging this ‘reading’ capability with free-space holographic ‘writing’ (spatial modulation) and a machine-learning





algorithm to link the two, see figure 7(b). An alternative strategy would be to structure the fibre itself and filter the modes by dichroism or resonant excitation.

Besides the obvious approach of linking multiple ONFs, scalability of quantum systems based on trapped atoms can be pursued at the microscale, e.g. by combining an optical lattice (for localization and selective interfacing of qubits) with an ONF (for efficient channelling of the information-carrying photons), see figure 7(c).

### Concluding remarks

ONFs offer a seamless connection between free-space beams and tightly confined evanescent fields, which brings optical trapping, manipulation, and probing of material objects to a new level of performance. After nearly two decades of research, nanofibres and their application potential are well understood and have been clearly demonstrated in numerous experimental studies, the foremost being optical trapping and probing of cold atoms in the pursuit of a nanofibre-based quantum network. Despite its advantages, ONF technology is still at the research-laboratory level, a long way from being implemented in commercial photonic instruments. In our opinion, the technology will only mature when the fabrication process and mode control become sufficiently accurate. Towards this goal, fabrication should incorporate *in situ* probing, whereas the issue with the modes could be overcome by combining holographic beam shaping in free space, mode analysis at the nanofibre waist, and machine learning to complete the feedback loop. We also envisage advances in chemically applied coatings to tackle the heat dissipation problem with vacuum-clad nanofibres, and more active implementation of micro- and nano-machining for precise structuring of the nanofibre and the guided fields. Advances in the next decade should showcase the true potential of these miniature devices.

### Acknowledgments

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## 5. Intracavity optical trapping

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### Status

Optical trapping based on feedback has attracted considerable attention because of its unique and precise control on the position of the trapped particle, laser intensity, and the exerted force or torque. There have been various approaches used to take advantage of the feedback control. Feedback can be used to control enhancement: for example re-positioning of the trap by monitoring the particle's position and sending a fast electronic signal in force clamping [59]; stabilizing the sample stage and achieving power stability by monitoring the trap laser intensity with a photodetector and adjusting the laser power [60]. In addition, feedback can be exploited in a deliberate arrangement, where it is used as a mechanism for single-molecule trapping, anti-Brownian electrokinetics [61] and, recently, in near-field trapping in liquid medium, self-induced-back-action (SIBA) [62].

All the feedback mechanisms mentioned above are extrinsic: they all require dedicated electronics and imaging as a part of the feedback loop. In 2019, Kalantarifard *et al* [18] presented a novel technique of intracavity optical trapping (ICOT) and introduced an intrinsic nonlinear feedback force, i.e. a force that arises only because the optically trapped particle is placed inside a laser cavity (figure 8). The main novelty of ICOT lies in the identification of a new mechanism for trapping microparticles using intracavity optical feedback, which is fundamentally different from the standard techniques already demonstrated in the past. This technique is based on intracavity optical forces that emerge from the influence of the optically trapped particle on the laser cavity.

According to the working principle shown in figure 8, there is an optomechanical coupling between the laser cavity and the trapped particle such that the particle's positions,  $r$  and  $z$ , and laser signal power,  $P$ , are correlated. When the particle moves to the right, left, and down, the power increases while, by lifting the particle up, the power drops.

The ICOT scheme works using an aspheric lens with a low numerical aperture (NA about 0.12 or less) compared to the standard optical tweezers that employ an objective with typically  $NA > 1$  (in a liquid medium). Therefore, as the most important benefit, this new kind of optical tweezers permits trapping at lower average laser intensity than alternative techniques. In general, any feedback modulation of the laser beam intensity can reduce the intensity on average. However, the internal feedback due to the laser cavity dynamics occurs within the timescale of nanoseconds, making it several orders of magnitude faster than any external feedback.

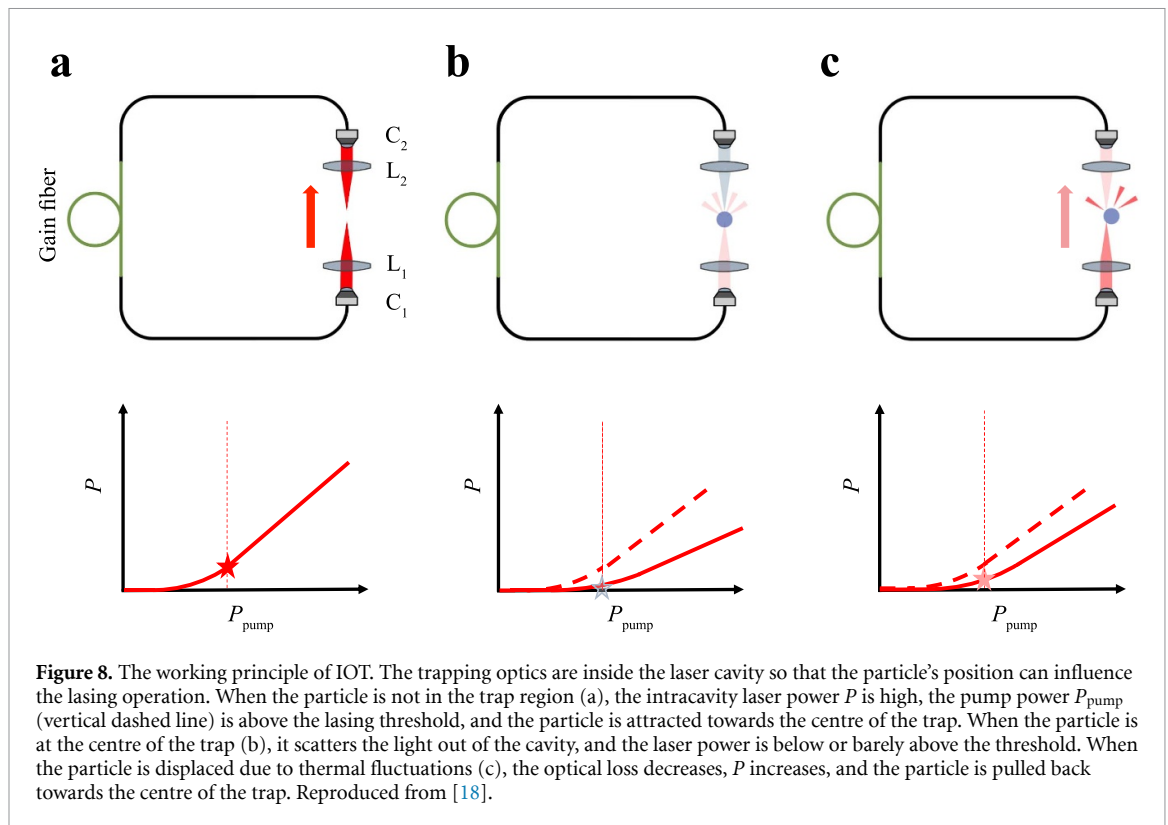
### Current and future challenges

Employing a low-NA lens instead of a high-NA objective lens in an ICOT system is one of the main advantages. Although the low-NA lens brings many advantages compared to the more costly high-NA objective, the weaker gradient force requires excellent adjustment and is accompanied by some challenges. Scattering loss of the trapped particle plays a significant role in ICOT systems. To take advantage of the feedback in the ICOT, the insertion loss of the laser cavity must be low, and the particle loss due to scattering should be significant. For small dielectric non-absorbing particles, where the particle size is much smaller than the wavelength ( $a \ll \lambda$ ) and the dipole approximation is valid, the power scattered by the particle in the trap rapidly decreases and the scattering loss in terms of the particle's displacement is much smaller than that of microparticles. Therefore, the nonlinear feedback that regulates intracavity trapping is negligible, and ICOT behaves as standard single-beam optical tweezers and cannot efficiently trap small particles at low intensity. This clearly shows that, while the intracavity feedback trapping is efficient at the microscale, it reduces to standard single-beam optical trapping at the nanoscale.

Due to the use of a low-NA lens in ICOT, the particle weight plays an important role in the stability of the trap in the axial direction for trapping of the objects with a high refractive index. As a result, the setup design is limited to inverted microscopes for particles with very low density and a high refractive index, such as polystyrene. Depending on the particle's refractive index and density, the intracavity trapping needs to be designed accordingly. Therefore, trapping microscopic beads in a vacuum or in a horizontal configuration could be challenging.

Position detection, especially in the axial direction, can also become challenging to some extent. As a standard tool for position detection, a quadrant photodetector requires a stable and low fluctuation in laser





power. However, because in ICOT, the intracavity laser power, and hence the output power, varies according to the particle's position, the high-resolution measurement of the position requires an understanding of the effect of power variation due to the position. Due to this complication, so far, the 3D tracking of the particle is mainly limited to 3D digital video microscopy, which is relatively slow as it is limited by the camera frame rate.

### Advances in science and technology to meet challenges

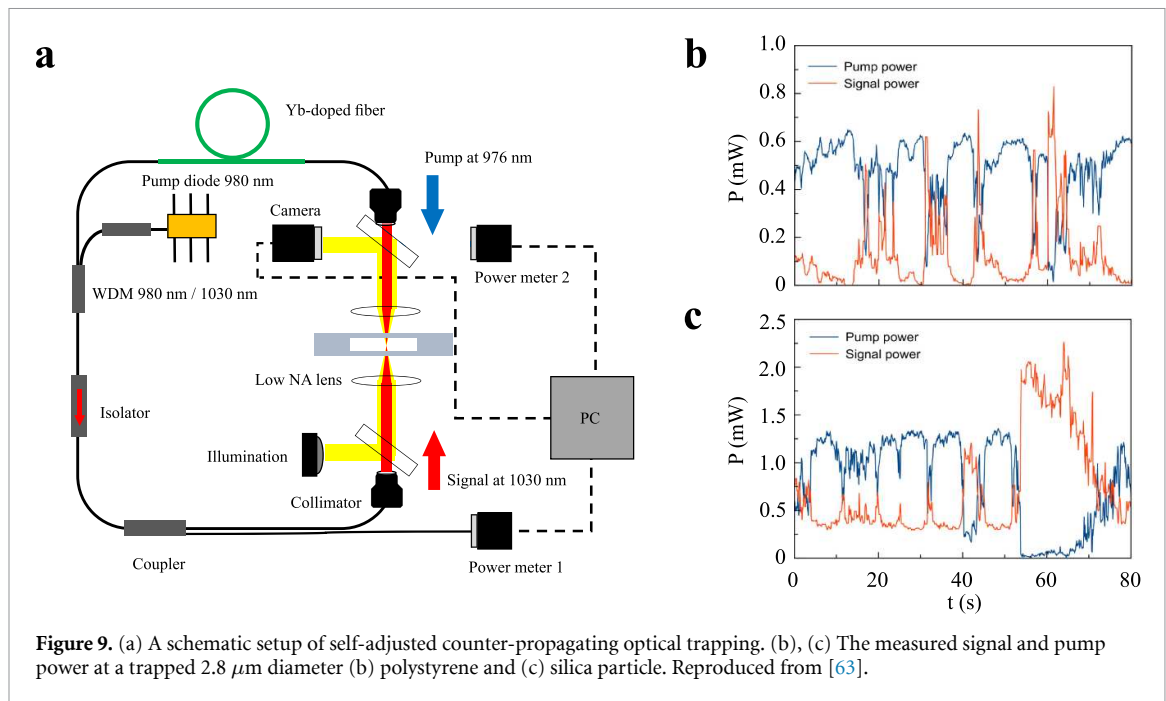
The advantage of optical feedback compared to electronic feedback is its uniquely high bandwidth ( $\approx 10$  MHz). The novelty of this approach opens many new possibilities to be explored in future works.

One of these possibilities is to study systems where the characteristic timescales associated with the laser and the motion of the optically trapped particle become comparable. In particular, one can expect its uniquely high bandwidth to be crucial when dealing with particles trapped in the air or a vacuum.

However, the ICOT in liquid can also, in principle, be scaled down to particles significantly smaller than the wavelength by changing the experimental parameters. A small innovative change in a fibre laser cavity [63] led to a new configuration called self-adjusted counter-propagating optical trapping with a single Gaussian beam and using an even smaller actual NA (0.087) that is capable of trapping smaller polystyrene particles compared to ICOT. In this scheme, the power at the sample switches between the signal and pump (which is now propagating in the opposite direction of the signal) such that, when the particle is in the centre of the trap, the laser signal power drops and the pump power rises, and this occurs automatically due to the displacement of the particle itself (figure 9). Having two self-adjusted counter-propagating beams improves the axial direction trap for smaller particles and brings another advantage to the trapping system in the horizontal design.

Another change, such as increasing the NA of the lens, would allow one to increase the losses due to the particle and therefore make ICOT more efficient. In another reconfiguration of the setup, the authors showed that by removing the isolator in the ring cavity, to make the light travel bidirectionally and then sending the light from both directions to the silica microparticle, the optical confinement per unit intensity is improved [64].

In terms of data acquisition and particle tracing, due to the advances in machine learning, particularly in image processing and deep learning, position detection and particle tracking in ICOT are no longer cumbersome, especially in the axial direction.



**Figure 9.** (a) A schematic setup of self-adjusted counter-propagating optical trapping. (b), (c) The measured signal and pump power at a trapped  $2.8 \mu\text{m}$  diameter (b) polystyrene and (c) silica particle. Reproduced from [63].

### Concluding remarks

ICOT is fundamentally different from other techniques as it is based on nonlinear feedback forces arising because the particle is inside the laser cavity. Position clamping, for instance, works based on (external) feedback on the trap power depending on the explicit measurement of the particle position. However, in the ICOT scheme, the feedback is intrinsic to the laser cavity, passive, and extremely fast. In addition, due to the existence of an optomechanical coupling between the particle position and the laser cavity, the power is self-regulating, and it does not require recalibration each time that the experimental details are modified.

The ability of trapping to employ ultralow light intensity at the sample (enabled by the use of a very low-NA lens) in ICOT can yield advantages when dealing with biological samples that are sensitive to light intensity. In comparison with alternative trapping techniques, where a low-NA objective lens is employed [65, 66], the ICOT achieves excellent results capturing and trapping particles and yeast cells [18] by achieving a major reduction in optical intensity exposure at the sample.

As the working principle of the ICOT, being the trap inside a laser cavity has attracted attention [67] to a new research field that is curious to find out how a trapped object can influence the lasing operation and to discover what further exciting science discoveries and applications will be obtained.

### Acknowledgments

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## 6. Metasurfaces for optical manipulation

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### Status

An optical metasurface is a dense 2D layer of scatterers with subwavelength dimensions and separations such that the layer appears locally homogeneous to an impinging electromagnetic field. The scatterers (or metaatoms) are typically designed to induce a specific phase and/or polarization state of the scattered field by utilizing optical resonances, such as localized surface plasmons in metallic metasurfaces (primarily Au) or geometrical resonances (Mie or waveguide modes) in metasurfaces composed of high-index dielectric materials. By systematically varying the scatterer dimensions, shape, orientation and/or separation across the metasurface, it is then possible to shape the light that is transmitted through or reflected from the surface. This makes it possible to construct compact counterparts to a wide variety of classical refractive or reflective optical components [68], the prototypical example being a phase-gradient metasurface operating as a ‘flat’ lens [69], but also multifunctional devices and miniature structures with tailored optical responses.

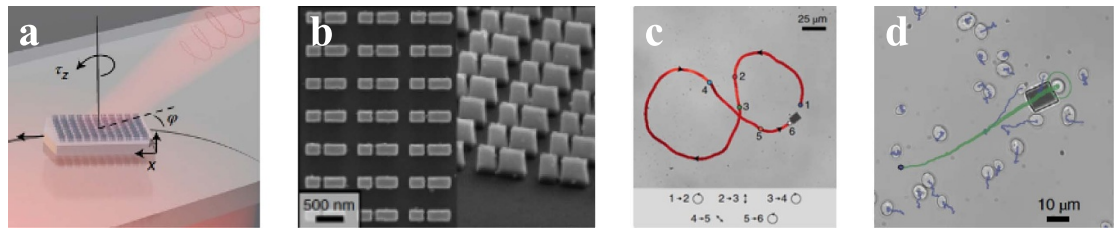
There are so far only a few experimental studies of metasurfaces within the context of optical manipulation, most of them very recent. Polystyrene beads have been trapped using a reflective Si metasurface operating as a parabolic mirror [70] as well as by Si metalenses [71], where multifunctionality obtained by overlapping the phase gradients corresponding to a lens and a q-plate to transfer orbital angular momentum was also demonstrated. Si metalenses with  $\text{NA} \approx 0.9$  have recently been used to optically levitate  $\text{SiO}_2$  particles in vacuum, with trapping efficiency that is comparable with conventional microscope objectives [21]. These results demonstrate that lithographically produced metastructures can exert optical forces without the use of traditional optical elements. Microscopic  $\text{SiO}_2$  particles with embedded anisotropic Si metasurfaces that are able to deflect light at high angles to provide optical propulsion and torque were recently demonstrated [72]. These ‘metavehicles’ are steered by altering the polarization of a single incident plane wave and were able to transport microscopic cargo across a surface in water, see figure 10.

### Current and future challenges

Several challenges need to be tackled to make metaoptics a competitive alternative to traditional optical components used for optical manipulation. These include, but are not limited to:

- Poor efficiency and polychromaticity: most current metasurfaces have comparatively low transmission or reflection efficiency compared to ordinary focusing optics, in particular outside the design wavelength.
- Poor focusing ability: optical tweezing typically requires high NA optics, meaning that the corresponding metalens phase gradient needs to be very steep at the periphery of a lens.
- Costly and advanced manufacturing processes: metasurfaces are typically fabricated using expensive electron beam lithography and advanced layer deposition and etching protocols, which hampers their widespread application.
- Computational complexity: current electromagnetic solvers cannot simulate an entire phase-gradient metasurface, which typically contains  $>10^4$  optically interacting metaatoms, in a self-consistent manner. This limits the possibility to optimize devices.
- Tunability: metaoptics devices are typically static in nature, which is a clear disadvantage compared to, for example, spatial light modulators.

The challenges listed above are general to the metaoptics field. All are active areas of research, though each one may be more-or-less critical to the field of optical manipulation. For example, efficient high-NA metalenses are needed for laser-tweezing in 3D, but they do not necessarily need to be polychromatic. Apart from the important but obvious advantage of shrinking the size and cost of components used for optical manipulation, the most impactful challenge in the long term will be to realize applications that are useful but practically unachievable using conventional optics and photonics devices. For example, ultracompact systems for optical trapping in lab-on-a-chip applications would probably need to incorporate light source(s), metaoptics, and detectors to bring real advantages; metaparticles could be made responsive to environmental cues to act as mobile sensors driven by light; and metasurfaces with simultaneously optimized phase, amplitude and polarization responses could be used to create entirely novel optical force fields for diverse applications.



**Figure 10.** Microscopic metavehicles powered and steered by embedded optical metasurfaces. (a) Radiative reaction forces and torques from an incident polarized plane wave transmitted through the metasurface provide propulsion and steering capabilities in 2D. (b) The metasurface is constructed from directional anisotropic Si nanoantennas and optimized for a wavelength of 1064 nm. (c) A metavehicle is driven in a ‘8’ pattern by manually varying the incident polarization. (d) A metavehicle is used to transport microscopic cargo: here, a baker’s yeast cell. Reproduced with permission from [72].

### Advances in science and technology to meet challenges

Several technological advances, many already under development, can be expected to impact optical manipulation research and applications based on metasurfaces in the short to medium time frame, some of the most important being:

- More precise and/or more cost-effective fabrication methods, such as extreme ultraviolet lithography and nanoimprint lithography.
- More powerful optimization methods, including techniques based on artificial intelligence (e.g. deep learning) and, perhaps, even quantum computation.
- New materials with lower loss, a higher refractive index, and/or with externally controllable optical properties (e.g. phase change materials).

Advancements based on combining metasurface concepts and technology with those developed in neighbouring areas, such as diffractive optics (see, e.g. [73]), nanolasers, optical sensors and actuators, and nanoantennas are also very likely.

### Concluding remarks

The field of optical metasurfaces has developed into one of the most active research areas in fundamental and applied photonics. Building on foundations in plasmonics, metamaterials, and nanooptics, optical metasurfaces offer the prospect of extremely thin, compact, and multifunctional optical components and devices. These could be integrated into optical manipulation systems to drastically cut size, complexity, and cost, thereby accelerating their widespread use, and enabling new applications of such systems. Moreover, because of their potentially very small size and mass, metasurfaces could themselves be designed as targets for optical manipulation, thus realizing a new class of microscopic structures driven by optical forces. Due to the rapid advances of the field and the enormous flexibility in terms of possible metasurface designs, there is certainly room for both novel creative applications and further refinement of concepts and devices for optical manipulation.

### Acknowledgments

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## Theory and simulation of optical forces

### 7. Geometrical optics

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#### Status

Geometrical optics was already known to the ancient Greeks. The most ancient surviving treaty on optics is Euclid's *Catoptrics*, written around 280 BC. Euclid writes that light travels in straight lines (rays) in homogeneous media. The law of reflection and the phenomenon of refraction were also known, and Hero of Alexandria demonstrated that, if we assume that the light always travels along the shortest path, we can derive the law of reflection using the laws of geometry. The modern formulation of geometrical optics stems from the works of Snell, Descartes, and Fermat. Later, geometrical optics was rederived within the framework of the general electromagnetic theory from Maxwell's equation [1].

Geometrical optics' fundamental concept is the ray, which has a power  $P$ , a propagation direction  $\hat{r}$ , and a polarization  $\hat{p}$ . The ray describes the light and its propagation through media. A homogeneous medium is characterized by its refractive index  $\tilde{n}$ , which is related to the medium dielectric constant  $\varepsilon$  through the relation  $\varepsilon = \tilde{n}^2$ . The refractive index is, in general, a complex quantity:  $\tilde{n} = n + ik$ , where the real part defines the light speed in the medium  $v = c/n$ , and the imaginary part  $k$  is non-zero for absorbing materials only and dictates how fast the optical power of the ray exponentially decays in its spatial propagation through the medium. The three fundamental laws of geometrical optics consist of (i) rectilinear propagation of a light ray in homogeneous media, (ii) the law of reflection, and (iii) Snell's refraction law occurring at the interface of two homogeneous media:  $\theta_r = \theta_i$  and  $n_t \cdot \sin \theta_t = n_i \cdot \sin \theta_i$ . The intensity of the reflected and transmitted rays following a ray impinging on the surface between two media in Snell's law is based on Fresnel's coefficients, which are defined for each component ( $p$  parallel,  $s$  perpendicular) of the ray polarization with respect to the plane of incidence. The Fresnel coefficients are derived from the electromagnetic theory by imposing the continuity conditions of the electric and magnetic fields (ruled by Maxwell's equations) at the interface between the two media [1]. Snell's law and the electromagnetic stress-energy tensor, which defines the energy and momentum carried by the light, are fundamental to explain the experimental evidence that light can apply forces to particles, which is the basis of optical tweezers [9, 74, 75].

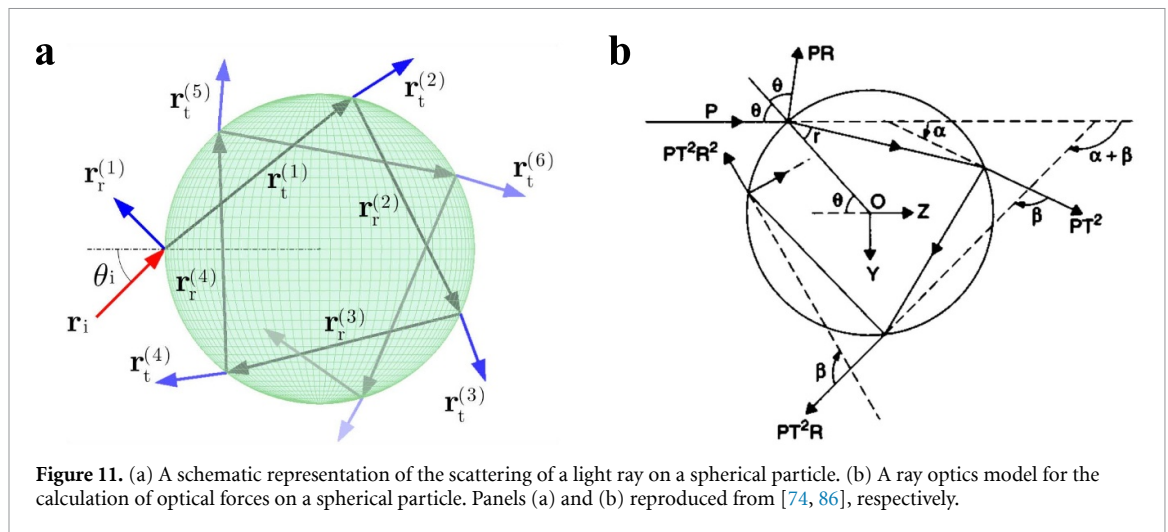
Geometrical optics has been successfully applied to model optical tweezers [9] and predicts the optical force applied on a dielectric particle [9] (figure 11). Geometrical optics is particularly useful in microscopic particles, whose size  $a$  (in the range of few to several microns) is much larger than the wavelength  $\lambda$  of the trapping laser beam which, for visible light is in the range of 380–780 nm in vacuum (and consequently reduced by a factor  $n$  in homogeneous media).

Geometrical optics has the limitation of not allowing one to predict effects related to the phase and spin of light, which are a peculiarity of the wave nature of light, because these features do not enter in the geometrical optics model. Despite this limitation, geometrical optics has been successfully employed to describe, for example, optical forces on cells [76], the deformation of microbubbles in an optical field [77], the optical lift effect, the emergence of negative optical forces [78], the forces on nonspherical particles [79, 80], Janus particles [81], absorbing particles [82], particles in a speckle light field [35], or trapped at a water–oil interface [83].

#### Current and future challenges

Geometrical optics provides an effective description of the interaction of light with matter and, in relation with optical tweezers, an intuitive and relatively simple explanation of the trapping mechanism. It is especially convenient in all the cases where the dimension of the particles is not small enough to allow full electromagnetic theory calculations. In fact, a complete electromagnetic theory calculation must include a number of terms that increase with the increasing size of the particle, and this might already become challenging in particles of few microns in size. However, geometrical optics does not provide only a 'fall-back' remedy, because it often captures the essence of the physical mechanism and provides an insightful picture without overwhelming non-essential details.

Geometrical optics is a well-established technique that works well in most of the standard cases, where there are analytic formulas provided by the theory [74, 82] and for symmetric conditions, like a spherical particle, or a focused or uniform Gaussian beam, and counter-propagating beams. In the standard and non-standard cases, codes and toolbox are available [84–86], in different programming languages, with different possibilities for customization.



At present, the main challenges for the calculation of optical forces based on geometrical optics are related to the number of rays that are required to accurately calculate force and torque (or, in general, the scattering) on a particle in a nonsymmetric situation, which can be a rather time-consuming task, e.g. in complex particle geometries (nonspherical and/or nonconvex in shape, non-uniform in refractive index), or complex optical-field dependence (non-uniform optical field). In general, an accurate calculation of the optical torque on a particle requires a larger number of rays than the calculation of the optical force. If, moreover, we are required to calculate the dynamics of a nonspherical homogeneous dielectric particle, the force and the torque do not only depend on the particle position, but also on its orientation. When the particle is non-homogeneous in its refractive index, or it moves in a non-uniform optical field, the situation is made even worse: there is often no available analytic expression for the force and the torques, and a pre-calculation of forces and torques on a fine spatial grid for all the orientational degrees of freedom is a very daunting task and not a viable option. Even if pre-calculation were a possibility, in the case of a different value of the particle's radius or refractive index we would be forced to restart from the beginning. Also, depending on the circumstances, a grid of different sizes would be preferable, further complicating the pre-calculation task.

Another situation where the application of geometrical optics can be time-consuming is the case of optical binding and, in general, the situation where interactions of many particles introduce nonlinearity, and many-body calculations are required. A way to partially solve the speed problem in geometrical optics calculations could be to provide the toolboxes with the option of parallelization or to exploit the presence of a GPU. However, adapting or rewriting the code is not optimal from the point of view of becoming dependent from a specific hardware that might become obsolete. On the other hand, a machine learning approach is starting to be used in combination with geometrical optics [87].

### Advances in science and technology to meet challenges

The parallelization of the ray scattering calculations and the exploitation of GPUs with ad-hoc adapted codes for geometrical optics could result in an increased calculation speed, but do not entirely solve the problem of the complexity and of having to repeat the scattering calculation several times.

Currently, a promising approach is offered by the application of machine-learning techniques. The fundamental idea behind the machine-learning approach to geometrical optics is that, once a network is trained to perform well for a certain set of parameters, then it can be used with a set of parameters that are in the range of the training parameters without re-training, even if the parameters do not match perfectly. Because of the intrinsic 'smoothness' of the transfer function that characterises the building blocks of a neural network, it is also possible to overcome the spurious discontinuities observed in geometrical optics calculations emerging in the case of grids with insufficient numbers of rays. Therefore, the computational effort seems to lay in the robust and smart training of the network. This would allow, in the future, the training of single neural networks which can accurately predict the optical forces and torques for a given general situation characterized by several parameter ranges, allowing faster calculation of the dynamics and statistical properties of optical systems.

### Concluding remarks

Geometrical optics is a well-known and established approach for effectively modelling optical tweezers and calculating optical forces and torques on microscopic particles in the ray optics approximation. Several



analytic and computational tools are available, which give accurate results within a fast or moderate computational time. More complex cases (nonspherically symmetric, non-homogeneous particles, non-uniform and/or complex optical fields, nonlinear effects) require a longer and more complex computational approach and, in many such cases, the calculation speed is still a challenge. The introduction of the use of GPUs and parallelization could partially solve the challenges. The currently emerging machine-learning approaches seem promising by consistently addressing the challenge of computational speed, taking it away from the calculation and moving it upstream into the training process of the neural network.



## 8. The dipole approximation

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### Status

The use of light (with wavelengths of several hundred nanometres) to manipulate a nanoparticle (with size of the order of the nanometre) can be analyzed using the single dipole approximation. In this approach, the optical interaction is directly obtained from the Lorentz force, and it is composed of two elements: the gradient force, proportional to the real part of a particle's polarizability and the gradient of the field's intensity, and the scattering force or radiation pressure, proportional to the imaginary part of the polarizability and the gradient of the field's phase [88]. In inhomogeneous spinning fields, the last force component, usually considered to be proportional to the Poynting vector, also depends on the value of the curl of the spin density of the light field [89].

Slightly larger particles and high-refractive-index materials may also be modelled by considering a dipole approach but, in this case, the magnetic response must also be contemplated. Dual equations are obtained for the force on these particles, together with a new term coming from the electric–magnetic dipole interaction [90].

The knowledge of the mechanical response of these small particles is fundamental not just from the nanometric point of view. The force on larger particles or complex systems may be analyzed by studying the collective response of groups of electric dipoles, through the so-called discrete dipole approximation. In this case, the interaction among the dipoles is analyzed via a multiple scattering process, where the field on every particle is given by the incoming field and the field scattered from all the other dipoles.

Thus, the knowledge of the dynamic behaviour of electric dipoles in complex environments and under structured light fields is important, not just from a fundamental point of view, but also as a basic tool to analyze the optomechanical response of larger systems with huge applications in the fields of photonics and nanotechnology. Among these applications we may highlight the nanometric control of the diffusivity, the improvement of radiation pressure propelling systems, and the full control of binding at the nanoscale.

### Current and future challenges

Although the calculation of the force on an electric dipole is an analytically manageable problem, it still presents fundamental challenges like, for instance, the measurement of the Belinfante's curl force, coming from the non-homogeneous spinning nature of the electromagnetic radiation. Another type of spin force, coming from the interaction between the electric and magnetic dipoles, has recently been measured [91], but the detection of the curl of the spin force acting merely on a single dipole is still lacking.

Another challenge is the use of optical forces on electric dipoles to manipulate the diffusivity of nanoparticles using electromagnetic fields. These fields could be used to either increase the diffusivity or decrease it. Specifically, the challenge is to achieve active matter propelled by optical forces. Also, by attaching groups of nanoparticles to larger systems, a noticeable radiation pressure could be achieved, growing harmonically with the number of electric dipoles and lacking the mechanical stress induced by the torque expected at the anchor point [92].

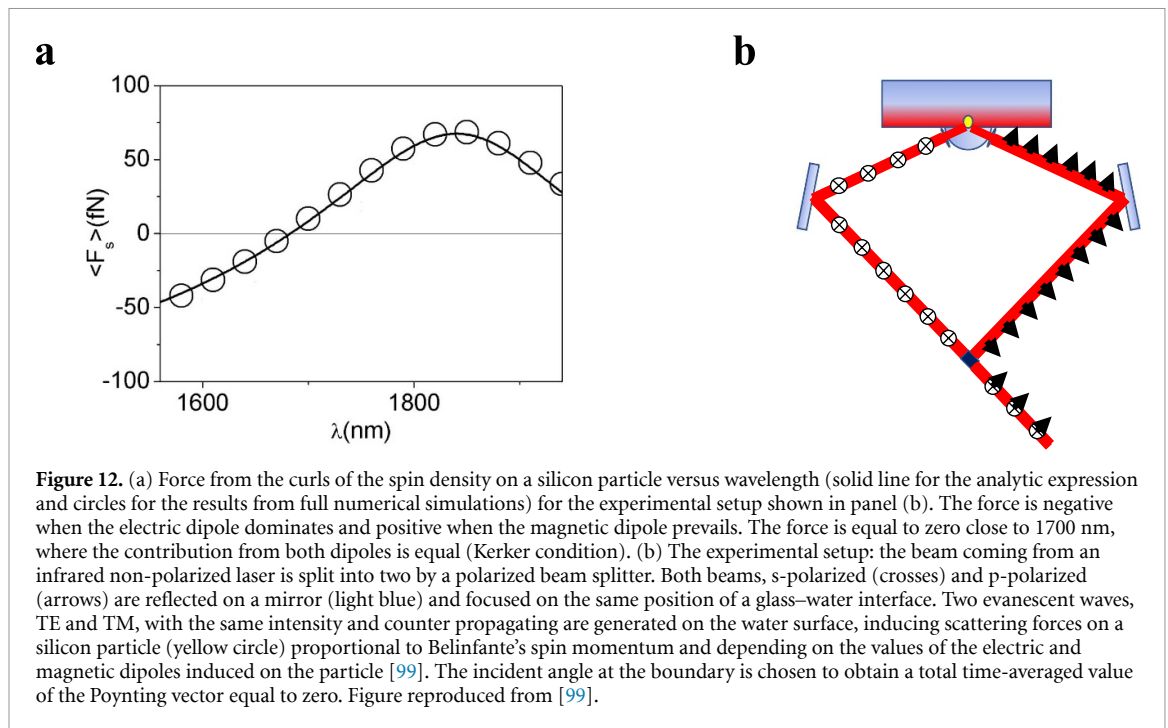
Another future challenge consists of being able to manipulate the optical interaction among nanoparticles, with the final goal of either structuring larger and more complex structures or tuning the coagulation properties of colloids at the nanoscale.

Optical forces on electric dipoles have also been proposed as a method for sorting different types of nanoparticles based on their mechanical response [93]. For example, a possible challenge is chirality sorting, based on the different optical forces felt by a particle with a non-scalar polarizability tensor when illuminated with circularly polarized light [94].

### Advances in science and technology to meet challenges

The technical advances needed to achieve the above-mentioned challenges, using optical forces on dipoles, have been theoretically analyzed and, from those studies, several experimental setups have been proposed [36, 43, 95–99].

Genuine forces coming from the spinning nature of the electromagnetic radiation and acting on a single electric dipole have been predicted, but never detected or gauged. Recently, an experimental setup to measure this force, proportional to the Belinfante momentum, has been proposed (figure 12). The experiment is based on the Kerker condition, a requirement subject to the coincidence between the electric



and magnetic response of a particle. The setup operates at the Kretschmann configuration, using two counter-propagating transversal waves (TE–TM) with the same intensity. Dipole optical forces on this system are only given by the curl of the spin density of the light field acting on each single dipole (electric and magnetic) independently, and not by the force coming from the interaction between both dipoles.

Meanwhile, to achieve full control of the diffusivity of nanoparticles, interfering light fields have been proposed. For example, a field consisting of two perpendicular stationary waves with tunable phases induces an optical vortex lattice. This vortex lattice can increase the diffusivity of the nanoparticles and induce collective motion. The radiation pressure forces appearing in the vortex lattice strongly increase the diffusion coefficient of an isolated particle and, when considering an ensemble of nanoparticles in a fluid, these optical forces may couple to the hydrodynamic forces, inducing a collective motion featuring ballistic superdiffusion [95]. Also, gradient traps may be used to decrease the diffusion. For example, speckles are a good option to tackle this challenge [36], using the value of the intensity as a trigger to reduce diffusion.

The manipulation at will of the equilibrium distance between two dipoles at the nanoscale, using optical forces, is also a challenge from a technological point of view. A possible solution is based on the use of the near-field binding (orders of magnitude larger than the usual far-field binding), tuning the equilibrium distance either by a periodic change in the polarization angle with respect to the axis joining both dipoles or by applying an external magnetic field [96].

However, the technological proposals to achieve isotropic bonding are completely different and, in this case, fluctuating random electromagnetic fields must be generated. This technological problem could be tackled by using scattering of light on disordered systems [43]. Analytically, these fields have been proven to generate different types of isotropic interactions, including long-range forces [97]. As already mentioned, the control of these central forces, using isotropic fields, could be used to induce attractive or repulsive regimes, promoting or avoiding coagulation at the nanoscale.

Finally, a new type of optical interactions has been predicted for dipoles with non-scalar polarizabilities, for instance, those found in nature for chiral particles. These types of polarizability tensorial-like responses could be artificially generated by a technology based on the magneto-optical response of some materials, like the n-doped polar semiconductor InSb. In these systems, the tensor properties of the polarizability are tuned by applying an external magnetic field. These ‘artificially generated’ tensorial dipoles also experience optical forces and torques that are strongly dependent on the spin and helicity of the electromagnetic field [98].

### Concluding remarks

In conclusion, the optical forces on nanoparticles with sizes much smaller than the radiation wavelength may be studied by considering the response of an electric dipole. Although they are analytically treatable, the results obtained from these small systems are far from trivial and turn out to be very useful when analysing

the response of more complex systems. Among others, future applications of the force on these systems are the nanometric control of diffusion and coagulation, the design of building-up methods based on the control of the dipole's binding properties, and the propulsion or sorting induced by electromagnetic radiation.

### Acknowledgments

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## 9. Generalized Lorenz-Mie theories for optical forces

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### Status

The Lorenz–Mie scattering theory was presented in the early 20th century for an infinite plane wave incident beam, providing correct analytical results for an arbitrary particle size and refractive index. However, the concept of the plane wave is an idealization and cannot be achieved in reality; therefore, a generalization for an arbitrary incident beam was needed, which became known as the generalized Lorenz–Mie theory (GLMT) [100]. The GLMT is, therefore, an extension of the classical Lorenz–Mie theory, in which the solution is usually written in the form of an infinite series of partial wave terms for any type of incident beam.

From the vast applications of the GLMT, here we will focus on its role in determining optical forces for arbitrary incident fields. Since the invention of optical tweezers, there has been a continuous and significant effort towards a complete description of optical trapping forces. Early models yielded a theoretical description for extreme ratios between the particle radius ( $a$ ) to the wavelength ( $\lambda$ ), either in the Rayleigh ( $a/\lambda \ll 1$ ) or geometrical optics regime ( $a/\lambda \gg 1$ ). To close this gap, a full electromagnetic solution was required and, since the GLMT used Maxwell’s stress tensor to deal with mechanical effects of light, it became one of the formalisms for rigorous optical force calculations. The advances in optical trapping experiments, in which force components can be precisely measured, allowed a comparison with theoretical forces, refining the models used. Also, most reports now present their results in terms of the forces instead of the radiation pressure cross sections that were more common in the past.

One of the earliest applications of the GLMT to optical forces dates back to 1988, when the radiation pressure on a scatterer was determined from the reduced momentum of the Poynting vector [101]. The partial waves coefficients, also known as beam-shape coefficients (BSCs), were determined for a beam model introduced a decade earlier, developed to produce higher-order corrections of paraxial Gaussian beams [102]. This model showed a reasonable agreement with experimental trapping forces and trapping efficiencies values when using a mild focused beam. High numerical aperture (NA) objectives, however, are required for stable 3D trapping of particles, and these high NA beams were not correctly described by the higher-order correction. Although the initial beams were a solution of Maxwell equations (i.e. Maxwellian beams), this was not true for the higher-order corrected beam model. A non-Maxwellian beam resulted in radial coordinate-dependent BSCs. These strongly convergent beams needed to be adequately described by a proper beam model, a Maxwellian beam, and preferably with parameters that are accessible experimentally.

### Current and future challenges

To validate the GLMT for the description of optical forces, it is necessary to obtain the BSCs of arbitrary beams and show that they correctly describe the incident beam. Moreover, the optical force predictions must be consistent with experimental results. Early experimental results measuring optical forces were obtained by balancing the optical forces with drag forces and determining the ‘escape force’. These point-wise results showed good agreement with predictions from GLMT calculations for displacements within the particle radius [103]. Later methods were richer, yielding the optical force profile on the particle as a function of its displacement from the focused beam [104].

The challenge to find a proper beam model for optical tweezers, and an analytical method to solve the BSCs, was found and demonstrated by a series of experiments, which also detected the diffraction effects present in the high numerical beams, morphology-dependent resonances, and spherical aberration effects, described in a recent tutorial for optical forces [105]. As a result, the BSCs could be determined analytically from their definitions, and the same model and procedure has been successfully applied in other fields.

Today, the GLMT is a mature framework used to describe the scattered wave by a symmetric scatterer for any type of Maxwellian beam. It has been successfully applied to investigate: trapping aggregates of

interacting plasmonic nanoparticles; the trapping of metamaterials, such as negative refractive-index particles; stability of the trapped particle in terms of the switching rate in time-division multiplexing of the trapping beam; optical binding using a resonant cavity evanescent wave trap; microrheology of gaseous media, photophoretic forces in aerosols; the effect of polarization on trapping of chiral spheres; and switching photonic nanojets within optical traps.

The application of the GLMT has not been restricted to only highly focused Gaussian beams, but it has also been extended to other Maxwellian beams. An alternative and more general method to determine an analytical exact expression for the BSCs, using Fourier transform of the angular momentum operator, was demonstrated [106]. Different types of incident beams have been applied for optical trapping within the GLMT: zero-order Bessel beams; vortex Bessel beams; standing waves; Laguerre–Gaussian beams; Airy beams and arrays of Airy beams; optical stretchers; optical conveyors as long-ranged tractor beams; frozen waves providing localized stationary longitudinal fields; pulsed laser beams considering linear and nonlinear effects; and guided modes within hollow-core photonic crystal fibres.

### Advances in science and technology to meet challenges

Research is a never-ending story, and most models are always tweaked for the upcoming trapping application. A few issues are worth highlighting:

- There are presently no analytical solutions to guided modes in hollow-core photonic crystal fibres, but to model the force within the GLMT an approximate mode model is used. We would expect an increase in experiments and simulations to validate guided mode models, possibly via optical forces.
- Analytical force expressions for particles inside cavities or waveguides that only consider the cavity e-m modes without the particle are approximations of the real problem. How the presence of the particle changes the e-m fields and evanescent modes should be considered. We expect, therefore, a complete analysis of the external cavity—particle e-m fields to calculate the force without approximations.
- Near-field interactions are another growing area of spectroscopy, such as tip-enhanced Raman scattering, which will probably be used to trap particles.
- Most optical force experiments that displace the beam with respect to the trapped bead are achieving this by tilting the beam at the back-objective aperture. It would be suitable to see a model for the focused beam in terms of this tilt, which would result in the trap displacement near the focus.
- The GLMT has been applied to symmetric objects, such as spheres, spheroids, and infinite cylinders, but if the correct boundary conditions are satisfied, or a superposition thereof, it would be possible to calculate the forces for other shaped objects yet to be determined.
- In structured metamaterials, optically cloaked objects have been theoretically demonstrated using plane waves that are incident on the objects. Given the appropriate metamaterial and requirements for the stress tensor, a shaped beam could be rendered invisible and could also trap a cloaked object with the GLMT.
- A field where GLMT was timidly employed was in optical binding to form optical matter. It is a field with several recent and important advancements, most of which could be well modelled using the GLMT.

In summary future developments are hard to predict but, considering it as an extrapolation of the recent timeline, experiments would be more complex, aggregating other fields of research to optical trapping such as nonlinear optics, nonequilibrium thermodynamics, and/or machine learning. However, the GLMT is a robust method to determine optical forces, which is currently unmatched.

### Concluding remarks

Since its birth, the GLMT has been used for a wide range of applications in optical trapping. Over the years, new beam models have been presented, as well as procedures for determining the BSCs. Recent developments in instrumentation for optical trapping, particle tracking, laser generation, and beam shaping, allow higher accuracy and finer tolerance for comparison between experimental results and optical force models, for which the GLMT holds great promise.

### Acknowledgments

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## 10. T-matrix approach for optical forces

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### Status

Since its formulation in the mid-60s, the transition matrix (T-matrix) method, summarized by Peter C. Waterman in his milestone paper dated 1971 [107], has become one of the most powerful, versatile, and popular techniques for a theoretical description of electromagnetic, acoustic, and elastodynamic scattering by particles and surfaces. The most recent attempt to outline the vast realm of this technique and its practical applications dates back to 2020, with a comprehensive publication database that includes more than 290 references, authored by Michael Mishchenko [108].

The T-matrix method is a complete wave-optical modelling of the particle–light interaction, recently extended to calculate the mechanical effects of light [109, 110] (figure 13a). It represents an ideal bridge between the dipole and the geometrical optics approximation, extreme cases of the classical theory of light scattering. It can be successfully applied in the intermediate range, when the scattering particle size is comparable with the light wavelength  $\lambda$  ( $x = 2\pi r/\lambda \simeq 1$ , where  $r$  is the radius of the particle). The T-matrix method has also proved to be a good approach when dealing with inhomogeneous particles and nonspherical particles that can be modelled as aggregates of spherical monomers.

The T-matrix method, also known as the null-field method and extended boundary conditions method, is based on the representation of the scattering function on the orthonormal basis of the spherical multipolar vectors that are solutions of the Maxwell equations. In this case, the scattering function, which is called the T-Matrix, acting on the amplitudes of the incident field, gives, as a result, the amplitudes of the scattered field. Among the different methods used to calculate the optical properties of model particles, in the near and far field, those based on the T-matrix are currently among the most accurate and efficient, particularly when applied to nonspherical particles composed of spherical constituents, i.e. clusters or aggregates of spheres, spheres with spherical (eccentric) inclusions, and multilayered spheres [111]. This technique takes into proper account the multiple scattering processes occurring among the spherical subunits composing the aggregate and the contribution coming from all the details of the model structure. The optical properties and mechanical effects of composite scatterers are analytically derived and can be exactly calculated without introducing any approximation, except the truncation of the expansion of the fields, thus being able to check the convergence of the results at every step.

In recent years, the T-Matrix method has been extended to the study of the mechanical effects of light in optical tweezers, where the incident radiation, modelled through the angular spectrum representation [112], consists of Gaussian beams [113], cylindrical vector beams [114], or Laguerre–Gauss beams [115].

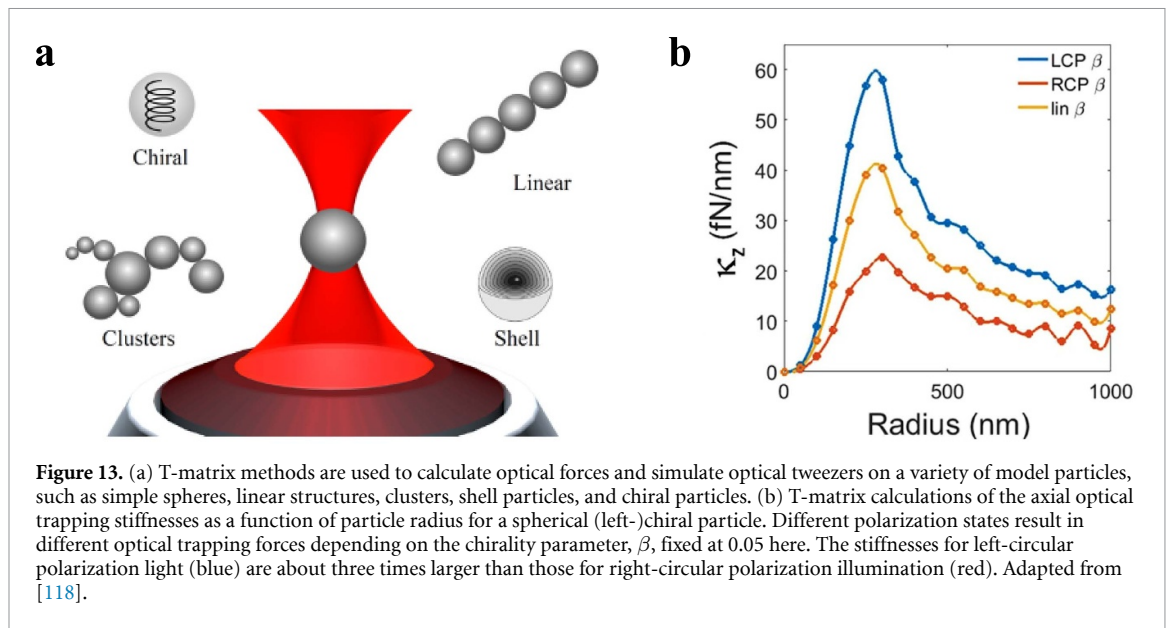
### Current and future challenges

As outlined above, the T-matrix is a consolidated method that manages to describe, analytically and numerically, the interaction between radiation and micro- and nano-structured matter, possibly modelled as clusters or aggregates of spheres. Due to its high numerical accuracy, this approach is suitable for benchmark computations. However, some important issues of current interest may pose a challenge. First, advances in nanofabrication made available a novel class of materials and metamaterials with unprecedented optical properties [116]. Electromagnetic fields generated by such complex structures and metasurfaces can permit optomechanical spatial control of submicrometric particles or molecules. T-matrix methods can accurately determine the resulting optical forces by accounting for the full interaction between the surface and the interacting particles [117]. This is particularly interesting when considering optical forces applied to chiral particles [118] (figure 13b). Within this context, properly engineered metasurfaces can represent a breakthrough in the selection and sorting of nano- and micro-particles on the basis of their optical activity.

Related to the above considerations, a relevant improvement of the T-Matrix numerical tools concerns its applications for the inverse design of nanofabricated patterns or metasurfaces for optimal optical manipulation in the surface proximity. This improvement can be achieved by interfacing the force-field data obtained with T-matrix simulations with automated procedures based on the use of neural networks [87].

Another future challenge concerns the development of some specific theoretical tools that are able to improve the calculations and modelling of optical forces on cosmic dust grains with complex shapes and composition for applications of optical tweezers in space [119]. The relevance of these applications in space science lies not only in the possibility of an in-depth study of the chemical and physical properties of powders, but also in investigating the role played by cosmic powders on the composition of planetary atmospheres.





### Advances in science and technology to meet challenges

To address the above challenges, using optical forces on micro- and nano-particles, a synergistic advance of the theoretical approach and of the experimental procedures is necessary.

As regards the study of the optical forces generated by metasurfaces, while the analytical approach based on the definition of the Maxwell stress tensor is complete and defined, providing, in a closed form, analytical expressions for transverse forces and radiation pressure, the numerical codes allowing their calculation must still be systematized. At the same time an improvement in the experimental methodologies capable of performing force measurements at the femtonewton order will be necessary. For this purpose, the force-detection technique used in optical tweezers has the required sensitivity and can be adapted for experiments.

The possibility of exploiting surface selection properties, based on the effect of optomechanical forces acting on nanoparticles with optical activity, pushes us to find a strategy based on artificial intelligence that can provide the best compromise in terms of sensitivity and ease of implementation. For this purpose, the convolutional neural networks seem to be the most advantageous choice and, in the near future, research in this field will focus on the design of this type of numerical protocols.

Finally, the theoretical analysis for space science applications of optical trapping constitutes a test bed for the technologies that will be developed, and can serve to address the strategies for the realization of experimental equipment.

### Concluding remarks

Since their first introduction light scattering techniques based on the T-Matrix approach have found applications in a wide area of science and technology, in particular as a fundamental tool for optical trapping. Over the years, the scientific community has found answers to many questions concerning the theory of optical trapping of particles at the micro- and nano-scale, also in the presence of surfaces, both in the far and near field. With the recent advances in nanotechnologies, new challenges are arising related to new possibilities for the nanofabrication of complex surfaces and metamaterials that can open novel routes for optical manipulation. The expertise acquired in the field of optomechanics and nanophotonics will allow us to face these challenges through a multidisciplinary approach.

### Acknowledgments

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## 11. Transverse angular momenta

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### Status

The angular momentum (AM) of light plays a crucial role in the field of optics. A beam of light, described as an electromagnetic wave, can carry two different kinds of intrinsic AM. The first is connected to a spinning electric or magnetic field vector and is denoted as spin AM (SAM). The most prominent example of the SAM of light is circular polarization [120]. Unlike SAM, orbital AM (OAM) is a consequence of the spatial structure of a beam or field. It usually emerges as an azimuthal phase gradient around singular points [121]. A plethora of applications reflects the significance of both OAM and SAM. Their utilization as information carriers in classical or quantum communications or for the manipulation of microscopic matter via optical AM transfer are just two examples. For a beam of light, the total AM density can be expressed as the sum of spin and orbital constituents, i.e.  $\mathbf{j} = \mathbf{s} + \mathbf{l}$ , where  $\mathbf{s}$  corresponds to the SAM density and  $\mathbf{l}$  to the OAM density. The individual spin and orbital parts are defined via the electric and magnetic fields by

$$\mathbf{s} = \text{Im}[\epsilon_0 (\mathbf{E}^* \times \mathbf{E}) + \mu_0 (\mathbf{H}^* \times \mathbf{H})] / 4\omega, \quad (1)$$

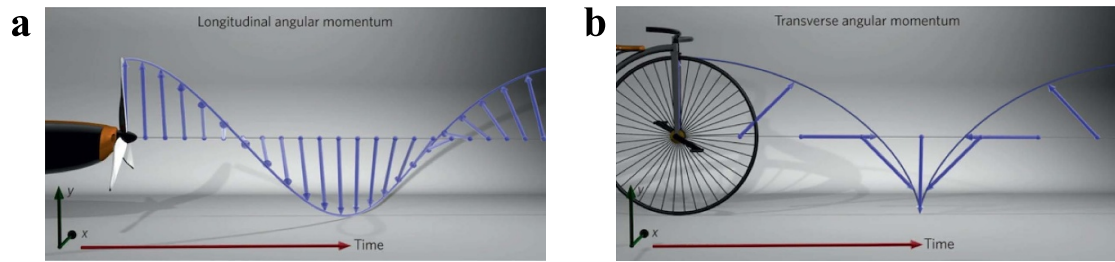
$$\mathbf{l} = \mathbf{r} \times \text{Im}[\epsilon_0 \mathbf{E}^* \cdot (\nabla) \mathbf{E} + \mu_0 \mathbf{H}^* \cdot (\nabla) \mathbf{H}] / 4\omega, \quad (2)$$

where  $\epsilon_0$  and  $\mu_0$  are the vacuum permittivity and permeability, respectively,  $\mathbf{E}$  and  $\mathbf{H}$  are the electric and magnetic field vectors,  $\omega$  is the angular frequency of light, and  $\mathbf{r}$  is the position vector.

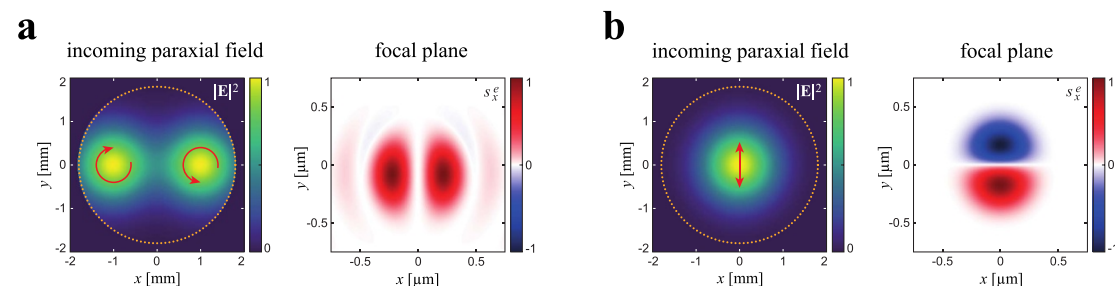
Hence, each of them comprises contributions by the electric and the magnetic field. One can easily see that for a circularly polarized plane wave propagating along the  $z$ -axis and described by its electric field vector  $\mathbf{E}_\pm = E_0 (1, \pm i, 0)$ , one obtains a position-independent non-zero longitudinal SAM density  $\mathbf{s} \propto E_0^2 \hat{\mathbf{e}}_z$ . In contrast, the OAM remains zero for an adequate choice of the coordinate system. Intrinsic optical OAM (independent of the coordinate system) arises in beams of light that possess a more intricate spatial structure. One prominent class of beams in this regard are the so-called Laguerre–Gaussian modes, solutions to the paraxial wave equation, which carry discrete values of OAM. If a particle is interacting with a focused beam that possesses AM, part of the AM might be transferred, resulting in a mechanical action. In conventional SAM or OAM, which is naturally aligned with the direction of propagation or the optical axis, either a spinning or orbiting motion of the particle about the optical axis has been observed experimentally [122]. However, it has been proposed that the orientation of AM is not restricted to be parallel or antiparallel to the optical axis [24, 123], opening new possibilities for the manipulation of 3D particle motion in an optical tweezers system.

### Current and future challenges

Apart from providing a great platform for the study of fundamental light–matter interactions, the dynamics of the medium, where a particle is optically trapped, can also be studied by optical momentum transfer [124]. The trapped particle then acts as a local sensor for, e.g. the local viscosity of the fluid. This is a huge advantage over other well-established non-local methods. However, in terms of rotational motion, the employment of light carrying only longitudinal AM may impose a severe restriction to such kinds of measurements. It would be thus highly desirable to transfer AM with an arbitrary orientation to trapped particles to enhance the potency of the aforementioned and many other techniques [123]. To achieve such full control over all rotational degrees of freedom of submicron-sized objects inside a simple optical trap, it is necessary to create a light field possessing not only longitudinal, but also transverse AM. Recently, it has been shown that upon tight focusing of light beams, a natural ingredient to optical tweezers, components of the SAM perpendicular to the direction of propagation arise [24, 123]. This effect occurs due to the superposition of out-of-phase transverse and longitudinal electric or magnetic field components [125]. Note that such a superposition does not take place for a collimated paraxial beam or plane wave, which are assumed to feature only transverse field components. Schematically, the longitudinal electric and/or magnetic field components that are necessary for the formation of transverse SAM result from the process of tight focusing because of a tilt of the wave vectors of the incoming beam towards the focal spot. The distinction and emergence of longitudinal and transverse SAM are schematically shown in figure 14. A spinning motion of the electric field vector



**Figure 14.** A comparison of longitudinal and transverse angular momenta. (a) Longitudinal SAM resulting from the polarization vector spinning around the optical axis, resembling the propeller of a plane. This type of SAM is present in a paraxial circularly polarized beam. (b) Transverse SAM, which occurs due to the electric field vector spinning around an axis orthogonal to the direction of propagation, analogous to the rolling wheel of a bicycle. Adapted from [124].



**Figure 15.** The incoming field distribution (paraxial beam) and the resulting transverse spin density component  $s_x^e$  in the focal plane (after tightly focusing the beam using a high-NA microscope objective) for (a) two laterally displaced circularly polarized Gaussian beams of opposite handedness [123, 126] and (b) a linearly  $y$ -polarized Gaussian beam. Integration of the spin density distribution in (a) results in a non-zero value, whereas it is strictly zero for (b). The local polarization states of the input beams are indicated by red arrows, and the dotted circles indicate the entrance aperture of the focusing optics. Calculation parameters: wavelength = 532 nm, numerical aperture = 0.9, beam radius = 1.2 mm.

about the direction of propagation results in longitudinal SAM (figure 14(a)), whereas transverse SAM is a consequence of a rotation of this vector around an axis perpendicular to the optical axis (figure 14(b)).

### Advances in science and technology to meet challenges

Recently, the utilization of transverse SAM in optical tweezers reached a new milestone. A trapped object was experimentally set in a spinning motion about an axis normal to the optical axis [126] following an earlier theoretical proposal [123]. The incoming field distribution consists, in principle, of two laterally displaced and circularly polarized Gaussian modes of opposite handedness (figure 15(a), left). Tight focusing of this beam results in a non-zero transverse SAM density distribution (figure 15(a), right), while the longitudinal SAM component vanishes [123]. The use of such an extraordinary field distribution is necessary here, as the utilized microspheres, measuring  $3.5 \mu\text{m}$  in diameter, are only sensitive to the integrated SAM density. The latter is in fact zero for the majority of light beams that are used for trapping or in optics in general.

In contrast to the total transverse SAM, almost every tightly focused beam exhibits a locally non-zero transverse SAM density [24, 127, 128] that can be sensed by subwavelength sized particles. As an example, for a linearly  $y$ -polarized Gaussian beam (figure 15(b)), we find a locally non-zero  $s_x^e$  distribution that is antisymmetric with respect to the  $x$ -axis. As a result, if a nanoparticle is placed therein, the sign of the transferred torque will depend on its position relative to the  $x$ -axis. Generally speaking, different paraxial input fields will result in different distributions of the transverse SAM in the focal plane, providing an enormous variety of possible landscapes for particle manipulations. The whole situation becomes even more delicate when also considering the magnetic spin density, as in the non-paraxial regime, electric and magnetic transverse spin densities can feature utterly distinctive spatial distributions [128]. Their superposition and interplay can lead to material selective highly tailorable optical forces.

### Concluding remarks

Since the inception and first mention of transverse angular momenta of light in general and transverse spin in particular about a decade ago, the corresponding field has grown substantially, also paving the way for various applications. In particular, within the context of optical forces, transverse components of the net spin

or the spin density hold an immense potential to be explored in the future. Intriguing pathways are represented by achieving full control over rotational degrees of freedom in optical traps, tailoring the interaction with chiral matter, as well as exploiting 3D spin density or spin vectors resulting from tailored electric and magnetic fields. Moreover, the induction of position- and material-dependent forces and torques acting on trapped particles opens new pathways for applications, for instance, within the context of optically driven micromachines.

## Measurement of forces and torques

### 12. Photonic force microscopy

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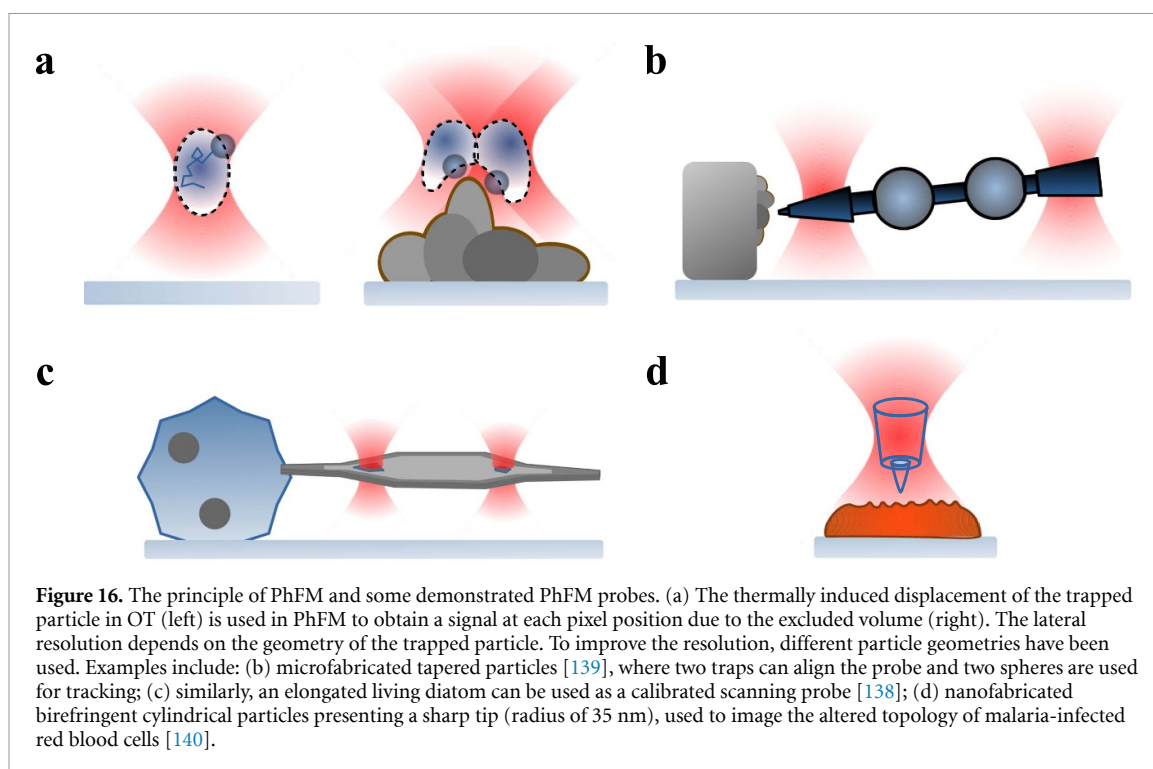
#### Status

Soon after their demonstration by Ashkin, the ability of optical tweezers (OTs) to simultaneously manipulate and detect the position of microscopic particles at high spatio-temporal resolution was recognized as instrumental for the development of a novel near-field scanning imaging technique, termed photonic force microscopy (PhFM) [129–132]. In PhFM, an optically trapped particle is used to scan and probe the local environment surrounding the sample (figure 16(a)). Similar to atomic force microscopy (AFM), imaging in PhFM is achieved by moving the sample by a piezo stage while the trapped probe mechanically interacts with the surface of the sample. The probe displacement is then used to reconstruct the image of the surface topography. In PhFM, similar to AFM, the displacement of the trapped probe is used to define the signal in each pixel (or voxel), while a piezo stage moves the centre of the optical trap over the sample. Crucially, with respect to AFM, the PhFM probe is held in position by its interaction with light in the laser focal region, creating a very soft optical spring, with a stiffness  $\kappa$  of the order of  $1 \text{ fN nm}^{-1}$ , three orders of magnitude less stiff than standard AFM cantilevers. Such extreme softness is one of the main features of PhFM, allowing the characterization of materials of extremely low rigidity, which are outside the scope of AFM. In contrast, due to the stiffness of the cantilever, high-quality AFM signals can only be achieved with relatively rigid samples. Combined with the fact that it can be easily used in liquid, this opens the way for PhFM imaging of the topography of soft biological materials [133], such as the membranes of living cells under physiological conditions, which are notoriously difficult to image in AFM without chemical fixation (which artificially rigidifies and kills the cells). Another unique aspect of PhFM (and OT) is the absence of contact between the probe and the instrument, not achievable with other scanning techniques. This has been used to expand the reach of the technique from surface topography to volumetric scanning imaging [134]. Despite resolutions that currently remain below those of standard AFM, the potential of PhFM to image soft and biological surfaces or volumes in living systems remains unique, thus inviting further developments.

#### Current and future challenges

The microscopic probe of the PhFM is, in liquid, an over-damped system, where inertial effects can be neglected up to frequencies of several hundreds of kHz. When imaging with such a probe, its confined Brownian motion is relevant, setting the constrain of ergodicity: the probe requires a characteristic time  $t_c = \gamma/\kappa$  (where  $\gamma$  is the drag coefficient of the probe) to fully explore the volume of the laser trap. This is related to the precision of the measured signal chosen to characterize the pixels of the image (typically the average or median vertical displacement of the probe). As the error of the mean decreases with the square root of the number  $N$  of independent measurements ( $N = T/t_c$ , where  $T$  is the total measurement time at one position), it is interesting to note that there is no theoretical limit to the precision of the measured signal. The precision limit is set by practical constraints: the drift degrades the accuracy of the measurement at long times, and the total imaging time should remain reasonable for the system under study. Therefore, good thermal, mechanical, and optical stability, that reduces the drift of the apparatus, together with a careful calibration procedure, is key to achieve high precision and accuracy. To minimize the total imaging time, it is necessary to reduce the characteristic time  $t_c$ . An increase in laser power leads to an increase in the trap stiffness  $\kappa$ , decreasing  $t_c$ . However, this is not always possible on delicate samples. A decrease in particle size decreases the drag coefficient  $\gamma$  but also the stiffness  $\kappa$ , unless a (trappable) higher refractive-index material is chosen.

Related to particle size is its geometry, crucial in any near-field scanning technique. In PhFM, the spherical dielectric particles typically used in OT have often been employed as scanning probes. While (sub-)microscopic spherical particles have geometrical limitations in achieving nanometre resolution in the lateral directions (the image is the convolution of the surface topology with the tip geometry), they are commercially available, the signals are straightforward to interpret, they allow nanometre resolution in the axial direction and, when their diameter is reduced to a few hundreds of nanometres, they have been shown to allow imaging with subdiffraction resolution [135]. To improve the lateral resolution, the potential of elongated probes has also been recognized and explored [136–140]. Elongated probes presenting a sharp feature also have the interesting capability to be manipulated by multiple independent traps (figures 14(c) and 16(b)), thereby probing unconventional samples, where the topography of interest is perpendicular to the sample plane.



### Advances in science and technology to meet challenges

For PhFM to reach full maturity, where it will be employed by a larger community outside of physics and developers, certain technical improvements will be required. The development of nonspherical probes will prove crucial to reaching lateral resolutions which approach AFM. Recent developments have enabled the massive nanofabrication of microscopic probes presenting a sharp tip (a few tens of nanometre in radius, figure 16(d)), which are easily able to be trapped [140]. An ideal scenario could be a trappable probe wherein: (1) its refractive index is maximized to obtain higher trap stiffness, (2) its size is minimized to give low drag, and (3) a feature as sharp as an AFM tip (of few nanometres radius of curvature) is present to interact with the sample to increase the lateral resolution. This would allow high-resolution images of soft samples while minimizing the total imaging time. Additionally, more reliable surface passivation protocols are needed for the probe in different environments to avoid deleterious aspecific adherence of the probe to the sample during imaging, and novel solutions need to be developed to improve the ability to image thicker or non-transparent samples.

Being based on a versatile technique like OT, PhFM can conceivably be expanded in other directions that can be combined with measuring topography. Different functionalities that have been demonstrated on solid substrates can be transferred to PhFM, adding to them the capability of spatial scanning. Interestingly, adding plasmonic structures on the trapped probe has been used to produce a ‘nano-trap in a micro-trap’ [141], where nanometre-sized objects can be trapped by the enhanced electromagnetic field created by a plasmonic structure on the trapped microscopic particle, effectively detaching the nanotweezers from the surface and allowing 3D nano-manipulation. The use of fluorescence-based techniques, such as super-resolution microscopy, fluorescence correlation spectroscopy, and fluorescence resonance energy transfer, combined with an enhancement-optimized engineered structure built on top of a PhFM probe could be used to detect the presence, position, and conformational changes in single molecules, opening up the possibility of imaging heterogeneity. Finally, by employing birefringent particles, by controlling and measuring the polarization state of the trapping laser, PhFM can be expanded to control and measure the optical torque on the scanning probe with pN·nm accuracy [142]. This effectively scales a macroscopic rheometer to the (sub)micron scale [143], opening the way for simultaneous topography and microrheological imaging, for example on cell membranes and other soft interfaces.

### Concluding remarks

PhFM was recognized early on due to its unique potential in topological and volumetric scanning of soft biological samples. However, due to key technical limitations, including limited lateral resolution, the need for parallel fabrication of a high number of colloidal probes, and an involved detection scheme, its development lagged behind other scanning near-field techniques. Today, several of these limiting factors can

be addressed. In particular, nanofabrication opens new possibilities in obtaining probes with sharp scanning features to achieve high lateral resolution. Moreover, by coupling PhFM and its scanning capabilities with other optical modalities, from plasmonic manipulation and sensing to active microrheology, it is assured that future developments hold promise for this versatile technique.

## Acknowledgments

We thank Ashley L Nord for useful comments. This work is supported by the ANR HiRes-PFM project Grant ANR-20-CE42-0005-01 of the French Agence Nationale de la Recherche. The CBS is a member of the France-BioImaging (FBI) and the French Infrastructure for Integrated Structural Biology (FRISBI), two national infrastructures supported by the French National Research Agency (ANR-10-INBS-04-01 and ANR-10-INBS-05, respectively).



### 13. Precision measurements with ballistic optical tweezers

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#### Status

Optical tweezers have a truly broad range of applications, spanning biomedicine, biophysics, quantum physics, and fundamental studies. Many of these applications rely on particle tracking and use measurements of the trajectory of the particle to learn about its environment. In biophysics, one could for instance learn about the molecular forces applied to the particle, or about how energy is dissipated/stored in the medium within which the particle resides. This ability to extract information about the environment of the particle at the nanoscale is truly powerful, for instance allowing discrete motor molecule steps and single-molecule binding events to be observed. However, a significant challenge has been to achieve measurements of the environment over timescales commensurate with the dynamics of the environment [144].

Typical optical tweezers operate in the Brownian regime, where the precision of the particle tracking measurement is sufficient to localise where the particle is in space, but insufficient to determine its instantaneous velocity. To determine the velocity, it is required to be able to resolve the position of the particle on a timescale that is fast compared to the momentum relaxation time [145], which for a microparticle in liquid is typically in the range of a microsecond. This is something that Einstein famously considered to be impossible [146]. As illustrated in figure 17, the position of a particle in an optical trap equilibrates only slowly with its environment—at a timescale given roughly by the inverse of the trapping frequency. As a result, optical tweezers measurements tend to be relatively slow, limited to second to millisecond timescales.

#### Current and future challenges

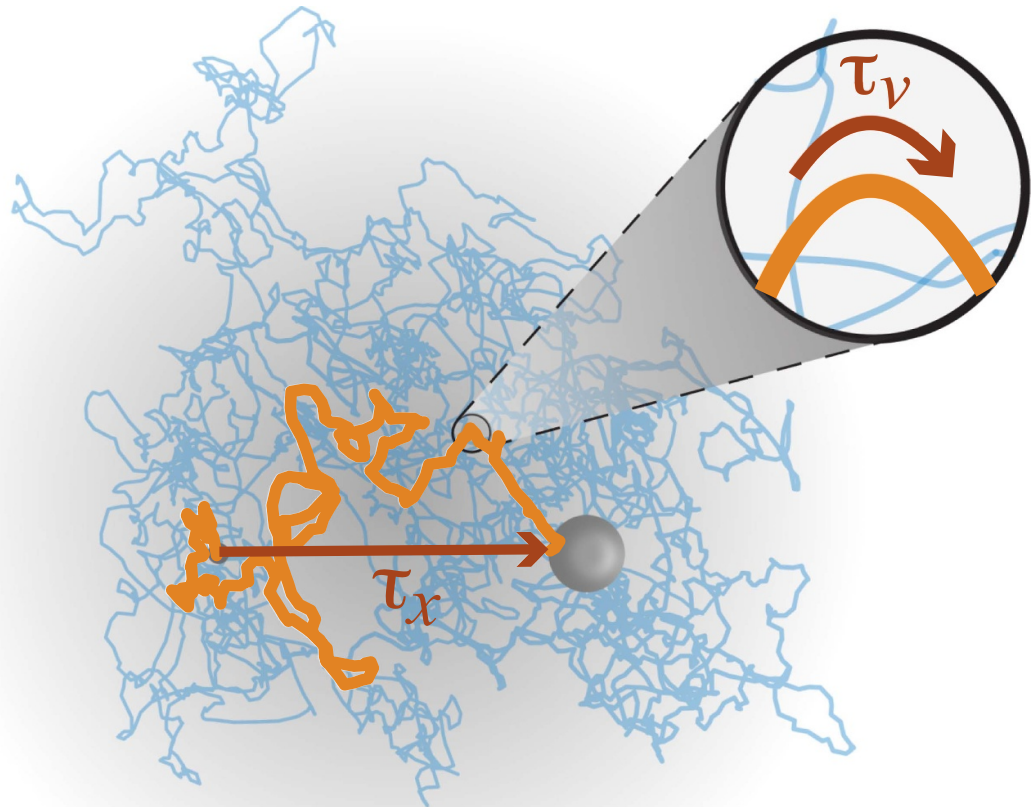
The challenge then is whether it is possible to reach the ballistic regime of optical tweezers, where the instantaneous velocity of the trapped particle can be observed and, if so, whether this could enable faster optical tweezer measurements. The justification for expecting that faster measurements may be possible in the ballistic regime is that the speed at which a probe can measure its environment is directly connected to how fast the probe equilibrates with its environment. The position equilibrates slowly, as discussed above. However, the velocity equilibrates fast—thus, the precise the physics that makes it challenging to measure the instantaneous velocity also provides the prospect to probe the particles' environment quickly, if one can measure it.

In principle, the precision of optical-tweezers-based particle tracking scales as the inverse square root of the detected optical power. Therefore, the solution to reach the ballistic regime appears obvious—just increase optical power. Unfortunately, the powers generally required to reach the ballistic regime for microscale particles are too high for a commercial optical tweezers detection system to handle. This led the Raizen lab to develop alternative custom detection technologies for optical tweezers, including the fibre-bundle technique shown in figure 18 (bottom left) [147, 148]. Using a custom photodetection system, they were able to reach the ballistic regime, proving Einstein wrong, and test the Maxwell–Boltzmann distribution for the first time for microparticles in a liquid [148].

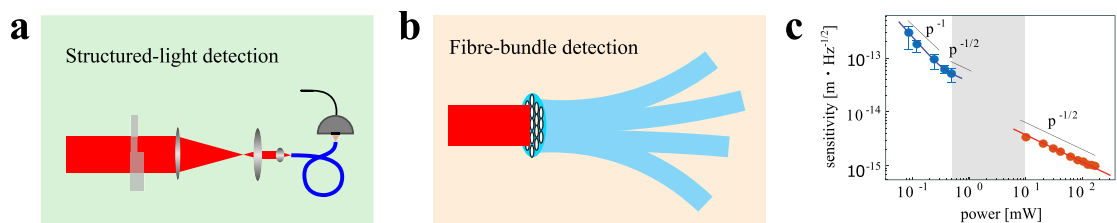
Later, in 2021, in a work by Madsen *et al* [34], my laboratory demonstrated an alternative method to reach the ballistic regime, which we term *structured-light detection*. This method has the advantage of being compatible with commercial photodiodes. It works by first recognizing that the vast majority of the optical trap photons that are transmitted through the optical tweezer carry no information about the position of the particle. By exploiting the different symmetry of the optical modes that carry and do not carry information, we were able to design a spatial filter to suppress the non-information-carrying light by a factor of a thousand. This filter combines a phase plate with a single-mode optical fibre, as illustrated in figure 18 (top left) and, when operating with around 200 mW of power, allowed us to achieve record particle-tracking sensitivity just above 1 femtometre-per-root-hertz (figure 18 (right)).

#### Advances in science and technology to meet challenges

Applying our structured-light detection technique, we showed that it is possible to accurately characterise the momentum relaxation time at very fast speeds. Since the momentum relaxation time is directly connected to the viscosity of the medium in which the particle resides, this allowed us to make viscosity measurements that were around four orders of magnitude faster than has been possible before, at speeds as fast as 20  $\mu$ s [34]. This now makes it possible to track the dynamics of viscosity, rather than simply treating it as a static material parameter. Some remaining open questions are: what viscosity dynamics are to be expected? In what sort of systems? And is it possible to apply these techniques to very small particles, thereby suppressing force noise (which scales as particle area) and allowing more precise measurements of molecular forces?



**Figure 17.** The motion of a particle in an optical tweezer. The position and momentum of the particle reach equilibrium with the environment at very different rates. The equilibration time for position ( $\tau_x$ ) is given by the time it takes the particle to explore the optical trap, or roughly the inverse of the trap frequency. The equilibration time for momentum ( $\tau_v$ ) is given by the typically much faster momentum relaxation time. Measuring the velocity (or momentum), therefore, provides a much faster way to probe the environment.



**Figure 18.** Detection techniques for precision optical tweezers. Top left: structured light detection developed in [34]. Bottom left: fibre-bundle-based detection developed in [147]. Right: sensitivity comparison of standard optical tweezers using standard split-detection (blue) and using structured-light detection (red) [34]. The sensitivity scales as inverse-power ( $p^{-1}$ ) at low powers, where the detector electronic noise dominates, and as inverse square root power ( $p^{-1/2}$ ) at higher powers.

To answer these questions requires advances in both science and technology. In science, a better understanding of out-of-equilibrium matter is required. We know that active matter can exhibit turbulence, vortex dynamics, and a range of other rich physics [34]. Vortices are thought to form fast propagating bands in strain-stiffening materials that carry along with them regions of high viscosity [149]. But whether such dynamics exists in other active materials, such as biological materials, and whether they might play a functional role in these materials, is not known. Models of biological active materials, such as the cellular cytoplasm, are needed to answer these questions.

Optical tweezers that can reach the ballistic regime within a living biological system are also required, and improvements in ballistic optical tweezers to enable operation with smaller particles. This will necessitate

technology development. A key challenge is to reach the ballistic regime with optical powers that are sufficiently low that they do not intrude on the biological specimen. This can be expected to especially be a challenge when using small particles, since their lower optical scattering and faster momentum relaxation greatly increase the difficulty in reaching the ballistic regime. Solutions could involve employing resonant particles, such as plasmonic particles, using structured light to increase the optical scattering [27], or even using quantum correlated light to improve the precision of the measurement at fixed optical power levels [150, 151].

### Concluding remarks

It is now possible to reach the ballistic regime of particle tracking in precision optical tweezers, and to employ this regime to perform exceptionally fast measurements of the environment of the particle. This has been used to determine nanoscale viscosity at speeds in the range of tens of microseconds. Now that the technology has been proven, there are prospects for a wide range of applications from direct measurements of the energetics of molecular binding to experiments that explain the role of the dynamics of viscosity in biological function. Some of these applications are accessible using existing technology. Others will require new developments and innovations.

### Acknowledgments

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## 14. Generation and measurement of torques

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### Status

Rotation of a non-absorbing birefringent particle in single-beam optical tweezers was first shown by Friese *et al* [122] using birefringent particles and circularly polarized light, while the optical torque wrench was shown by La Porta and Wang [152]. The effect has since revolutionized optical tweezers where, not only can one generate translational forces, but also apply torques. This facet has been used extensively in physics, where rotations have been used in topics ranging from fluid dynamics, rheology, exotic effects in vacuum, and in biology, where controlled torques were applied to cells and even single molecules [153]. Meanwhile, in some cases, new paradigms were opened with new insights into twisting of molecules like kinesin during stepping [154]. It is here that we have to realise that a rigid body can have three translational degrees of freedom while simultaneously having another three rotational degrees of freedom. The above-mentioned method only explores what can be called the in-plane (or yaw) motion. There are still the two out-of-plane modes, namely the pitch and roll motions. Pitch motion was partially realized when asymmetric cells were rotated using two trapping beams, but that was still far from the generation of controlled torques on spherical particles, where the drag is minimized. Controlled roll torques have even today remained elusive. These out-of-plane modes become prominent, particularly in proximity to surfaces when the rotational symmetry is broken. Moreover, there are a plethora of biological problems where such a mode can provide a wealth of additional information. The roll motion has so far only been explored with nanowires, where nanoscale kinks were studied to ascertain the rotational motion.

### Current and future challenges

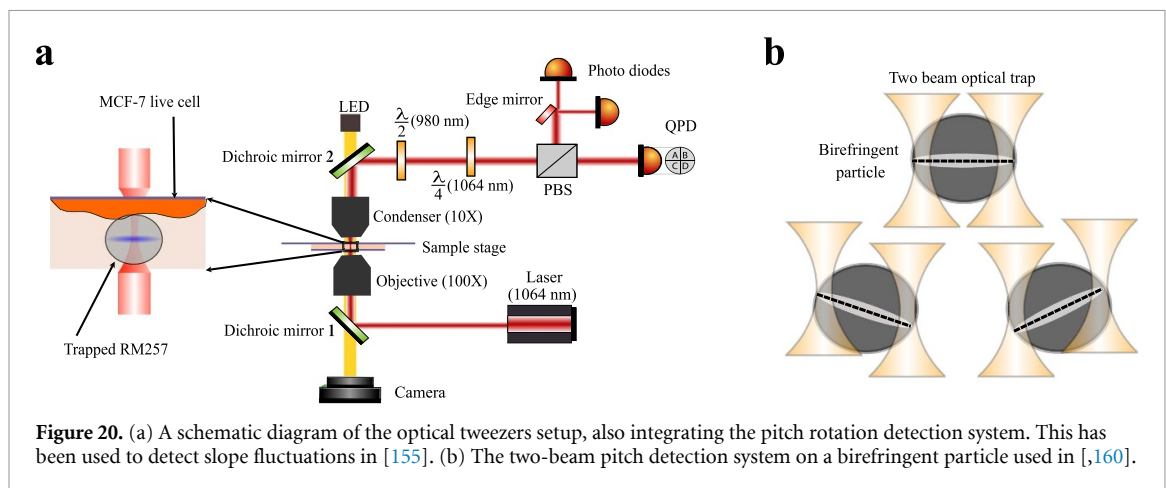
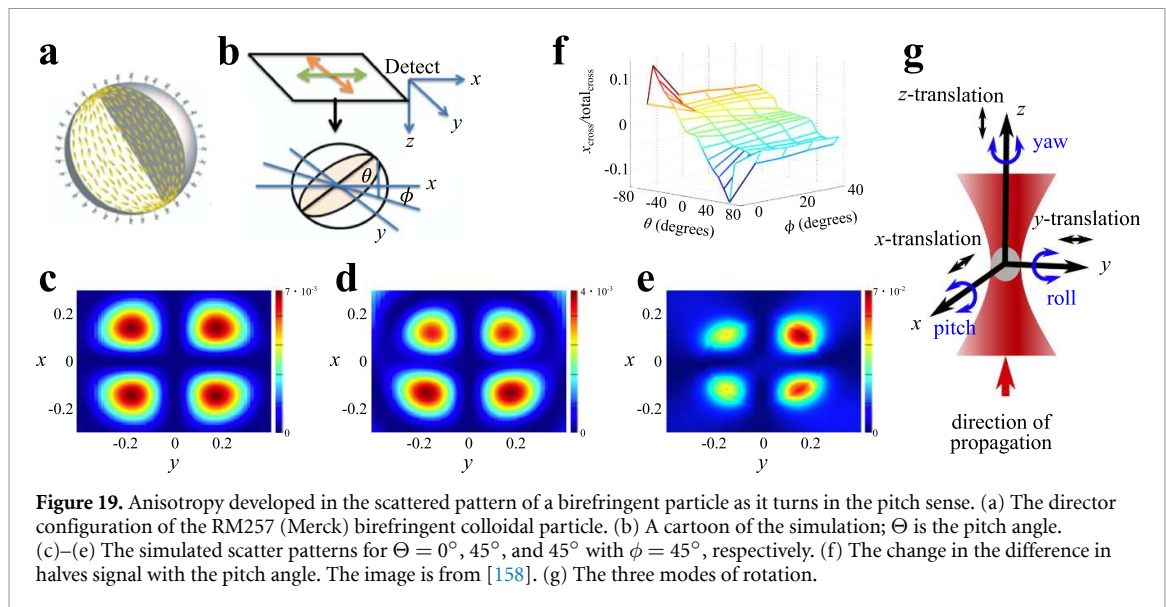
Conventionally, in optical tweezers, the polarization of light was used to generate yaw rotational motion. However, it is not very useful when trying to turn in the pitch and roll sense because it is difficult to generate a single optical tweezers beam, where the polarization rotates orthogonal to the Poynting vector enough. There have been some studies where small ellipticities were generated in the transverse sense with a single beam, but that is hardly enough to spin a birefringent particle where the restoring torque has to be overcome. It is here that other means have to be explored. Nonetheless, the pitch and the roll mode dynamics differ from the yaw mode, particularly in proximity to surfaces. The knowledge of the pitch mode is useful in problems like the study of membrane fluctuations in cells, where one can envisage ‘slope fluctuations’ [155] instead of the normal fluctuations alone, the tug of war between molecular motors, local rheology of the cell cytoplasm [156], and the study of local diffusion of proteins on domains where the pitch angle can provide additional information. It is believed that during the process of endocytosis in a cell, the particle turns. Moreover, interesting information can be obtained when tethers are pulled out of cells, which then twist while contracting.

It is well known that birefringent particles turning under circularly polarized light in vacuum also exhibit pitch and yaw rotations which are all but uncontrolled [157]. If ways can be designed to avoid this rotation, the cooling to quantum states might be more realisable. Moreover, it can be envisaged that out-of-plane rotations can have significant effects when forcing fluids into interfaces when spinning continuously at the microscale.

Molecular motors like kinesin-1 and myosin-5 are known to move in a hand-over-hand fashion while turning. It is believed that both right-handed and left-handed motion is equally possible. One may ask whether that hypothesis is correct, thereby providing valuable insights into the functioning of life at the nanoscale. In an active bath, the correlation between the rotational mode and the translational mode of a spherical particle can provide a wealth of information.

### Advances in science and technology to meet challenges

One of the first attempts at turning a particle in the pitch sense uses two optical tweezers beams in holographic tweezers and moves one of the focal spots to reorient the particle. While this works for anisotropic particles very well and, in some cases, even spherical particles, there is always a possibility that the particle will spin freely. It is for this reason that a scheme was suggested to use a birefringent particle in two trapping beams and then change the position of the focal spot of one beam. The problem with this scheme is that the particle has to be large enough to fit two independent beams. There are other schemes too,



where other means can be used in addition to the confining single optical tweezers beam, like convection currents [159] or magnetic fields in optically compatible magnetic materials, which can even do roll motion [160]. Recently, a scheme was suggested which used two oppositely inclined tweezers beams to generate a pitch spinning polarization configuration [126]. In all these methods, there are two external stimuli used to turn in the pitch sense. One can also put the optically trapped particle onto the stage gently and move the stage parallel to the surface to generate pitch motion [161]. This works for particles smaller than one beam waist of the trapping laser.

To detect the pitch rotational motion, a new scheme was suggested where the anisotropy in the lobes of the scatter pattern between two crossed polarizers for a birefringent particle was used, shown in figure 19. This was used to determine cell membrane ‘slope’ fluctuations [155], a new concept which is derived from the gradient of the normal membrane fluctuations, as shown in figure 20. Here, the anisotropy in the scatter pattern is detected using the difference in halves of a split photodiode. The technique of determining the pitch angle to high resolution can be used in combination with a two-beam rotation generation method on a birefringent particle to realise the optical pitch torque wrench [162]. Using this, one can think of applying controlled pitch torques on surfaces like membranes, which is relevant during situations like cell endocytosis.

### Concluding remarks

The generation and detection of yaw optical torques has been explored extensively over the past 20 years. However, the optical torques in other two degrees of freedom are only beginning to be explored. The pitch rotation was recently detected using the degree of anisotropy of the scatter pattern of a birefringent particle

under crossed polarizers in optical tweezers. This can be used in combination with a two-beam pitch rotation configuration to generate pitch torque wrenches. The roll mode is yet to be explored but a combination of optical and magnetic forces can be a start if the appropriate particles, which can simultaneously be optically confined without heating and bear magnetic properties, are used. Such modes of rotation can have many applications, particularly in proximity to surfaces, when the yaw dynamics vary from pitch and roll.

### Acknowledgments

We thank the Indian Institute of Technology, Madras, India for their seed and initiation grants. This work was also supported by the DBT/Wellcome Trust India Alliance Fellowship IA/I/20/1/504900 awarded to Basudev Roy.



## 15. Direct optical force and torque measurements

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### Status

Force and torque measurements with optical tweezers [1] provide insights into mechanical effects on the microscale in a quantitative manner. Using an optically trapped particle as a probe, ‘photonic force microscopy’ became a prime tool to study, e.g. forces acting on biomolecules such as DNA. The particular strength of optical trapping is its ability to measure forces in the piconewton range.

Originally, force measurements emerged from position measurements that used the deflection of the trapping beam by the particle, for a sensitive but robust detection of particle displacement induced by an external force. The force is then determined indirectly from the displacement [163]. Placing the detector to measure beam position in the back focal plane (BFP) of a lens collecting the transmitted trapping light makes this approach compatible with dynamic optical tweezers. In this configuration, the signal depends only on the relative position between the particle and trapping spot. This method is straightforward to implement, employing a four-quadrant photodiode (QPD) or a position sensitive detector (PSD). As it provides high sensitivity and high temporal resolution, it became the most widely used force-detection method.

Inducing a rotational motion by applying optical torque [122, 164] has many applications, e.g. to measure viscosity in the constrained environment of a cell. More generally, torque measurements provide extra information that is crucial for obtaining a complete notion of the mechanical effects of light, in particular for particles with asymmetric shapes or non-isotropic materials. For such particles, torque measurements turn out to be more demanding due to the larger parameter space (orientation of the particles besides its position) that needs to be covered. Conventional force-detection methods cannot be easily extended to torque measurements, because the sensor signals (from a QPD or PSD) are insufficient to uniquely determine all the components of force and torque. For a continuously rotating particle one can instead resort to observing the periodicity of the motion as a measure of the applied optical torque.

An alternative route to force and torque measurements is provided by methods that directly measure the rate of linear or angular momentum transferred between the trapping light and the particle [165–167], which can be deduced from the change in the angular distribution, or equivalently, from the light distribution in the BFP. The principle is explained in figure 21. As it is based on the conservation of linear or angular momentum, respectively, this method is calibration-free and suitable for particles with arbitrary shapes and unknown optical properties, in complex optical trapping landscapes or in complex micro-environments.

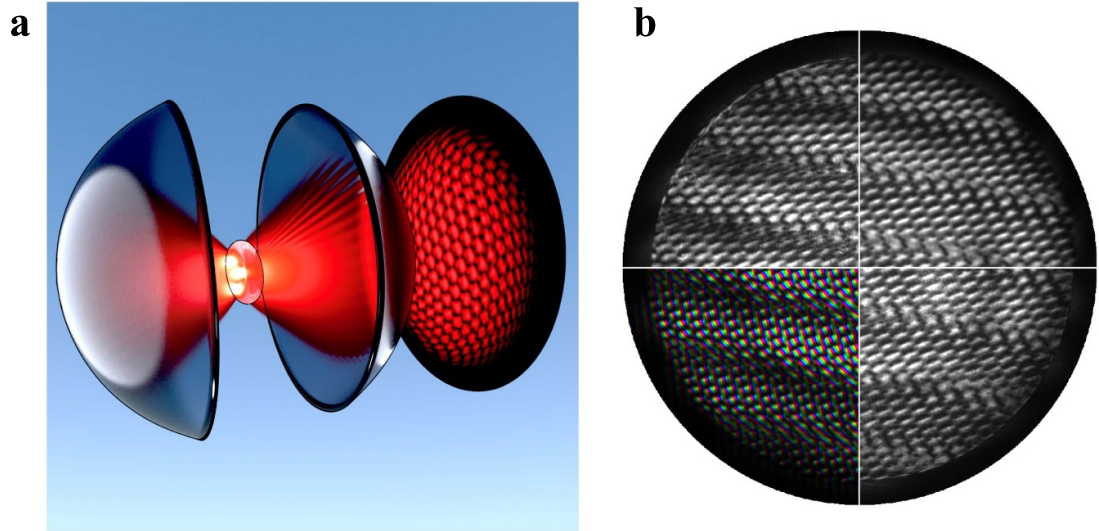
### Current and future challenges

As for any measurement method, the accuracy of the obtained results is a central issue. The indirect position-based force-detection methods require calibration to relate the particle displacement to the force. To this end, a known force is applied. Often thermal forces or drag forces are used, as they can be calculated as long as some parameters, such as the size of the particle and the viscosity of the buffer, are known. In practical applications, however, it is a non-trivial task to obtain these input parameters with good accuracy. Furthermore, statistical data analysis that takes into account all relevant effects requires careful operation [168]. As a consequence, experiments are largely restricted to simple settings, e.g. well-characterized microspheres in water, operated in the linear regime of the trapping potential. Force measurements with biological specimens of unknown or strongly varying properties are still challenging with indirect methods.

Direct force-detection methods do not suffer from these limitations, but to bring into effect the advantage of this method being calibration-free, one has to ensure that sufficiently accurate results are obtained in a broad range of settings. One obstacle is the loss of some of the scattered light, as typically only the trapping light in the forward direction can be detected. For weakly scattering objects (such as cells) this is a minor issue, but for strong scatterers (such as polystyrene beads) one has to take the backscattered light into account [167].

In many applications, in particular in the life sciences, the variability of the specimens and settings demand multiple repetitions of the measurements to obtain valid results. For this, high throughput by parallelizing data acquisition is desirable. However, all methods that analyze the light distribution in the BFP have the issue that, in the far-field, contributions from simultaneously trapped particles overlap, which essentially limits force and torque measurements to the single-particle case. With time-sharing techniques to create the optical traps, which require fast beam steering, this can be extended to sequential force measurements on several particles.

Holographic optical tweezers, which provide highly flexible trapping of many particles, are severely affected by this limitation of conventional force-detection schemes. One possibility to overcome this is



**Figure 21.** The principle behind direct optical force and torque measurement. The schematic sketch on the left explains the basic idea: an optical trapping beam coming from the left is focussed into several trapping spots, some of which are occupied by trapped micro-objects which scatter light. The high-NA condenser lens on the right (sketched as a focussing surface) collects all forward-directed light, scattered and unscattered, and images the resulting far-field interference pattern into its BFP. The interference pattern is captured by a camera, and the phase of the field is retrieved by an iterative search algorithm (propagating the field back and forth between trapping and the focal plane and utilizing knowledge about the position of the trapping spots as a constraint). Using the conservation of linear (or angular) momentum of light, optical forces (or torques) acting on the particles can be inferred, since the difference between the known incoming and the measured momentum that is inferred from the interference pattern constitutes the force (or torque) acting on the particle. It is even possible to find the force or torque on only a specific particle rather than the total force acting on all of them together. The image on the right shows an experimental example of an interference pattern observed in the BFP. The lower-left quadrant is replaced by the phase and amplitude of the reconstructed field (encoded in hue and luminosity) and the upper-right quadrant by the retrieved intensity.

imaging-based position detection, which is, however, sensitive to drifts in the trapping position that may affect the accuracy. Alternatively, holographic force detection [169] measuring the complex field, i.e. phase and amplitude in the BFP, provides complete information about the field. From this one can calculate the field in the focal plane, in essence using Fourier transform. There, particles are separated and individual forces can be determined from the individual scattered fields. Simultaneous measurements for up to ten particles have been realized. While there is no fundamental limit to scale this up to even more traps, an experimental demonstration of highly parallel force measurements for hundreds of particles has yet to be demonstrated.

Torque measurements are still challenging. Current approaches usually rely on the idea of direct measurements: circularly polarized light, which exerts a torque on a birefringent or asymmetric particle, experiences a change in the polarization state, which reflects the torque strength. In a more general setting, the orbital angular momentum of light also needs to be taken into account. This, however, requires measurements that are sensitive to the phase of the light field, e.g. by recording interference patterns [170].

A general concern with the trapping of small particles is the ubiquitous presence of noise due to thermal forces. While it masks other forces and thus limits the obtainable accuracy, thermal motion contains valuable information about, e.g. the trapping parameters.

### Advances in science and technology to meet challenges

Force and torque measurements are essential to obtain complete information about mechanical conditions and, in consequence, to reach full control of optically trapped particles. This includes using feedback control, for which high temporal bandwidth is sought.

High-resolution detection of the scattered light with a camera preserves all the information and thus delivers the highest flexibility. This, however, increases the burden of data processing. Eventually, the maximum frame rate of the sensor places restrictions on the temporal bandwidth, which ideally should reach above the cut-off frequency of the optical trap. Continuous progress in camera technology and computing power, especially of accelerators (GPU, FPGA), will push the limits further up. This needs to be matched by fast algorithms and optimized software implementation that fully employ the available computing resources.

Data analysis requires sophisticated statistical analysis to reveal the sought-after data, often hidden in noise due to thermal motion. Bayesian inference manages to do this in an efficient manner, i.e. requiring a minimal amount of data. There also appears to be a rising trend to utilize methods from machine learning

[87], in particular deep neural networks, for data processing. This could also be helpful for the related task of determining the position and orientation of a particle with an asymmetric shape, as often force and torque measurements are useless without corresponding position information. Unfortunately, with position there is no fundamental conservation law as with momentum.

### Concluding remarks

To date, powerful methods for force and torque measurements are available. Progress is expected to overcome the still existing limitations regarding accuracy and throughput and to broaden the range of applications, in particular for measurements with biological specimens with complex shapes. Force and torque measurement methods should be studied together with methods for position and orientation measurement. Only then a complete picture about important physical parameters, such as material stiffness or the force/extension relationship, is obtained. Furthermore, detailed information about forces together with knowledge of the structure of a specimen will provide insight into internal forces (stress) and induced deformations (strain). From this we expect a huge range of applications in biomedical research. To be successful in this area, simplicity and robustness must be valued.

### Acknowledgments

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## 16. Using Bayesian inference for the calibration of optical tweezers

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### Status

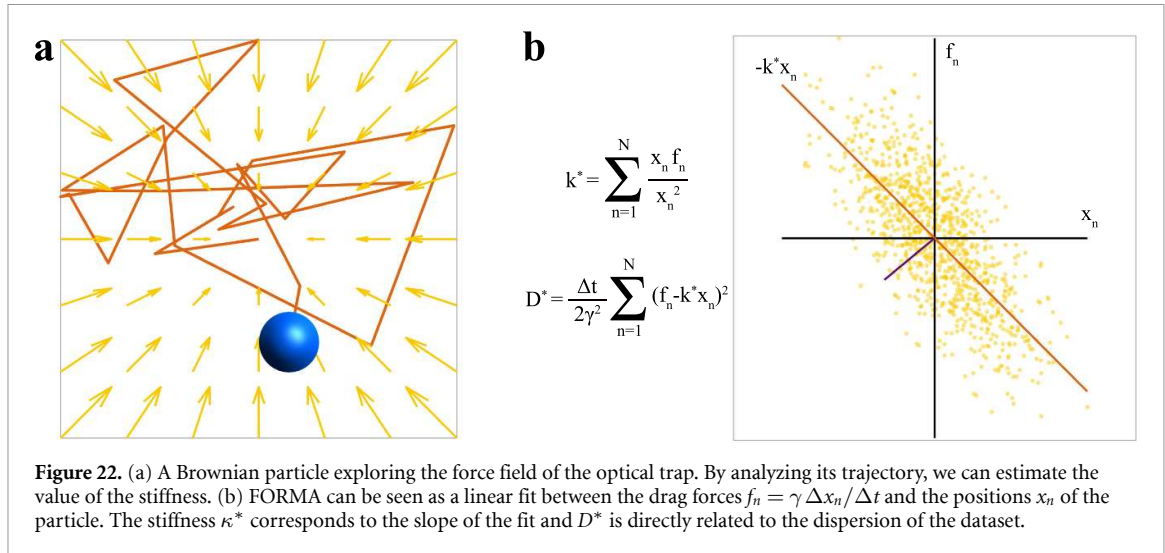
Optical tweezers enable sensing forces in the range from femtonewtons to piconewtons using probe beads to study, e.g. mechanical properties of macromolecules or to explore limits of small thermodynamic systems [16]. Generally, we infer the forces from the response of a trapped bead to the external stimulus by following different mathematical and practical prescriptions that have been developed for more than 30 years since the invention of optical tweezers by Arthur Ashkin.

Calibration methods can be classified as either passive or active. Passive methods rely on the information provided by the Brownian trajectory of a particle trapped in static optical tweezers, while active methods use harmonic time-dependent external forces [171]. There are also direct force-measurement techniques that aim to retrieve optical forces directly from the detection of the change in momentum that light suffers when it is scattered by the probe bead [169]. Here, we will focus our discussion on the passive approach, considering that the introduced concepts can be extended to other techniques. We will also consider spherical probe beads as the main subject. Extensions or generalizations can be found in the references. Also, here we primarily focus on the discussion of calibration in the over-damped regime; nevertheless, it is important to mention that most of the methods mentioned here can be extended to the under-damped regime (see [172, 173] for instance).

At first approximation, only conservative forces are considered. Under this assumption, the Boltzmann distribution is widely used to retrieve arbitrary-shaped potentials under any type of surrounding fluid, such as water, air, or viscoelastic fluids, with only the need for a long-time statistically equilibrated trajectory of the trapped bead. This is a very general approach since it does not depend on the properties of the fluid. When the probe bead is tightly trapped by the optical trap, the force turns proportional to the distance from the equilibrium point of the trap, equal to that of an ideal spring with stiffness  $\kappa_x$ . This regime is of broad interest in most applications where optical tweezers are used as force transducers. Several methods have been developed from this perspective, relying on analytical expressions that account for the main properties of the optical tweezers directly or through model fitting. The equipartition method is the simplest, allowing us to estimate the stiffness directly from the variance of the trajectory of the bead at a known temperature. More sophisticated methods enable estimation of the diffusion in addition to the stiffness. Typically, these include the autocorrelation function (ACF) [174], the mean square displacement (MSD) [174], and the power spectrum density [168]. Based on the long-standing Fourier analysis, the latter comprises a sophisticated methodology that enables analysis in the frequency domain via fast computing routines, making it one of the most popular and reliable methods [16, 168]. The accuracy, precision, and speed to estimate the force of optical tweezers depend on the selected method as well as on the intrinsic noise, frequency sampling, data length, and bandpass filtering in data acquisition.

Today, it is necessary to design methodologies that enable accurate estimates of the interesting parameters as well as their errors in experiments that are conducted in far-from-ideal conditions or within the limits of the accessible technology. For instance, there may be the interest to retrieve general force fields where the non-conservative forces are non-negligible, in systems out of equilibrium or where the potentials are far from the harmonic regime. For this purpose, the incorporation of all the known information of the system, such as the nominal size of the bead and fluid viscosity at room temperature, together with their uncertainties, is relevant to improve estimations.

Recently the method FOrce Reconstruction via MAXimum-likelihood-estimator analysis (FORMA) was introduced, tackling several of these drawbacks: FORMA does not require the potential to be conservative, it is less data-intensive, and its simplicity allows one to perform fast and easy estimations. FORMA uses a maximum-likelihood estimator or, within the context of Bayesian inference, a flat prior, i.e. we do not have *a priori* any knowledge about the parameters of interest (figure 22). However, the BayEsian FOrce Reconstruction (BEFORE) method uses a full Bayesian analysis which, in principle, can incorporate arbitrary prior information that results in an enhancement of the inferred parameters [16].



**Figure 22.** (a) A Brownian particle exploring the force field of the optical trap. By analyzing its trajectory, we can estimate the value of the stiffness. (b) FORMA can be seen as a linear fit between the drag forces  $f_n = \gamma \Delta x_n / \Delta t$  and the positions  $x_n$  of the particle. The stiffness  $\kappa^*$  corresponds to the slope of the fit and  $D^*$  is directly related to the dispersion of the dataset.

### Calibration using Bayesian inference

We will focus on the case of a Brownian particle in a harmonic potential in the over-damped regime. The Langevin equation is then given by:

$$\gamma \frac{dx(t)}{dt} = -\kappa_x x(t) + \sqrt{2D} W_x(t),$$

where  $\gamma$  is the friction coefficient,  $\kappa_x$  is the trap stiffness,  $D$  is the diffusion constant, and  $W_x(t)$  is Dirac delta correlated white noise. Friction and diffusion are related by  $D = \frac{k_B T}{\gamma}$ . For this choice of model, we can derive the probability  $P(\{x_n\}_{n \geq 1} | \theta)$  to observe a trajectory at a collection of measured positions  $x_n \equiv x(t_n)$  based on the model's parameters  $\theta$ .

From  $P(\{x_n\}_{n \geq 1} | \theta)$ , we can either obtain observables and contrast their formulas with experimental measurements or use statistical (Bayesian) inference. Alternatively, we can think of the particle's trajectory as the signal carrying the information of the force field, which is passed through a noisy channel (the thermal bath). In this new light, one can use information theory to reconstruct the optical forces [175]. Indeed, in the first case, the expectation of an observable  $O(\{x_n\}_{n \geq 1})$  is

$$O(\theta) = \int \{dx_n\} P(\{x_n\}_{n \geq 1} | \theta) O(\{x_n\}_{n \geq 1}),$$

which can be used as a model fit to estimate the parameters of interest. This includes, for instance, the MSD and the ACF methods. However, since the statistical content of the force field is richer if we directly consider the particle's trajectory rather than a given observable, we can use Bayes' rule to write down the parameter's posterior distribution, that is:

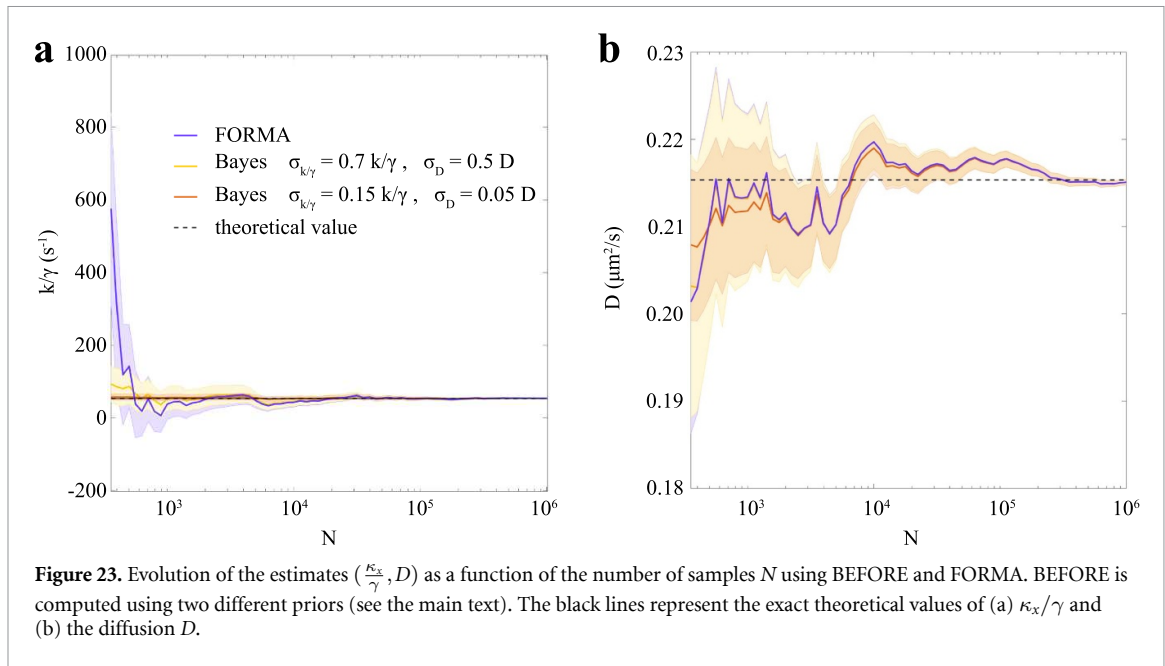
$$P(\theta | \{x_n\}_{n \geq 1}) = \frac{P(\{x_n\}_{n \geq 1} | \theta) P(\theta)}{Z(\{x_n\}_{n \geq 1})},$$

where  $P(\theta)$  contains information of the model's parameters prior to performing an experiment and  $Z(\{x_n\}_{n \geq 1})$  is a normalization factor.

FORMA corresponds to looking for the optimal parameters  $\theta_*$  that maximize the posterior distribution with a flat prior ( $\theta_*$  called maximum-likelihood estimators)  $\theta_* = \arg\max_{\theta} P(\{x_n\}_{n \geq 1} | \theta)$ . BEFORE considers instead a conjugate prior so that the posterior is easily computable and no maximization is needed, retaining all statistical information of the inferred parameters. One can show that using a Gauss-inverse gamma prior distribution, the posterior distribution for the pair of parameters  $(\kappa_x / \gamma, D)$  becomes

where  $\text{InvGamm}(x)$  is the inverse gamma distribution,  $\mathcal{N}(x)$  denotes Gaussian distribution, and the parameters  $\alpha_N$ ,  $\beta_N$ ,  $\gamma_N$ , and  $K_N$  depend on the particle's positions  $\{x_n\}_{n=1}^N$ .





**Figure 23.** Evolution of the estimates  $(\frac{\kappa_x}{\gamma}, D)$  as a function of the number of samples  $N$  using BEFORE and FORMA. BEFORE is computed using two different priors (see the main text). The black lines represent the exact theoretical values of (a)  $\kappa_x/\gamma$  and (b) the diffusion  $D$ .

In case we have no data, that is when  $\{x_n\}_{n=1}^N = \emptyset$ , then the posterior distribution is simply the prior that contains the information we have on the system *before* performing the experiment:

$$P(\kappa_x/\gamma, D)(x, y|\emptyset) = \mathcal{N}(x|K_0, \gamma_0 y) \text{InvGamm}(y|\alpha_0, \beta_0),$$

where  $\alpha_0$ ,  $\beta_0$ ,  $\gamma_0$ , and  $K_0$  are so-called hyperparameters: they must be chosen to reflect the information *a priori* that we have about the physical system. The marginal posterior distributions have a series of advantages as, for instance, all their moments can be obtained explicitly as, for instance, the estimates for  $\kappa_x/\gamma$  and  $D$ . The explicit formulas can be found in [16].

To illustrate the power of this method, in figure 23(a) we show the results of Monte Carlo simulations. Here, we have taken the values of  $\kappa_x = 1 \text{ pN}/\mu\text{m}$ ,  $\gamma = 0.0188 \text{ pNs}/\mu\text{m}$  (thus  $\kappa_x/\gamma = 53.05 \text{ s}^{-1}$ ), and  $D = 0.215 \mu\text{m}^2 \text{ s}^{-1}$ , and discretise the Langevin equation. The sampled position was taken every  $\Delta t = 10^{-4} \text{ s}$ . We have then generated a single trajectory and see how the posterior marginals and estimates evolve in parameter space as a function of the number of samples.

Figure 23(b) shows the evolution of  $\kappa_x/\gamma$  and  $D$ , using FORMA and BEFORE as a function of the number of sampled points  $N$ . To understand the advantages of incorporating *a priori* information of the parameters, we performed two different estimations of BEFORE using two different priors with different levels of accuracy. Hypothetically, we assume *a priori* information to be taken by normal distributed random variables,  $\mathcal{N}(53.05 \text{ s}^{-1}, \sigma_{\kappa_x/\gamma})$  and  $\mathcal{N}(0.215 \mu\text{m}^2 \text{ s}^{-1}, \sigma_D)$ . The error bars in FORMA correspond to the asymptotic value of the error when  $N$  is large [16]. As the number of points in the trajectory increases, providing the method with more data, the inferred parameters improve accordingly. From this figure, as better information is provided, faster and more accurate estimations are retrieved from BEFORE. This contrasts sharply with FORMA and any other existing method, for which neither *a priori* information can be incorporated nor the whole posterior distribution of the parameters is obtained.

### Current and future challenges

As the uses of optical tweezers evolve and the variety of phenomena explored increases in complexity, the accuracy of experiments becomes more challenging. Moreover, some attention has been paid to time-dependent processes, where the stiffness of the trap might change over time and the trajectory of the particles is shortened. In some experiments, optical potentials might not be harmonic, resulting in the system not reaching its equilibrium state. The study of living matter with optical tweezers has also brought additional challenges as the conditions of the surrounding fluid might not be ideal and the imaging of beads may be affected by the inhomogeneity of the living tissue, compromising, in turn, the quality of the data set.

### Advances in science and technology to meet challenges

As we mentioned, the implementation of better statistical algorithms will enable the extraction of more information from a given data set. One important aspect here will be to assess the uncertainty coupled to a



measurement based on certain conditions and availability of information. This will not only give us a more reliable way to quantify the precision and accuracy of an estimate but also could reveal core aspects of the behaviour of the particles under the influence of optical tweezers, such as the production of entropy and the irreversibility of stochastic processes.

### Concluding remarks

More general methodology that accounts for subtle forces in far-from-ideal conditions using all the information at hand is provided by the Bayes' rule (BEFORE). Here, we gave a brief introduction of BEFORE that illustrates the applicability and its conceptual advantages in the calibration of optical tweezers. We showed how the entire information of the parameter's distribution is retrieved, and how valuable *a priori* information can be incorporated to obtain faster and more precise estimations.

### Acknowledgments

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## 17. Optical tweezers calibration with deep learning

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### Status

The analysis of microscopic force fields is crucial for a wide range of experiments, including optical tweezers, DNA stretching, and nonequilibrium physics [1]. This analysis is usually made by modelling the force field using various parameters that are estimated using particle trajectories. This information can then be used to understand the underlying dynamics, to predict a future state of the system, or to calibrate the experimental setup. The calibration of such systems sometimes needs to be performed in real-time [176]. The most well-studied example is the force field of optical tweezers, where the force has the form  $F = -kx$  (where  $k$  is the stiffness of the harmonic trap and  $x$  is the distance from equilibrium). For this case, there are many standard calibration methods that already exist, such as the variance method, autocorrelation method, and power spectrum methods [1]. The variance method directly determines the stiffness from the variance of the particle position in the trap ( $k = k_B T/x^2$ , where  $k_B T$  represents the thermal energy). The autocorrelation method determines  $k$  by fitting the decorrelation curve of the particle position in the trap. The power spectrum method is also a powerful method, especially at high frequencies, which fits the power spectrum of the Brownian particle to a Lorentzian and infers the stiffness. All these standard algorithms work well when the measurements contain sufficient data points and are error free [1]. More efficient standard algorithms include linear maximum-likelihood methods [177] that apply a linear regression, which makes a first-order approximation to the force around the equilibrium point. This allows more accurate and faster calibrations of force fields compared to standard algorithms [177], as well as the ability to calibrate non-conservative force fields, such as a rotational force field.

### Current and future challenges

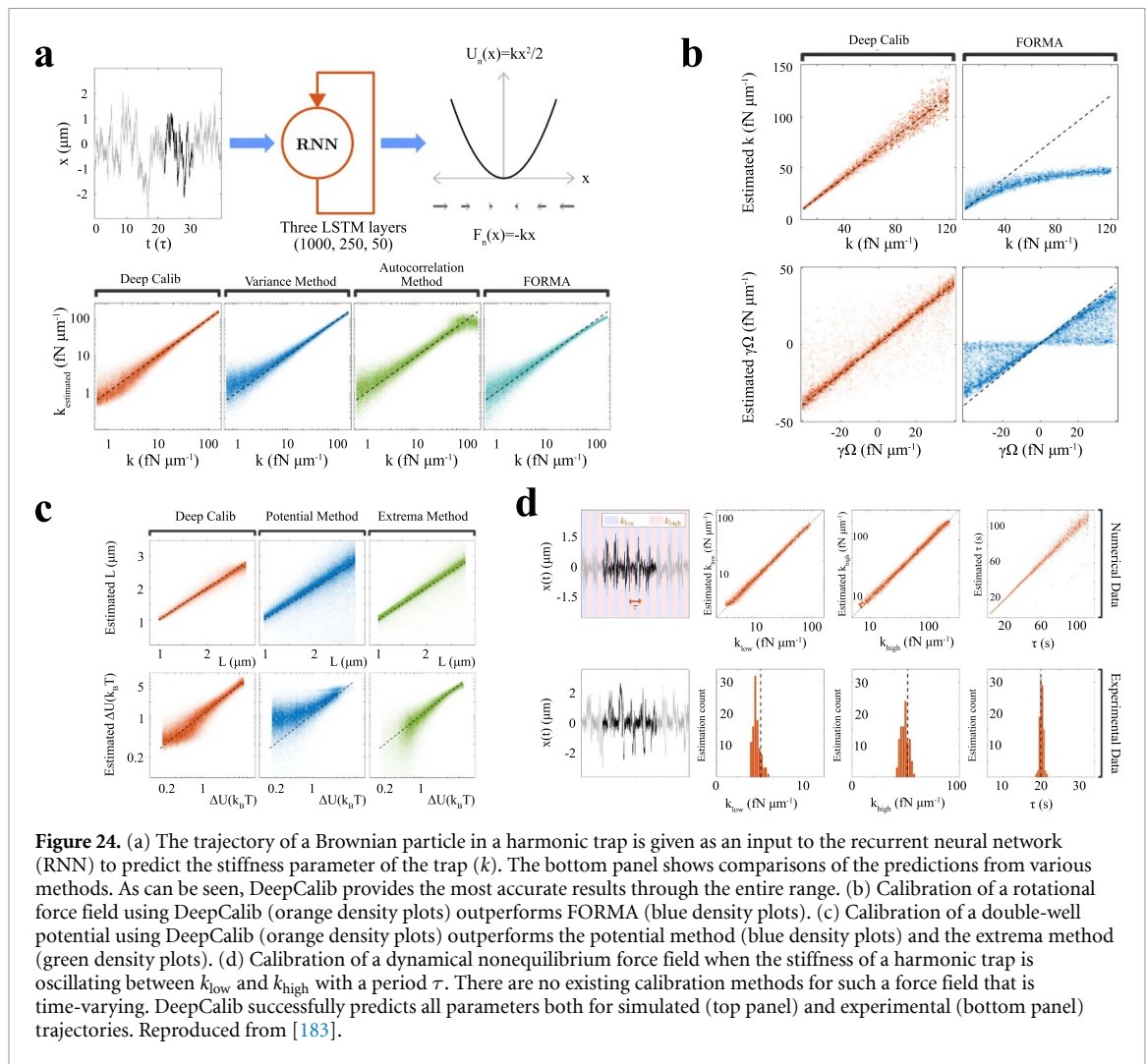
As microscopic environments are stochastic, the calibration methods require more data for higher accuracy due to the need for averaging. If there is enough statistical information in the data, averaging of displacements provides accurate force measurements [178]. However, this is often not possible in biophysics. Moreover, the available calibration techniques for non-standard force fields are very limited. Examples include non-harmonic potentials, rotational force fields, and dynamic nonequilibrium force fields. As the number of parameters that is to be estimated from a trajectory increases, the amount of data required for an accurate measurement grows exponentially for complex potential landscapes. Although maximum-likelihood algorithms, such as FORMA, can do better in these potential landscapes, they only work if the data acquisition has high frequency and the force field is not time-varying.

There are also experimental setups which need real-time calibration if the system is subject to change or degradation over time. Examples of such systems are forces generated by electrodes inside liquid environments, chemical forces, and bacterial forces.

There are also challenges in the field in data acquisition. The more advanced techniques allow faster and more accurate particle localization. Specifically, the advancements in photodetectors have recently improved single-particle tracking and enabled trajectory measurements at very high frequencies [179]. In addition, the advancements in data-driven image analysis methods facilitated the possibility of enhanced image analysis [180, 181].

### Advances in science and technology to meet challenges

While the need for more advanced calibration methods for experimental setups increases, data-driven analysis methods, such as recurrent neural networks, have become known as a very powerful tool to extract information from time-series data. This has led to the development of DeepCalib [182], a free software package that uses deep neural networks to calibrate force fields from trajectories. Specifically, DeepCalib uses long short-term memory (LSTM) layers to extract information from trajectories and uses simulated data to train the neural network. Particularly for shorter trajectories or smaller force values, when the calibration is challenging, DeepCalib is proven to work better than other algorithms for harmonic potential, as shown in figure 24(a). In addition, DeepCalib can accurately calibrate non-conservative rotational force fields better than the existing methods. In this case, the force field has two parameters, the central force stiffness  $k$  and the rotational parameter  $\Omega$ . Although it is accurate for lower values of the  $k$ , FORMA struggles at higher force values because the data points become uncorrelated. DeepCalib is able to estimate the parameters of the force



**Figure 24.** (a) The trajectory of a Brownian particle in a harmonic trap is given as an input to the recurrent neural network (RNN) to predict the stiffness parameter of the trap ( $k$ ). The bottom panel shows comparisons of the predictions from various methods. As can be seen, DeepCalib provides the most accurate results through the entire range. (b) Calibration of a rotational force field using DeepCalib (orange density plots) outperforms FORMA (blue density plots). (c) Calibration of a double-well potential using DeepCalib (orange density plots) outperforms the potential method (blue density plots) and the extrema method (green density plots). (d) Calibration of a dynamical nonequilibrium force field when the stiffness of a harmonic trap is oscillating between  $k_{\text{low}}$  and  $k_{\text{high}}$  with a period  $\tau$ . There are no existing calibration methods for such a force field that is time-varying. DeepCalib successfully predicts all parameters both for simulated (top panel) and experimental (bottom panel) trajectories. Reproduced from [183].

fields better than FORMA, as shown in figure 24(b). The difference in DeepCalib becomes more easily visible as we look at more non-standard cases, such as a double-well potential. Here, the force field is parametrized by the equilibrium distance  $L$  and the energy barrier height  $E_B$ . As shown in figure 24(c), DeepCalib provides more accurate results when predicting the parameters of a double-well potential. Finally, and most importantly, DeepCalib can calibrate any force fields, such as time-varying force fields that yield a dynamical nonequilibrium system. In this case, a harmonic potential with switching stiffness from  $k_{\text{low}}$  to  $k_{\text{high}}$  with period  $\tau$  is considered. It is shown in figure 24(d) that DeepCalib can very accurately calibrate all the parameters of a short trajectory for such a challenging case, both for numerical data and for experimental data. It is also shown that DeepCalib is more robust than the standard algorithms against measurement noise, diffusion gradients, and reality gap [182].

### Concluding remarks

With the introduction of DeepCalib, it becomes evident that a data-driven, neural network approach for the calibration of microscopic force fields outperforms the standard methods in challenging conditions and limited available data. More importantly, DeepCalib can be applied to non-conservative or time-varying force fields where no standard calibration methods exist. With these advantages and the great robustness to measurement noise, inhomogeneous environments, and reality gap between experiments and theory, DeepCalib is a very powerful and flexible tool for analysing trajectories to extract the force fields. It allows for just a minor change in the code to immediately adapt to a new force field, while standard techniques totally change if a different force field is considered. Therefore, DeepCalib is ideal for the calibration of complex and non-standard force fields from short trajectories and it is readily available as a free Python software package [184]. It also proves that the recurrent neural networks are a very powerful tool to analyze Brownian

trajectories. Similar techniques have also been applied, for example, to characterize anomalous diffusion trajectories, and have also been shown to be very powerful [[183](#), [185](#)].

### Acknowledgments

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## Microrheology

### 18. Microrheology for quantitative non-invasive mechanical measurements

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#### Status

Optical-tweezers-based microrheology has emerged as a powerful tool to measure the local mechanical properties of soft viscoelastic materials in a minimally invasive way [186, 187]. Unlike other rheological methods, such as atomic force microscopy or bulk rheometry, measurements are not just limited to the surface of a material or require large volumes. Therefore, applications range from measurements of biopolymers [186] to the determination of local mechanical properties inside living systems like cells [187] and even whole organisms.

In general, there are two distinct forms of microrheology, as illustrated in figure 25. Passive microrheology is the most common due to its experimental simplicity [188]. The position of a probe particle, embedded inside the material, is monitored using video microscopy or laser interferometry. In thermodynamic equilibrium, particle fluctuations are purely due to thermal motion and can be linked to the complex shear modulus  $G^*$  using the generalized Stokes–Einstein relation [188]. Due to relatively small displacements, this method is prone to experimental drift and general noise-related errors. Additionally, it is fundamentally limited to passive systems that remain in thermodynamic equilibrium during the full measurement period. Recently, great scientific effort has been devoted to active systems, such as living cells, which introduce, beside the thermal fluctuations, an additional active motion on the probe particles [187, 189]. This active component is interesting as it allows one to understand general active systems and also renders passive microrheology as performed today unusable because the activity breaks the thermodynamic equilibrium. Active microrheology, in contrast, circumvents these limitations [186, 187]. Here, optical tweezers are used to apply well-defined, typically oscillating forces to the particle. At the same time, the particle position is observed. This can be done using the same laser, an additional detection laser, or video microscopy. The ratio of particle displacement and force yields access to the response function  $\chi^*$  of the material from which, in turn, the complex modulus  $G^*$  can be deduced. As it is less susceptible to experimental noise and able to quantify even active and soft nonlinear systems, this method has become the standard approach to investigate the local mechanics of living systems [187]. Furthermore, comparing the resulting mechanical properties to the spontaneous fluctuations of the free system allows direct quantitative access to the active forces acting on the probe particle [190].

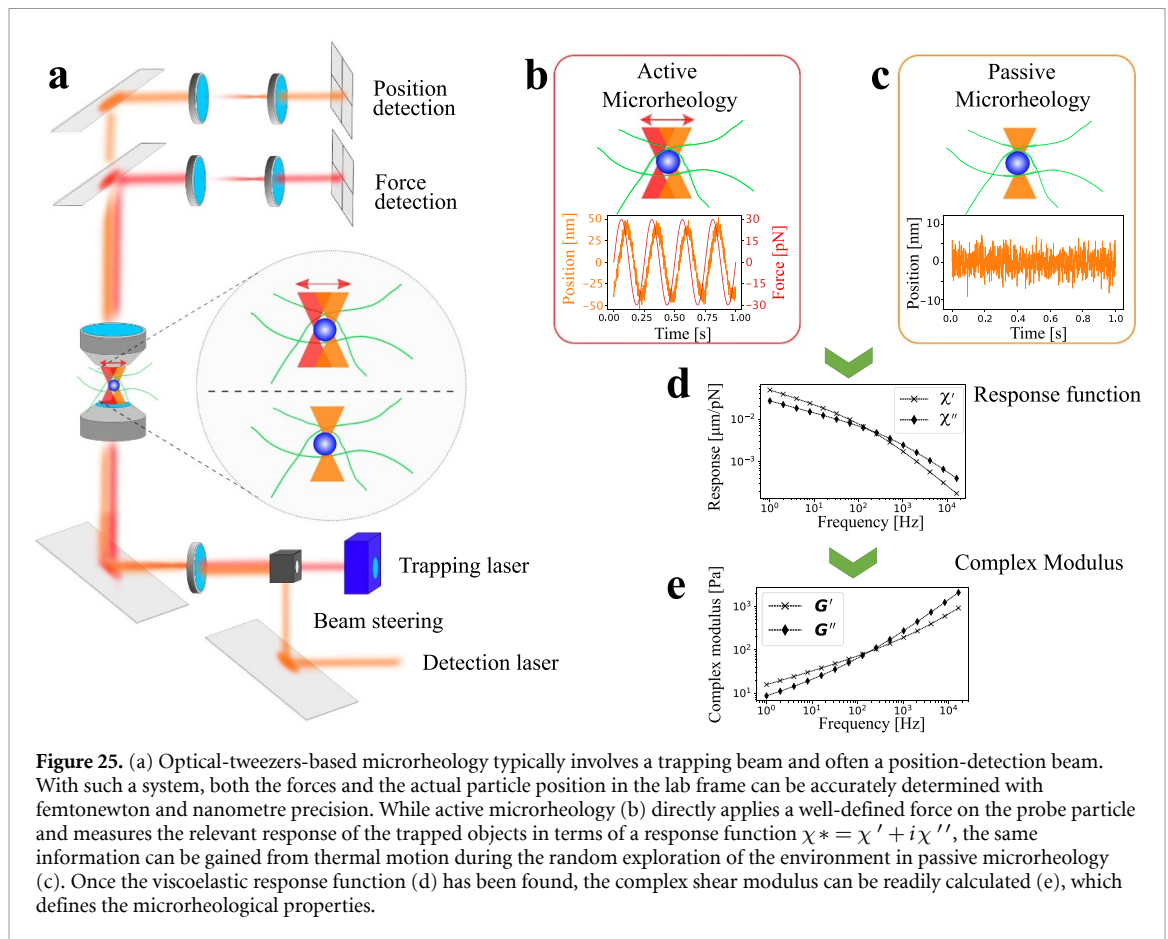
Understanding active but also nonlinear microscopic systems is among the most pressing problems that hinder our advancement in the generation of complex smart materials, and also in the quantitative description of complex and fast-changing systems like biological and artificial cells.

#### Current and future challenges

One major challenge in microrheology measurements is the instrument's complexity. The limited availability of commercial systems and the specialist skills and knowledge required to run optical-tweezers-based microrheology measurements puts it in a scientific niche. Additionally, since particle deflections in the nanometre regime are measured, these setups are extremely sensitive to noise. Mechanical vibrations (e.g. from camera cooling fans), stage drift, electronic noise, and temperature fluctuations all disturb these highly sensitive measurements. As the overall optical forces are limited, only soft materials of up to approximately 1 kPa can be measured. Furthermore, microrheology experiments have a limited throughput as only single particles are trapped at a time. Also, since the optical pathway of each measurement position is unique, the optical trap needs to be calibrated at each measurement position.

A second challenge lies in the measurement of materials with a nonlinear stress–strain relationship. In the past, there has been an increasing appreciation of the importance of nonlinear mechanical responses, which are ubiquitous in nature. However, with few exceptions [191], all reported optical tweezers microrheology experiments are performed in the *linear* regime, i.e. a mechanical regime, where the measured stiffness is independent of the applied strain. The reason for measuring the linear regime is two-fold. Firstly, the trap stiffness, limited by laser power and sample heating [192], does not allow large deformations and secondly, the theory for analysing data is only valid for small deflections.

A third challenge is a fundamental limitation of the measurement of living matter, namely its ability to adapt to external stimuli at sufficiently long time scales. Microrheology measurements that induce slow deformations thus do not measure a mechanical response function, but rather cellular adaptation. Infinitesimal small deformations would not stimulate the cell, but would also not provide a signal in



inherently noisy systems. In addition to deformations, local heating induced by the optical trap affects cellular behaviour.

A fourth challenge is that, although objects that are larger than the trapping wavelength (or radius of the trapping focal point) can be trapped, force measurements are not possible since the assumed linearity between force and bead displacement does not hold. This might be solved using the momentum transfer method, as in [187].

Hence, the main challenges are related to experimental complexity, measurement precision, and force generation.

### Advances in science and technology to meet challenges

The roadmap to improve or even overcome these current limitations can be drawn by a mixture of technical improvements, which are mostly already within reach. The force limitation can be improved by two approaches. Firstly, using 800 nm lasers reduces the heating in an aqueous environment by almost one order of magnitude if compared to the typically used 1064 nm lasers [192]. Unfortunately, in the 800 nm regime, only expensive Titan Sapphire lasers are available at the required power of more than 1 Watt. The introduction of a more powerful near-infrared laser at a wavelength of about 800 nm with high-quality beam profiles would immediately increase the reachable optical forces in the non-heating regime by an order of magnitude. Secondly, this can be further enhanced by protocols that allow the generation of probe particles with higher refractive indices. Unfortunately, such particles would inherently lead to an increase in reflection, which can only be overcome by anti-reflection coatings that are achieved by refractive index gradients [29].

To gain access to the nonlinear regime, relevant for many contemporary questions, again, the force application capacities of tweezers are the main hurdle. Firstly, the nonlinear stiffening often leads to mechanical properties that are not testable anymore with the common 100–200 pN forces, and require several nN. Hence, so far active optical-tweezers-based nonlinear microrheology has only been carried out in soft DNA gels [191]. Besides deforming the material to the nonlinear regime using the tweezers itself, the systems can also be prestressed.

A further improvement will be systematic multiplexing of the lasers, thus allowing multiple measurements in parallel to overcome the drawback in throughput. Using high-speed beam steering, this is



already possible [193]. Multiplexing also enables two-particle microrheology [194], which allows the determination of force propagation in complex and structured materials.

Another approach to overcome the limited measurement efficiency would be fully automatized approaches, where the system will rapidly and automatically switch from one probe bead to the next one. This would not only allow one to increase the measurement statistics, but also to observe mechanical changes over a long time, for example in cells during migration or differentiation. Such automation approaches are currently under development, but might require the use of deep learning approaches to correctly identify suitable probe particles.

A final way to boost microrheology would be to extend the current theoretical analysis methods of passive fluctuation observation, which mostly rely on equilibrium thermodynamics. Recent approaches, like the observation of broken detailed balance, have opened new directions to extract the active forces from simple passive measurements. More refined and general approaches here would allow one to perform high-speed video tracking to directly access the viscoelastic material properties and active forces in driven nonequilibrium systems.

### Concluding remarks

The potential of optical-tweezers-based microrheology has not yet been unleashed, but to gain a substantial advancement of the method, it needs to become more accessible to a wide number of potential users. An outstanding potential for future experimental breakthroughs lies in an automated user-friendly system, which could ideally be even commercially available and exploits 800 nm high-mode-quality lasers. Such systems would pave the way for high throughput and local characterization not only of simple passive materials, but also of currently engineered smart materials, as well as living biological and active biomimetic systems. In particular, characterization of the viscoelastic transitions within such materials with high temporal and spatial resolution is only possible using optical-tweezers-based microrheology, making it the relevant tool for local characterization. Hence, if the field manages to follow the here-suggested roadmap, optical-tweezers-based microrheology has the potential to become the main method for quantitative cell biology, as well as the key characterization tool for the currently emerging fields of active and smart materials.

### Acknowledgments

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## 19. Active microrheology

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### Status

The evaluation of the response of a material to an external mechanical stress is of utmost importance, both in fundamental research and in industrial product development [195]. Indeed, the study of rheological properties, namely viscosity and elasticity, allows one to obtain fundamental information about both the material structure at the microscopic level and the characteristics of the involved molecular bonds. In recent years, considerable attention has been devoted to the development of microrheometers, i.e. devices able to evaluate the response of small volumes of materials (in the range of nano- or pico-litres). This fact is particularly relevant for biomaterials, as an example, or when dealing with samples available in small volumes because of their cost or their low reproducibility. In addition, microrheometers allow one to investigate the material response with high spatial resolution, helping to understand the supramolecular organization and mesh-size of network-structured materials.

Active microrheology techniques are based on the insertion of microprobes in the material under test. Such probes are moved under the effect of an external force that induces a local stress  $\sigma$ , i.e. a force per unit area. Rheological properties can be inferred by recording the relative material response in terms of strain, i.e. the amount of deformation, and the strain rate.

Magnetic or optical forces [196] are ideally suited for this application because they can be applied on the probe without physical contact (thus not modifying the medium under test), and their intensity and spatial distribution can be controlled with high precision. In particular, the exploitation of optical forces was pushed by the development of micro-opto-fluidic systems, which have been largely investigated and developed in the last decade [197]. Opto-fluidic chips, based on the integration of microfluidic channels and optical waveguides on the same substrate, offer the chance to develop miniaturized microrheometers in which the optical force is applied by counter-propagating (and diverging) beams. We note that optical systems for active microrheology can rely either on focused-single-beam optical tweezers or on counter-propagating (and freely diverging) beams [198]. In the first case the beads are usually moved by exploiting the gradient component of the force whereas, in dual-beam tweezers, the motion is determined by the scattering component of the optical force. The latter configuration, as will be shown in the following, can provide several benefits for rheology applications, making this method highly versatile and well suited for a wide range of materials [199].

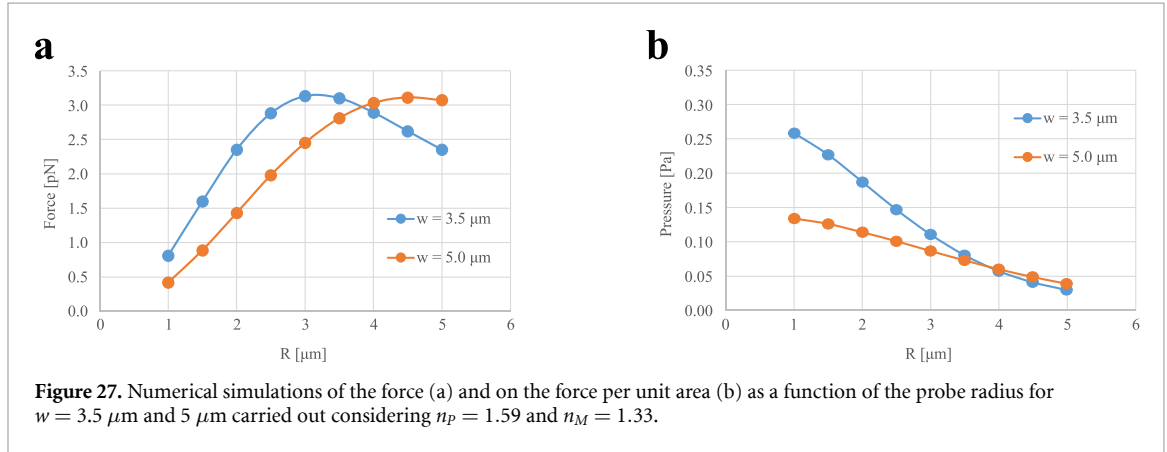
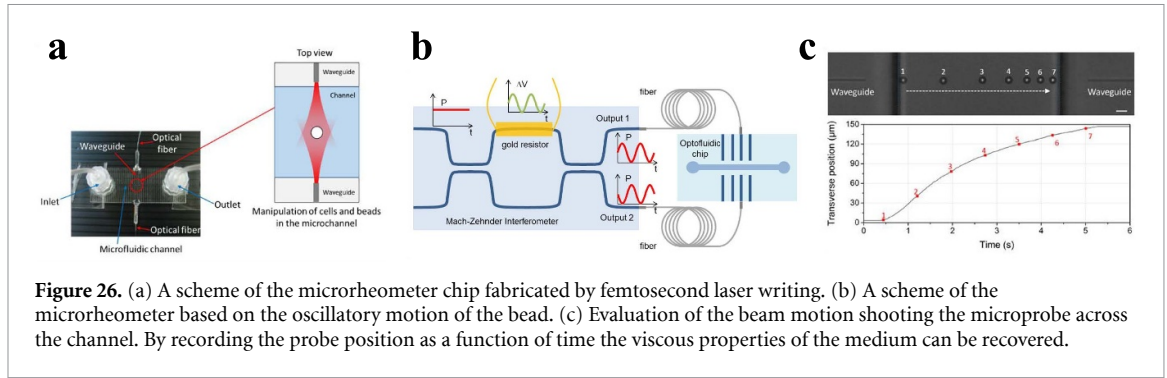
In figure 26, we show the basic scheme of a microrheometer, fabricated in fused silica by femtosecond laser writing [200]. The laser beams emitted by the two opposite waveguides are used to trap one microprobe immersed in the fluid under test (beam power  $\approx 1$  mW). By unbalancing the power levels of the two beams a net force is exerted on the bead: its motion along the channel is dependent on the optical force spatial profile and on the fluid viscoelastic properties. Two different kinds of measurements can be performed:

- (i) Using an external modulator it is possible to periodically unbalance the optical power coupled to the waveguide. With this approach a time-varying optical force and the consequent microprobe oscillation is induced, thus mimicking the behaviour of oscillatory rheometers [201]. By recording and analysing the bead motion both the elastic and viscous response of the fluid can be recovered.
- (ii) By trapping the microprobe close to one side of the microchannel, and then abruptly decreasing the power emitted by the waveguide on the opposite side, it is possible to 'shoot' the microprobe across the microchannel [199]. The measurement of the probe motion provides information on the viscous response of the fluid.

The integrated microrheometer has been initially validated by characterizing well-known fluids, such as water-glycerol mixtures, providing very reliable results. The potential of the system has then been confirmed by accurately measuring the regimes of the mechanical response of non-Newtonian fluids, such as DNA hydrogels and yield stress materials [202, 203].

### Current and future challenges

The exploitation of the scattering component of the force ( $F_S$ ), instead of the gradient component ( $F_G$ ), offers several advantages for rheological measurements. Indeed, in the large particle regime optical force can



be obtained by decomposing the optical beam into rays, and then by calculating the scattering and gradient force components ( $F_S$  and  $F_G$ , respectively) for each ray [8, 204]. The forces exerted on a spherical particle of index  $n_p$ , immersed in a medium of refractive index  $n_M$ , by each optical ray are given by the following equations:

$$F_S = \frac{n_M P}{c} \left\{ [1 + R \cos(2\theta)] - T^2 \frac{[\cos(2\theta - 2\gamma) + R \cos(2\theta)]}{[1 + R^2 + 2R \cos(2\gamma)]} \right\}$$

$$F_G = \frac{n_M P}{c} \left\{ [R \sin(2\theta)] - T^2 \frac{[\sin(2\theta - 2\gamma) + R \sin(2\theta)]}{[1 + R^2 + 2R \cos(2\gamma)]} \right\}$$

where  $P$  is the power carried by each ray,  $c$  is the light velocity in vacuum,  $R$  and  $T$  are, respectively, the reflection and transmission Fresnel coefficients that consider an optical ray forming an angle of incidence  $\theta$ , and with a refraction angle  $\gamma$  inside the particle. By summing up the forces due to each ray the overall  $F_S$  and  $F_G$  for the whole beam is calculated. It is important to point out that by increasing  $\Delta n = n_p - n_M$  the scattering force grows monotonically, while the gradient force displays more complex behaviour and can even be reversed in high-refractive-index particles.

Moreover, the graph reported in figure 27(a) shows the dependence of the optical scattering force exerted by a freely propagating Gaussian beam (power 10 mW, waist  $3.5 \mu\text{m}/5 \mu\text{m}$ ) on particles with a radius varying from 1 to  $5 \mu\text{m}$  and positioned immediately at the waveguide output. It can be easily observed that choosing a radius comparable with the bead size provides the conditions of maximum applied force, at the same time maintaining a good trap stability in the transversal direction. Meanwhile, figure 27(b), reporting the pressure (stress) applied by the particle on the external medium, shows that reducing the probe size allows a significant increase in the applied stress, although this is paid for by a reduction in trap stability.

In a fully integrated device, due to the excellent spatial and temporal control over force application an optimal trade-off can be obtained between these constraints. Force intensity up to 1 nN, with good trapping stability, has been demonstrated, also making possible the reliable investigation of the viscoelastic properties

of a vast class of materials in a nonlinear viscosity regime. As an example [203] reports the results obtained on an aqueous suspension of packed, swollen microgels, a well-studied example of simple yield stress fluids.

### Advances in science and technology to meet challenges

Different scientific and technological advancements could largely contribute to the opening up of new scenarios in optical microrheology.

1. The versatility of the microrheometer is strongly dependent on the range of stress that can be applied to the fluid. Higher stress calls for high optical power coupled to the microfluidic channel (up to 2 W were used for yield stress materials, producing a stress of  $\approx 1$  Pa). Therefore, a great limitation is now given by propagation losses of the on-chip waveguides that are reported in the  $\text{dB cm}^{-1}$  range. Moreover, a major source of power loss in the currently available systems is due to the coupling losses between optical fibres, used to carry the laser radiation from the source to the chip, and the integrated waveguides. This can be ascribed to optical mode mismatch between the two guiding structures, other than coupling misalignments.
2. The integration of tunable lenses on-chip could enable one to focus the optical beams down to the desired size and position, enabling better spatial control in the measurement and optimizing the trap's strength and stability. Although the integration of tunable lenses is quite challenging, it must be highlighted that different approaches for the realization of microfluidic lenses are currently being tested and considered in the scientific literature, even if for different applications.
3. Exploitation of high-index microbeads could sensibly increase the applied stress for a given optical power, thus also decreasing the limitations associated with thermal effects that can in principle hinder the measurement. With the state of the art, the availability of high-refractive-index ( $n > 2$ ) microbeads that are transparent in the 980–1070 nm range is quite limited, but it must be noted that the described configuration theoretically allows one to use probes with  $n_p$  up to 5 (a value much higher than that usable with focused-beams optical tweezers) without losing the trapping effect, while largely increasing the applied scattering force.

### Concluding remarks

Integrated microrheometers based on a dual-beam laser trap constitute a new class of devices able to provide low sample consumption while ensuring excellent calibration and measurement repeatability, as no alignment of optical components is required, in contrast with microscope-based optical tweezers. Additionally, due to the possibility of using high-index beads, and to the lack of beam focalization, the constraints imposed by localized sample heating are extremely relaxed with respect to standard configurations.

By combining these aspects, the reported microrheometers ensure an unprecedented versatility, making it possible to carry out stress-controlled active measurements, in both the linear and nonlinear regime, on a wide range of materials, from aqueous polymer solutions and soft gels to stiffer materials, thus opening the way to the development of low-cost, miniaturized, and largely automated microrheometers.

### Acknowledgments

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## Trapping nanoparticles

### 20. Optical trapping of nanostructures

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#### Status

The trapping of nanostructures within the field of optical trapping is long established. The original 1986 optical tweezers paper devotes much of its attention to the limitations of the new 3D trapping technique, and demonstrates trapping of a 26 nm diameter silica sphere, with clear predictions that smaller particles should be feasibly trapped as well. These ideas were quickly taken forward by Ashkin and Dziedzic to explore biological material in the form of tobacco mosaic viruses, with a diameter of around 20 nm but a length of about 3  $\mu\text{m}$ , hence trapping nanorods for the first time and setting up a discussion around the role of the shape and size of trapped particles, as well as initiating the use of optical tweezers in the biological sciences.

This early work quickly progressed from the trapping of dielectric particles, which had been considered optimal due to their low scattering cross sections. Svoboda and Block [205] demonstrated that, in the nano-regime (here around 35 nm), metallic and dielectric particles had comparable scattering properties, but as the metallic particles had much higher polarizabilities, trapping was stronger.

Work building on these early ideas has mushroomed in the subsequent decades, and there is a plethora of target particles in a range of fields, spanning nanotubes and nanowires, made from polymers, glass, semiconductors, and graphene among others, through to more conventional particles made from more exotic materials, such as diamond, quantum dots, and up-converting material [206]. Trapping has been demonstrated in liquid media, in air, and in vacuum, and has been shown to enable the creation of nanoparticle clusters. Near-field approaches, such as plasmonic nanotweezers, moving away from traditional free-space optical tweezers, have also made significant demonstrations in this area.

Applications of nanoscale trapping have become increasingly viable with the development of these approaches, making use, for example, of naturally occurring nanoparticles. These have included exploring subdiffusion dynamics inside cells, trapping inside living organisms, assembly of nanowire devices using holographic tweezers, and probing quantum limits using vacuum-trapped nanoparticles.

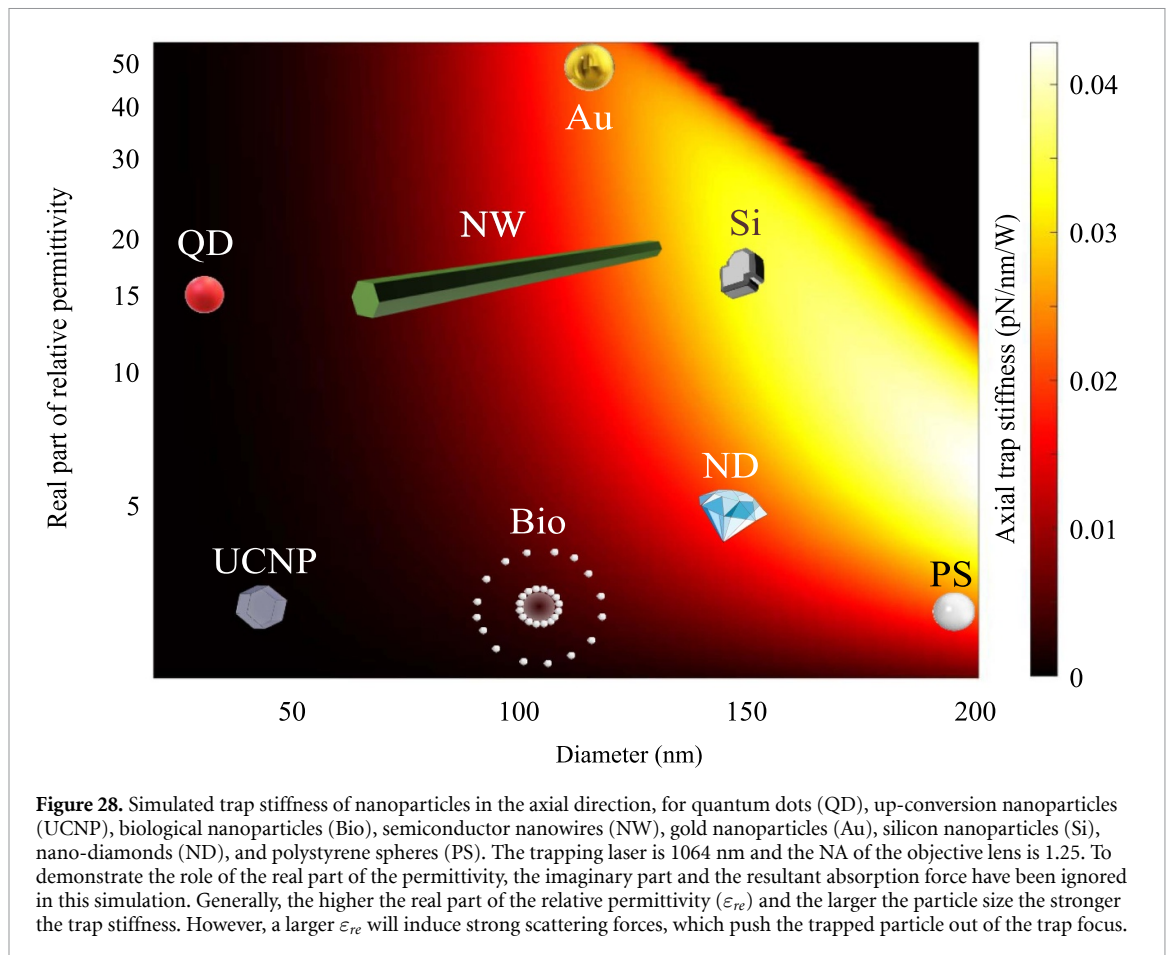
The push in recent years has been in research aimed at functional nanoscale optical tweezers, aiming to probe truly nanoscale phenomena, within cells, for example, and to make use of the properties offered by the nanoparticles themselves to seek new opportunities in imaging, rheology, magnetic field sensing, temperature sensing, and as a means to explore quantum effects in bulk materials, such as optical cooling. Hybrid approaches, utilizing optical fields to induce other effects, such as thermal forces, have also received attention.

#### Current and future challenges

These advanced functional nanomaterials expand the sensing ability of optical tweezers, yet there are still important issues concerning trapping efficiency and manipulation capabilities, which currently hinder the progress in this field.

Generally, higher relative permittivity and a larger size lead to stronger trap stiffness (figure 28). Nanostructures mostly come at the price of small polarizability ( $\propto$  volume), limiting their trap stiffness. Optimal performance can be achieved using metallic nanoparticles ( $\approx 50$  nm) but, typically, to obtain stable trapping, one might use  $\approx 100$  mW power in the near-infrared and the heat generated prevents sensitive biological measurements [207]. Other types of nanoparticles, including biological nanoparticles, have lower trapping efficiencies due to their smaller refractive index ( $\approx 1.4$ – $1.5$ ). Near-field optical trapping, including evanescent field trapping, plasmonic trapping, and photonics hot-spot trapping, have a demonstrated potential for trapping nanostructures, especially for low-index materials; however, the trapped probe is usually located in a fixed position or within 2D, losing the 3D manipulation capability.

The low polarisability of nanostructures leads to a low scattering cross section, which prevents the use of traditional scattering detection to measure the trap stiffness, limiting the capability of systems for real-time position tracking, particle localization within the trap volume, 3D force detection, and particle metrology. It also poses a challenge for the detection of single-particle trapping events, as the particle sizes are well below the diffraction limit.



Intracellular trapping nanostructures for sensing and studying the interaction between nanoparticles with organelles has the potential to lead to new insights in cell biology. However, the intracellular trapping environment can make direct application of tweezer technologies difficult. In particular, when nanostructures enter a cell via endocytosis, they will be encapsulated by a vesicle, leading to aggregation, changing the trapping properties, and destroying the functionalized particles' surface. Another challenge of intracellular trapping is that the cytoplasm has a higher refractive index and viscosity than water, decreasing the efficiency of trapping probes. The high laser power required to overcome the lower trapping efficiency may heat and damage the organelles.

The manipulation capability of nanostructures, for example, to control the trapping orientation of nanoparticles remains a challenge. Multispot holographic optical tweezers have been demonstrated to orient micrometre-long nanowires; however, orientation control of asymmetric nanostructures with nanometre-size dimension is currently limited to polarization effects, and predominantly 2D trapping. Finally, due to the diffraction limit, the laser trapping spot is usually about ten times larger than nanoparticles, limiting the trapping efficiency and the trapping confinement area.

#### Advances in science and technology to meet challenges

Enhanced polarisability of materials is one of the key tools for increased optical forces and for extending the trapping limits at the nanoscale. Highly polarisable materials, including semiconductors (e.g. Si, GaAs), are suitable candidates that can avoid issues with heating. High-index dielectrics can also exhibit geometric resonances (e.g. Mie resonances) that can further improve trapping efficiency [208]. Beyond this, new mechanisms that enhance polarisability, for example, Zeta potential [209], super-radiation [210], the ion resonance effect [211], and plasmonic shells [212], may be employed to enhance the effective gradient force. Hybrid trapping schemes that incorporate fluidic or thermal forces can also be highly effective for nanoscale trapping [213].

Engineering the physical geometry of particles has been profoundly successful in micrometre scale trapping and micromanipulation. With, for example, two-photon polymerization or other lithographic processes, shape optimization has been used to enhance forces and torques, and to enhance force detection. Nanoscale lithography can similarly be useful for structuring objects of particular sizes and shapes that can



be used for control orientation. Nanolithography will also be advantageous in bringing uniformity to objects that may otherwise have substantial size dispersion. Other types of nanostructures have natural shapes that will maintain a fixed orientation in a trap. These can also be exploited in certain applications. The alternative to particle engineering is optical beam shaping, to optimise the optical potential, an approach which has to date shown more promise for larger particles over nanoparticles [27]; advances in approaches using point spread engineering are likely needed to enable flexible nano-trapping approaches in the future.

High-fidelity detection of forces and positions is essential for force-sensing applications. The challenge when extending back focal plane interferometry is the need to detect a diminishingly small signal in a strong background. Calibration of position detection from individual objects is also essential, as the variability in size can be substantial ( $>10\%$ ), even in the most well-controlled fabrication processes. With the smaller particles also comes faster Brownian motion, meaning that both sensitivity and bandwidth need to be maintained. Fluorescence-based methods are a viable alternative and, in certain circumstances, also solve the individual sizing issues. Bespoke detection schemes that enhance the measurable signal also hold much promise. Detection of orientation for anisotropic particles will also be important. Total force-sensing approaches avoid the problem of force calibration but, for strongly scattering objects, both forward and backscattered light need to be recorded for accurate determination.

Finally, localization remains a key challenge. Trapping volumes in gradient force tweezers generated by diffraction-limited optics are necessarily large compared to the nanoparticle dimensions. Therefore, whilst confined, the nanoparticles are free to move within this space. One possibility for reducing the nanoparticle motion is to use laser-based cooling, which suppresses the Brownian motion [214]. Whilst there are opportunities to create smaller trapping volumes, using, for example, super-oscillations, it is near-field geometries, such as plasmonic nanostructures and photonic crystal cavities, that can deliver truly nanoscale trapping volumes with reduced power requirements. The progress of near-field trapping towards advanced applications requires the development of a number of auxiliary functions, such as reconfigurability for translation, 3D position detection, and integration with the intended application; enabling technologies, such as metaoptics [21], will help advancement across all these areas.

### Concluding remarks

In summary, the field of nanoscale trapping is very much still an open and active area of research. The delivery of new technologies and approaches will be crucial in unlocking the full potential of the trapping of nanostructures and their intended applications. These innovations will come from the application of new materials, nanoscale engineering techniques, novel trapping techniques, and bespoke detection schemes and beam shaping.

## 21. Optical nanotweezers

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### Status

Optical trapping [9], recently recognized with one-half of the 2018 Physics Nobel Prize, has emerged as an important tool in biology and life science by providing the means to manipulate biological objects and measure forces associated with biomolecular interactions. In standard optical tweezers, a tightly focused laser beam is used to exert strong gradient forces to stably trap microscopic specimens near the laser focus. However, the diffraction limit precludes propagating light to be focused to subwavelength volumes, thus preventing stable trapping of nanosized objects ( $<100$  nm). Evanescent electromagnetic fields in the vicinity of optical nanoresonators have the capability to scale optical traps down to the nanometre scale. This is achieved by spatially confining the light field to deeply subwavelength spots, while enhancing the local light intensity. Furthermore, the high sensitivity of nanoresonators to minute perturbations of their close surroundings offers a convenient way to track the trapped specimen dynamics by monitoring small changes in the resonant light. Different approaches, based on plasmonic resonances [215] in noble metals, Mie resonances [216] in high-refractive-index low-loss dielectric or semiconductor materials, and dielectric photonic crystal cavities [217], have enabled one to extend optical trapping beyond what conventional optical tweezers can do, ultimately reaching the single-molecule level (figure 29) [218].

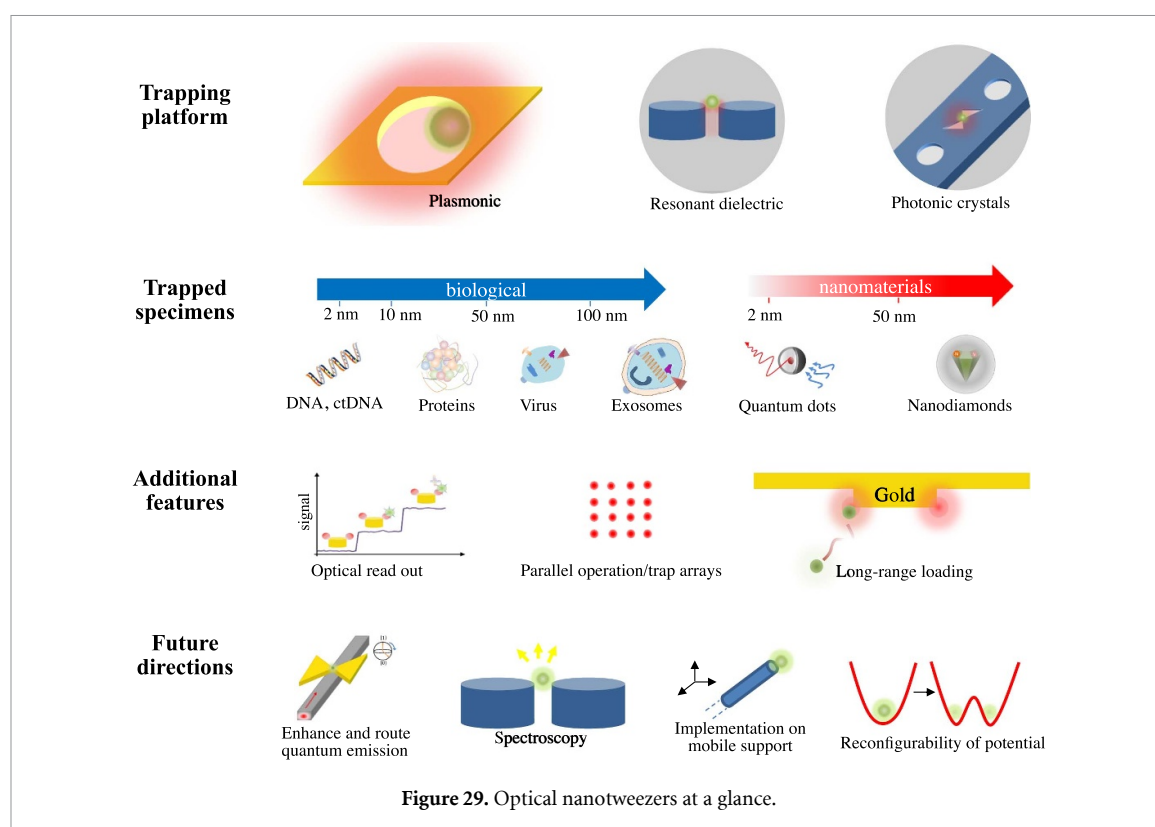
### Current and future challenges

Despite their clear potential, optical nanotweezers have not yet become a transversal enabling tool used by researchers from other communities to address scientific questions. This is in part due to several remaining challenges related to trap loading, 3D manipulation of the trap object, and photothermal heating.

- (i) *Trap loading*—while near-field optical potential enables one to extend trapping to nanometric specimens, their subwavelength confinement raises the practical challenge of efficient trap loading. One default approach relies on Brownian diffusion but it suffers from being slow and non-deterministic. The applicability of nanotraps is conditioned by the availability of controlled methods to deliver the specimen to the trapping site. A high loading throughput is desired for systematic experiments and to reach statistically relevant data.
- (ii) *Material losses*—depending on the operating wavelength and the choice of material platform, optical losses can become a limitation. First, they lead to a local temperature increase which, if excessive, can alter the integrity of sensitive specimens like biological systems. Additionally, temperature gradients also introduce other dynamics, such as buoyancy-driven fluidic convection, increased Brownian motion, and thermophoresis. For instance, when repulsive, thermophoretic motion can reduce the overall trapping stability. Another consequence of optical losses is the broadening of the resonance bandwidth, which can limit the efficiency of feedback-based trapping mechanisms like the SIBA effect [219], as well as of the readout of the specimen dynamics.
- (iii) *Control over the trapped specimens*—while most efforts so far have focused on new nanophotonics platforms capable of pushing trapping to smaller sizes down to the single-protein level, the field would greatly benefit from further control over the trapped specimen. In particular, accurate 3D manipulation would enable a controlled interaction with other systems, relevant, for instance, to the assembly of nanomaterials or molecular interaction. Furthermore, reconfigurability of the trapping potential would open up new opportunities in the study of complex nanoscale dynamics or collective effects in trap arrays.

### Recent advances and future prospects

The past decade has seen substantial research activities on new optical nanotweezer approaches to address the aforementioned challenges in the field. Capitalizing on recent advances in nanophotonics, all-dielectric optical nanotweezers can overcome the photoheating effect present in their plasmonic counterpart. While Mie resonances provide lower field enhancements, the reduced temperature rise drastically reduces any influence of fluid convection, Brownian motion, and thermophoresis, and thus relaxes the optical trapping potential requirements for stable trapping. For example, silicon nanoantennas achieved stable trapping of



20 nm dielectric spheres, while ensuring a negligible temperature rise of 0.04 K [216]. One exciting future direction to further relax the trapping laser power requirement with negligible heat generation and narrow bandwidth resonances involves harnessing non-scattering anapole modes or bound states in the continuum in all-dielectric resonators [220].

With respect to dynamic particle loading and dynamic manipulation, hybrid approaches that combine optical and RF electric fields offer a solution to mitigate the need to rely on slow Brownian diffusion and achieve fast transport of particles to the nanotrap. For example, a recent paper reported opto-thermo-electrohydrodynamic tweezers [221] that harness the balance between optically induced electrothermoplasmonic flow and AC electro-osmotic flow to initiate long-range transport and trapping of single protein molecules away from the high-intensity laser focus to mitigate photothermal damage.

The use of optical nanotweezers to simultaneously perform trapping and sensing of small molecules and biomolecular interaction has also generated enormous interest. For example, aperture optical nanotweezers have been shown to be capable of measuring antibodies binding to proteins, proteins binding to DNA, and small molecules (such as drugs) binding to proteins [222], which may find applications in understanding the pathogenesis of diseases and for antibody screening. Also, they have lately proved practical to monitor fast conformation dynamics of single proteins and tackle biological questions, which could not be addressed even when using very sophisticated characterization techniques.

Another important future direction is to combine nanoscale optical trapping with spectroscopic techniques, such as Raman, fluorescence, or infrared absorption, to probe the biochemical properties of trapped objects at the single-particle level. Such a capability is particularly attractive for single extracellular vesicles (EVs) analysis towards understanding the heterogeneity of single nanosized vesicles, such as exosomes and exomeres.

Last, but not least, when integrated at the extremity of a mobile support, optical nanotweezers are also promising for deterministic positioning of single quantum emitters to nanophotonic cavities for generation and manipulation of the non-classical light on-chip [223]. The use of optical nanotweezers combined with rapid electrothermoplasmonic loading may help overcome the challenges of limited scalability and throughput of atomic-force-microscopy-based manipulation.

### Concluding remarks

Optical nanotweezers are crucial towards the isolation, manipulation and interrogation of nanoscale objects. Future developments will benefit from the latest advances in nanophotonics, enabled by all-dielectric

nanostructures, and a combined use of other non-optical forces, as well as from an extensive engineering effort to turn them into a more accessible technology, readily available to other scientific communities.

We envision that optical nanotweezers will significantly impact both biological sciences and the nanoassembly of heterostructures, for instance, within the context of quantum photonics. In biology, they offer new opportunities to gain a further understanding of the interaction between biological molecules or to monitor single-molecule responses to external controls. In the fast-growing field of EVs, optical nanotweezers could enable one to trap and analyze individual nanosized EV populations to further understand the impact of heterogeneity on EV molecular cargo content and function. Within the context of quantum technology, we envision that optical nanotweezers could play a key role in the assembly of integrated hybrid quantum photonic circuitry, as well as in the development of compact levitation systems for optomechanics and ultrasensitive force sensing [223].

## 22. Optomechanical manipulation of nanodiamonds

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### Status

Diamond is a hard, ultrastable, and non-toxic material that is chemically inert. These properties together with the possibility of efficient surface functionalization make nanodiamonds (NDs) an ideal bio-compatible agent for conducting advanced biological studies [224]. NDs also exhibit strong optical activity, both in Raman scattering and through embedded fluorescent molecular complexes. They can host a multitude of optically active colour centres, such as nitrogen-vacancy (NV) and silicon-vacancy (SiV) centres, which provide direct sensing modalities to the surrounding thermal, magnetic, and electric fields [225]. Finally, diamond has a high refractive index of about 2.4 and a low absorption in the visible and infrared spectrum, allowing strong optical confinement and manipulation, while minimizing heating or damage to the surrounding environment. Ultimately, the combination of all these properties makes NDs containing optical defects a powerful tool for applications as fluorescence markers in biology as well as nanoscale sensors in liquid environments [224].

The NV centre in diamond holds a prominent position in quantum technology, as it is a robust room-temperature spin system with optically addressable and readable spins [224–226]. Many proposals investigate their potential within the context of hybrid quantum systems, suggesting the coupling of NV spin degrees of freedom to the motional degrees of freedom of a high-Q mechanical oscillator, realized, for example, through a levitated ND in vacuum [225, 227]. Such hybrid systems could be employed for foundational tests, such as for probing the boundaries between classical and quantum physics and exploring the realm of quantum gravity [228].

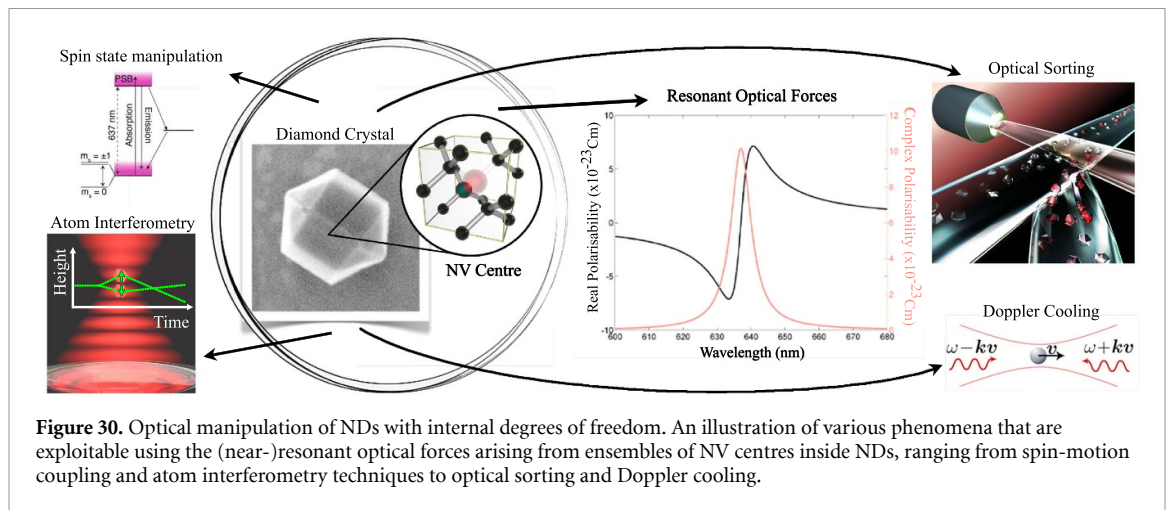
Ensembles of optically active colour centres in NDs offer enhanced optical forces due to their atomic-like polarizability [225]. Analogous to dipole traps in atomic physics, the associated forces with colour-centre resonances are wavelength and state-dependent, allowing the toolbox of atom trapping to be applied to the manipulation of a mesoscopic object, as illustrated in figure 30. Uniquely, the colour centres are concentrated on a length scale much smaller than the wavelength of light, enabling cooperative effects to play a significant role [210]. This goes well beyond the typical atom-trapping context. Addressing the internal degrees of freedom might also enable optical cooling methods from atomic physics to be applied to a mesoscopic levitated object. Yet, at this point in time, a number of important challenges related to the interplay of trapping lasers, colour centres, and the diamond material itself remain unsolved.

### Current and future challenges

Two key challenges for unlocking the full potential of optically trapped NDs lie in the understanding of the photo-physics of the different colour centres within a strong optical trapping field and determining the interplay of material impurities with the laser light [225].

Controlling material purity is paramount in optical trapping as embedded defects can induce strong trap-laser absorption causing heating of the particle [227, 229]. As mentioned previously, a key requirement for many of the aforementioned levitation proposals is that the NDs must be trapped in ultrahigh vacuum to ensure the highest possible Q factors, and to minimize decoherence arising from background gas collisions. The removal of gas collisions, however, eliminates conductive cooling leaving radiative cooling as the only mechanism for heat loss. Hence, whilst diamond has a high thermal conductivity, it is of no use in this regime. Further, being optically transparent in the near-to-far-infrared, diamond has low emissivity and therefore exhibits minimal radiative cooling. Without a mechanism to lower the internal temperature of a levitated nanoparticle, NDs have been reported to heat up and eventually burn or graphitise below  $\approx 20$  mBar due to the absorption of the trapping light by defects and impurities on the surface and inside of commercially available NDs [229].

Adding to the challenge of material purity, understanding the interplay between the unwanted ND impurities and the desired colour centres is essential for optimizing the optical and spin properties of the ND system [225, 230]. Traditionally, the NV centre is considered as a stable, optically addressable, and readable spin system. However, when involving an additional trapping laser, the optical and spin dynamics of the NV centre as a whole are impacted heavily by the surrounding NV centres and the surrounding impurities, as well as all of the bound surface charges. These interactions lead to many undesirable effects, such as blinking, heating, fluorescence quenching, ionization, spin depolarization, and spin decoherence, which all diminish or fully suppress the desirable properties of the NV centre [231].



Finally, unlike silica spheres, which can be made to a high degree of purity and uniformity, NDs typically come with large variations in size, shape, and composition/colour-centre concentration. This is eminent since observations of different NV centre samples have exhibited contradictory effects [231], to the point where dramatic differences in optical properties within a single sample have been observed [210]. Size variations lead to strong variations in the trapping strength and asymmetric/nonspherical shapes can strongly enhance the noise in experiments and lead to unwanted complex in-trap dynamics, such as rotation and libration. Furthermore, many of the aforementioned detrimental effects are exacerbated by the lack of ND particle consistency in terms of colour-centre concentration, which limits the ability for systematic study and analysis of each contributing effect.

#### Advances in science and technology to meet challenges

Due to the potential opportunities and the anticipated impact of exploring trapped ND systems with optical defects, significant effort has been devoted to overcoming the aforementioned challenges. The different approaches can be summarized into four distinct groups.

The most obvious approach and ultimately the most ideal avenue in the long term is material engineering, i.e. to comprehensively study, analyze, and grow ND material under better-controlled conditions [230]. Significant work has already been undertaken to analyze the charge donor and acceptor effects arising from surrounding impurities on the spin dynamics of NV centres in NDs [225].

One promising approach for addressing the strong variability in ND material properties is the sorting of ND samples according to specific desirable criteria [232]. Passive size sorting based on mechanical methods (routinely used for nanoparticles) can be combined with sorting according to colour-centre concentration. The latter sorting modality again relies on the exploration of optical scattering forces arising from the (near-)resonant complex polarisability of NV centres (figure 30). Ultimately, it might even be possible to sort NDs according to their radiation (quantum) properties, such as the degree of cooperativity [210].

Meanwhile, a number of research groups are putting up with the existing ND material but instead are applying *in situ* experimental techniques to mitigate some of the negative effects of the trapping laser on the spin-optical properties of the NV centres. Fast gating of the trapping laser has been demonstrated, which enables the ND–NV spin sensor to be manipulated and read out during the dark intervals of the gated trapping light [231]. Trapping with 1550 nm light demonstrably reduces the detrimental effects of the trapping laser, although this does not entirely eliminate the problem [227]. Typically, these approaches only solve a single issue and are more a band-aid than a complete elimination of the root cause.

Lastly, there is also the possibility of using alternative optical defects for various proposals [225]. Whilst NV centres are the most prominent defect in diamond, there are more than 500 optically active diamond defects, each with their own individual optical, magnetic, and spin properties. The most prominent are SiV centres and germanium-vacancy centres [230]. Yet, many of the more intrinsic material-related issues persist for those defects too. Finally, other optically active nanoparticles, such as nanorubies or rare-earth-ion-doped nanocrystals, might offer a viable alternative for the realization of advanced levitation proposals.

#### Concluding remarks

Overall, combining NDs with embedded optically active defects and optical trapping has become a robust tool in biological applications, now routinely used in the community. Material improvements, such as better uniformity in terms of ND shape and colour-centre concentration, might enable a completely new regime of



experimentation, where optically trapped NDs could enable quantitative fluorescence measurements. NDs with engineered colour-centre content could enable the precise and externally controlled mapping of nanoscale magnetic and thermal fields, e.g. in living cells.

Understanding the complex interplay of the diamond matrix and the internal charge dynamics is key to the realization of better ND oscillators and, as a consequence, successful implementation of a number of optical levitation proposals that would enable experimentalists to build hybrid quantum systems and advanced sensors capable of probing the boundaries between classical and quantum physics and quantum-gravitational effects.

## Acknowledgments

This work was funded in part by the Australian Research Council (ARC) Centre of Excellence for Engineered Quantum Systems (CE110001013) and through an ARC Discovery Project Grant (DP170103010). C L is a Sydney Quantum Academy (SQA) Fellow and acknowledges support through the SQA.

## 23. A label-free approach to seeing individual biomolecules and their interactions

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### Status

In 2012, the optical trapping of a single protein was demonstrated using a double-nanohole (DNH) in a metal film [218], as shown in figure 31. The protein, bovine serum albumin, showed natural conformational switching between open and closed states in the trap, as confirmed by changing pH and forcing the protein into the open state. Compared to other works that looked at the folding dynamics of proteins [233], the DNH approach was tether-free and label-free. The optical tweezer held the protein in place, so no tether was required. The label-free attribute, however, really makes this technique transformative.

Labels change the nature of the biomolecule. They are expensive, finicky, and they give an indirect signal. They limit the observation time to the lifetime of the label and limit the speed to the rate at which photons can be counted from the label [233]. While they have advanced our understanding profoundly, many are looking to new label-free approaches, such as iScat [234] and NEOtrap [235], to analyze biomolecules in their native state. The DNH (or more generally shaped-aperture) approach may become a standard tool in single-molecule biophysics, drug discovery, and antibody screening.

Using the DNH tweezer, it has been possible to measure antibodies binding specifically to proteins, proteins binding to DNA, small molecules (such as drugs) binding to proteins, and many other protein interactions [236]. It is possible to measure the affinity of these interactions, which is important for drug discovery, antibody screening, etc. These affinity studies are possible at equilibrium and on a single protein—very little sample is required. We have worked on unprocessed samples, which shows potential for speeding up analysis, removing expensive purification steps, and looking at active processes in real time: e.g. looking at the secretion products from individual hybridoma cells in real-time antibody screening.

The shaped-aperture approach has been combined with nanopores, which directs the protein/biomolecule to the aperture [237], for studies of both weak and strong interactions with immunotherapy targets [238, 239]. The tweezer also solves the overly fast translocation problem of nanopores. It is simpler, however, to use the tweezer without the nanopore (and vice versa), and simplicity often trumps performance. The shaped-aperture allows one to literally watch proteins work. There are no other ways of doing this, allowing unprecedented observations of all the states involved. It is possible to watch a single protein for many hours, but with a time resolution that is limited only by the detector speed (i.e. the application is not photon-starved).

### Current and future challenges

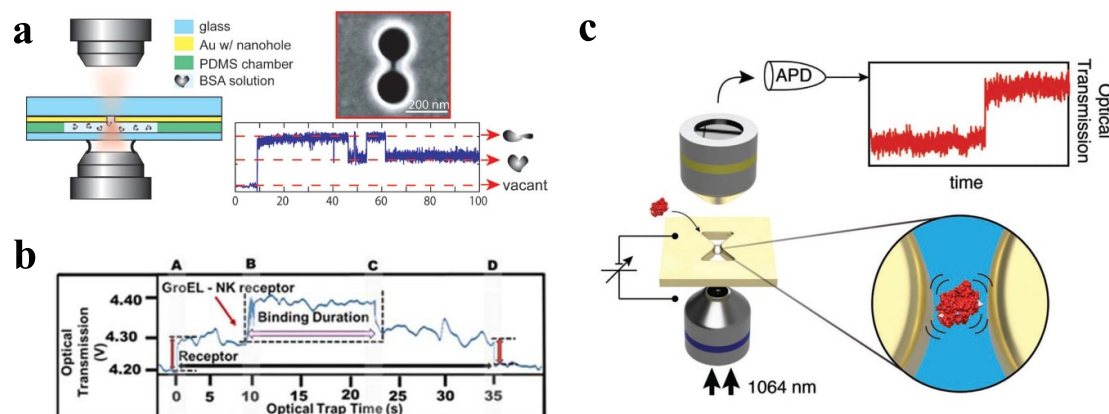
Significant effort has been spent on developing the protein trapping technique since 2012 [218]. A common challenge with any new technique is that there is a healthy level of scepticism for these approaches. Since 2019, however, other groups have demonstrated the application to biomolecules in the single digit nanometre range, so this challenge is now resolving [218, 233–239].

Considering the promise for applications in drug discovery, antibody screening, and single-molecule biophysics in general, the main remaining challenge is ease-of-use. The approach combines three fields: nanotechnology, laser tweezers, and biochemistry. It is complicated. Widescale adoption of this approach will likely require a simplification and a combination of the laser-tweezer and the nanotechnology parts. In this way, biochemists in academia and industry can treat those parts as a single ‘black-box’ and focus on probing biomolecules and their interactions.

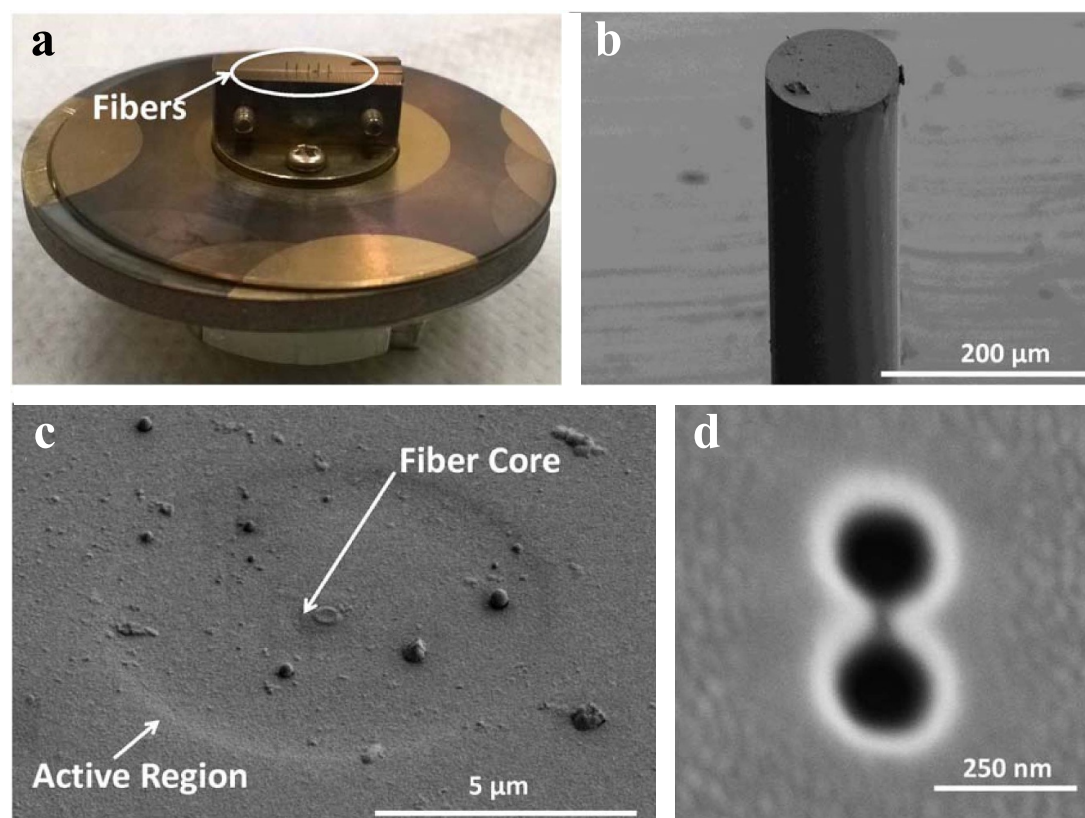
A second challenge is heating. Typically, biomolecules become more thermophobic as the temperature is increased. Proteins are thermophilic at lower temperatures but become thermophobic just above room temperature. Nanostructured metals are prone to extreme heating due to plasmonic resonances. This means that the laser tweezer could repel biomolecules of interest, making it harder to trap them. It is still possible to trap thermophobic particles, but the time-to-trap increases, and this makes the trapping inefficient.

On the topic of not repelling biomolecules, surface interactions should also be controlled. Certain surfaces, like glass, pick up a large surface charge in aqueous environments. This serves to repel molecules of interest and it should be avoided for the same reason as for thermophoretic effects. We have noticed that switching to a non-aqueous environment, such as hexane, allows much more rapid trapping of nanoparticles. Based on the concentration of nanoparticles in solution, we expect that the time-to-trap is milliseconds, which is true for hexane but for aqueous samples it is longer.

Another challenge is extending to different types of proteins and environments. So far, most studies have focussed on globular or other free-solution proteins, whereas membrane proteins are also of great interest.



**Figure 31.** (a) Optical trapping of single protein bovine serum albumin (BSA), with the microscope setup shown (left), a scanning electron microscope image of a DNH (right-top), and optical transmission vs time in seconds (right-bottom) showing trapping and switching between open and closed states. (b) Optical trapping of the protein beta-amylase in nanopores combined with a shaped aperture. (c) Non-specific receptor binding with weak affinity for immunotherapy applications. Reproduced with permission, copyright American Chemical Society (2012) [218], Wiley (2019) [237], Institute of Physics (2021) [239].



**Figure 32.** DNH fabricated at the end of fibre for scalable trapping. (a) The mount used for placing fibres in evaporator and focussed ion beam (FIB) milling machines. (b) An electron microscope image of a fibre, with (c) a close-up of the core region etched with HF and (d) a close-up of FIB-milled DNH. Reproduced with permission, Optica (2014) [240].

Looking at proteins within a cell would also be an outstanding achievement, although this may prove too challenging with aperture-based trapping.

A final challenge is in throughput and scalability. Looking at biomolecules one-by-one is likely too time-consuming to have the level of impact required for antibody screening and drug discovery applications. Multiple traps are desired that can rapidly analyze biomolecules in parallel, each quickly gating between trapping events to obtain the biomolecule of interest.

### Advances in science and technology to meet challenges

A simpler way to do shaped-aperture trapping is to integrate the platform on the end of a standard optical fibre [240], as shown in figure 32. Ideally this approach will be easy to fabricate and will use standard parts that are robust and low-cost. Making the nanofabrication low cost will likely make use of colloidal nanofabrication that has high throughput, uses inexpensive materials, and does not require esoteric nanofabrication equipment. With the fibre-end approach, the optical tweezer can be used to probe standard microwells, which is the playground of many biochemists.

To avoid heating, the likely solution is to work away from plasmonic resonances. It is for this reason that these are not referred to as plasmonic tweezers, because I believe you specifically want to stay away from plasmonic resonances to avoid heating. It is possible to have field enhancements with nanostructured metals without invoking plasmonic resonances. In fact, early theory on ‘nanometric optical tweezers’ recognized that ‘non-resonant’ illumination was desirable to avoid thermal damage, and strong fields can be achieved with sharp features [241] and/or gaps without invoking plasmonic resonances.

To avoid electrostatic interactions with the surface, it is necessary to use surfaces that do not charge as much, or to treat the surfaces to avoid charging. We have carried out surface coating to minimize surface interactions [218], and we have promising results from plastic substrates that charge less than glass. Several groups have worked on the creation of phospholipid bilayers on surfaces in plasmonics and nanopore studies. For metals, this usually requires an additional thin film coating. It is possible that this can be added to the shaped-aperture platform as well to allow for trapping of membrane proteins.

The fibre-based approach above also solves the scalability challenge. With successful incorporation at the end of an optical fibre, it is easy to see how this can be scaled up and parallelized. For example, eight fibre probes can be attached to a single probe station and simultaneously address eight different microwells. Stepping through these microwells, one may envision 96-well-plate scanning. Having 96 fibres probing the entire well plate at once is another possibility. The fibre-based approaches benefit from this modularity that has already enabled tremendous advances in fibre optic communication. An alternative approach is to use a holographic optical tweezer approach to address multiple traps at once.

### Concluding remarks

Biotechnology is advancing rapidly. New technologies have provided unprecedented control of our genetic material and the proteins they produce. Yet our understanding of how these proteins function is still lacking. Single-molecule methods, such as shaped-aperture optical trapping, provide a new window into the biophysics of proteins and other biomolecules. To expedite real impact, these tools will have to remove complexity barriers associated with nanofabrication and optical tweezers, so that they become standard tools for biochemists and other scientists. If massively scaled up, they present disruptive potential to the fields of drug discovery, antibody screening, and other related industries. While only a handful of groups around the world have demonstrated shaped-aperture trapping of proteins so far, their exciting demonstrations show potential for vast impact.

### Acknowledgments

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## Trapping in gas and in vacuum

### 24. Optical levitation in gaseous media

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#### Status

Optical manipulation was introduced in 1970 when Arthur Ashkin trapped a single particle in water using two counter-propagating beams to balance the scattering forces. A year later he managed to trap a particle with a single, vertical beam in air, where the particle's weight counteracted the scattering force [242]. This optical levitation technique has since then been used to levitate particles in gaseous media. The field of optical trapping, however, really took off when Ashkin demonstrated optical tweezers in 1986. Here, the same microscope objective is used both to trap and observe an object, and due to the particles' buoyancy, very low trapping powers are needed. These huge advantages propelled optical tweezers to a standard built-in tool in many commercial microscopes. They can be combined with all kinds of optical detection techniques and are now frequently applied in fields outside optics.

The design of optical traps has always been fundamentally intertwined with the surrounding media, which could be a liquid, gas, or vacuum. When trapping in a liquid, there are strong mechanical and chemical interactions between the trapped object and the media. Here, solid particles, liquids enclosed by a membrane (vesicles or cells), or insoluble liquids can be trapped. In vacuum, on the other hand, the particles can be non-intrusively trapped, but only solid particles or liquids with very low vapour pressure can be investigated. As a consequence, the intermediate case of trapping in gaseous media constitutes the most general method for experimental work on isolated samples of microscopic liquids.

Although trapping in air was performed at the very beginning of the field of optical manipulation, it is only in recent years that the activities in the field have emerged [243]. In optical levitation, particles are trapped with a long focal length lens, producing a trap with low stiffness. This allows a trapped particle to be used as an extremely sensitive force probe [244], and environmental properties like air friction can be easily controlled and have led to unique visualizations of fundamental physical properties [245]. A very important and emerging application of optical levitation is in the field of microchemistry, where samples with a very high surface to volume ratio can be investigated. Here, the long working distances from the trapping lens allow access for various excitation and detection schemes. Optical levitation has also been used to investigate optical phenomena, such as whispering gallery modes (WGM) [246] and optically induced rotation [247].

#### Current and future challenges

Optical levitation is the ideal system for the development of methods to investigate the chemistry of microscopic isolated samples of liquids. It is then the liquid itself, due to the surface tension, that creates the interface between the trapped liquid and the surrounding gas. This is very different from other types of experiments on microscopic amounts of fluids, where the liquid is confined by the wall of, e.g. a micropipette or a microfluidic system. Many interesting experiments have been conducted, but the field is still in its infancy.

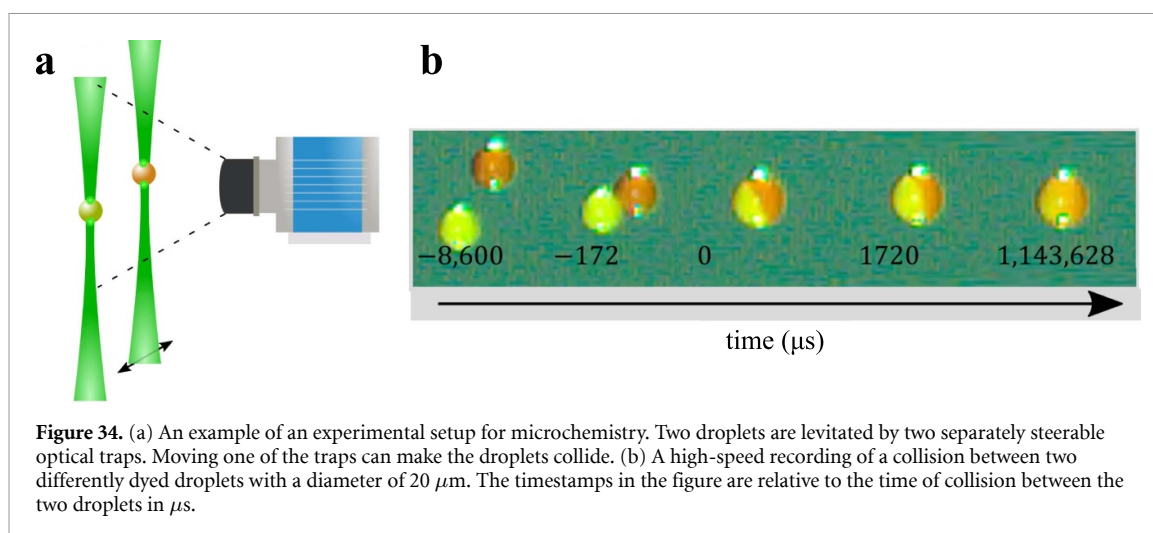
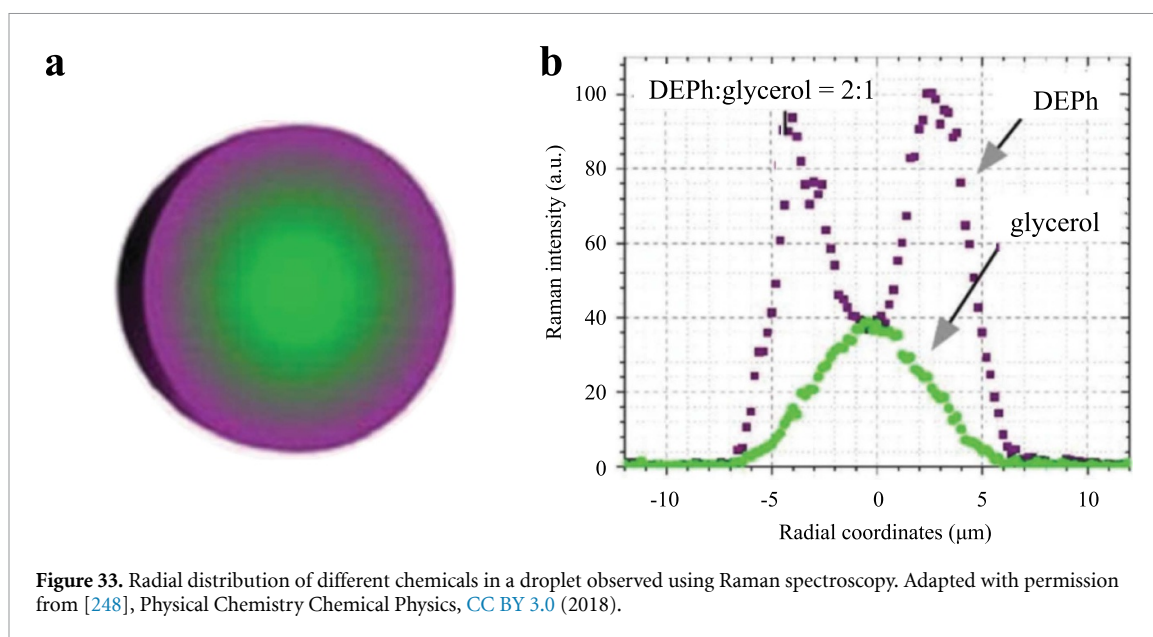
A main challenge in the field is to develop the optical levitator into a complete system for microchemistry, where three classes of experiments can be identified. First, optical levitation can be used to study the intrinsic properties of the trapped liquid. Trapping is then conducted in an inert gas, which only has the function to create a viscous force assisting in the trapping process. The feasibility of this has been shown by Kalume *et al* [248], who used Raman spectroscopy to observe the formation of a shell structure in a droplet consisting of two different solvents (figure 33).

Second, methods for studies of the interaction with the surrounding media can be developed. This is of high relevance in aerosol science [249] since the absorption and emission of molecules and also larger particles have implications in a wide range of fields, such as environmental science, cloud formation, or the spreading of viruses.

Third, the interaction between two different droplets can be studied using a dual optical levitator, where the spatial position of the two trapped droplets can be independently controlled. Figure 34 shows a proof of principle experiment, where the interaction between two different liquids is studied with high spatial as well as temporal resolution. These experiments show the potential of using optical levitation in microchemistry research. However, a lot of development is needed before the full potential of the experimental scheme is obtained.

Another important application of optical levitation is the study of optical processes, and in particular scattering. A single scatterer with a fixed location, where the size can be tuned, provides opportunities to





reveal information that is normally hidden when light scattered from multiple sources is integrated. Mie scattering, for example, can be used to measure the size and refractive index of the particles [250]. Optical levitation here gives unique experimental possibilities since the size of the trapped particle can easily be varied by evaporation or condensation.

#### Advances in science and technology to meet challenges

There are currently many interesting developments in the field of trapping in gaseous media, at the same time as there are many remaining challenges. The main technological advancement required to make optical levitation a widespread technique would be to construct an experimental system where particles can be readily dispensed and trapped, in precisely the same way as there are now plug-in units for optical tweezers that can be incorporated in commercial microscopes. The most important required advances in science and technology are:

- *Development of more efficient trapping to avoid the very powerful lasers needed today.* This is of particular importance for experiments using multiple traps. One possible solution is the use of acousto-optical trap. In an acousto-optical trap, the acoustic field could do the main part of the work to counteract gravity, while the optical trap would provide the stability and control. This would reduce the laser power necessary to trap, and also expand the range of sizes that can be trapped to six orders of magnitude, ranging from nm up to mm.



- *Development of a reliable dispensing mechanism.* Optical tweezers can simply pick up particles dispensed in a liquid sample, whereas van der Waals forces make it difficult to release particles into the gas phase. Many different techniques exist, including laser-induced acoustic desorption, microdroplet dispensers, piezoelectric transducers, and ultrasonic nebulizers, but there is still no reliable dispense-on-demand system available.
- *Incorporation of an environmental control in the optical levitator.* Today, various experiments have been conducted under different environmental conditions, such as the composition of the surrounding gas, pressure, and temperature. However, there is not yet a system available where these parameters can be freely varied while the liquid droplets are dispensed into the system on demand simultaneously.
- *Development experiments and theory of directional Mie-resonance spectra.* Mie spectra have been shown to be made up of a series of Fano resonances, where their evolution is directly dependent on the material properties, i.e. refractive index and optical absorption. Therefore, the evolution of material properties on the surface of droplets could be measured *in situ* during processes like evaporation or chemical absorption.
- *Development of the use of cavity ringdown spectroscopy (CRS) together with Mie resonances.* Levitated particles have been placed inside mirror cavities to investigate their properties using CRS [251] but, at a Mie resonance, particles themselves act as cavities. The observation of a decay in the scattering of a particle during a resonance would mean that CRS could be performed without the need for an external cavity and could allow instant measurement of trace contaminants in a droplet.

### Concluding remarks

Optical levitation is an eye-catching technique with a broad range of applications, from demonstrations of physical principles to fundamental research. Many experiments using optical levitation of liquid droplets in gaseous media have been initiated. The main experimental challenge is to combine the different technologies to dispense and trap droplets, control the environment, induce reactions, and finally detect the processes using advanced detection schemes. When an experimental system that combines these technologies has been developed it is expected that optical levitation will become a universal tool that will be applied for experimental studies of physical and chemical as well as optical processes of importance in many different applications, such as combustion, printing, devices for inhalation, and atmospheric sciences.

### Acknowledgments

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## 25. Rotational optomechanics of spinning particles

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### Status

Levitated optomechanics is the trapping and isolation of mesoscopic particles at low pressure. As the pressure is reduced, the translational motion of the particle changes from over-damped to under-damped oscillations, i.e. the oscillations become increasingly coherent. This decoupling from the thermal environment also allows the motion to be cooled using feedback schemes. Overall, this leads to very high-quality factor systems with very long decoherence times, ideal for a suite of sensing and measurement studies. Ashkin first levitated dielectric particles under vacuum conditions in 1977, but the field of levitated optomechanics has only taken shape in the last decade and subsequently made rapid progress including, in 2020, the first demonstration of cooling a levitated nanosphere to the quantum ground state [32].

Going beyond translational motion, introducing a rotational degree of freedom opens up exciting prospects. An anisotropic particle (either due to its shape or to birefringence) experiences a torque in the presence of circularly polarized trapping light, which causes continuous rotational motion around its centre of mass, at an angular velocity restricted by viscous drag. In low-pressure environments, such spinning particles can reach rotational frequencies in the GHz regime (figure 35) [252]. The rotation can add an inherent stability to the particle motion [247] and also couple in intriguing ways to the translational motion of the particle. Translational stabilization is beneficial in studies of the interactions between particles and surfaces (e.g. quantum friction, as detailed below) and multiparticle interactions such as optical binding (covered elsewhere in this roadmap). Moreover, rotation can be used to average-out the effects of inhomogeneities, such as fixed electric dipole moments in the particles.

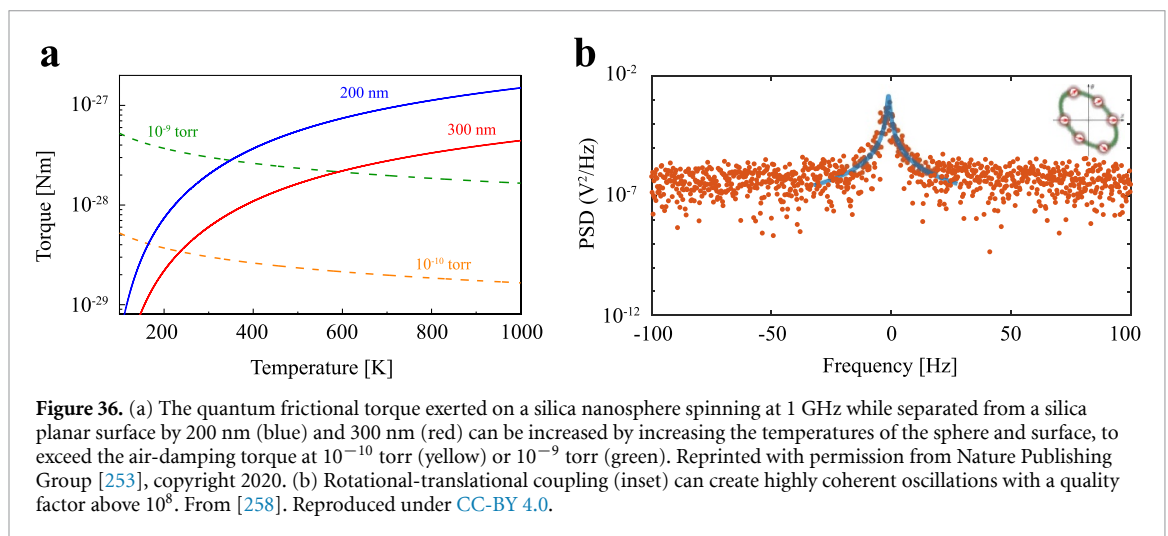
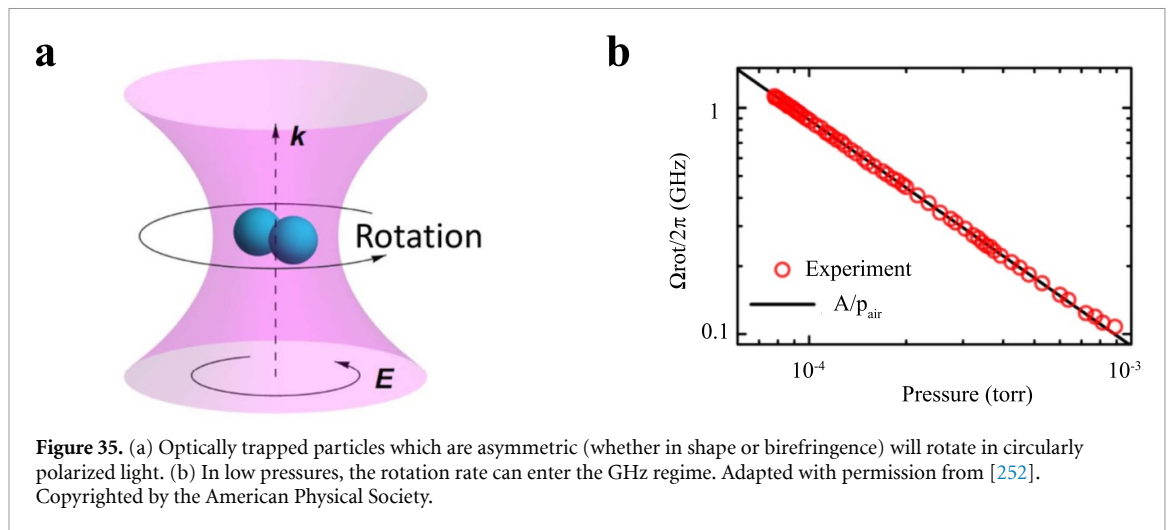
More broadly, harnessing the rotational motion of optically trapped particles offers enticing prospects in both applied and fundamental science. Pressure sensing with levitated rotating particles has been demonstrated as an alternative to mm-scale magnetically levitated spinning-rotor pressure gauges, with advantages of higher spatial resolution and insensitivity to external magnetic fields [253]. External forces and torques influence the rotation rate: a frequency-locked rotating nanorod has been demonstrated to offer a non-resonant force sensor [253], while external torques as small as  $10^{-28}$  Nm can be measured with rotating particles [254], surpassing torque sensitivities in cryogenically cooled tethered systems by orders of magnitude. Ultimately, in ultrahigh vacuum, where the drag on the particle is negligible, material properties of the rotor, such as the tensile strength, can be probed [252].

### Current and future challenges

One major challenge in levitated optomechanics is the demonstration of mesoscopic quantum phenomena, taking advantage of the excellent isolation from environmental noise afforded by levitation. Cooling all rotational and translational degrees of freedom to the quantum ground state is an open challenge. However, while the observation of quantum phenomena with translational degrees of freedom requires significant cooling to the motional ground state, quantum phenomena may be seen in rotational dynamics without this cooling requirement [255], with potential applications in quantum-enhanced torque sensing at the  $10^{-30}$  Nm level and tests of wavefunction collapse models.

Rotating levitated particles provide a promising platform in the search for so-called quantum friction. For two surfaces undergoing parallel relative motion at constant speed, the vacuum electromagnetic fluctuations are predicted to cause a force counteracting the motion. The existence of quantum friction is itself under debate [256], and experiments have yet to unambiguously measure its effects, due primarily to the fact that the force is incredibly weak. However, for a room-temperature 150 nm diameter silica sphere, rotating at 1 GHz, 200 nm from a silica surface, the quantum frictional torque is predicted to be  $10^{-28}$  Nm, comparable to recently achieved torque measurements with levitated particles rotating far from any surface [254]. An unambiguous measurement of the quantum frictional torque in a regime of negligible air damping will require a background pressure below  $10^{-9}$  torr (figure 36(a)). Therefore, the principal current challenge is to combine state-of-the-art achievements in rotation rate, background pressure, and stable confinement close to a substrate, in a single experiment. A future challenge will be the detection of the orders-of-magnitude weaker vacuum friction: the drag force exerted on a rotating particle in free space.

An intriguing prospect is the possibility of observing another elusive fundamental phenomenon: Zel'dovich amplification of electromagnetic waves by a spinning object [257]. In this phenomenon, rotational energy can be transferred from matter to the light if the object's rotation rate is greater than the



angular frequency of the light divided by its topological charge. State-of-the-art experiments can generate beams of light with topological charges as high as  $10^4$ , and optically trapped particles can achieve rotation rates of  $10^9$  Hz, suggesting that Zel'dovich amplification of infrared light might be observable. The challenge will be in sufficiently focussing such long wavelength light with such high values of topological charge onto nanoscale particles, although future increases in angular velocity would reduce the required wavelength of light and ease this challenge.

#### Advances in science and technology to meet challenges

Advances in the material properties of particles are likely to have wide-ranging impacts on rotational levitated optomechanics. An early material used in rotational studies was vaterite, a positive uniaxial birefringent crystal of calcium carbonate: micron-sized spheres of vaterite were rotated at MHz rates [247]. The birefringence of the vaterite particle allows an unforeseen new understanding of light-matter interaction. From a particle perspective, this results in effects such as the nonsymmetric coupling between rotational and translational degrees of freedom, leading to forces that are linearly non-conservative. A repeated sequence of small translations and rotations, which return the particle to its initial configuration, transfer energy between the optical field and the particle. Some trajectories increase in energy, accumulate momentum, and show coherent characteristics leading to self-sustaining motion arising, even from stochastic thermal forces. This generates oscillations with a quality factor in excess of  $10^8$  (figure 36(b)), which is highly attractive for sensing [258]. Separately, from the perspective of light, inhomogeneous circularly polarized light has components of optical momentum that circulate around the beam axis, resulting in additional forces which may be revealed by the birefringent nature of the trapped object. However, synthesis of nanoscale vaterite is challenging, and rotational levitated optomechanics has so far required the development of alternative rotors, such as rods or dumbbells of silica. The introduction of more exotic materials to the levitated toolbox are likely to herald further new advances.

The choice of particle material also plays an important role in the challenges outlined above. The quantum frictional torque is resonantly enhanced if the surface and sphere have common phonon polariton modes (e.g. if they are constructed from the same material). A further judicious choice of the material of the particle and surface may increase the value of this torque by orders of magnitude, e.g. by exploiting a resonance between the surface polariton frequency of the material and the rotational frequency of the sphere, to promote photon tunnelling between the sphere and medium [259]. Predictions suggest this will allow experiments to detect quantum friction at much higher pressures (around  $10^{-4}$  torr). Meanwhile, the plausibility of observation of Zel'dovich amplification increases with the rotation rate of the particle: new materials may need to be investigated, which have sufficient tensile strength to withstand rotation rates in the tens or hundreds of GHz.

### Concluding remarks

The effects of rotation have, to varying degrees, surprised and encouraged research in the area of levitated optomechanics. This is a degree of freedom that is adding immense value to the field and opening up new studies in both the classical and quantum domains. As we progress in cooling, torque fluctuations due to the quantization of the field may dominate the motion. Entering this domain may allow for concepts such as squeezing of light to be used to control rotation [260]. The next decade is likely to see exciting twists in the light–matter interaction story.

### Acknowledgments

The authors acknowledge funding from the UK Engineering and Physical Sciences Research Council (EP/P030017/1).

## 26. Dynamics and applications of an optically levitated nanodumbbell

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### Status

Due to their great isolation from the thermal environment, optically levitated nanoparticles in vacuum have great potentials in precision measurements and the study of fundamental physics. While most experimental works in levitated optomechanics have focused on spherical particles, there is growing interest in the use of nonspherical nanoparticles [261, 262]. Compared to spherical particles, nonspherical particles offer the opportunity to study the rotation and libration (torsional vibration) besides the centre-of-mass motion. Among nonspherical particles, silica nanodumbbells stand out as they have been experimentally levitated in a high vacuum (figure 37) [252]. A silica nanodumbbell can be created by chemical synthesis or by merging two levitated silica nanospheres together in optical tweezers. The bonding between the two nanospheres is remarkably strong [252]. Because of its anisotropic shape, its optical polarizability along its long axis is larger than those along the two short axes. Circularly polarized optical tweezers can transfer the spin angular momentum of photons to the levitated nanodumbbell and drive it to rotate (figure 37(a)) [252, 263]. Record high rotation speeds beyond 5 GHz have been reported with a levitated nanodumbbell in a high vacuum (figure 37(b)) [254]. In linearly polarized optical tweezers, the long axis of the nanodumbbell will tend to align with the electric field of the optical tweezers. It will be a novel analogy of the famous Cavendish torsion balance with an unprecedented torque detection sensitivity of the order of  $10^{-28}$  Nm/ $\sqrt{\text{Hz}}$  (figure 37(d)) [252]. Recently, a levitated nanoparticle has detected a torque as small as in just 100 s [254]. Such an ultrasensitive nanoscale torque detector will be able to study Casimir torque [264] and quantum vacuum friction near a surface [254]. Besides torque sensing, a levitated nanodumbbell can also be used to create macroscopic rotational quantum superposition states to test the limit of quantum mechanics. Cooling will be required for most quantum applications. The three centre-of-mass motion modes and two librational modes of a nanodumbbell have been cooled simultaneously with active feedback (figure 37) [157]. Recently, parametric feedback cooling was used to cool the libration of a levitated nanodumbbell to sub-kelvin temperatures [260]. Depending on the laser power, the heating due to photon shot noise can dominate, limiting the cooling performance when the air pressure is below  $10^{-7}$  torr (figure 37(d)) [252, 260].

### Current and future challenges

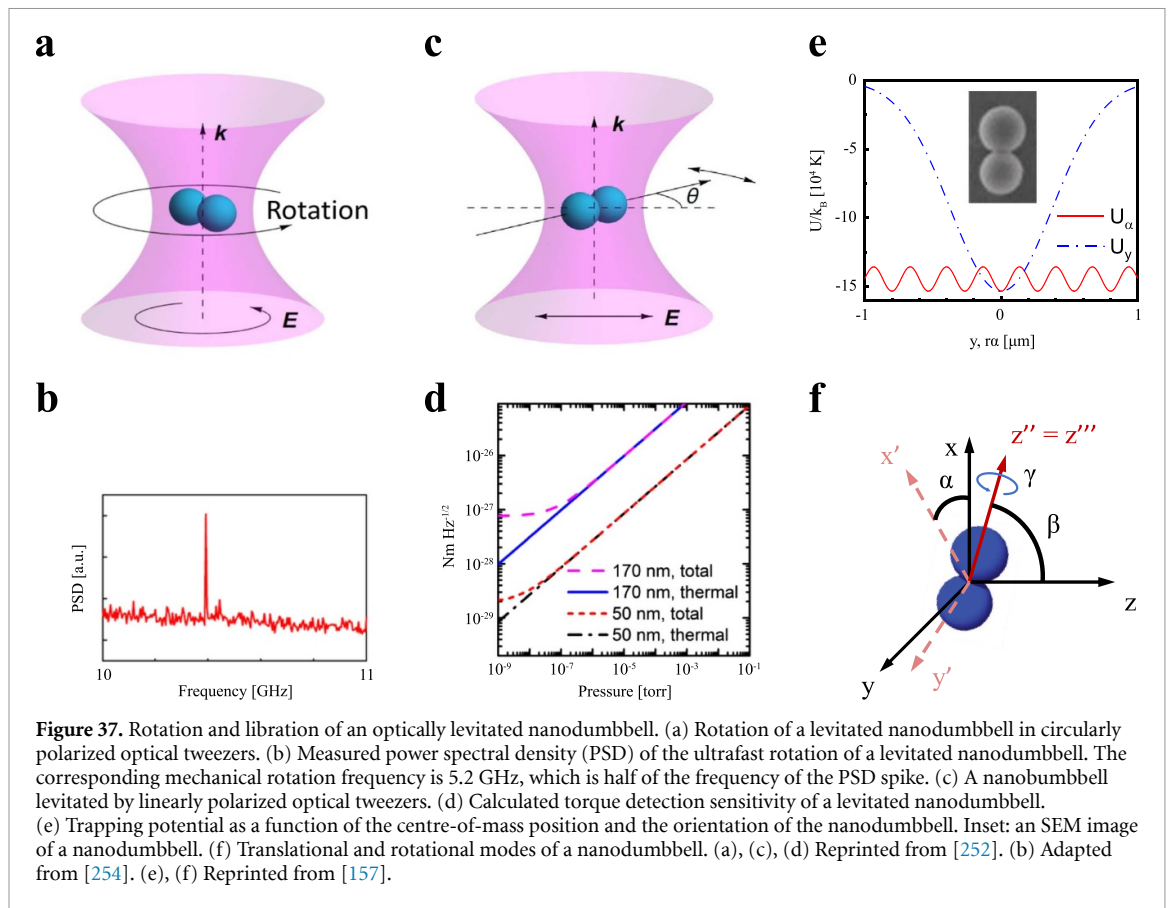
The maximum rotation speed of a levitated nanodumbbell is limited by its breakdown due to the centrifugal force, as detailed in [252]. At a rotation speed of 5 GHz, the maximum stress in a nanodumbbell with a diameter of 150 nm is expected to be more than 100 GPa. To detect the vacuum friction, a nanoparticle will need to be driven to rotate at high speed near a surface with a submicrometre separation in a high vacuum. To make sure the vacuum friction is larger than the traditional friction due to air damping, the pressure of the residual air will need to be below  $10^{-9}$  torr [254], which will be challenging to achieve.

Ground-state cooling will be required for many quantum applications. But it has not been achieved with a levitated nanodumbbell. The feedback cooling of a levitated nanodumbbell was hindered by the coupling between different modes due to the uncooled rotational motion around its long axis [157]. Because of the symmetry of a nanodumbbell, its free rotation around its long axis does not couple to the optical tweezers directly. Hence, this rotation mode cannot be cooled by a laser beam directly. This uncooled mode can cause heating of other modes.

Because a nanodumbbell (about 150 nm) used in optical levitation experiments so far is much smaller than the wavelength of the trapping laser (typically 1550 nm), the nanodumbbell appears as a simple spot on the optical image of the scattered light [252]. The shape and orientation of the nanodumbbell is not directly observable from the optical image. It is thus often difficult to understand the system and interpret experimental results. It is also time-consuming to pump a vacuum chamber to a high vacuum after a nanodumbbell is captured in air at 1 atm. Only silica nanoparticles have been trapped in a high vacuum successfully, which limits the application of the system. Other nanoparticles such as diamond have not been optically trapped in a high vacuum due to laser heating. For certain applications, the torque signal to be detected is static. Thus, a lock-in amplifier cannot be used to improve the sensitivity of the system.

### Advances in science and technology to meet challenges

Currently, the geometry of a levitated nanodumbbell is confirmed indirectly by the asymmetry of its air-damping rates. Direct visualization of the shape and orientation of a levitated nanoparticle will provide more information about the system, especially when the nanoparticle has an irregular shape. Many



super-resolution optical imaging techniques beyond the diffraction limit have been developed for biological imaging. Some of these techniques, such as structured light illumination, will also be suitable for imaging the shape and orientation of an optically levitated nanoparticle. Currently, a nanodumbbell is first captured in the air at 1 atm, and then pumped to vacuum. This process is slow, especially if a pressure below  $10^{-7}$  torr is required. Bake out is often required to achieve a pressure below  $10^{-7}$  torr, which is time-consuming and may cause the loss of a levitated nanoparticle. Capturing a nanodumbbell in a vacuum directly will speed up such a process. A cryogenic environment can also reduce the air pressure and heating effects due to residual air molecules. Only silica nanodumbbells have been trapped in a high vacuum so far. To trap other functionalized nanoparticles, internal temperature cooling or a combination of optical tweezers and an ion trap will help to trap other nonspherical particles in a high vacuum.

Quantum ground state cooling is required for many applications. To avoid the cooling limitations due to the free rotation of a nanodumbbell around its long axis, we can use more asymmetric nanoparticles, such as a nanodumbbell with a small nanoparticle on its side. This can break the rotation symmetry of a perfect nanodumbbell and couple all six degrees of freedom to the optical tweezers. To achieve 6D ground state cooling of a levitated nanodumbbell, we can use cavity coherent scattering cooling with elliptically polarized and shaped optical tweezers [265]. Coherent scattering strongly enhances the interaction by using the high-intensity trapping laser for cooling as well. We will need to trap a nanoparticle near a surface to study surface interactions. The reflected light and the incoming light will interfere and form a standing well near the surface, which has a potential minimum about  $1/4$  wavelength away from a high-refractive-index surface. It will automatically determine the position of the nanoparticle and the surface. We may also enhance the nanodumbbell–photon interaction by trapping a nanoparticle using a nanoscale photonic crystal cavity [266].

### Concluding remarks

Silica nanodumbbells have been optically levitated in a high vacuum [157, 252, 260]. The dynamics of their motion are highly nonlinear. Circularly polarized optical tweezers have driven them to rotate at GHz frequencies. A nanodumbbell levitated in linearly polarized optical tweezers will be an analogy of the famous Cavendish torsion balance. Optically levitated nanodumbbells will be excellent torque detectors for the study of Casimir torque and quantum vacuum frictions near a surface. Once cooled to the quantum regime, they can be used to investigate rotational quantum mechanics in unprecedented regimes. Rotational quantum



superposition states of nanodumbbells can be used to study continuous spontaneous localization. They may also be used to search for dark matter candidates.

### Acknowledgments

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## 27. Optical binding

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### Status

Multiple scattering of light induces structured interactions, or optical binding forces, between collections of small particles (figure 38). These forces depend on the morphology of the optical field and on the shape, composition, and distribution of the particles comprising the ensemble. When wide loosely focused beams are used, many particles can be encompassed and, for modest laser power, the binding forces are sufficient to promote various modes of self-organization within moderately sized ensembles. For symmetric configurations of dipolar particles, binding interactions appear to be conservative with systems satisfying the Boltzmann distribution. For lower-symmetry systems, the underlying non-conservative characteristics of optical forces start to express themselves, giving rise to various nonequilibrium effects.

Optical binding of a pair of dielectric microspheres was first observed at an interface, then in an isotropic fluid [267]. Although the form of the interaction has been exhaustively analyzed for simple, highly symmetric cases, larger and more complex systems are less tractable. Nevertheless, a range of structures have been synthesized that can be dynamically reconfigured in one or more [268] dimensions by holographically modifying the incident field. Due to the non-conservative nature of the binding interaction, optically self-organized structures can execute a range of complex, often periodic motions. Examples include sorting and separation of microparticles [269], the generation of self-sustained oscillations in optically bound chains [270], and complex coordinated rotations of collections of spherical or elongated [271] particles in beams carrying angular momentum.

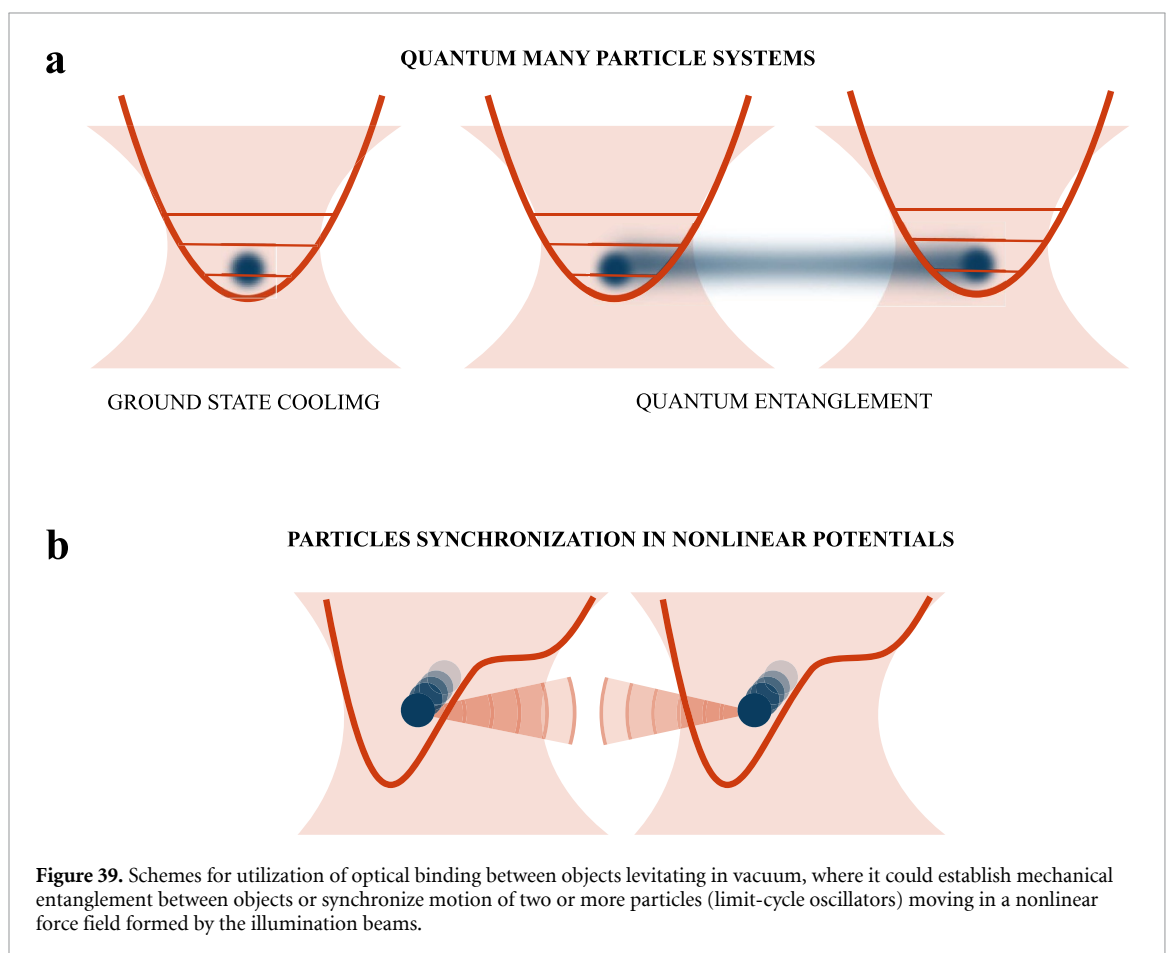
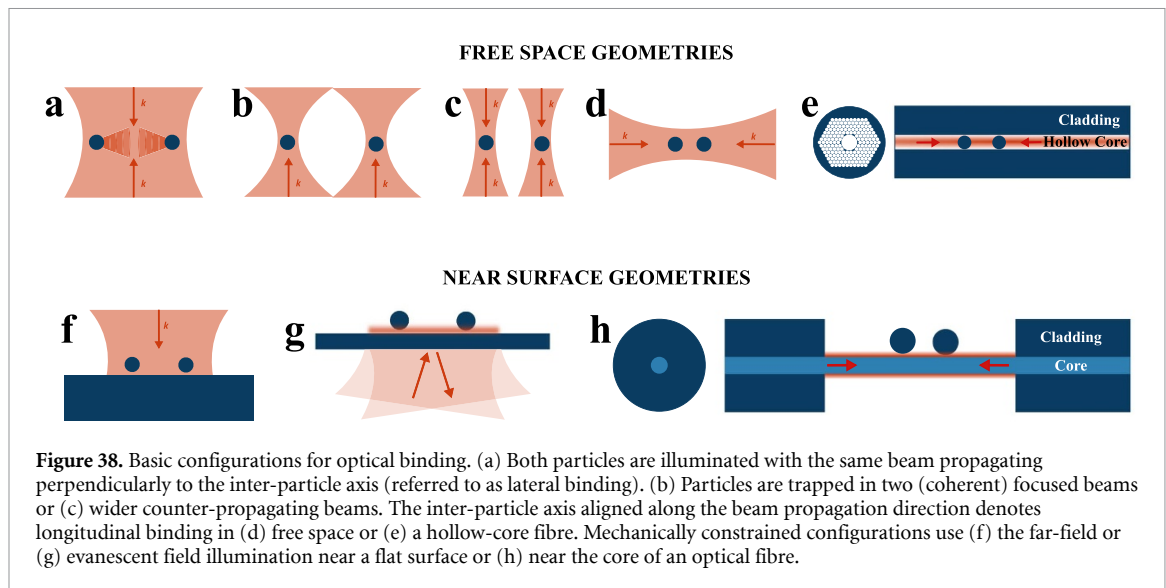
Shifting from over-damped aqueous environments to vacuum opens up multiple new frontiers. While the optical control of single particles in vacuum (i.e. optomechanics) continues to break new ground in the fields of weak force sensing and quantum technologies, collective optomechanics, involving optically interacting particles, remains relatively unexplored. The most common experimental systems rely on complex fabrication methods (e.g. coupled membranes, photonic nanobeams, toroidal microresonators). In contrast, systems based on optical levitation of discrete particles constitute an entirely new type of light–matter interface, which removes many of the constraints of the established approaches and offers easy tunability of all system parameters. To date, only a few studies of optical binding in vacuum have been reported. Bykov *et al* [272] reported long-range optical binding mediated by intermodal scattering within an evacuated hollow-core photonic crystal fibre. Arita *et al* [273] showed binding between rotating birefringent microspheres. Svak *et al* [274] exhibited tuneable longitudinal binding between multiple particles in cross-polarized counter-propagating laser beams and characterized their interaction, modal behaviour, and nonlinearity. Riesel *et al* [275] studied the tunability of mutual optical coupling between two nanoparticles levitated in separated optical traps.

### Current and future challenges

Optically bound systems present an intriguing combination of scientific challenges in nonequilibrium statistical mechanics, stochastic thermodynamics, macroscopic quantum mechanics and, additionally, in control and information theory. Applications range from the synthesis of novel metamaterials or optical robotics to sensing and quantum technology.

A major challenge for optical self-organization in over-damped systems concerns the connection between the system parameters (e.g. the incident optical field, the shape and composition of the particles) and the probable results of the self-organization process. This relationship is highly non-trivial since, in general, the forces acting on the system are non-conservative so that the Boltzmann distribution will probably not apply. Indeed, the resulting ensemble may not be at equilibrium at all. Although a general theory may never be available, insight may be derived through deeper understanding of optical interaction forces, basic properties of nonequilibrium steady states (especially in terms of entropy production), and transitions between such states [276]. Such concerns are shared with the rapidly growing field of active colloids, and a more detailed understanding could lead to the engineering of novel metamaterials or even complex mobile assemblies performing useful work at the nanoscale.

The same challenges are present in under-damped systems, although the underlying dynamics are further complicated by the presence of inertia, permitting the formation of more general dynamical attractors, including limit cycles or even autonomous chaos (figure 39). Ever-present thermal fluctuations provide an opportunity to study the statistical mechanics of numerous exotic dynamical systems from the synchronization of noisy under-damped oscillators (which could be periodic or chaotic), to the



redistribution of energy in the famed Fermi–Pasta–Ulam–Tsingou problem. In addition to fundamental interest, the ability to prepare and control such systems could have applications in sensing.

Taking collective levitational optomechanics into the quantum regime presents the most substantial challenge. The combination of feedback and cavity cooling recently resulted in ground-state cooling of a single nanoparticle [32, 277]. An analogous approach, applied for example to the separation of two or more particles in appropriately nonlinear potential landscapes, could lead to the macroscopic entanglement of multiple degrees of freedom. Finally, we note that collective levitational optomechanics contains the required ingredients to, in principle, allow the preparation of macroscopic classical or quantum time crystals, perhaps functioning as quantum memories or interfacing with other quantum technology.

**Advances in science and technology to meet challenges**

The current progress in the technology of beam shaping via spatial light modulators, amplitude, and frequency beam modulation, and overall computer control of the experiments paves the way to the demanding experiments with a single levitating nanoparticle in high vacuum, where its mechanical energy is decreased via cavity or feedback cooling schemes to reach the lower levels of a quantum harmonic oscillator. The first experiments to reach the ground state of the quantum harmonic oscillator [32, 277] demonstrated the feasibility of this approach. However, synchronized cooling of several levitating nanoparticles is still in its infancy and advanced feedback protocols must be developed for cooling systems with many coupled degrees of freedom, manufacturing, and automatic launching of high-quality spherical and nonspherical particles with controlled optical properties to avoid, e.g. heating effects, advanced 3D tracking methods for systems with multiple particles, and a wide range of time scales.

**Concluding remarks**

Optical binding forces are an extremely complex and general form of interaction, dependent on the morphology of an external optical field and on the form of the particles comprising the ensemble. In highly symmetric cases, the interaction can appear conservative—allowing the formation of crystalline arrangements. More generally, optical binding is a nonlinear, non-conservative, many-body interaction. These characteristics make optically bound systems an ideal platform for studying driven self-organization of fluctuating structures that may be static or, alternatively, may execute a range of complex motions. In under-damped systems, the dynamical properties are modified by inertia, allowing systems to accumulate momentum, resulting in far richer behaviour, which may include limit cycles, and quasi-periodic or chaotic motion. In combination, these characteristics make the collective optomechanics of levitating systems an ideal test bed for studying the stochastic thermodynamics of collections of self-sustained periodic or even chaotic oscillators. By exploiting sophisticated feedback methods, developed for single-particle optomechanics, these complex coupled systems may be taken into the quantum regime, permitting the synthesis of entangled systems of particles or even macroscopic time crystals.

**Acknowledgments**

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## Insights into statistical physics

### 28. Nanothermodynamics and statistical physics

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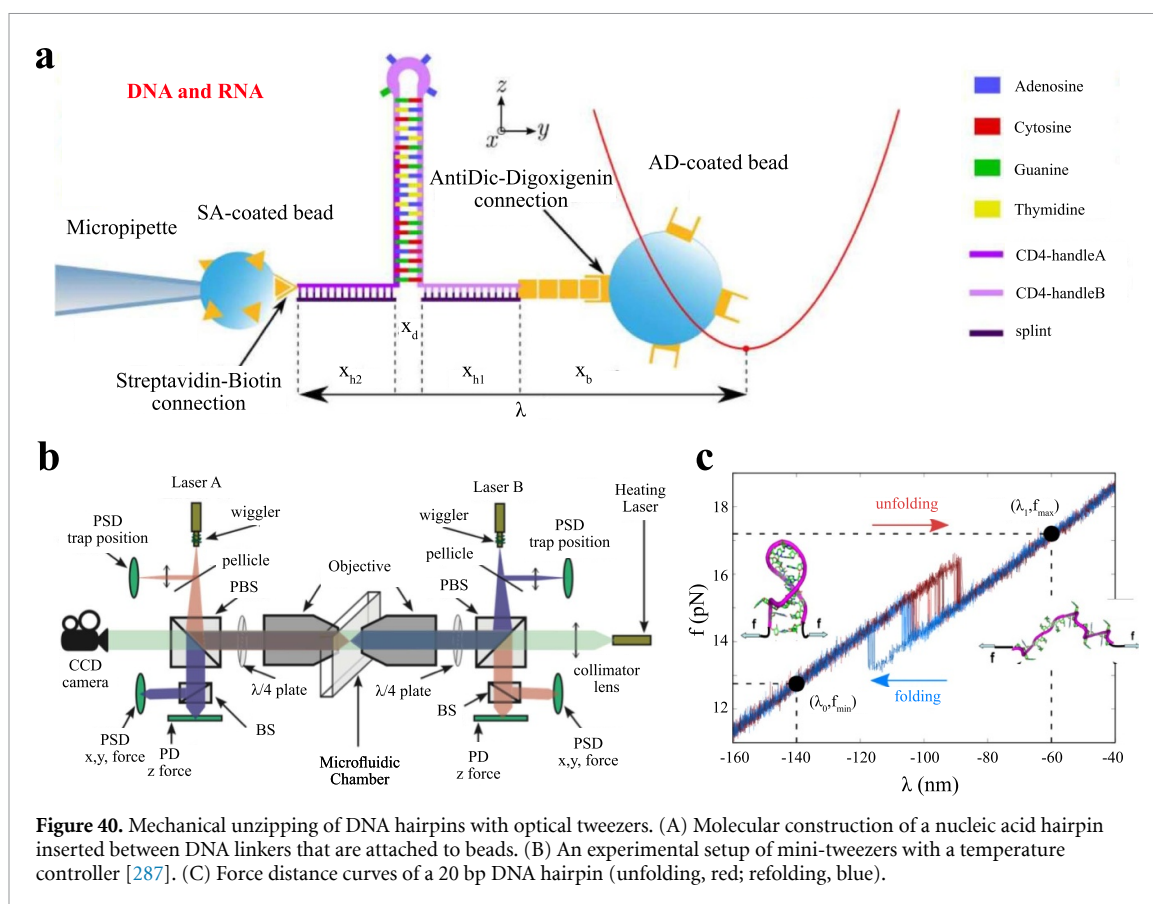
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#### Status

Single-molecule tools, and optical tweezers in particular, have revolutionized the way we interrogate biological matter. By measuring energies on the scale of thermal fluctuations, optical tweezers can monitor individual molecular trajectories and reactions, opening up new avenues in thermodynamics and kinetics at the nanoscale [278]. With optical tweezers we can now follow the folding of individual nucleic acids and proteins with submillisecond time resolution, and identify kinetic intermediates and misfolded structures that were previously hidden to bulk assays, reaching the bar of the  $1 \text{ kcal mol}^{-1}$  energy accuracy in molecular thermodynamics (figure 40). Besides investigating intramolecular reactions, optical tweezers have been used to characterize intermolecular interactions for biophysical and biomedical purposes, from protein–DNA and ribonucleotide complexes, to ligand binding (e.g. metal ions, polycations, peptides, dendrimers), and protein–protein interactions. Besides their many applications in biophysics, optical tweezers have found relevant applications in thermodynamics at the nanoscale or nanothermodynamics. Known as the thermodynamics of small systems [279], the prospective of exerting and measuring tiny forces (in the piconewton scale) on small objects (colloidal particles, molecular systems, electrical devices) over nanometre distances, has spurred intense research activity in stochastic thermodynamics [280]. Work in the 1990s in the field of nonequilibrium statistical mechanics led to the transient (Evans–Searles) and stationary (Gallavotti–Cohen) fluctuation theorems. These results demonstrated the existence of a symmetry relation for the entropy production (i.e. the heat dissipated to the environment) during a time interval  $t$ ,  $S_t$ , in a nonequilibrium process,  $P(S_t)/P(-S_t) = \exp(S_t/k_B)$ , where  $k_B$  is Boltzmann's constant. Consequential to these results are the nonequilibrium work and fluctuation relations by Jarzynski and Crooks for isothermal processes. Jarzynski equality permits us to derive free-energy differences ( $\Delta G$ ) from irreversible work ( $W$ ) measurements by exponentially averaging the work over many repetitions of the experiment,  $\Delta G = -k_B T \log \langle \exp(-W/k_B T) \rangle$ , where  $T$  is the temperature of the environment. The importance of these results is grounded in the fact that many molecular transformations can only be performed irreversibly: unfolding and folding melting curves often exhibit hysteresis. In mechanical unzipping experiments (figure 40) the ends of a single DNA, RNA, or a protein are mechanically pulled apart by moving an optical trap relative to an immobilized bead or surface (single-trap setup) or a dumbbell (dual-trap setup). By repeatedly unfolding and refolding a molecule, it is possible to extract the folding energy  $\Delta G$  by using the Jarzynski and Crooks nonequilibrium work relations. Since their first experimental tests, many applications and extensions have been developed [281].

#### Current and future challenges

Thermodynamics, a discipline inherited from the industrial revolution, applies to all scales. Elementary particles, atoms, molecules, living cells, superconductors, human beings, black holes up to the entire Universe, all comply with the laws of thermodynamics. As Einstein put it: 'Classical thermodynamics [...] is the only physical theory of universal content which I am convinced [...] will never be overthrown'. Thermodynamics is a conceptual framework encompassing many extraordinary events, from the self-assembly of viral particles to the birth of a cell from another cell. These systems obey thermodynamics, and despite the fact that we regularly use them in the lab, they escape our understanding. The second law inequality (i.e. the entropy of the Universe keeps increasing) is probably the most striking law in nature, qualitatively distinct from conservation laws (such as energy and momentum). The second law has always amazed scientists; in 1887 Maxwell proposed his famous paradox of a small, smart, and effortless being, that beats the second law by meddling with the molecular motion. Only much later, in the 1960s, Landauer and Bennett understood that information was key for the logical operations of the demon (storage and erasure of bits) giving rise to the thermodynamics of data processing. Together with stochastic thermodynamics, the new field of thermodynamics of information has emerged, a new discipline that puts information, entropy, and work on common grounds [283]. The Landauer limit sets an equivalence between energy and information,  $1 \text{ bit} = k_B T \log 2$ , similar to Joule's mechanical equivalence between work and heat. This makes it possible to experimentally measure information and test feedback fluctuation theorems. The



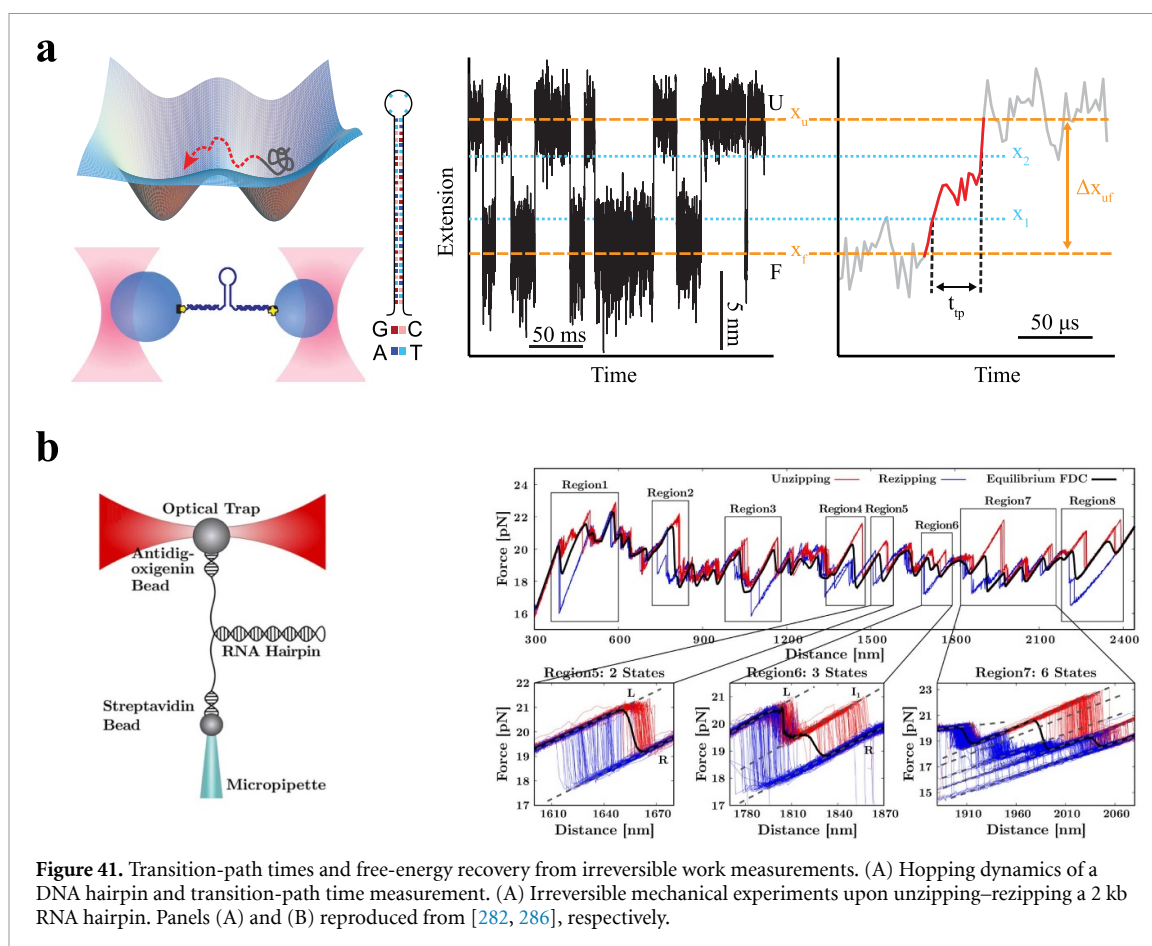
**Figure 40.** Mechanical unzipping of DNA hairpins with optical tweezers. (A) Molecular construction of a nucleic acid hairpin inserted between DNA linkers that are attached to beads. (B) An experimental setup of mini-tweezers with a temperature controller [287]. (C) Force distance curves of a 20 bp DNA hairpin (unfolding, red; refolding, blue).

thermodynamic uncertainty relations [284], recently derived by Seifert and colleagues, set a lower bound for the entropy production in nonequilibrium states. The bound is given by the ratio between the (squared) average of a current (e.g. the speed of a molecular motor) and its variance. The key question of experimentally measuring the entropy production, stands out as a primary goal in the field (see for instance, [285]). Besides the average entropy production, the spectral densities of entropy fluctuations are key structural features related to the efficiency of molecular machines. Future challenges are the study of motor enzymes (e.g. helicases and polymerases), where chemical reactions are involved and operate out of equilibrium. Although optical tweezers permit us to monitor an enzyme's movement and the work exerted by the optical trap, we cannot simultaneously monitor the adenosine triphosphate (ATP)-fuelling hydrolysis reaction. In this case, the experimental variables needed to determine the entropy production are inaccessible, and information is only partial.

### Advances in science and technology to meet challenges

Optical tweezers permit us to measure kinetics [286] and thermodynamics [282] of molecular transformations with unprecedented resolution (figure 41). From the energy of the native structures of DNA, RNA, and proteins to the binding of ligands (e.g. restriction enzymes, peptides, etc) and the experimental verification of the law of mass action. Nanothermodynamics also requires the measurement of enthalpies ( $\Delta H$ ) and entropies ( $\Delta S$ ), in which contributions to the overall free-energy difference are highly balanced for weak biomolecular interactions (enthalpy–entropy compensation). The sole knowledge of  $\Delta G$  does not tell us anything about the  $\Delta H$  and  $\Delta S$  contributions, which are typically much larger due to enthalpy–entropy compensation. Upon DNA hybridization, the two strands of the DNA helix form specific hydrogen bonds between complementary bases (A-T and G-C). While the average  $\Delta G$  is  $\approx 1\text{--}2 \text{ kcal mol}^{-1}$  per base pair, enthalpies and entropies are roughly ten times larger ( $\Delta H \approx 8 \text{ kcal mol}^{-1}$ ,  $T\Delta S \approx 6 \text{ kcal mol}^{-1}$ ). The key to nanothermodynamics is the heat capacity change ( $\Delta C_p$ ) in a biomolecular reaction. The  $\Delta C_p$  tells us about changes in configurational entropy, a relevant quantity in protein folding and self-assembly reactions. The recent development in temperature-controlled optical tweezers has represented an important step in this direction, which has permitted us to experimentally demonstrate that protein barnase folds in a funnel-like energy landscape, where the transition state forms a dry molten globule [287].





**Figure 41.** Transition-path times and free-energy recovery from irreversible work measurements. (A) Hopping dynamics of a DNA hairpin and transition-path time measurement. (A) Irreversible mechanical experiments upon unzipping–re-zipping a 2 kb RNA hairpin. Panels (A) and (B) reproduced from [282, 286], respectively.

Instrumental developments in optical tweezers should narrow the gap between the complexity of molecular systems and the limited number of measured variables. Future technological developments aim to combine optical tweezers with other techniques, such as fluorescence (fleezers) and light polarization measurements (angular optical traps) [60], or even electrical measurements (e.g. nanopore translocation [288]). These developments aim to bring light onto additional reaction coordinates beyond molecular extension that will greatly contribute to expand our knowledge of energy and information. The possibility to simultaneously track several experimental variables permits us to monitor the evolution of several reaction coordinates in an enlarged multidimensional energy landscape, a crucial step to measure entropy production in nonequilibrium systems. Finally, one might also ask about a bottom-up approach for thermodynamics, i.e. whether developments in stochastic thermodynamics may have an impact on macroscopic systems. An exciting venue of research might extend thermodynamics of information to particle assemblies and macroscopic objects [289], where trajectories of subsystem variables lead to entropy fluctuations, for example in bristle bots and kilobots (small but macroscopic robots), and even in animal behaviour (e.g. flocks of birds). These and other exciting questions await us in the future.

### Concluding remarks

Nanothermodynamics investigates energy and information processes in nanoscale systems, where the energies involved are comparable to the thermal noise. Biomolecular systems are of particular interest because their thermodynamic behaviour is determined by evolutionary biological processes operating at many scales: from the molecular scale (i.e. the genotype) to the cellular scale and higher (i.e. the phenotype). Understanding those energy processes operating at the molecular scale in living matter paves the way to unifying nonequilibrium physics and biology within the framework of information theory, evolution, and life. By measuring energy and information, optical tweezers combined with other techniques, permit us accurate and better measurements of entropy production and information, in molecular and cellular systems, and beyond. Nanothermodynamics shows the path to measure information in a bit-wise sense in biological processes, where the key steps of autonomous Maxwell demons (measurement, feedback, and information erasure) are naturally encoded [290]. As put forward by François Jacob [291], evolutionary processes are akin to bricolage (do-it-yourself), where nature uses everything that is available to improve

what does already exist. It is for this reason that evolution operates at all scales and times, giving biological structures that make up living beings their unique and marvelous complexity.

### Acknowledgments

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## 29. Experimental nonequilibrium statistical physics with optical tweezers

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### Status

Finding the fundamental rules governing the state and dynamics of systems far from thermal equilibrium remains an open challenge in physics. The leading approach to address this challenge, in a universal way, is to find generalizations of the theoretical framework of thermodynamics and statistical mechanics that apply to such systems. These include attempts to extend the definition of state functions, e.g. temperature and pressure, defining thermodynamic quantities as averages on a single phase-space trajectory level, and looking at large deviations of a system from its average state. All of these approaches rely on our understanding of the fluctuation spectrum of the system, which is generally unknown far from thermal equilibrium.

Onsager was the first to realize that very close to thermal equilibrium, and in contact with an ideal heat reservoir, temperature relates the system's response to a small perturbation to its thermal relaxation from such a fluctuation. This result is known as the fluctuation–dissipation theorem. Intuitively, this means that the same physical processes govern both the random fluctuations of the system and its dissipation. Focusing on the fluctuations in driven systems, a set of fluctuation theorems connecting the probability of thermodynamic favourable paths in phase-space to that of unfavourable ones was recently discovered and unified [280]. In the past three decades, optically driven colloidal particles were used to validate such theoretical predictions for systems out of equilibrium. These also include the generalized forms of the fundamental fluctuation–dissipation theorem [292] and a range of fluctuation theorems [293–295].

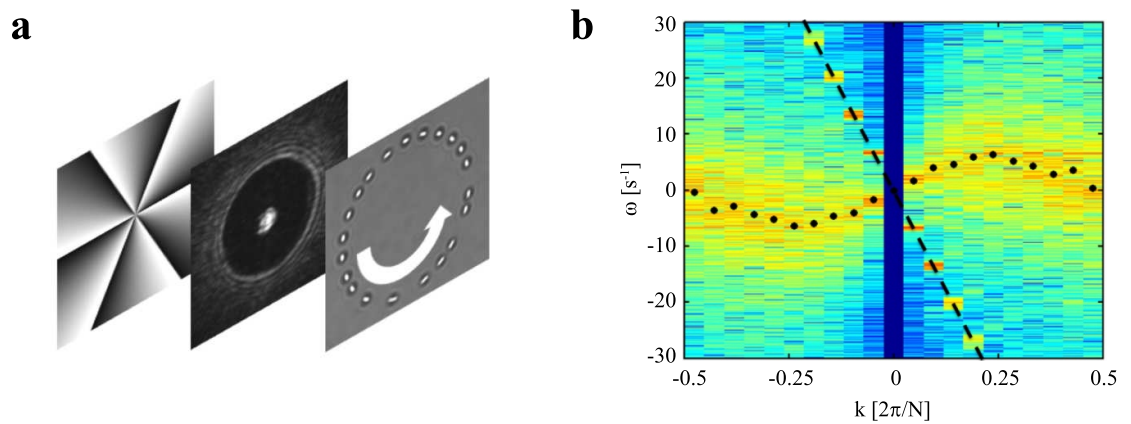
To study the spectrum of fluctuations experimentally requires mesoscopic small systems in which the probability of large fluctuations is finite. It is also beneficial that their dynamics be accessible on the single-particle level. These necessities led to the use of optically driven colloidal particles as a paradigmatic model system for the field [280]. The characteristic timescale for thermal relaxation of a suspended colloidal particle is several orders of magnitude faster than the typical driving timescale of an optically driven particle. This timescale separation implies that one can decouple the effect of the slow driving degrees of freedom and the fluctuation spectrum of the bath, a common feature of many experiments performed on dilute colloidal suspension (see, for example, figure 42 [292, 296]).

### Current and future challenges

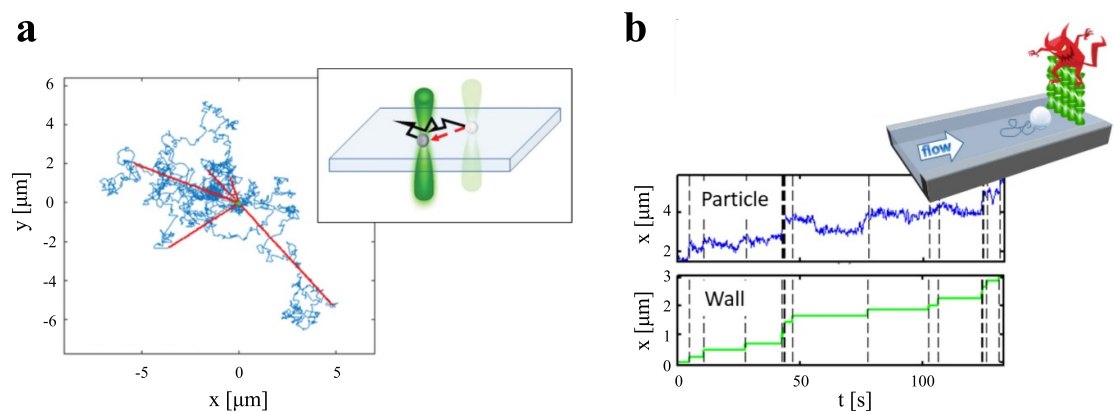
The motivation for the study of nonequilibrium statistical physics is to better describe our world, which is generally out of thermal equilibrium. Natural systems, and especially living matter, are usually subjected to non-conservative forces and currents; they include many interacting entities, and they change with time. Even at a driven dissipative steady state, their spectrum of fluctuations is rarely purely thermal. Therefore, the next challenge in experimental studies of nonequilibrium statistical physics using optical tweezers is to construct experiments that address some of these differences. Optical tweezers and, specifically, computer-controlled optical tweezers based on time-multiplexing beams or holographic technology have been instrumental in offering a versatile range of possible driving protocols. These are also essential for future progress.

The first challenge is to go beyond timescale separation and decipher the effect of coupling between the driving and fluctuation spectrum on the state of a system far from thermal equilibrium. Several ways to couple thermal fluctuations and driving in colloidal suspensions have been implemented. One approach to couple driving and fluctuations is to do so by hand. Specifically, this involves the use of feedback-controlled driving protocols, in which driving is dictated by the instantaneous state of the system at the time of measurement. This fruitful approach culminated in experimental studies of information machines: processes that convert measured information about a system to extractable work [289], and of stochastic resetting processes [297] (figure 43). Irrespective of which approach is used, the relation between dynamics and fluctuations remains beyond the scope of present understanding.

The effect of interactions on the state of a many-body system is not trivial to calculate, more so far from equilibrium. Using dense colloidal suspensions and computer-controlled optical tweezers affords a direct way to study many-body model systems out of equilibrium. A range of interactions between colloidal particles beyond the ever-present hard-core repulsion and hydrodynamic interactions is available, e.g. using magnetic and electric fields. The challenge, however, in conducting experiments with driven many-body systems is double. The first is conceptual; a theoretical description of the system is either unavailable or hard to obtain due to the long-range hydrodynamic interactions between colloidal particles. Second, single-particle tracking of dense regions in the colloidal suspension is challenging and may give ambiguous results.



**Figure 42.** Holographic optical tweezers are used to create an optical vortex in the sample plane of a microscope. Laser light is reflected off a spatial light modulator (SLM) placed in a plane conjugated to the sample plane, acquiring an angular sawtooth phase pattern. The laser beam is then focused through a high numerical aperture microscope objective, forming a ring-like optical trap in the sample plane. (a) Shown, left to right, are the phase pattern on the SLM, the resulting light pattern, and the trapped particles. The trapped particles rotate around the ring at constant angular velocity while exhibiting phonon-like breathing modes. (b) The measured dispersion relation of these vibrations is given by deterministic equations of motion and is uncorrelated to thermal noise. The thermal noise determines the width of each dispersion mode.



**Figure 43.** Feedback and control driving protocols, where driving depends on the instantaneous state of the system. (a) Stochastic resetting: thermal fluctuations determine the trajectory of a diffusing particle in a quasi-2D colloidal suspension. The bead is trapped and returned to the origin, resetting the system, after some random time. (b) An information engine: a particle diffuses in a quasi-1D channel near an optically repelling wall. Whenever the particle diffuses far enough from the wall, against the flow, the wall is brought slightly closer to the particle.

### Advances in science and technology to meet challenges

The technical challenge of accurately tracking many close active and driven particles is a significant obstacle in the future studies of microscopic systems far from thermal equilibrium. One difficulty that arises within this context is distinguishing between very close objects. This is compounded by the fact that images of close particles are distorted in many cases, leading to inaccurate localization. This challenge can be addressed by modifying the colloidal particles, the imaging techniques, or the analysis method. The development of core-shell colloidal particles with dark or low refractive index shells and a visible core is an essential step towards obtaining distinguishable particles and is currently pursued [298]. Other imaging techniques, such as holographic imaging, enhance distinguishability and improve localization significantly, but require further development. Finally, machine learning for image analysis might provide a way to circumvent the need to localize each particle individually.

The second hurdle in this respect is the ability to track each particle. Specifically, if particles move between consecutive images a larger distance than half the distance between them, it becomes hard to determine which is which. Technically, this can be solved for many-particle systems using fast cameras, decreasing the time the particles move in between images. However, high-speed imaging comes at the price

of limited measurement duration. The development of fast cameras that store images continuously for long durations is necessary.

### **Concluding remarks**

The extension of the framework of statistical mechanics to describe nonequilibrium conditions is limited by the lack of experimental observations in controlled and straightforward systems. Optical tweezers have emerged as a leading and ideal setup for such experiments. Taking these experiments closer to reality by coupling driving to fluctuations and looking at many-particle systems will provide crucial observations beyond current theory. These could pave the way towards establishing an extensive theoretical framework for statistical mechanics far from thermal equilibrium.

### **Acknowledgments**

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### 30. Light-assisted organization of active colloidal matter

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#### Status

The phenomenon of spontaneous pattern formation in nonlinear matter links together various fields of theoretical and experimental physics, highlighting similarities in externally driven nonlinear self-organization in different scientific branches from physics, chemistry, or biology over sociology and economy to astrophysics. The investigation of periodic or quasi-ordered spatial structures arising out of local interactions under the presence of an external driving field above a certain threshold is of high importance for a deeper understanding of many natural and artificial dissipative systems far from equilibrium. Optics play an important role in this investigation, since light is capable of creating (quasi-)periodic, disordered, or chaotic patterns in configurations similar to active resonators, and since the feedback inherent to these systems naturally creates a dissipative nature of the interaction with matter, and diffraction supplies spatial coupling. A simple optical single-feedback model is described by Firth [299], where a functional nonlinear optical material is coupled to a feedback mirror, thereby creating a wealth of spatio-temporal patterns.

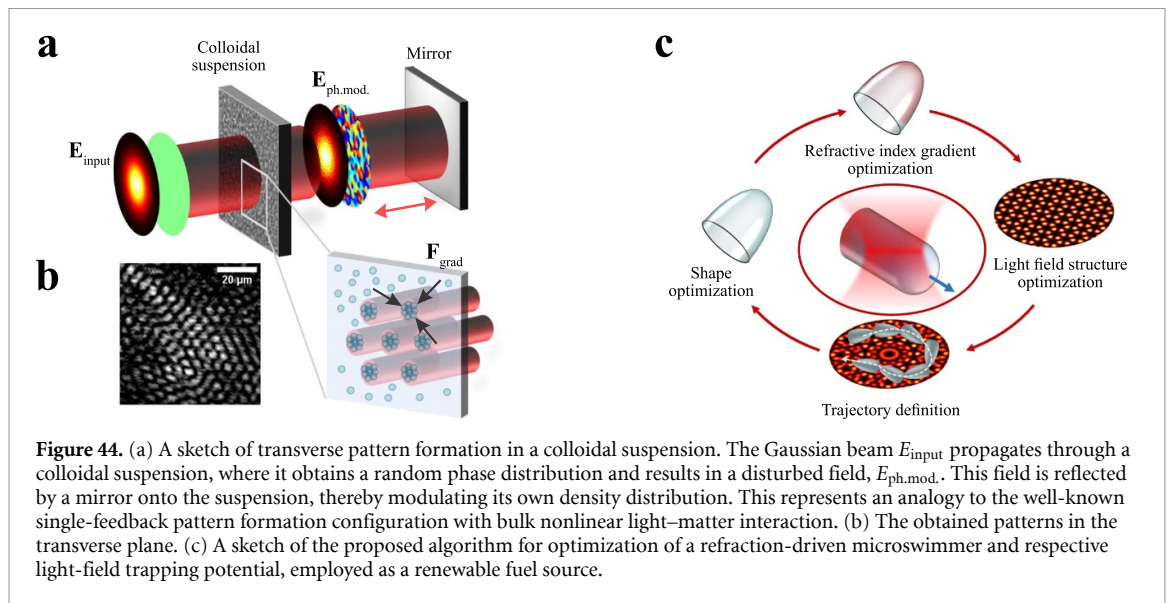
While most of the early experimental implementations of pattern formation have used bulk nonlinear optical materials, cold and hot atomic vapours were also shown to exhibit self-assembly, being driven by the collective interaction of single entities. This feedback-driven collective behaviour together with the previously shown self-assembly of colloids in an optical tweezer [300] are the solid reasons for one to also expect colloidal soft matter to exhibit self-organized pattern formation in a single-feedback configuration.

To realize dissipative self-assembly of colloidal matter far from equilibrium, a colloidal suspension is placed in an optical feedback system. The driving mechanism [301] is schematically shown in figure 44(a): a homogeneous Gaussian wave propagates through a thin layer of a colloidal suspension and obtains, therefore, a random phase distribution, induced by the initially inhomogeneous density of colloids. The wave being reflected by a feedback mirror propagates back to the colloidal layer, such that phase fluctuations are transformed into intensity fluctuations due to interference effects. Each colloidal particle—in the particular experiment these are polystyrene spheres suspended in water—experiences gradient forces, caused by the inhomogeneity of the light field, which pulls them into the intensity maxima while scattering forces are cancelled by the counter-propagating geometry. In this way, the optical feedback drives spontaneous pattern formation in a colloidal suspension. Thereby, the simple single-feedback configuration enables colloidal pattern formation while paving the way for active control over the self-organization process in colloidal matter. This approach allows for the simultaneous spatial confinement of multiple objects achieved in a single Gaussian beam representing an alternative setup to conventional optical tweezers. Since the optical forces strongly depend on the refractive landscape, i.e. the shape and 3D refractive index profile of the trapped particles, the corresponding parameters can be tuned accordingly to define the spatial dynamics driven by light.

#### Current and future challenges

The single-feedback configuration represents a great model system for the investigation of spatial self-assembly of dielectric nanospheres, demonstrating complex collective behaviour of soft matter under homogeneous illumination in various geometries. However, for many applications, such as targeted drug delivery or environmental remediation, a defined directional and controllable motion of the colloidal particles is desired. A promising, but challenging approach, allowing one to fulfil these requirements, is the implementation of functional and active soft matter capable of converting external energy into a directional movement. The impressing progress in the field of active microrobots [302, 303] in recent years exemplarily demonstrates the wide variation of mechanisms that can be employed to induce self-propulsion of colloidal particles, thus creating an ‘artificial fuel’ for the system. The most widely spread propulsion mechanism is based on chemical reactions, which may be catalyzed by light. However, the reaction products are often toxic for a living environment and, moreover, the induced propulsion direction can barely be controlled. An approach often employed to control the particles’ trajectories is their manipulation by a magnetic field [304]. Although a couple of successful experimental implementations of active control over spherical or more complexly shaped microswimmers with a magnetic field was demonstrated, sculpting a free-shaped 3D trajectory of a propelled soft particle is a demanding challenge. Here, again, light comes into play. Employing light as a renewable fuel source for the soft colloidal particle propulsion is firstly a particular advantage with respect to biomedical and environmental applications. Secondly, structuring light to obtain more complex





artificial fuel landscapes is already a resolved question [305]. Despite these clear advantages, until now, light structuring is only moderately employed for control over the trajectory and the speed of single swimming soft particles. In addition, the majority of until now proposed light-induced micromotors are driven by ultraviolet or infrared light sources and thus cannot be tunable in a broad spectral range, limiting the potential application fields to specific light sources.

Microfabrication of such a versatile light-driven particle, which is not wavelength selective, biocompatible, and able to demonstrate defined directional motion under illumination is one of the current challenges in the field. Here, employment of optical forces well known from the optical tweezers approach can be a smart solution for the next generation of soft colloidal microswimmers or even microrobots.

### Advances in science and technology to meet challenges

As outlined above, a promising approach to tackle the challenge of externally controlled directional soft-matter motion is to employ light as a driving fuel. Thus, the motion of single entities strongly depends on their shape and refractive index distribution being defined by light scattering and refraction. Recently, light-driven spatial self-organization of symmetric and asymmetric nonspherical colloidal particles was demonstrated experimentally under Gaussian beam illumination [306]. Varying the shapes and materials of the microswimmers together with spatially structuring illumination landscapes pave the way for observation of novel collective spatio-temporal dynamics in initially stochastic soft matter.

One promising procedure towards arbitrary sculpturing the 3D shape of a colloidal microswimmer is its fabrication by soft laser lithography. A pioneering demonstration of the directed motion of micrometre-sized wedges produced by a two-photon polymerization (2PP) process and additionally covered by a gold reflective nanolayer is published in [307]. Additionally, a 2PP process allows a continuous change of the refractive index distribution for certain materials, enabling laser-writing particles with gradient refractive index distributions. Thus, incident light on that particle acts as a direction-sensitive fuel and controls the transfer of the resulting momentum difference into mechanical motion. An experimental investigation augmented by numerical calculation of refraction-only-driven bullet-shaped particles can be found in [308].

Hence, the motion of a single particle is completely defined by its refraction properties and incident light field potential. The progress of the past decades in the field of spatial light modulation provides the control tools to tune both properties: firstly, the refractive index and the shape of a colloidal microswimmer using the soft lithography approach and, secondly, spatially structured light illumination. Moreover, a promising approach for computer-based definition of these control parameters is employment of machine learning algorithms (schematically shown in figure 44(c)), which have already found numerous applications in soft-matter research in recent years [309].

Colloidal microswimmers fabricated using soft lithography can be driven by light with a broad spectral range, as required, for instance, by environmental applications due to increasing conversion efficiency of the broad sunlight spectrum into the particles' motion. Moreover, the employment of refraction-driven microrobotics for biomedical applications, such as cell inspection or drug delivery, takes advantage of the light-source tunability, and the driving wavelength can be chosen according to the absorption spectrum of the investigated object. Additionally, the substrate used to fabricate a microswimmer employed in the soft

lithography process can even be biocompatible as, for instance, natural hydrogels. Thus, the proposed microfabrication approach has great potential, since it covers a broad range of requirements for emerging applications of artificial soft microrobots easily, and does not request additional chemical functionalization of any type.

### **Concluding remarks**

Self-organization of soft matter driven by light is a broad rapidly developing field with versatile possible applications in medicine, biology, environmental studies, and others. Moreover, the fundamental principles of self-assembly demonstrate complex nonlinear dynamics and are of particular theoretical interest. The evident potential of artificial soft-matter systems to mimic natural swarming dynamics drives research on functionalization and control over single microswimmers, making them transfer light energy into the directional movement. Both theoretical and numerical investigations in this field are strongly supported by machine learning approaches and, we believe, within the next decade will contribute to the development of highly efficient bioinspired light-responsive materials and will discover novel application potentials.

### **Acknowledgments**

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## Combination with spectroscopy

### 31. Raman scattering in (thermo)plasmonic tweezers

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#### Status

Optical spectroscopic interrogation of small systems such as molecules, nanoparticles, and microstructures in a solution is relevant to various aspects of science and (bio)analytical technology. Due to the small size of such entities, they undergo Brownian motion in a fluid at room temperature. To effectively interrogate them over a period of time, there is a necessity to confine these Brownian objects in space and time. Over the past few decades, optical trapping and tweezing methods have been extensively utilized to trap and probe micron-scale objects in a fluid with considerable success. Such tweezing platforms have also been integrated with optical spectroscopy methods, including fluorescence, Raman scattering, and various nonlinear optical methods.

Particularly, Raman scattering, in the form of Raman optical tweezers, has been utilized to study a variety of trapped systems, including biological cells and microstructures. Although Raman scattering is a powerful spectroscopy tool that is utilized to capture the chemical fingerprint of molecules and materials, it still suffers from low optical cross sections compared to Rayleigh scattering and fluorescence. Surface-enhanced Raman scattering (SERS) has emerged as a powerful tool to detect single molecules in a solution [310–312], wherein molecules interact with metallic nanostructures. The enhanced Raman signature is predominantly facilitated by the electromagnetic enhancement mechanism, in which plasmonic fields around the metallic nanostructures play a critical role. This makes SERS a chemically-specific, single-molecule spectroscopy tool at subwavelength scale.

There is an imperative to combine single-molecule Raman scattering with optical trapping, tweezing, and pulling [313] methods, especially at the micro- and nano-scale. Such integration not only expands the toolbox of solution-phase single-molecule optical spectroscopy methods, but also can be harnessed for micro- and nano-fluidic applications, where temporary confinement, aggregation, and release of molecules and nanostructures can alleviate the problem of clogging of fluidic channels. This has implications in clinical diagnostics and *in vivo* probing of molecules and nanostructures, where spatial, temporal, and spectral evolution of these entities can be probed concomitantly.

This has motivated researchers to combine nano-optical tweezer methods with single-molecule Raman microscopy methods and, to this end, emerging platforms based on plasmonic and dielectric nanophotonic elements have been explored to enhance and control force fields, together with electric and optothermal fields.

#### Current and future challenges

The integration of nanophotonic tweezer platforms with Raman microscopy methods brings with it new challenges and opportunities. Below we note specific questions and aspects from various viewpoints:

*Optical trapping viewpoint:* what are the optimized tweezer configurations for Raman scattering from individual nanostructures and single molecules? Can we utilize a single laser beam to concomitantly trap and perform Raman spectroscopy? If yes, what are the optimized illumination configurations? What are the advantages of using evanescent-wave Raman tweezers? Can they be extrapolated to optical fibre platforms for single-molecule detection? These questions are yet to be addressed in detail, and combining the optical tweezer toolbox with Raman spectroscopy can bring with it a new perspective and challenges.

*Molecular dynamics viewpoint:* what information can be obtained by studying Raman spectral evolution of macromolecules such as proteins and DNA in nano-optical tweezers? Can we effectively probe the conformational changes of individual biomolecules under nano-optical Raman tweezer confinement? Recently, plasmonic nanopore-based single-molecule spectroscopy has gained prominence. Specifically, the extraordinary acoustic spectroscopy method of Wheaton *et al* [314] has opened up a new direction to probe acoustic vibration ( $0.1\text{--}10\text{ cm}^{-1}$ ) of macromolecules in a trap. Understanding spectral evolution of complex biological systems and their interactions in such a platform will add new insights.

*Raman spectroscopy viewpoint:* traditionally, Raman spectroscopy in tweezer platforms probes spontaneous vibrational energy transitions of molecules and materials. Apart from this, nonlinear optical methods, such as coherent Stokes, and anti-Stokes Raman scattering and stimulated Raman scattering, can add great value to the interrogation of molecules and nanostructures. Integration of these nonlinear methods with nano-optical tweezers is yet to be explored in considerable detail.

*Plasmonics/nanophotonics viewpoint:* plasmonic and dielectric metasurfaces and metamaterials have opened up new avenues to control light at subwavelength scales. Adapting these materials for nano-optical Raman tweezing brings new opportunities, where parameters such as optical phases, amplitude, polarization, and spectral signatures can be tuned to control optical forces and Raman spectral enhancements. In such a scenario, the design and development of metasurfaces requires dual optimization of force fields and spectral enhancement features, and this will be an interesting direction for research in computation electromagnetism, where machine learning methods can be implemented.

*Optothermal interaction viewpoint:* excitation of molecules and materials, even in a solution phase, leads to optical heating. This heating effect is pronounced when a wavelength-resonant nanostructure (such as a plasmonic nanoparticle) is used for co-trapping and field enhancement. Such optothermal fields, if optimized, can be used as an advantage in nano-optical tweezers. An example of such a platform is thermoplasmonic tweezers [310, 312], in which optothermal fields around a plasmonic nanostructure are harnessed to trap and manipulate nano-colloids and spectrally interrogate molecules in the trap. Attention is needed to address a variety of questions such as: how do (bio)molecules interact with such an optothermal field in a trap? What are the new opportunities of opto-thermophoretic interactions with molecules and materials in such a trap?

We wish to emphasize that the above viewpoints are not exhaustive, and there are many interesting questions and challenges that we foresee as this field evolves.

### Advances in science and technology to meet challenges

Below, we discuss some relevant developments in nano-optical tweezers that have been or can be adapted to perform single-molecule Raman microspectroscopy.

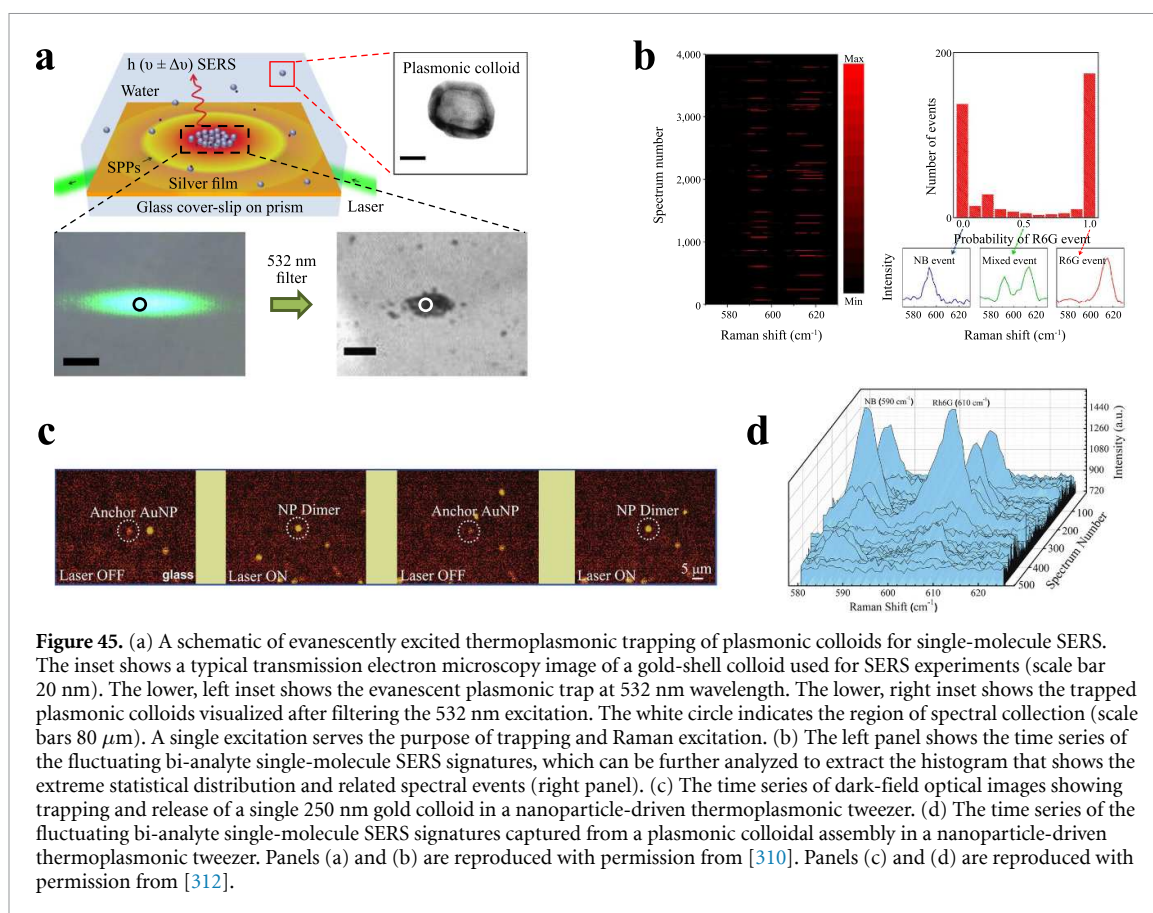
*Single-molecule SERS tweezers:* evanescent-wave thermoplasmonic tweezers with single-molecule detection sensitivity have been realized [310] for a large-scale plasmonic colloidal assembly (figure 45(a)). In this study, a plasmonic metal film is excited in an evanescent-wave configuration to trap a millimetre-sized assembly of plasmonic colloids. These assemblies are reversible, and can facilitate multiple plasmonic hot-spots for single-molecule bi-analyte SERS detection and analysis (figure 45(b)). A relevant aspect is that such an assembly can also be used for remote trapping of plasmonic colloids.

Recently, single-nanoparticle-driven thermoplasmonic Raman tweezers with single-molecule detection sensitivity have been realized [312]. The aim of such a platform is not only to trap and probe a single plasmonic colloid (figure 45(c)), but also to perform single-molecule SERS (figure 45(d)) in a small colloidal assembly driven by a single gold nanoparticle. This technique can be harnessed to trap and study the dynamic spectra of individual entities, such as biomolecules and nanoparticles.

Examples of optothermal tweezers which can be harnessed as single-molecule Raman tweezers:

- Tong *et al* [315] were one of the first to show microfluidic optical aggregation of plasmonic nanoparticles and the resulting SERS from those structures in a trap. Their study showed the ability of SERS traps to be adapted to microfluidic platforms.
- Wheaton *et al* [314] devised a double-nanohole-based plasmonic tweezer platform that can probe vibrational dynamics of nano-objects in an acoustic phonon regime. The significance of this work stems from the fact that Raman Stokes shifts as small as  $0.1 \text{ cm}^{-1}$  can be probed using this method.
- Fränzl *et al* [316] realized thermophoretic tweezers that can confine single amyloid fibrils for a period of more than 60 min. They also track the evolution of individual fibrils and measure its rotation diffusion constants.
- Liu *et al* [317] extensively studied opto-thermoelectric effects to capture and probe nanoscale entities, and their adaptation of antenna-based structures holds promise for resonance-enhanced SERS trapping studies.
- Jiang *et al* [318] utilized a so-called 'antenna-in-a-box' plasmonic tweezer platform to trap and study single quantum objects. This innovation can potentially be adapted to Raman trapping studies of individual biomolecules.
- Hong *et al* [221] showcased the ability to trap and probe individual biomolecules using opto-thermo-electrohydrodynamic tweezers. This has opened up new abilities to manipulate molecular systems and can be useful for Raman trapping studies.
- Gucciardi *et al* [319] utilized Raman tweezers to trap and interrogate micro- and nano-plastics in sea water. This is one of the most important applications of Raman nanotweezers, and has a direct impact on water pollution monitoring and control.

The above list is in no way comprehensive, but gives an overview of what has been achieved and what can possibly be adapted to study single molecules in Raman nano-optical tweezers.



**Figure 45.** (a) A schematic of evanescently excited thermoplasmonic trapping of plasmonic colloids for single-molecule SERS. The inset shows a typical transmission electron microscopy image of a gold-shell colloid used for SERS experiments (scale bar 20 nm). The lower, left inset shows the evanescent plasmonic trap at 532 nm wavelength. The lower, right inset shows the trapped plasmonic colloids visualized after filtering the 532 nm excitation. The white circle indicates the region of spectral collection (scale bars 80  $\mu\text{m}$ ). A single excitation serves the purpose of trapping and Raman excitation. (b) The left panel shows the time series of the fluctuating bi-analyte single-molecule SERS signatures, which can be further analyzed to extract the histogram that shows the extreme statistical distribution and related spectral events (right panel). (c) The time series of dark-field optical images showing trapping and release of a single 250 nm gold colloid in a nanoparticle-driven thermoplasmonic tweezer. (d) The time series of the fluctuating bi-analyte single-molecule SERS signatures captured from a plasmonic colloidal assembly in a nanoparticle-driven thermoplasmonic tweezer. Panels (a) and (b) are reproduced with permission from [310]. Panels (c) and (d) are reproduced with permission from [312].

### Concluding remarks

Combining Raman spectroscopy with optical tweezing methods based on nanophotonic platforms provides multiple opportunities to probe molecules and nanostructures down to a single copy limit. Such an endeavour has an impact not only in probing fundamental questions in chemical and optical physics, but also on applications such as *in situ*, *in vitro*, and *in vivo* bio-analysis and pollution monitoring. With the development of scanning probe methods, such as tip-enhanced Raman scattering, optical nano-Raman tweezing methods and their limits can be pushed to study intra-molecular vibrations in a trap. Such innovations will indeed open up uncharted research directions for the future.

### Acknowledgments

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## 32. Spectroscopic tweezers for micro- and nano-plastics detection

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### Status

Optical tweezers (OTs) enable trapping and manipulation of micro- and nano-particles dispersed in fluids, by exploiting the tiny forces exerted on matter by tightly focussed laser beams [110]. The first demonstration of OTs dates back to 1970 by Ashkin, a Nobel prize winner in 2018. Raman analysis in an optical trap (Raman Tweezers, RT) was first demonstrated by Ajito and Torimitsu [320], who showed the spectra of 40 nm polystyrene (PS) spheres. Hybrid instruments combining OTs with fluorescence and Raman spectroscopy are becoming increasingly popular, as they enable contactless measurements of size and composition. A variety of spectroscopic optical tweezers (SOTs) were implemented, integrating both single-trap and dual-trap configurations with confocal microscopy, total internal reflection, stimulated emission depletion microscopy, coherent anti-Stokes and surface-enhanced Raman spectroscopy (SERS) [60, 110].

RTs are gaining attention as a unique analytical tool for environmental sciences and food analysis, capable of detection and chemical identification of micro- and nano-plastics (MNPs) [319, 321–323]. Plastic items subject to atmospheric weathering do fragment into small debris called microplastics (size < 5 mm), and then fragment further down to small microplastics (<20  $\mu\text{m}$ ) and nanoplastics (<1  $\mu\text{m}$  [324]). Such particles are today almost ubiquitous in water ecosystems, soil, and air, from urban to remote areas [325]. Their spread into the alimentary chains is observed in food items (seafood, fruits, and beverages), and represents a potential threat to human health [326]. Occurrence data are, however, limited (for microplastics) or lacking (for nanoplastics) due to technological gaps in the detection and identification of sub-10  $\mu\text{m}$  particles [327]. RTs, with their ability to measure the size and chemical composition of individual particles, in complex fluids and down to the nanoscale, feature peculiar advantages with respect to standard SEM/EDX, micro-FT-IR, and micro-Raman techniques.

Future technological advancements of SOTs are expected to provide affordable and practical solutions to some of the major knowledge gaps to understand the fate of MNPs in the environment and food. These include chemical identification and quantification of the size, mass, and number of particles; detection in complex media, including liquid-digested samples; more sensitive light-based methods for fast nanoplastics identification down to the 10 nm level; portable equipment for automated and intelligent analysis of MNPs in batch volumes; integrated strategies for the concentration of small particles and detection surface contaminants; methods to monitor the fragmentation of individual MNPs under weathering and digestion conditions.

### Current and future challenges

To meet the methodological demands in environmental and food analysis, next-generation SOTs need to be compact, sensitive, fast, versatile, and deployable in the field. Challenges will change and become harder as we move towards the nanoscale, and include:

- *Quantification of particles* by size, mass, and material poses difficulties at different levels. Brownian diffusion of MNPs requires procedures to avoid re-counting. Ideally, particles should be driven in a confined stream to SOTs, be identified and measured one-by-one, and then be (optically) disposed, or better, sorted according to their nature. MNPs' weights vary from sub-femtograms (for 100 nm particles) to nanograms (10  $\mu\text{m}$  diameter). Mass determination via optical means is a formidable challenge that should be afforded in liquid environments.
- *Multispectral analysis*. Detection and sizing of sub-200 nm particles is demanding because of the low visibility of dielectric particles and diffraction-limited resolution. Fluorescence-tweezers, combined with far-field nanoscopy [328], are a promising solution to measure dye-stained nanoplastics [329] optically trapped in transparent media or in digested samples crowded with organic residues with subdiffraction resolution. A faster label-free classification tool could be obtained by implementing SOTs with deep-UV laser fluorescence, coherent anti-Stokes Raman, stimulated Raman or near-infrared absorption (780–2500 nm) spectroscopy [330].
- *Enhanced sensitivity* will be needed to tailor MNP detection towards the 10 nm scale. Plasmonic optical tweezers (POTs), by exploiting the enhanced spatially confined near-fields at the surface of plasmonic nanostructures [331], can be used to trap very small particles, for thermophoretic concentration and SERS. Integrating POTs with SERS is a promising solution towards high-sensitivity detection of surface contaminants.





**Figure 46.** Field-deployable spectroscopic optical tweezers will be designed to be compact and integrated with fluidic circuits capable of extracting samples from the environment, and filtrate and concentrate particles, prior to multispectroscopic analysis for plastic particle classification by size and materials.

- *Field-deployable setups* (figure 46) will require thoughtful consideration of system design trade-off, integrating fluidic circuitry for sample extraction (e.g. from ponds and rivers), multistage filtration (removal of debris and living organisms  $>20\ \mu\text{m}$ ), and pre-concentration (real samples can be highly diluted). A major challenge is the design and coupling of microfluidic circuitries to concentrate particles and drive the stream towards the trapping and sensing area. Dielectrophoretic and acoustophoretic techniques integrated in microfluidic chips could do the job. Compact optomechanical components will be needed, such as lasers, spectrometers, light detectors, and motorized and piezo stages for positioning. Accurate spectral assignment and large volumes of data (thousands of spectra) will pose challenges requiring artificial intelligence tools.
- *Particle's fragmentation*: studying the fragmentation of individual (trapped) particles offers unique opportunities to understand the degradation paths of MNPs. Challenges involve the design of OTs with sample compartments that emulate photo-oxidation, thermal/mechanical stress, and digestive erosion, integrated with sensitive particle-size determination tools.

### Advances in science and technology to meet challenges

As SOTs are based on photonic, (micro)fluidic, nano-engineered components and materials, developments in the field will benefit from technological advances in the design of photonic compact components, a smart integration among optomechanical and fluidic parts, and the addition of efficient nanoscale elements.

To afford the challenges, SOTs will likely exploit multiple laser beams for trapping and analysis, and be designed around complex lab-on-chip architectures. These will host input channels (for sample loading but also to add chemicals and/or enzymes and simulate digestion processes), followed by compartments for trapping and spectroscopic analysis, and output channels for selective disposal/sorting (e.g. by material and shape). Advances in microfluidics materials and design will be needed to fabricate compartments that are resistant to strongly acidic/basic environments, thin enough to provide access to high-NA microscope objectives, from both the top and the bottom, that permit imaging, trapping, position tracking and spectroscopy. Compartments need to be properly coupled to fluidic channels that are large enough to grant laminar flows and process volumes at speeds of  $1\ \text{l h}^{-1}$ . Compact multi-axis piezoelectric stages will be required for precise MNP positioning under the OTs. Integration of ultrasonic transducers would enable particle concentration by acoustophoresis.

Advances in lab-on-chip technology will embed nanostructured plasmonic and metamaterial surfaces in fluidic circuits, enabling POT platforms for nanocontrol of small dielectric particles, thermoplasmonic concentration, and plasmon-enhanced spectroscopy. New methodologies will be needed for SERS detection of MNPs and chemicals absorbed at their surface in a POT. Optical approaches to measure a particle's mass in air and vacuum are emerging, based on force modulation and levitodynamics techniques [332], but new

methods will be needed to tailor the sensitivity below the picogram regime and for measurements in liquids. Integrating wavefront shaping with spectroscopic detection is expected to speed up MNP classification, via the generation of multiple traps.

The development of dyes capable of selectively tagging different plastics would permit fast material discrimination, by implementing SOTs with multiwavelength lasers. Advances in deep-UV CW laser technology ( $\lambda_L < 250$  nm) will enable label-free fluorescence detection of MNPs ( $\lambda_{FL} > 300$  nm) and fluorescence-free Raman analysis ( $\lambda_R < 270$  nm). Single-particle photo-oxidation and fragmentation studies will benefit from variable wavelength UV-lasers in the UVB and UVA range (280–315 and 315–400 nm). White-light lasers can enable SOTs in the near infrared (NIR). Objectives corrected for chromatic aberrations up to 2500 nm will be needed for precise light focussing and collection.

Portable wi-fi-controlled Raman spectrometers, even handheld, are on the market. A clever coupling of these instruments with SOTs is a starting point towards compact field-deployable setups. All the parameters will be controlled remotely and the results will be visualized on rugged notebooks or tablet screens, empowered by artificial intelligence for particle classification and big data analysis.

### Concluding remarks

In conclusion, SOTs are taking their first steps in the fields of environmental sciences and food analysis. Their first applications to real-world samples, limited to Raman analysis, have been shown. Either when used to trap and analyze single particles or when coupled to field-flow fractionation techniques, SOTs have the potential to fill the technological gap in MNP detection. Future research and development will be oriented towards the exploration of the full potential and limits of SOTs in terms of sensitivity, size limitations, multispectral analysis, and chemical information that can be extracted from contaminated MNPs and in complex environments. Portable SOT configurations will enable on-site data acquisition (e.g. on a boat, dock, along a production line, or even in an underwater vehicle), allowing scientists a broad spatial coverage (rivers, lakes, ponds, seas) and enabling them to collect time-series data.

### Acknowledgements

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## Biophysical applications from biomolecules to cells

### 33. Mechanosensitivity of molecular bonds and enzymatic reactions

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#### Status

Mechanical energy is one of the driving forces of living systems. Animals, tissues, and cells respond to mechanical stimuli and adapt to them. This capacity is inherently coupled to the susceptibility of enzymatic reactions and molecular bonds to mechanical force, which shape the energy profiles of biomolecule structural states (figure 47(a)). Therefore, mechanochemistry and mechanoenzymology, i.e. how mechanical forces affect chemical and enzymatic reactions (figure 47(b)), is at the base of mechanotransduction processes, which translate mechanical signals into cascades of biochemical reactions that shape gene-expression profiles and live cell function.

Optical tweezers have been applied to investigate the force dependence of enzymatic reactions since the mid 1990s. Studies on molecular motors, such as myosin and kinesin, have pioneered the field and allowed the measurement of nanometre-sized motor steps, piconewton forces, and kinetics on a time scale of few milliseconds. As the spatial resolution of the technique improved, it became possible to directly observe the movements of enzymes, such as RNA polymerase, which reads DNA in single base pair steps ( $\approx 0.35$  nm) to synthesize mRNA [333], and the ribosome, which moves mRNA in single codon steps ( $\approx 1$  nm) during protein synthesis [334]. The achievement of optical tweezers with angstrom resolution was, thus, a major breakthrough in the field, revealing for the first time how force influences transcription and translation processes.

Meanwhile, improvements in temporal resolution allowed researchers to dissect the chemomechanical cycles of motor proteins with increasing detail, unveiling multiple conformational changes during force production in myosin and kinesin motors. These discoveries pushed optical tweezers towards few-microsecond temporal resolution, which represents the current state of the art [144, 335].

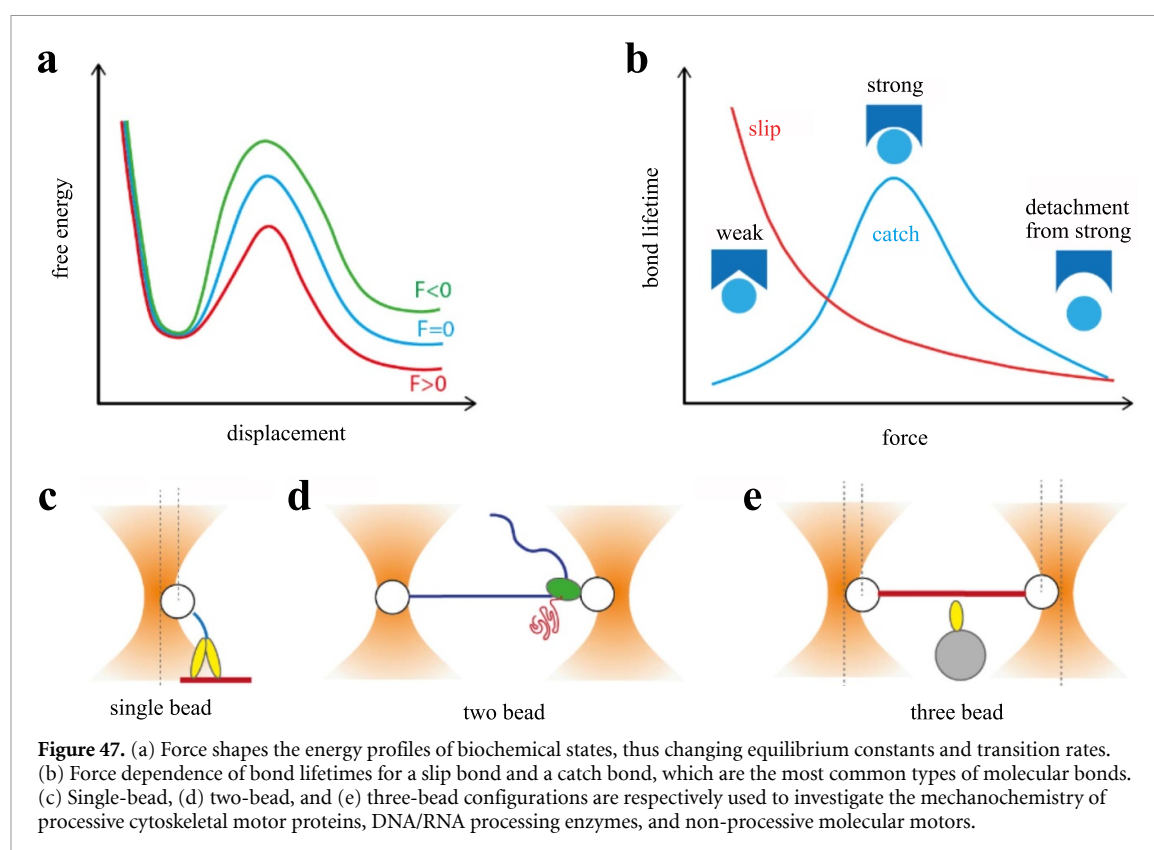
The achievement of such detailed measurements was made possible by the development of a plethora of different experimental configurations. Among the most common, a single-bead assay is usually applied to processive motors, such as conventional kinesin and myosin V (figure 47(c)), a suspended two-bead assay has been employed to investigate DNA- and RNA-processing enzymes with angstrom resolution (figure 47(d)), while a three-bead assay is used for non-processive motors, such as muscle myosin (figure 47(e)) [60, 336].

Another important class of experiments enabled by optical tweezers investigates the kinetics of molecular bonds and their force dependence. Such studies have allowed the understanding of important biomolecular interactions, such as receptor–ligand interactions, which underlie the communication of cells with the external environment, or interactions of proteins with the cytoskeleton, which are implicated in cell shape, mechanics, and motility. Two approaches have mainly been used to study the load dependence of molecular bonds: dynamic force spectroscopy and force-clamp spectroscopy. In dynamic force spectroscopy, force on the bond is increased at different loading rates and the rupture forces are measured. In force-clamp spectroscopy, the bond lifetime is measured under different constant forces. While the latter method allows direct measurement of the load dependence of bond lifetimes (figure 47(b)), the two approaches have their own pros and cons, and theoretical frameworks to switch from one measurement to the other have been developed [337].

#### Current and future challenges

Recent decades have seen impressive advancements in optical tweezers resolution. Spatial resolution has reached the limit dictated by thermal forces, which are inherently present in single-molecule studies in aqueous solution at room temperature. Temporal resolution has reached the limit imposed by the mechanical relaxation time of the bead probe and the connected biological molecules, which is also a constitutive element of the experimental method. Current resolution limits will be difficult to overcome, but the spatial and temporal resolution limits that have been reached, on the angstrom and microsecond scales, respectively, will be sufficient to explore fine details of most enzymatic reactions and biomolecular interactions. The application of state-of-the-art techniques to a plethora of motor proteins and molecular bonds will allow us to explore fine details of their function and mechanical regulation.

Meanwhile, the research field is now facing the big challenge of increasing the complexity of *in vitro* reconstituted systems to bring them closer to real-world biological systems. Typical optical tweezers



experiments involve the study of the interaction between two single molecules, whereas multimolecular interactions and complex regulatory mechanisms are most common in cells.

Prototypical examples are the molecular complexes that form at junctions between cells (adherens and tight junctions), between cells and the extracellular matrix (focal adhesions), or between the nucleus and the cytoskeleton (LINC complex), which comprise a large number of adaptor proteins that link the cellular or nuclear membrane to the cell cytoskeleton (figure 48(a)). Although these molecular complexes together with mechanosensitive ion channels are supposed to play a pivotal role in mechanotransduction processes, their mechanoregulatory properties are largely unexplored, also because of the lack of adequate techniques to study multimolecular interactions with sufficient detail.

Similarly, the mechanistic properties of motor protein function have been mostly explored through the interaction between a single motor protein (or functional subdomains) and a cytoskeletal filament; whereas molecular motors in cells are regulated by a large number of binding partners, cytoskeletal filaments are arranged in complex networks through an array of actin and microtubule binding proteins, and the different motor proteins work in teams that are connected through lipid vesicles (figure 48(b)).

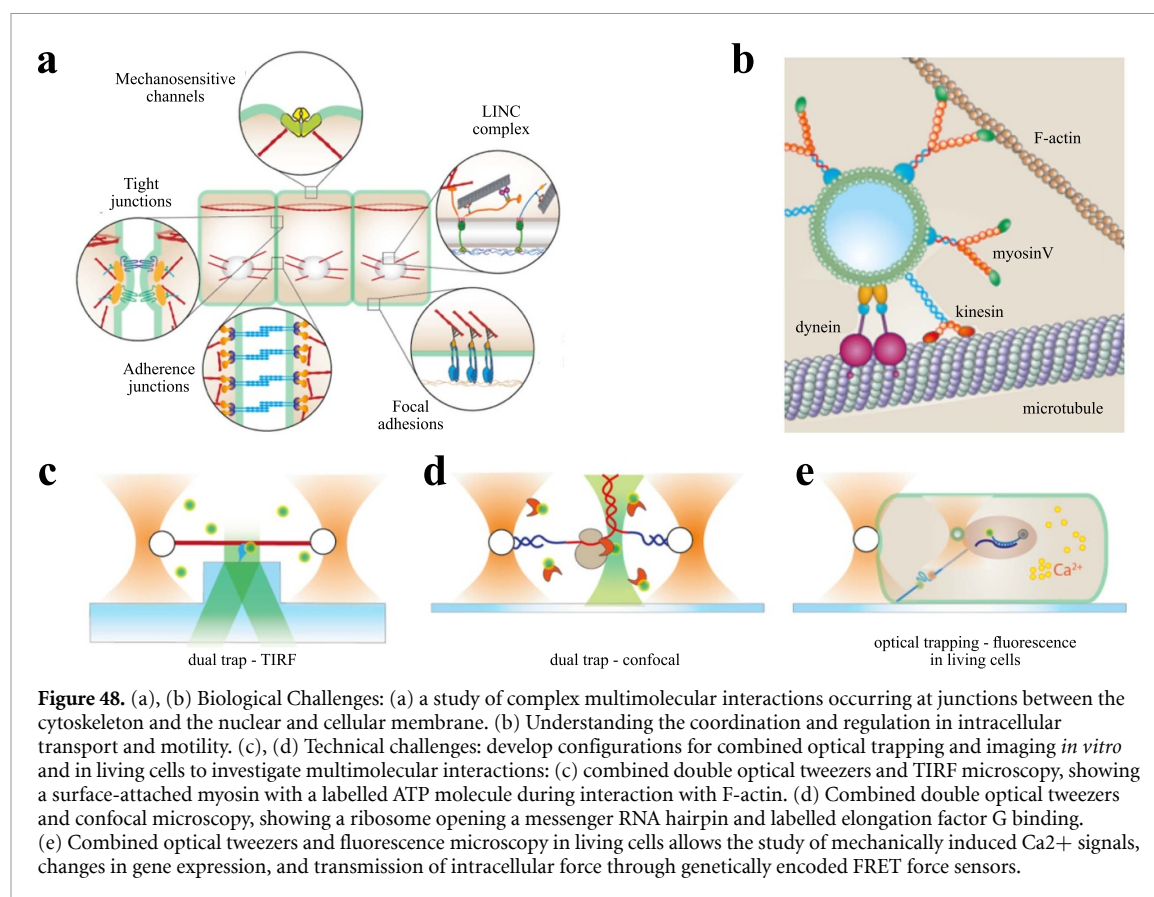
Moreover, optical tweezers *in vitro* experiments are usually performed under non-physiological conditions. For example, ATP concentration in motor protein experiments is usually in the micromolar range to slow down motor speed and better distinguish steps, whereas ATP in cells is in the millimolar range. Analogously, experiments are performed at room temperature (22 °C) instead of 37 °C, and salt concentration is usually lower than in the cell cytosol to increase the number of molecular interactions and statistics. However, extrapolation of these data to physiological conditions is not trivial and the emerging features might differ significantly from what occurs in cells.

### Advances in science and technology to meet challenges

Future advances in the field will critically rely on the development of novel methodologies and techniques for the study of the mechanochemistry and mechanoenzymology of biological systems under experimental conditions that closely mimic the cellular environment. Ideally, future technologies should enable researchers to investigate single molecules in real cellular or multicellular systems.

The need to increase the complexity of nanomechanical measurements *in vitro* is pushing the field towards combining optical tweezers setups with techniques that allow the simultaneous detection of multiple signals. Optical tweezers have been frequently combined with fluorescence microscopy, due to its specificity and single-molecule sensitivity. Pioneering efforts in this regard were driven by Yanagida's laboratory, where a combination of a three-bead assay with total internal reflection fluorescence microscopy was developed to





detect the binding of fluorescently labelled nucleotides to muscle myosin to observe the chemomechanical coupling between force production and ATP hydrolysis [338] (figure 48(c)). More recently, a suspended dumbbell assay was combined with single-molecule fluorescence microscopy and microfluidics to investigate homologous recombination by RAD51 proteins on single-stranded DNA [339]. Later, Comstock *et al* combined angstrom-resolution optical tweezers and confocal microscopy with single-molecule sensitivity to detect changes in DNA extension induced by protein binding [340]. A similar configuration was later used to investigate how a ribosome's internal conformational changes are coupled with the activity of translocation factors to unwind mRNA secondary structures [341] (figure 48(d)). Heller *et al* combined optical tweezers with stimulated emission depletion (STED) super-resolution microscopy to investigate binding of transcription factors on DNA and their diffusive search of target sequences with high spatial resolution [342]. Such combinations of optical manipulation and fluorescence microscopy (also known as fleezers) will open the way to studies on the multimolecular interactions occurring at cellular junctions between adaptor proteins and cytoskeletal filaments, a fundamental step towards a better understanding of mechanotransduction mechanisms.

Significant efforts have also been made in the field of motor proteins to study how teams of motors coordinate their stepping. Different assays have been developed to study motor cooperativity in teams of kinesin motors, multiple processive myosin V, or arrays of muscle myosin motors interacting with unregulated [343] and regulated [344] actin filaments. An impressive effort allowed Lombardo *et al* to reconstitute *in vitro* 3D actin networks onto which fluid-like liposomes were transported by Myosin Va teams [345]. The authors were able to define each actin filament's 3D spatial position using super-resolution stochastic optical reconstruction microscopy (STORM) and the 3D trajectories of the myosin-transported liposomes moving within the actin network by single-particle tracking. We foresee that the application of optical tweezers within this or similar assays will allow a better understanding of how motor proteins experience force in living cells.

### Concluding remarks

Methodologies that allow one to probe single enzymatic reactions and molecular bonds in living cells are the ultimate step towards understanding the complex multimolecular interactions that occur *in vivo*. Among the many applications, optical tweezers have been applied in living cells to measure the strength of single molecular bonds and single steps of motor proteins while, in combination with fluorescence microscopy, to

probe mechanically induced ionic or genetic signals [346] (figure 48(e)). A promising tool for the measurement of force in living cells with molecular detail is given by force sensors based on Forster resonance energy transfer (FRET) [347], which can be genetically encoded and combined with optical tweezers, opening the way to investigate how mechanical signals propagate in living cells [348]. Still, the complexity of the cellular environment poses notable limitations with regard to accessing quantitative measurements with single-molecule detail, and future developments of novel and complementary techniques will play a key role in advancing the field.

## Acknowledgements

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## 34. Cell mechanics and mechanotransduction

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### Status

Applications of optical tweezers to biological systems have been, and remain, one of the outstanding successes of the technique. Very shortly after the first optical tweezers experiments, Arthur Ashkin showed that damage-free optical trapping of biological objects could be facilitated using near-infrared laser light [13]. In this early work both whole cells (bacteria, protozoa, yeast, red blood cells), and subcellular structures (chloroplasts within green algae, organelles within protozoa) were trapped and manipulated without damage. Optical trapping of living cells and subcellular structures continues to have important impacts in fields ranging from environmental biotechnology to molecular genetics and cancer.

In this section we review applications of optical tweezers to biological systems, where the tweezers are utilized to either measure mechanical properties or mechanically stimulate a response. We highlight a few key examples from a substantial literature that demonstrate the versatility of optical tweezers across scales, from intracellular signalling to movement of the whole organism, and encompassing both biological and synthetic biological systems.

Optical tweezers have been used to measure global-cell properties, such as the elasticity of whole red blood cells, finding a link between the mechanical properties of cell deformability and medical conditions such as diabetes [349]. Alternative trapping geometries, such as the fibre-based optical stretcher [350], have also been used to induce whole-cell deformation for mechanical phenotyping of, e.g. cancer cells. Alternatively, mechanical properties of localized areas of the cell, for instance a region of the cell membrane, can be measured using a microbead handle to pull a membrane tether (figure 49(a)). From the applied force (inferred from the displacement of the microbead in the calibrated trap) and the extent of the tether, the membrane stiffness can be determined. De Belly *et al* [351] used this method to measure membrane stiffness of pluripotent stem cells, elucidating the signalling mechanism that regulated the decrease in membrane tension required for subsequent shape change at cell differentiation.

Bolognesi *et al* [352] pulled tethers from a pair of synthetic vesicles by drawing them apart after adhesion, thus forming interconnected compartments which remained chemically distinct, as shown by fluorescence imaging (figure 49(b)). Vesicles were also stimulated to fuse and merge using laser light to heat gold nanoparticles attached to the vesicle surfaces (figure 49(c)). Here, three vesicles contained separate components required for protein synthesis, leading to expression of green fluorescent protein (GFP) in the fused vesicle, also referred to as the cell mimetic microreactor.

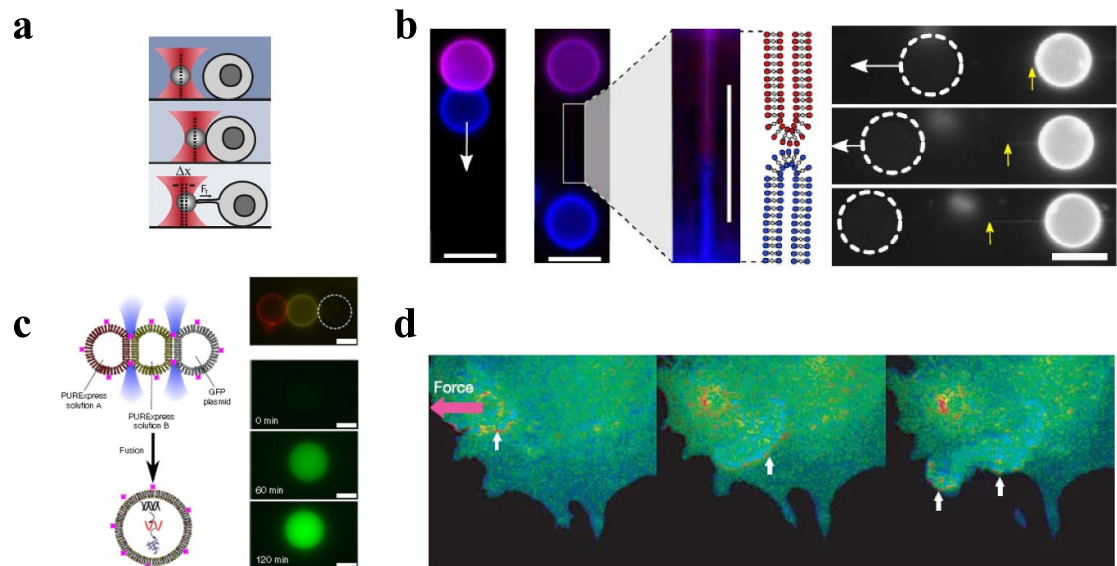
Insight into the biochemical response of a cell to mechanical stimuli was previously obtained by Wang *et al* [353], who applied a force to the transmembrane integrins using an optically trapped microbead, and observed the subsequent wave of activation of Src across the cell using Forster resonance energy transfer (FRET) (figure 49(d)).

### Current and future challenges

Although optical tweezers have enabled remarkable progress and discoveries in the life sciences, many challenges remain, both physical and biological, that will require significant scientific and technological advances.

One such challenge is optical trapping *in vivo*. While considerable insight has been gained from *in vitro* experiments on single molecules and cells, even these experiments are not straightforward. Frequently, the molecules or cells under study are purified or freed from their 'normal' surrounding complex environments of the intracellular space or the extracellular matrix, respectively. Furthermore, since cells, from bacteria to human cells, form part of larger 3D systems, it is clearly desirable to scale up experiments to multicellular systems, tissues, or even whole organisms, particularly when considering signalling between cells, or physiological function.

One field where cell–cell interactions are key is immunology. Interaction between cells is at the core of the immune response, and influences virtually all aspects of immunity; however, it is difficult to obtain precise control over experimental parameters, such as interaction times or interaction strengths. Optical tweezers certainly have a role to play in immunological studies as they have the facility for precise control over cell–cell interactions (both temporally and spatially), which aids the development of quantitative immunological models, particularly through the use of peptide-coated beads to mimic antigen-presenting cells since the molecular density on the bead surface is known and can be controlled [354].



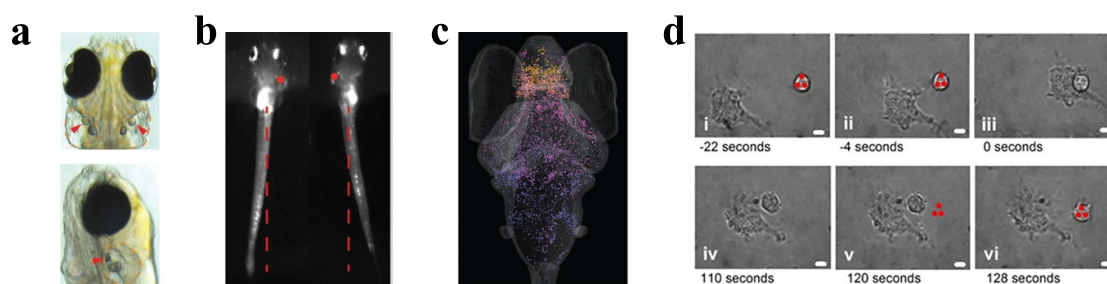
**Figure 49.** (a) Membrane tether pulling from pluripotent stem cells using optical tweezers. A microbead handle is adhered to the cell membrane and pulled away from the cell. The displacement of the bead from the trap equilibrium position ( $\Delta x$ ) and the tether length is used to calculate the membrane tension ( $F_T$ ). (b) Tether pulling between biomimetic vesicles. The vesicles are brought together using optical tweezers, they adhere, then are pulled apart (white arrows), forming a thin strand between the two, with no mixing of the contents of the vesicles. The left images show vesicles containing purple and blue fluorophore, and the right image shows fluorescent (white) and non-fluorescent (dashed circle) vesicles. Yellow arrows indicate anchor points where the two vesicles adhere. Scale bar = 10  $\mu\text{m}$ . (c) Vesicle manipulation and fusion using optical tweezers. Three vesicles containing (i) tRNAs, amino acids and rNTPs, (ii) ribosomes, T7 RNA polymerase and other factors, and (iii) GFP plasmid (specifically, the DNA template and the transcription machinery and translation machinery) are fused by heating gold nanoparticles attached to the surface of the vesicle and GFP protein is synthesized in the fused vesicle. The fused vesicle is labelled the 'cell mimetic microreactor'. Scale bar = 5  $\mu\text{m}$ . (d) Visualization of the cellular biochemical response to mechanical force. A fibronectin-coated microsphere handle is adhered to the cell membrane via integrin receptor proteins and is pulled using optical tweezers (applied force shown by pink arrow). The resulting FRET signal showing Src activation was observed as a blue wave (indicated by the white arrows) traversing the cell to a distal location. Panel (a) reproduced from [351] under Creative Commons CC-BY. Panels (b and c) reproduced and adapted from [352] under Creative Commons Attribution 4.0 Public License. Panel (d) reprinted with permission from Springer [353].

Further challenges include the extraction of quantitative data from trapping in complex environments, which often requires precise calibration of the optical trap derived from observing the Brownian motion of a trapped particle. While this is straightforward and routinely performed for spherical particles in water, to calibrate the optical trap *in vivo* or *in cyto* is challenging for a number of reasons: the trapping beam is distorted as it passes through the cell membrane, the cytoskeletal network, and membrane-bound organelles of the cytosol, plus the trapped object itself may be irregular in shape and in a crowded and complex environment with spatially and/or temporally varying refractive index and viscoelasticity throughout the volume. Additionally, active processes within cells, e.g. polymerization and depolymerization of the cytoskeleton, continually exert forces on a trapped particle. As a result of this complexity, standard calibration methods that are based on predictable thermal fluctuations alone can no longer be used. For optical tweezers to be used at their maximum potential as a force sensor or force actuator for living systems, alternative strategies are urgently required.

### Advances in science and technology to meet challenges

Some progress towards meeting these challenges can be made using physical techniques. For example, imaging through highly scattering biological tissue can be enabled using adaptive optics technology [17]. In adaptive optics the wavefront aberrations introduced by propagation through a turbid medium are corrected via phase control of the incoming laser beam. This can be achieved using a spatial light modulator (SLM) to pre-compensate the phase shifts produced by scattering. Furthermore, advances in technologies have enabled dynamic corrections with speeds of several kHz.

Alternatively, a judicious choice of specimen can greatly aid *in vivo* optical trapping experiments. The transparency of the zebrafish embryo has led to its role as a model system for studying the mechanisms of development and disease. Otoliths (calcium carbonate crystals or 'ear stones') in the embryo inner ear (figure 50(a)) are responsible for acceleration sensing. Optical tweezers have been used to apply a force to otoliths *in vivo* to mimic motion of the organism [17]. The embryo's tail was observed to move in response to the force exerted on the otolith, thereby demonstrating a behavioural response of an entire organism that was



**Figure 50.** (a) Top and side views of the zebrafish embryo, showing the inner ear (marked with dashed orange circles) and the otoliths (indicated with red arrows). Otoliths are around  $55\ \mu\text{m}$  in diameter. (b) Movement of the embryo tail (from the red dashed line) in response to an applied optical force on the otolith (marked with a red dot). (c) Distribution of neuronal intensity profiles in the brain of the zebrafish embryo. (d) A study of interaction forces between suspended T-cells and adherent dendritic cells. The three red dots show the positions of holographically generated optical traps that are used to steer the T cell and measure adherent forces. Panels (a)–(c) reproduced from [17] under Creative Commons Attribution 4.0 Public License. Panel (d) reproduced from [355] under Creative Commons Attribution License.

stimulated by optical tweezers (figure 50(b)). Additionally, the use of optical tweezers on these structures meant that the organism could be held stationary and therefore imaged with high resolution using selective plane imaging microscopy. Whole-brain calcium imaging with cellular resolution was achieved using genetically encoded calcium indicators, generating a brain-wide map of the cells of the vestibular system (figure 50(c)).

Holographic beam shaping using SLMs also enables dynamic shaped traps, for example a triple-beam trap used for the study (and control) of cell–cell interactions, such as in the initial stages of an immune response (figure 50(d)). Here, the force between T-cells and dendritic cells was measured, and a significantly greater force was required to separate T-cells from their specific antigen-presenting dendritic cells compared to those without the antigen [355]. Significantly, a change in the measured adhesion force due to the intervention of pharmacological therapies demonstrates the emerging role of optical tweezers in drug discovery for inflammatory disease and immunotherapy research.

Most of the work described so far measures or exerts forces in the image plane (2D), but cells and multicellular systems are 3D. Accurate and high spatial resolution 3D tracking of trapped microspheres is possible using a novel technique that images multiple focal planes simultaneously [356]. This method permits accurate 3D trap calibrations that are necessary to make force measurements and perform microrheology in 3D biological systems.

### Concluding remarks

Despite the complexities inherent in optical tweezers experiments on biological systems, the progress that has been achieved to date is remarkable. However, significant challenges remain when applying the method to arbitrary systems that are not chosen for favourable properties, e.g. embryonic stem cells that are not sensitive to external mechanical cues [352], or organisms that are optically transparent [17]. Recent technological development has gone some way to meeting these challenges, and in the process revealed yet more fascinating biology. Further advances may be envisaged through the combination of optical tweezers with complementary techniques, such as super-resolution microscopy, selective plane imaging microscopy, multiplane imaging, spectroscopy, high-throughput (microfluidic) technology or acoustic trapping, as well as the development of novel molecular probes to elucidate cell signalling mechanisms in response to the stimulation and interaction experiments made possible by optical tweezers. In turn these can be expected to realise advances in emerging application areas, such as neuroscience, immunology, or synthetic biology. In conclusion, optical tweezers are a unique tool that enable remote, non-contact manipulation, and exertion of forces on single cells and subcellular structures. As such they are expected to reveal new biology across scales: from molecular pathways to cell behaviour and fate to whole animal behaviour and phenotypes.

### Acknowledgments

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### 35. Quantifying material properties of living matter

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#### Status

Optical tweezers are one of the few nano-tools capable of reaching inside living organisms and soft matter, essentially without perturbing the system while making precise measurements of forces, distances, and material properties. Thus, they are a highly valuable tool to quantify the physical properties of biological matter that influence the processes that are essential for life. Here, we present their application to the investigation of the material properties of the live cell cytoplasm.

A convenient way to characterize material properties of the cellular cytoplasm is to follow the stochastic motion of a tracer particle, which can be endogenous or artificially placed inside the cell, as exemplified in [357], where lipid granules in *S. pombe* cells were tracked. In this case, the optical tweezers are merely used for their ability to precisely track the position,  $x(t)$ , of a particle with refractive index contrast as a function of time,  $t$ . Using photodiodes, such tracking measurements can be performed at frequencies up to the MHz range, thus uncovering viscous and viscoelastic properties in a large frequency range. This is important because the viscoelastic properties of biological tissue depend strongly on the probing frequency, with passive and active processes taking place at different time scales.

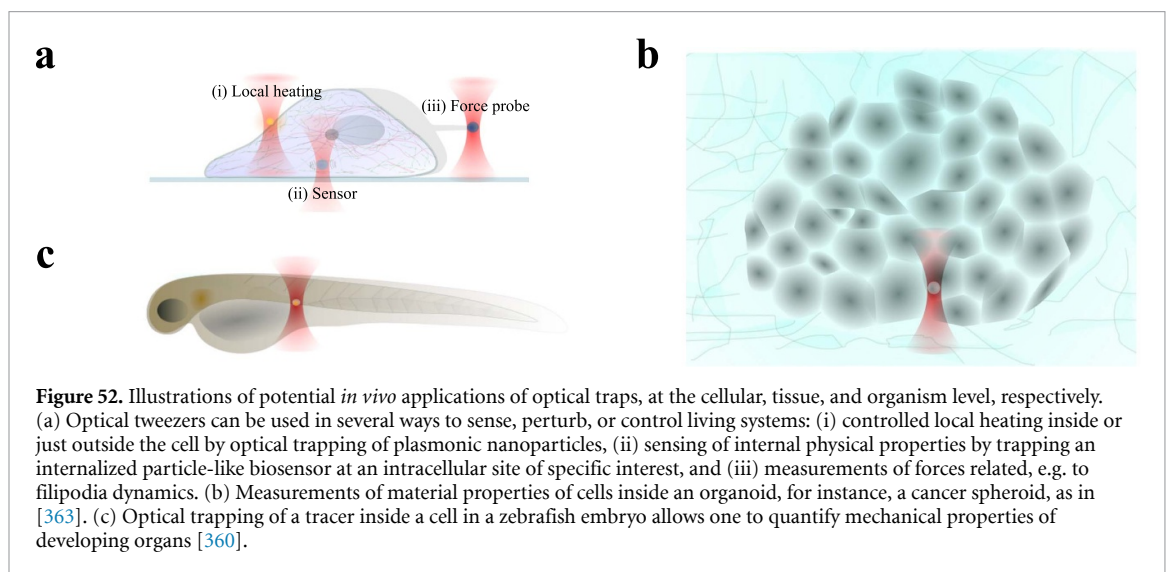
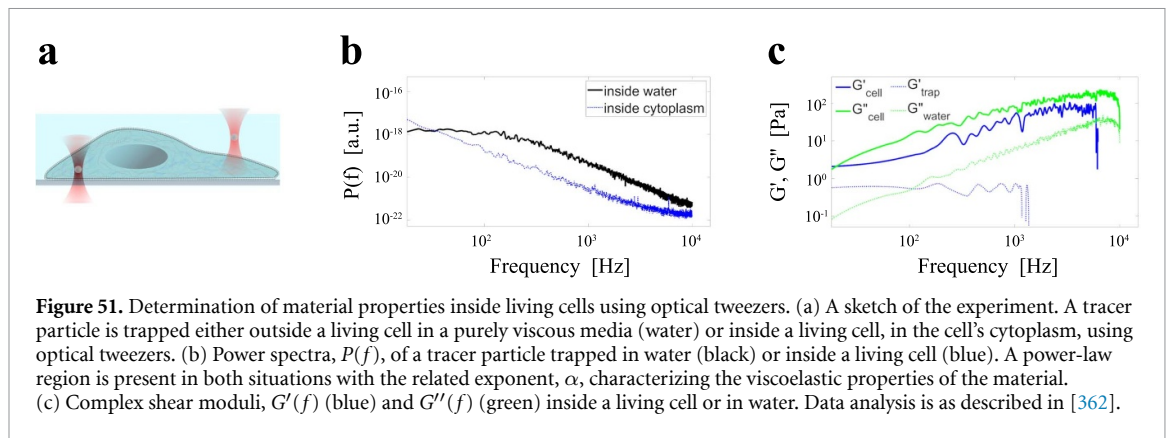
An informative physical parameter which can be extracted from a positional time series is the scaling exponent,  $\alpha$ . This exponent characterizes the root-mean-squared displacement of the probe particle,  $\langle \Delta x^2(t) \rangle \propto t^\alpha$ , while also characterizing the power-law behaviour of the positional power spectrum,  $P(f) \sim f^{-(1+\alpha)}$ , which is typically present in the kHz range, relevant for cytoskeletal dynamics. Also,  $\alpha$  appears in the complex shear modulus with real and imaginary frequency-dependent parts,  $G'(f)$ ,  $G''(f) \sim f^\alpha$ , describing the viscous and elastic components. Figure 51 displays an example of  $P(f)$ ,  $G'(f)$ , and  $G''(f)$ , obtained from tracking tracer particles in water and inside living viscoelastic embryonic stem cells. In a viscoelastic medium, the tracer particle is influenced both by the viscous and elastic components of the medium (the cytoplasm) and by the (weak) optical trapping potential, where a simple inverse relation between  $\langle x^2 \rangle$  and the trap spring constant does not hold. To address this, one needs to employ appropriate procedures [358, 359]. When carefully avoiding the frequency range affected by the trapping potential, an analysis, as illustrated in figure 51, provides quantification of material properties with subcellular precision inside individual cells, tissues, or whole organisms. Examples of this are provided in the following section.

#### Current and future challenges

A biophysical challenge addressable by optical tweezers is to link material properties of live matter with processes that are essential for the cell cycle that regulate reproduction, differentiation, and growth. In one example, the cell cycle of fission yeast *S. Pombe* [357] was addressed. By analysing the scaling exponent,  $\alpha$ , the cell cytoplasm was found to be significantly more viscous and less stiff when the cell is undergoing mitosis (active cell division) in comparison to when it is in the interphase. This was attributed to the higher abundance of cytoskeletal biopolymers, such as actin or microtubules, increasing the stiffness of the cytoplasm during the interphase. A recent study [187] used optical tweezers to address the same important question with Madin–Darby canine kidney cells as the model system: phagocytosed 1  $\mu\text{m}$  particles were tracked and the study concluded that the cytoplasm (however, not the cortical region) became softer and more viscous during mitosis, in accordance with the observations in *S. pombe* [357]. One way for the cell to control the cytoplasmic viscoelasticity is through protein-mediated crosslinking of actin filaments, as also recently probed by optical tweezers [361].

The differentiation of stem cells is of crucial importance for the development of a functional organism. Stem cell differentiation depends strongly on the mechanical properties of the substrate on which they are cultured, or on the niche in which they grow, and it is a challenge to understand how cell fate relates to material properties of the cell itself and of its niche. Optical tweezers experiments have correlated the development of pancreatic organoids and the viscoelastic properties of the matrix in which they are embedded. These studies have found that the degree of pancreatic branching depends on the stiffness of the matrix [362]. Also, optical tweezers were used to investigate the material properties at subcellular level in the gut region of live and physiologically competent zebrafish embryos (as illustrated in figure 52(c)); these studies found that the cells comprising the gut were significantly more elastic than those in surrounding tissues, and related these differential mechanical properties to organ development [360].





It is a major challenge to understand how cancer cells turn metastatic and how this may be circumvented. Optical tweezers have also uncovered how the properties and behaviour of cancer cells are linked to the material properties of the cell and its matrix. A tumour is often discovered because the tissue has an increased stiffness, caused by an increased density of collagen fibres in the extracellular matrix. Optical tweezers were used to demonstrate that only invasive cancer cells can adjust their cytoplasmic material properties in response to the material properties of their matrix [363]. Also, it was shown that cancer cells belonging to a spheroid and leading the invasion into collagen matrices are more viscous compared to cells in the spheroid centre.

### Advances in science and technology to meet challenges

While optical tweezers are powerful tools to quantify and map out material properties in living cells with subcellular resolution, thereby helping to overcome the challenges outlined in the preceding section, one needs to be aware that intracellular material properties change as a function of time. Hence, it is important to control the frequency or timescale of observation. A conclusion drawn at a certain frequency or timescale might only be relevant for this particular condition. Also, if one uses, e.g. endocytosed or phagocytosed particles, the properties probed are (only) those of the related pathway and not of the entire cytoplasm (unless there has been a specific release from the pathway). Hence, it is important to advance the technology and the subsequent analysis to meet the challenge of observing viscoelastic properties at specific and well-defined frequencies relevant for the mechanism at play.

To conduct optical tweezers measurements in a nearly non-invasive manner, and thereby overcome challenges related to working *in vivo*, it is necessary to advance the technology even further to avoid, or minimize, temperature increase and phototoxicity in live specimens due to absorption of the laser light. Based on absorption in water and of biomolecules like haemoglobin, a laser wavelength in the near-infrared region seems preferable. Heating and phototoxicity may further be reduced using a structured or pulsed trapping laser beam rather than a CW Gaussian beam profile [364]. However, even when using CW lasers and typical laser powers (up to some 100s mW), such as in the studies presented here, the observed

temperature increase is typically less than 1 K. Further, particle types that allow a reduction in laser power while still measuring a significant signal magnitude will be highly useful for overcoming current challenges. As an example, highly doped upconversion nanoparticles [211] give the promise of applying significantly higher forces than that proven possible by optical tweezers and with particles which appear to be non-toxic for living cells. This would be an important step in advancing quantitative force measurements in living cells and organisms, as well as for optical tweezers, to approach a force range that, until this date, has only been achievable by atomic force microscopy (AFM). While optical tweezers can be operated in an almost non-invasive manner, also deep inside living organisms, AFM cannot reach inside a living cell, or a living organism, without perturbing the membrane, hence, causing serious physiological damage.

Another promising method to overcome current challenges in sensitivity and to actively perturb or control cellular systems is to introduce particle types that may trigger cellular responses or act as intracellular biocompatible sensors, as illustrated in figure 52. One example of such nanoparticles are nanodiamonds with NV defects, a system that has demonstrated capabilities as sensors of temperature or magnetic fields. Plasmonic nanoparticles are also quite interesting, as their temperature increase can be controlled externally by the trapping laser, and their local heating can be used to provoke and control cellular responses.

### Concluding remarks

Optical tweezers can provide quantitative information on material properties of living organisms, at the single-molecule, (sub)cellular, tissue, and whole-organism level. Such information is crucial to link material properties to biological function and to obtain a general mechanistic insight into soft and living matter. The raw data from an optical tweezers measurement often consist of a time series carrying information on the physical properties of the probed system. Analyses of such time series are likely to be considerably refined in the years to come, for instance, by employing machine-learning-based approaches. As a result, much more information on the probed system may be found. When passive observation of the time series of the stochastically moving trapped particle is combined with active relaxation measurements, both the trap characteristics and the viscoelastic moduli of the cytoplasm may be extracted [358–361], providing the promise of precision in quantification of forces that are also inside live organisms. In conclusion, optical tweezers based on near-infrared light are a versatile almost non-invasive tool, and future refinements in both instrumentation and data analysis, as well as a clever choice of probe particles, are likely to bring ground-breaking insights into both materials science, biology, biomedicine, and biophysics in the years to come.

### Acknowledgments

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### 36. Cellular studies using quantitative phase imaging

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#### Status

Of critical importance to optical tweezers (OTs) are the shape and refractive index of objects under study. It is perhaps natural then that OTs should be paired with technologies that can access this information. A variety of different optical techniques have been used to gather information about the phase changes created when light propagates through a transparent microscopic object. These include digital holographic microscopy (DHM), quantitative phase microscopy, and quantitative phase imaging. Typically, these techniques utilize interferometry-based imaging technology that retrieves information about an object under study by interrogating the phase structure of the transmitted or reflected light to gain multidimensional information about a sample, such as the 3D morphology of an object, its refractive index, and its associated dynamics. This results in a versatile label-free imaging modality that has attracted considerable research interest in quantitative biological cell imaging [365–368]. This method may be used to detect subcellular structures as well as the morphology of entire tissue slices, and because no external labelling is required, it can be used to assess dynamical processes from milliseconds to days [369].

Although many optical trapping experiments utilize dielectric microspheres, most biological experiments at the micron-size scale utilize objects which consist of complex shapes with spatially/temporally varying refractive indices. Within this context, DHM/OT enables discrimination of ‘trappable’ objects and apprehension of the effect of optical forces on objects under study. DHM has also been shown to be an effective way to evaluate the amount of photodamage, if any, caused by the trapping beam. This also allows for adaptive trapping of biological specimens and feedback on the effects of optical trapping of a biological entity.

Integrating OTs with DHM has enabled biologists to quantitatively study cellular forces, morphological changes, and mechanical properties, such as cellular deformation and elasticity. For instance, OTs combined with DHM have been used as a portable system for precise dynamic measurements of cells, such as red blood cells (RBCs) [370]. Furthermore, this integration has been applied to detect axial changes in RBC shape caused by OTs, enabling the determination of the biophysical (both mechanical and material) changes of the cells by measuring the refractive index and elasticity simultaneously.

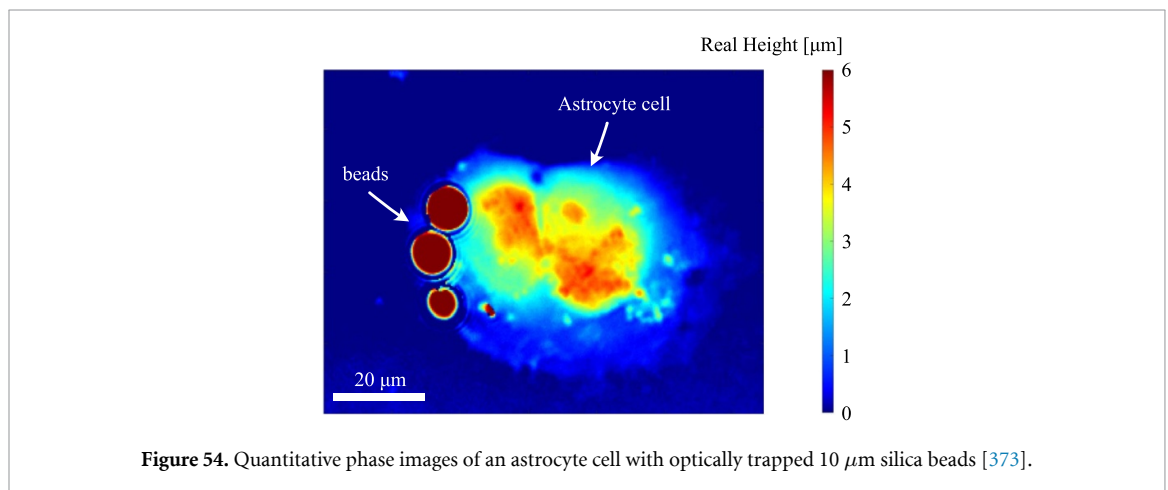
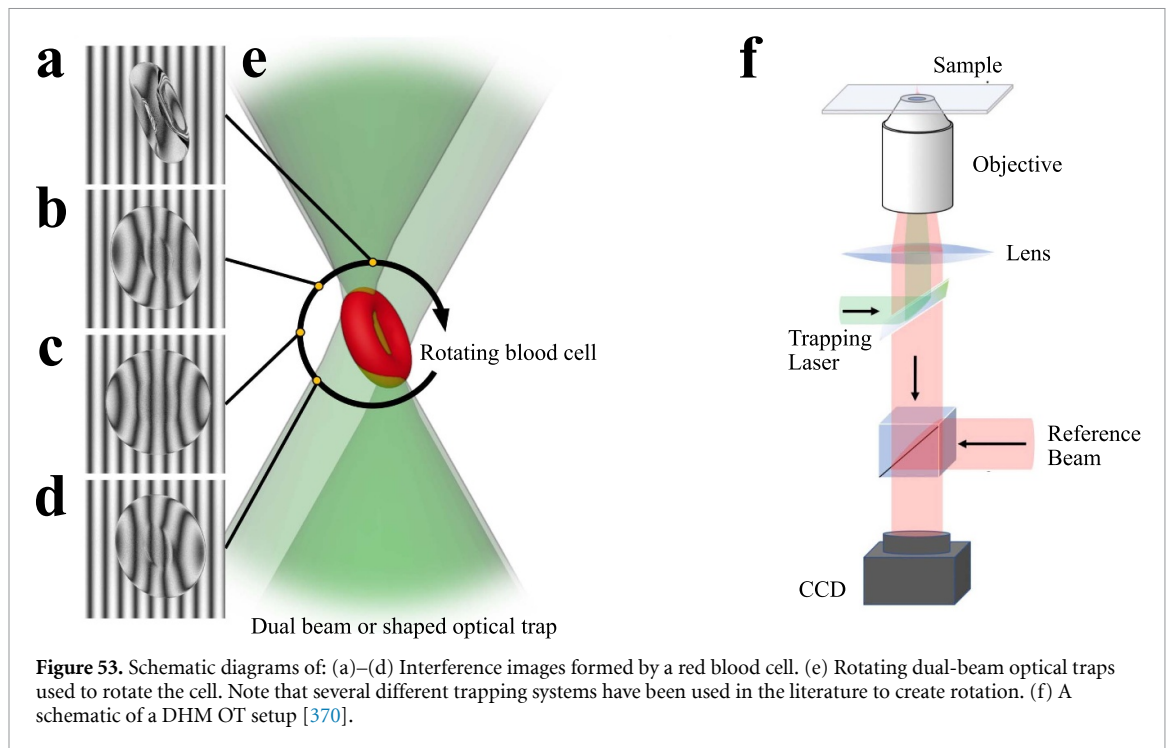
This methodology can also be used for tomographic phase microscopy (TPM) by introducing mechanical actuation and rotation to objects under study. This in turn facilitates tomographic measurements, which can be used to give a truly 3D view of the refractive index and morphology (see figure 53).

#### Current and future challenges

As mentioned previously, one of the advantages of DHM/OT is the capability to simultaneously manipulate and interferometrically measure cells of interest (see figure 54). This enables access not only to the cell’s refractive index but also to morphological changes taking place in the cell. As both the morphology (thickness) and intracellular refractive index are derived from the optical path length of light passing through the cell, it is often necessary to keep one parameter constant in order to accurately calculate the other. Despite this, this functionality has been widely applied to study RBCs and other simple cell types, such as yeast cells; the potential of the technology to conduct experiments with other larger and more physiologically complex cell types has yet to be fully utilized. Although, 3D measurement of the refractive index (TPM) and adaptive optical trapping techniques have been shown previously, this technology still requires significant development [371]. The increased complexity of less homogenous cells means that combined manipulation and measurement cannot be achieved without substantial finesse. A notable limitation of OTs is the capacity to make measurements of a large number of cells. Other methods, such as taking advantage of the random rolling of cells as they flow in a microfluidic channel, might be a better option [372].

Another under-utilized area of investigation is the trapping of submicron objects. These nanoscale objects are of significant interest in both biological and non-biological contexts, and label-free imaging of small particles in the cell such as mitochondria, vesicles, and other organelles is desirable. As with all optical imaging systems, DHM is fundamentally diffraction-limited, making the determination of particle properties like the refractive index difficult. Despite these limitations, nanoparticles can be influenced by optical forces and often exhibit significant refractive index differences from their surrounding environment; however, so far there has been little attempt to use combined OT/DHM systems to either actuate or measure nanoscale particles.

One challenge for DHM/OT systems, which is shared by many biophotonics systems, is the physical integration of different technologies into a single optical train. For instance, many DHM systems have



traditionally used a reflective coverslip inside a Michelson interferometer setup to achieve high-precision phase measurements [373]. When the sample is microscopic, matched objectives are used to eliminate aberration across the arms of the interferometer.

Since this design is not easily compatible with OTs, transmissive techniques have been developed. These techniques improve integration between OTs and DHM, but can also limit resolution and introduce aberration, which must be subsequently corrected.

#### Advances in science and technology to meet challenges

With improved access to information about the optical properties of objects under study computational processing becomes even more necessary to utilize this information fully. There has recently been an increase in the use of artificial intelligence algorithms for the optimization of OTs. This approach may also provide a route to improve the processing of data from DHM/OT systems. Advances in computation and processing could decrease computational overheads while improving trapping performance.

Improvements in digital holographic techniques may provide access to information about submicron particles; several super-resolution phase-contrast methodologies have been proposed that may increase access to submicron particles. However, label-free super-resolution imaging remains challenging. While improving resolution via oblique illumination or by using composite Fourier holography images can lead to improvements in resolution, images are still limited to a few times the native resolution of the objective. To achieve the improvement required for nanoparticle or even single-molecule imaging, new phase-imaging

modalities must be designed. Currently, pump–probe-type experiments have been suggested as possible solutions to the imaging of small particles, though this itself brings several problems, such as photon flux and phase sensitivity. Ultimately any solution will require extensive study.

Another useful application of OTs is photonic force microscopy (PFM), in which 3D information from a sample can be retrieved by evaluating the interference of scattered light as an optically trapped bead scans the sample. Combining OTs for PFM to a DHM can overcome the RI/thickness coupling problem, by providing additional information about the morphology of the sample under study.

Although many of the topics discussed so far have involved sophisticated optical setups, it is worth noting that wider adoption of this technology necessitates that it becomes simpler and cheaper. Along these lines, several papers have already shown how consumer products such as DVD pickups can be used to create compact cost-effective tools [371].

Another area where simplification of the technology may be possible is the integration of spatial light modulator technology, which can be used for both holographic optical trapping of particles and for phase shifting and aberration correction in DHM. This has previously been combined effectively to image and trap. Clearly, the simplification of more sophisticated systems poses a challenge in the long term; however, increased use of computer processing may be able to alleviate some of the physical constraints [371].

### Concluding remarks

Two factors of importance in cellular studies are how cells are observed and how cells are probed or manipulated. While holographic methods allow advanced label-free observation, OTs allow precise non-destructive biomechanical tests. Fundamentally, the technology discussed here represents a way to understand how light propagates and scatters at the cellular level and, in gaining such an understanding, we improve both aspects. This adds much to biophotonics, but challenges still exist in utilizing the technology to its full potential. Improved digital equipment and processing have enabled phase measurements to be taken faster and more reliably and optical traps to be moved with greater dexterity and ingenuity. One would expect this trend to continue. However, it is unlikely that future systems will be simply refinements of current designs. Investigations into biological phenomena will continue to drive greater integration of different technologies and will also require a diversity of approaches to probing cells. Meanwhile, trapping at the limits of our current proficiency will require the development of new, as yet unknown, technologies.

### Acknowledgments

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## 37. Optical and spectral analysis of single cells

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### Status

All living cells react to external stimuli via a multitude of cellular responses. The response type and amplitude depend on the level of stimuli of the extracellular environment and internal stochastic fluctuations of cell transcription and translation [374]. Cells are rarely clonal, nor their response homogenous. Even in a population of genetically identical cells, the response can be slightly different. However, in traditional biological settings, only averaged response values are considered upon external stimulation of a cell population. As such, the distributions of the reaction kinetics and the response outcomes may be misleading. To overcome these limitations, the research field of single-cell analysis has emerged in recent decades, combining a large set of technologies and analysis tools. Among these are the optical tweezers used in a non-invasive manner to trap and manipulate single cells.

Budding yeast is a commonly used unicellular model organism of eukaryotic cells and they are easily trapped and manipulated using optical tweezers. Combining optical tweezers with advanced imaging or spectroscopic techniques can provide high temporally and spatially resolved information. Such data can complement cellular information attained via traditional methods and reveal details that advance our understanding of underlying biological mechanisms. For example, suspended yeast cells trapped with optical tweezers were analyzed based on their biochemical content using Raman spectroscopy, which resulted in probe-free metabolic data acquisition [375–378]. The real-time acquisition modality provided by optical tweezers also permitted the monitoring of dynamic responses upon extracellular stimuli, such as osmosis [379].

When imaged with fluorescence microscopy, fluorescent reporter proteins expressed in genetically modified yeast provide single-cell information on a subcellular level (see, e.g. figure 55). As such, both intensity information (corresponding to the amount of the tagged protein in question) and localization, migration, or diffusion velocities of the fusion protein can be acquired. Incorporating fluorescence imaging and optical tweezers in the same optical setup also allows one to select individual cells to analyze from a cell population based on unique features, such as which reporter proteins they express [380].

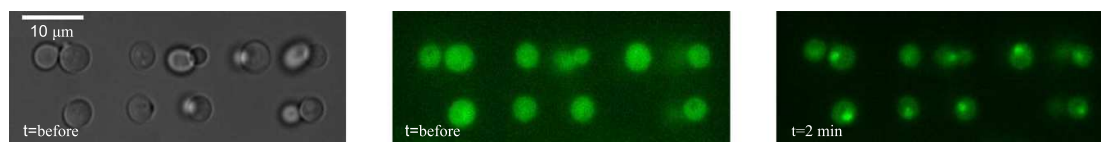
Adding microfluidics to the toolbox further augments the options and enables time-lapse [381, 382] and perturbations [383, 384] studies that are impossible to perform in bulk without disturbing the equilibrium (see, e.g. figure 56). Advancing the technology to manipulate more sensitive cells (e.g. mammalian cells [385]) in complex environments in conjunction with probe-free imaging modalities will add to the analysis possibilities. Such data will boost the biological understanding of single-cell and intercellular behaviour of importance to clarify the onset and development of human disease.

### Current and future challenges

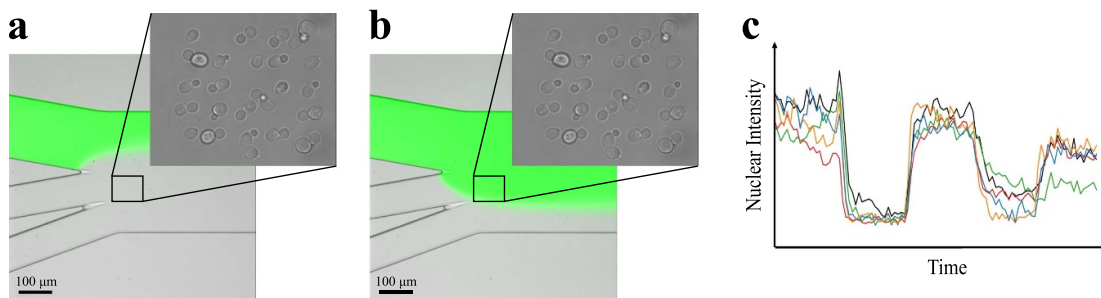
The use of optical tweezers in combination with other techniques offers a wide range of research opportunities. This combination can significantly increase data quality and experimental efficiency. One area of particular interest regards mammalian cell analysis, ranging from blood and cancerous cell analysis to single-cell and organoid manipulation. However, the technology must be user-friendly and more accessible to reach its full potential and transition from fundamental research fields to life-science-oriented fields. This involves calibration approaches that are adaptable to the living system in question. Currently, no such standardized protocol is available; instead, specially trained personnel are required.

Further, parallelized, high-throughput setups are preferred to attain trustworthy diagnostics, sensing, or drug-testing results. Such endeavours set high standards on the readout and may require novel technologies for imaging, sorting, or sensing in combination with control of the optical tweezers.

For long-time studies, mammalian cells require a much more controlled environment than, e.g. yeast cells. Mammalian cells need a narrow interval of temperature, humidity, and specific gas ratios, and the possibility of a perfused environment is beneficial. Also, biocompatible materials for living cells need to simultaneously be consistent with the wavelength of the optical tweezers and possibly with that of an optical readout. A mismatched scenario might affect the outcome and provide a false readout. Finally, any possible photodamage must be taken into consideration to avoid induced photodamage or thermal stress due to trapping or imaging.



**Figure 55.** Examples of single yeast cell data acquired from cells trapped with an optical tweezer, attached to the bottom of a microfluidic chamber, and imaged with fluorescence microscopy. The leftmost and middle images display the cell array in the bright field and fluorescence modality before the extracellular environmental change. Initially, the fusion protein (Hog1-GFP) resides in the yeast cytosol (green). Upon exposing the cells to high osmolarity, the fusion protein migrates and, after 2 min, primarily resides in the nuclei, as visualized in the rightmost image.



**Figure 56.** Environmental cellular perturbations are enabled around yeast cells positioned using optical tweezers in a microfluidic chip. (a), (b) Initially, the cell array is exposed to the solution introduced from the lower inlets (upper panel). As the infusion rate of the upper inlet channel is increased, the cell array is instead exposed to the chemical molecules therein (lower panel). Raising the lower inlet channel infusion rates while decreasing the upper one alters the environment to the initial state again. This cycle can be repeated to perturb the system while monitoring the cell response. (c) Image analysis data from single-cell responses during perturbation reveal a fluorescent fusion protein originally residing in the cytosol that migrates into the nuclei upon the altered environmental milieu. Once the environment returns to its original state, the fusion protein exits the nucleus and awaits the next cycle before migrating back to the nucleus. Providing compensation for possible fluorophore bleaching, the continuous attenuation of the response amplitude in the repeatedly exposed cells may reveal an adaptation or desensitisation response.

### Advances in science and technology to meet challenges

First, portable and affordable setups will make optical tweezers technology accessible to the conventional biological and medical research community. This involves compact fibre lasers and optical designs that allow simultaneous imaging and optical tweezing.

Second, automatic tweezers alignment and calibration software are necessary to avoid having to rely on specialized technicians to install the setup. With today's advancements in machine learning, automatized software to initiate cell manipulation or measurement could be applied. Further, such algorithms can also track and trap individual cells in an automatized way for further analysis, e.g. upon cell replication, isolating the daughter cell from the mother cell [386]. Another possible application is automatic detection and manipulation of, e.g. lipid vesicles, augmenting them close to a given cell surface, and then, to follow their potential uptake and intracellular fate while monitoring metabolic and morphological cell responses, e.g. via Raman spectroscopy, holographic tomography or fluorescent microscopy.

As a cell sorting tool, one single trap might not meet the required speed for high-throughput compared to what existing available fluorescence-activated cell sorting-systems can provide. Holographic optical tweezers would partly overcome this limitation, and such automatic manipulation systems have already been reported [387]. As post-experimental cell analysis is highly valued for different off-chip analyses, combining custom-made microfluidics and machine learning, automatic detection, and sorting into compartments for dedicated treatment will be possible. For instance, optical tweezers can facilitate access to specific cells for downstream intracellular biochemical analysis after an optical cellular analysis.

Further, most adherent cells thrive in a 3D setting surrounded by other cells. Mammalian cells can therefore be cultured as spheres or organoids, useful for cell–cell interactions, tissue engineering, and stem cell differentiation studies. Such organoids are established by following various protocols, and microfluidics-based approaches have proven highly controlled and consistent. Using optical tweezers to sort by size, cellular content, or other measurable properties opens up an avenue of analysis opportunities that were before not even acknowledged.

**Concluding remarks**

Moving into the field of mammalian single-cell analysis is highly interdisciplinary, where the requirements of the living system must be made compatible with that of the optical system. Close collaborations across disciplines are necessary to identify suitable and relevant applications and significantly improve the success rate. Physiologically relevant cell environments will ensure reliable data; meanwhile, long-term optical and biochemical cell studies can reveal whether the cells experienced any possible negative impact by the handling and analysis *per se*. By combining high-frequency imaging modalities of high spatial resolution with sorting capabilities in microfluidic devices, intra- and inter-cellular behaviour can be monitored, unveiling complex signalling events that can be perturbed in real-time. Such quantitative data can help explain complex mechanisms underlying cell functionality and dysfunctionality to understand disease progression and find possible treatments.

**Acknowledgments**

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### 38. Raman tweezers for single-cell analysis and sorting

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#### Status

Understanding biological heterogeneity at the single-cell level is a frontier of biomedicine and precision medicine. Indeed, single-cell analysis can provide insight into the origin, differentiation and heterogeneity of cancer cells, as well as detect the response and resistance of individual cells to drug treatment. Conventional methods based on the use of fluorescence probes or immunochemical staining require, as a prerequisite, a known cell phenotype or require the use of selective biomarkers or probes for which the expected alterations are known. Labelling can require several extensive and time-consuming sample preparation steps, affecting cell viability or perturbing normal cell function. It can suffer from non-specific binding and photobleaching, making long-term analysis difficult. Multiplexed detection is limited by the broad spectral profile of the fluorescence and the relative crosstalk. In addition, traditional biological assays, such as quantitative reverse transcription polymerase chain reaction (qRT-PCR) and Western blotting, are unable to capture differences at the single-cell level, resulting in loss of information on cell-to-cell heterogeneity.

Raman spectroscopy is a vibrational spectroscopic approach that provides information about the chemical composition, molecular structure, and molecular interactions in cells and tissues. Although it is difficult to assign individual bands to single biomolecules because of the cell complexity, a specific fingerprint may be obtained, non-destructively, and without needing exogenous labels. The use of chemometric tools of supervised and unsupervised data analysis can then be applied for cell identification and classification [388]. Since 2002, Raman spectroscopy has been applied in combination with optical traps to study single cells, bacteria, spores, and other biological systems in their aqueous environment [376]. The Raman tweezers approach allowed real-time and continuous monitoring of the expression of specific proteins of single trapped bacteria under antibiotic stress [389] and for non-destructive sorting of living microorganisms [390]. Dual-beam Raman tweezers have been developed for the stretching of single red blood cells and measuring their deformation, allowing both mechanical and chemical properties to be analyzed simultaneously [391] (figure 57).

Although these experiments provide the intrinsic biochemical profile of the cells in a given state, the relatively low sorting throughput greatly hampers their broader applications.

#### Current and future challenges

When cell trapping and Raman classification is synchronized with multichannel microfluidic devices, automated and fast Raman cell sorting becomes possible. An integrated optofluidic platform for Raman-activated cell sorting (RACS) has already been demonstrated to be complementary to the more standard fluorescence-activated cell sorting [392]. In the RACS platform, optical tweezers are employed to trap the single cell from the bulk cell suspension, the single-cell Raman signal provides an intrinsic label-free 'fingerprint' of biochemical components in the cell for the purpose of functional classification or identification, and then the cell of interest is moved and separated from the cell suspension for physical isolation and collection. This system has been used for label-free isolation of yeast and bacterial cells for further amplification and cultivation [393]. However, it still suffers from low throughput due to the intrinsically weak Raman signal and the semi-automated operation, in which cells are identified and manually sorted one-by-one.

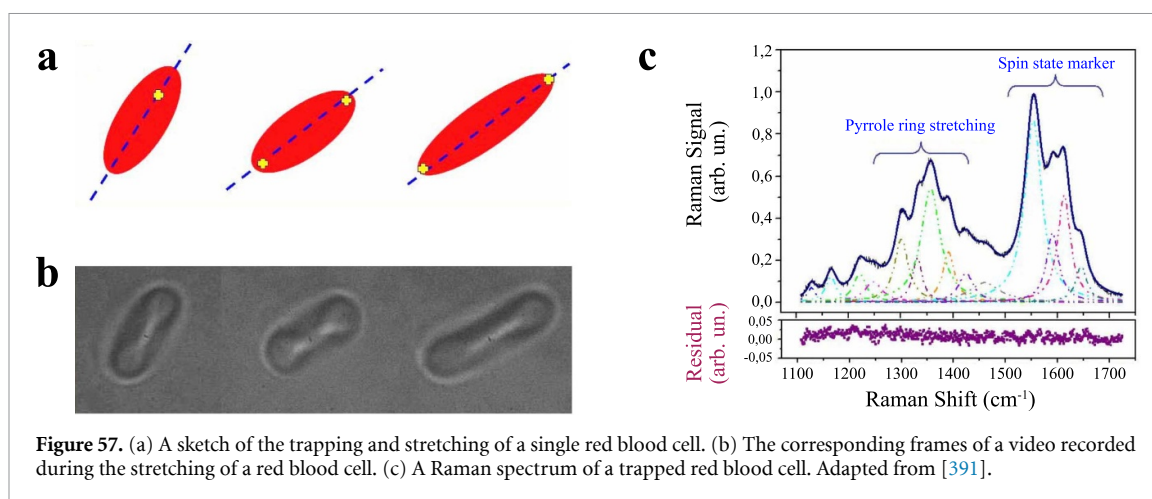
As schematized in figure 58, two challenges should be taken into account to accomplish high-throughput RACS:

1. To improve the rate of single Raman spectra acquisition by employing advanced Raman techniques.
2. To improve the quality and the efficiency of the RACS platform by employing microfluidics-based cell manipulation techniques.

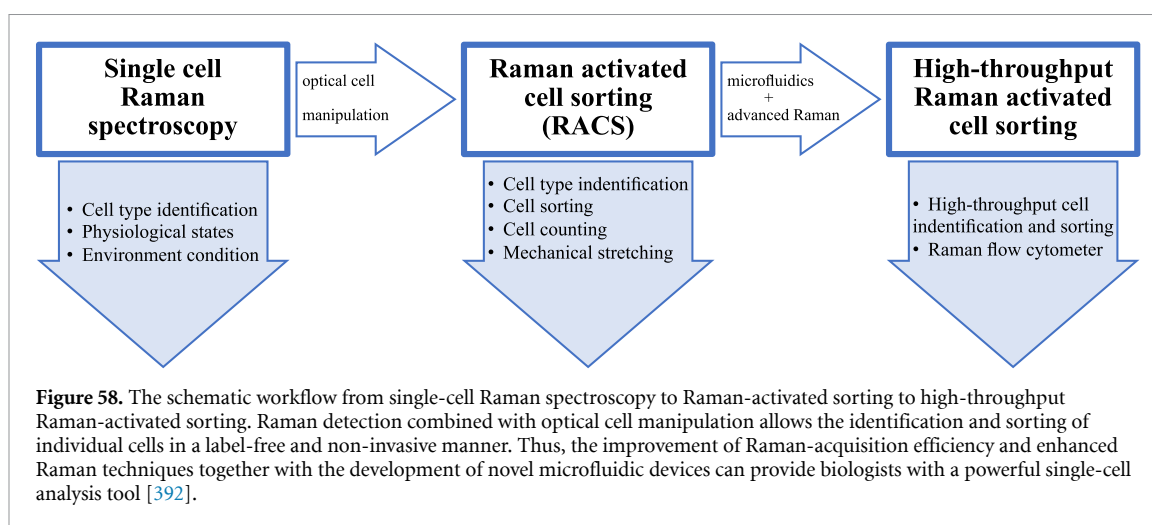
#### Advances in science and technology to meet challenges

With the current available instruments, a single-bacteria Raman signal can be acquired within milliseconds. The sensitivity of Raman detection can be further enhanced by employing novel Raman instruments, including laser sources, optical filters, and low-noise and sensitive EMCCD cameras.

A variety of enhanced Raman techniques have been developed and demonstrated, including surface-enhanced Raman spectroscopy (SERS) and tip-enhanced Raman spectroscopy. The use of metallic nanoparticles or metallic tips can amplify the Raman signal by as much as 10–14 orders of magnitude,



**Figure 57.** (a) A sketch of the trapping and stretching of a single red blood cell. (b) The corresponding frames of a video recorded during the stretching of a red blood cell. (c) A Raman spectrum of a trapped red blood cell. Adapted from [391].



**Figure 58.** The schematic workflow from single-cell Raman spectroscopy to Raman-activated sorting to high-throughput Raman-activated sorting. Raman detection combined with optical cell manipulation allows the identification and sorting of individual cells in a label-free and non-invasive manner. Thus, the improvement of Raman-acquisition efficiency and enhanced Raman techniques together with the development of novel microfluidic devices can provide biologists with a powerful single-cell analysis tool [392].

strongly increasing the sensitivity of the signal detection. Indeed, SERS has been used to study the dynamic release of drugs in living cells with resolution of few attograms at millisecond time scales [394].

However, SERS cannot be considered really label-free. Alternatively, coherent anti-stokes Raman spectroscopy and stimulated Raman spectroscopy can achieve 3–5 orders of enhancement of a selected Raman spectral band. These techniques can significantly increase the signal intensity, but require a greater complexity for the instrumentation as well as interpretation and reconstruction of the data. However, the utilization of Raman tags (e.g. alkyne, deuterium, metal-carbonyl complex) can be used to detect small target molecules inside cells. Indeed, they provide specific bands in the silent region of the Raman spectra of cells, reducing the background and therefore improving the signal detection.

The alignment in the flow between the single cells and the Raman detection spot is also crucial for high-efficiency signal acquisition. In the cell trap–release strategy, an individual cell can be trapped accurately at the Raman detection spot for signal acquisition before being released by periodically applying a trapping force. Alternatively, an integrated fibre laser for single-cell trapping and single-cell Raman acquisition has been demonstrated for target cell sorting [395]. Microfluidics-based cell manipulation techniques can elevate the efficiency of single-cell Raman analysis. With regard to the cell-isolation procedure, a fast continuous mode could be produced in a microfluidic device designed for the isolation of target cells from a cell flow [392]. A microfluidic glass chip incorporates functionalities to separate cells from a reservoir, and accommodates laser fibres for the trapping and sorting of single cells according to the Raman-based classification. The developed RACS enabled the acquisition of Raman spectra from more than 100 000 individual cells and fully automated sampling of 1000 single cells in less than 20 min [396].

### Concluding remarks

The development of advanced optical designs for the Raman spectrometer, the involvement of sophisticated microfluidic devices, and the use of chemometric tools of supervised and unsupervised data analysis have revolutionized the combination of Raman spectroscopy and optical tweezers for single-cell analysis. Indeed,

the integrated optofluidic platform for Raman-activated cell sorting provides high analytical potential, thus overcoming the problem of the complex sample preparation steps that affect fluorescence-based approaches. It allows measurements of the intrinsic molecular makeup of cells, providing a higher number of parameters in a label-free and non-destructive manner. Because no sample preparation is required, cells can simply be trapped and measured. In summary, the single-cell Raman sorting platform provides biologists with a powerful single-cell analysis tool to explore the scientific questions or applications in many areas of biomedicine.

### Acknowledgments

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## Optical forces in space

### 39. Space tweezers for cosmic dust characterization

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#### Status

Dust is everywhere in the Universe. Up to the mid-20th century, cosmic dust was only considered as an annoying fog obscuring starlight. In about half a century, such a view has totally changed: dust plays a vital role in many processes, going from the formation of planets, stars, and galaxies to the ignition of a potentially life-bearing chemistry. The importance that cosmic dust, in the form of interstellar, interplanetary, and planetary dust particles, has gained in recent years is driving the study of its nature, composition, and evolution [397].

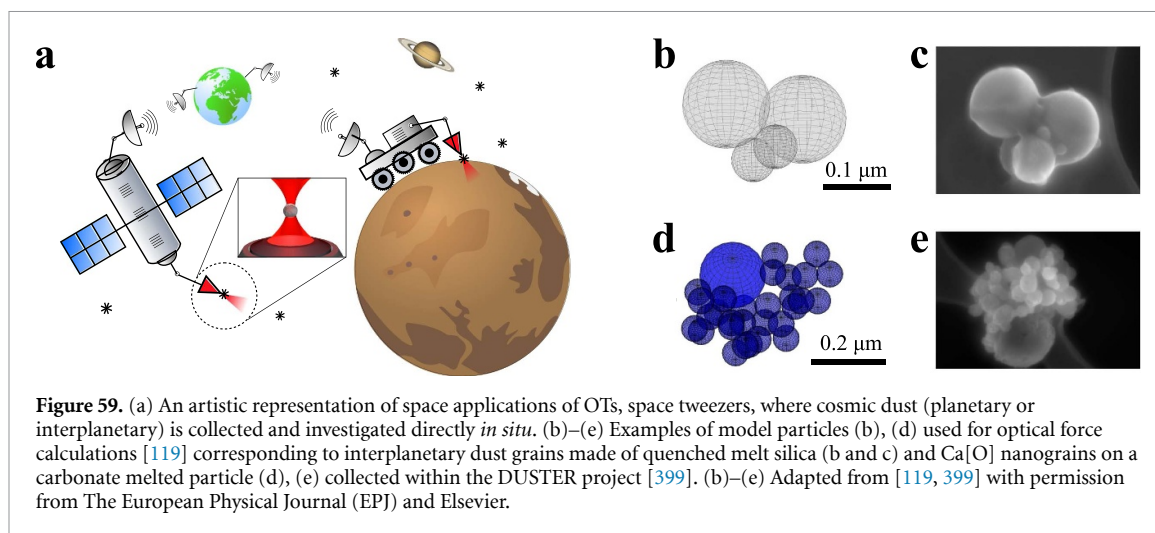
Optical tweezers (OTs) have shown their remarkable capability to trap, manipulate, and characterize a wide range of microscopic and nanoscopic particles, in liquids, air, and vacuum [16, 243], finding applications in a wide range of fields: from biology, soft matter, and ultrasensitive spectroscopy to atomic physics, nanoscience, photonics, and aerosol science [1]. The coupling of OTs with a Raman spectrometer (Raman tweezers) has opened up novel and interesting scenarios, allowing the chemical and physical analysis of trapped particles through their vibrational fingerprints [1]. Despite the significant advances in optical trapping techniques and the many examples of cosmic phenomena driven by radiation pressure, the application of OTs to space exploration and dust characterization (space tweezers) has yet to be developed [119, 398].

The application of space tweezers to study the solar system opens up perspectives for the analysis of cometary particles, dust particles in the Martian atmosphere, and/or on the Martian and lunar surfaces (figure 59(a)). Such analysis is strategic for the characterization of the chemical and physical properties of such particles with curation facilities designed for uncontaminated handling of extraterrestrial samples returned by research expeditions [399]. The direct implementation and application of optical trapping and Raman tweezers to space materials open doors to new information that is currently unreachable without bias. In space missions, different techniques have been successfully used to collect or characterize samples [399]. However, they are limited because of the unavoidable sample modification or contamination due to the collection media. An OT system mounted on stratospheric instruments, onboard cometary probes, or on landers and rovers to Mars or to the Moon, would offer a great opportunity for the *in situ* characterization of extraterrestrial particles, without introducing any contamination.

#### Current and future challenges

Challenges for space tweezers combine both theoretical and experimental aspects. From the computational point of view, the diversity of dust particles in an astrophysical context implies a richness of models that need to be developed to calculate the optical forces. For model spherical particles such forces can be calculated by using exact electromagnetic solutions of the scattering problem [1]. However, realistic dust grains are far from exhibiting these simple shapes (figures 59(c) and (e)). Aiming to replicate realistic dust scattering properties, different model particles have been proposed that include aggregates (figures 59(b) and (d)), stratified agglomerate debris, or Gaussian random particles [400, 401]. While the use of these more sophisticated model geometries better represents physical reality, the increased detail in the morphology comes with the drawback of a higher demand for computational power, limiting the number of configurations that can be numerically explored.

From the experimental point of view, OTs have been mostly employed to trap and manipulate micron-sized objects in liquid environments rather than in air or in vacuum. While liquid media minimize the effects of external perturbations on a trapped particle and the effect of inertia on its dynamics [16], trapping in a low-viscosity medium (air or vacuum) is more challenging. The trapping stability can be affected by external perturbations generated by airflows, acoustic shocks, thermal drift, mechanical vibrations, and also by the intensity noise of the trapping laser [243]. Furthermore, liquid media can suspend the particles for a long time before and after trapping, allowing the operator to select and trap a specific single particle within a multitude of particles. In contrast, in air tweezers setups, a large number of particles need to be launched, which eventually approach the laser focus under gravity and are trapped passively [243]. Optical trapping in air or at low pressure poses challenges to select a specific dust grain, position it, or store it for subsequent characterization [402]. Once the particle gets out of the trap it is generally lost and it is difficult to retrieve it. In air OTs the numerical aperture (NA) of the focusing objective can never be greater than unity, giving rise to scattering forces that can overcome the trapping forces. Moreover, long working



distance objectives and lenses (with a lower NA) are often used in air tweezers setups to prevent lens contamination from the sprayed or launched samples [243]. Because air is less efficient than a liquid in dissipating heat, an absorbing particle trapped in air can produce photophoretic forces and convective forces, generated by airflows which often can destabilize the trapped-particle dynamics [243].

#### Advances in science and technology to meet challenges

In recent years much effort has been devoted to the accurate modelling of optical forces acting on complex-shaped particles [1], making it possible to calculate such forces for particles in a given position and orientation. However, there is always a compromise between the calculation accuracy and the calculation speed. When studying the particle dynamics of systems where the inertia needs to be considered (for example in air or vacuum), the equations of motion need to be integrated using a very short time step and the optical force needs to be computed in each of these time steps. While the traditional force calculation becomes prohibitively slow to explore these systems, recent advances in machine learning for optical force calculations [87] significantly increase this calculation speed. This is crucial for the accurate modelling of particles of complex shapes. On the other hand, this improvement in the calculation time could allow real-time adjustments of the light intensity and beam shape to enhance the trapping of a given particle in OT experiments.

From the experimental point of view, several experimental configurations have been developed to achieve stable 3D trapping in air or vacuum. For instance, setups with counter-propagating beams can be used to balance the effect of the radiation pressure on a trapped particle [3] and they can also be realized with optical fibres [403]. Structured light beams, such as Bessel, hollow, or vortex beams can be used instead of Gaussian beams, either in horizontal or vertical configurations [243, 404, 405]. In addition, configurations with a single beam, such as the confocal-beam trap, combine the simplicity of a single-beam trap and the robustness of a dual-beam trap. In this configuration, a spherical concave mirror reflects back the incident focused beam, forming a symmetric counter-propagating beam [243]. Finally, the stability of a single-beam trap can also be increased by a feedback device that, by controlling the laser power, improves the trapping stability or can even realize laser cooling of the particle motion [16].

#### Concluding remarks

Space tweezers can be used to trap and characterize extraterrestrial particulate matter. From the theoretical point of view, it is possible to exploit scattering theory to calculate optical forces on a variety of complex particles of astrophysical interest, simulating atmospheric and planetary environments. Meanwhile, in recent years much effort has been devoted to build versatile, stable, and more compact setups that can be used to trap micro- and nano-scopic particles in controlled laboratory experiments. Space tweezers applications for non-destructive, non-contact, and non-contaminating investigation of extraterrestrial particles will pave the way towards new information on space materials that are currently unreachable with the instrumentation used in space missions. However, several different challenges still need to be faced, e.g. controlled capture, selection, and storage of single grains, improved stability for trapping in extreme environmental conditions, and general protocols to optically characterize levitated dust. This means that optical trapping and optical manipulation of particles in space and on planetary body surfaces still need some improvements in the experimental setups. Meanwhile, applications in curation facilities, designed for the uncontaminated

handling and preliminary characterization of extraterrestrial samples returned by space probes, appear more at hand.

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## 40. Diffractive solar sails

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### Status

Solar sails have recently been tested in space, and more missions are planned in the coming years. Navigating the heavens using solar radiation pressure provides multiple advantages not afforded by rocket propulsion: continuous acceleration, an inexhaustible energy source, and massless propellant, respectively providing non-Keplerian orbits, long durations, and a large delta-V [382]. Modern optical design and fabrication techniques open up opportunities to produce more efficient sails compared to the century-old idea of a flat reflective film concept. Just as a jet fighter is designed differently to a crop duster, so too will future solar sails be designed for specific space objectives. Depicted in figure 60 are high delta-V missions like solar polar orbiters and long duration missions like sub-L1 halo orbits, both enabling heliophysics science observatories and warning systems for debilitating Earth-bound coronal mass ejections [406].

The current status of solar sailing is akin to the early days of air flight when significant innovations emerged after sustained flight was demonstrated. Over the next decades sailcraft missions may explore difficult-to-reach parts of the solar system, embarking on spiral trajectories towards, away, and over the Sun. Other near-term missions may include Earth-orbiting satellites that benefit from the experiences of the ongoing Lightsail-2 mission of the Planetary Society [407]. For longer time spans, one may envision both solar and laser-driven sails that probe interstellar distances on hyperbolic trajectories, perhaps visiting neighbouring exoplanets [408]. Both science and the emerging space economy may benefit from relatively low-cost, CubeSat/SmallSat compatible solar sails—especially if optical scientists can enhance the associated figure of merit. For example, diffractive sails were recently proposed to achieve higher momentum transfer efficiencies than a flat reflective sail for spiral trajectory missions [409].

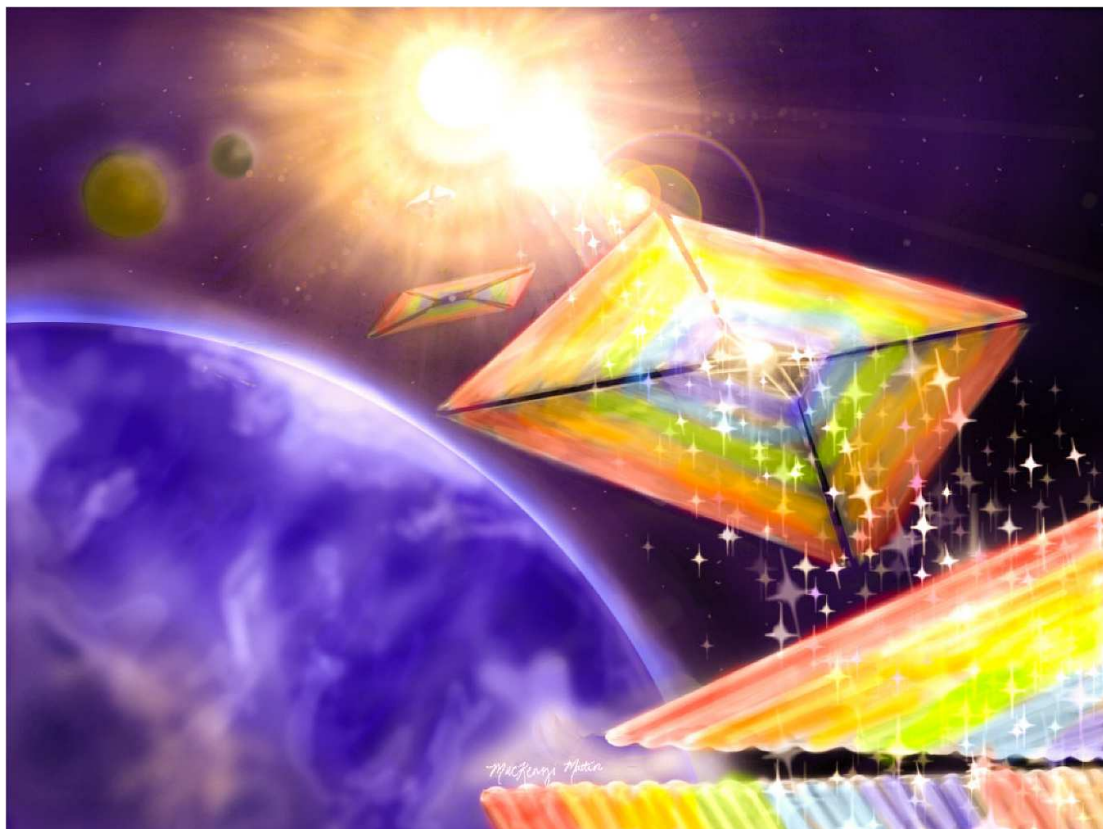
Advancement opportunities include: (1) design and fabrication of Sun-facing sails with a high momentum transfer efficiency component perpendicular to the sunline; (2) low mass-to-area ratio sails using metasurface or polarization diffraction grating principles; (3) sail elements that are electro-optically switchable; and (4) robust optical materials that both withstand the harsh space environment (e.g. ionizing radiation and extreme temperature cycles) and are immune to packaging and unfurling damage. The fabrication of diffractive sails may include roll-to-roll imprint technology followed by adhesive stitching to achieve large areas. Before launch the finished product must be folded into a small volume package and mounted to a deployment system comprised of low-mass booms to support the gossamer sail. Once in space, the sail is unfurled and readied for action.

### Current and future challenges

Perhaps counter to intuition, the component of radiation pressure force directed away from the Sun is less important than the perpendicular component when discussing the inner and outer planets or high solar latitudes [409–411]. Whereas the force directed away from the Sun elongates orbital ellipticity, the latter enables spiral trajectories that are essential for rendezvous missions. After a rocket positions the spacecraft beyond the influence of Earth's gravity, navigation towards (away from) the Sun is achieved by tangentially decelerating (accelerating) from an initial quasi-circular orbit at 1 AU.

A dimensionless figure of merit (FOM) for such missions may be expressed as  $\text{FOM} = (\sigma^*/\sigma) \sin\Theta$ , where  $\Theta$  is defined as an equivalent scattering angle for a Sun-facing sail,  $\sin\Theta = \cos\theta_i \sin\theta_s$ , where  $\theta_i$  is the projection angle of sunlight upon the sail,  $\theta_s$  is the net scattering angle measured with respect to the Sun line and averaged across the solar spectrum and all scattering angles,  $\sigma^* = 1.54 \text{ g m}^{-2}$  is a solar constant, and  $\sigma = M_{\text{sc}}/A$  is the sailcraft areal density, where  $M_{\text{sc}}$  and  $A$  are, respectively, the sailcraft total mass and sail area. Current space technology provides areal densities of the order of  $100 \sigma^*$ . For a traditional ideal sail obeying the law of reflection, the optimum incidence angle is  $\theta_i = 35.3^\circ$  [1], resulting in a scattering angle  $\theta_s = 2\theta_i$  that provides  $\text{FOM} = 0.77(\sigma^*/\sigma)$  and  $\Theta = 50.3^\circ$ .

A challenge for optical scientists is to enhance the FOM. An upper value occurs for a Sun-facing sail  $\theta_i = 0^\circ$  together with a uniform grazing scattering angle  $\theta_s = 90^\circ$ , resulting in  $\Theta_{\text{max}} = 90^\circ$  and  $\text{FOM} = 1.00(\sigma^*/\sigma)$ . Further enhancements to the FOM may be achieved by reducing the sailcraft mass  $M_{\text{sc}}$  by using a multifunctional sail that allows for the elimination of mass components, such as those used for attitude control, communication, or thermal management. For example, an electro-optically controlled sail, though higher in mass, may provide net mass savings due to the elimination of attitude control devices. The first challenge for optical scientists is to achieve an equivalent scattering angle significantly greater than  $\Theta = 50.3^\circ$  (preferably a value approaching  $90^\circ$ ).



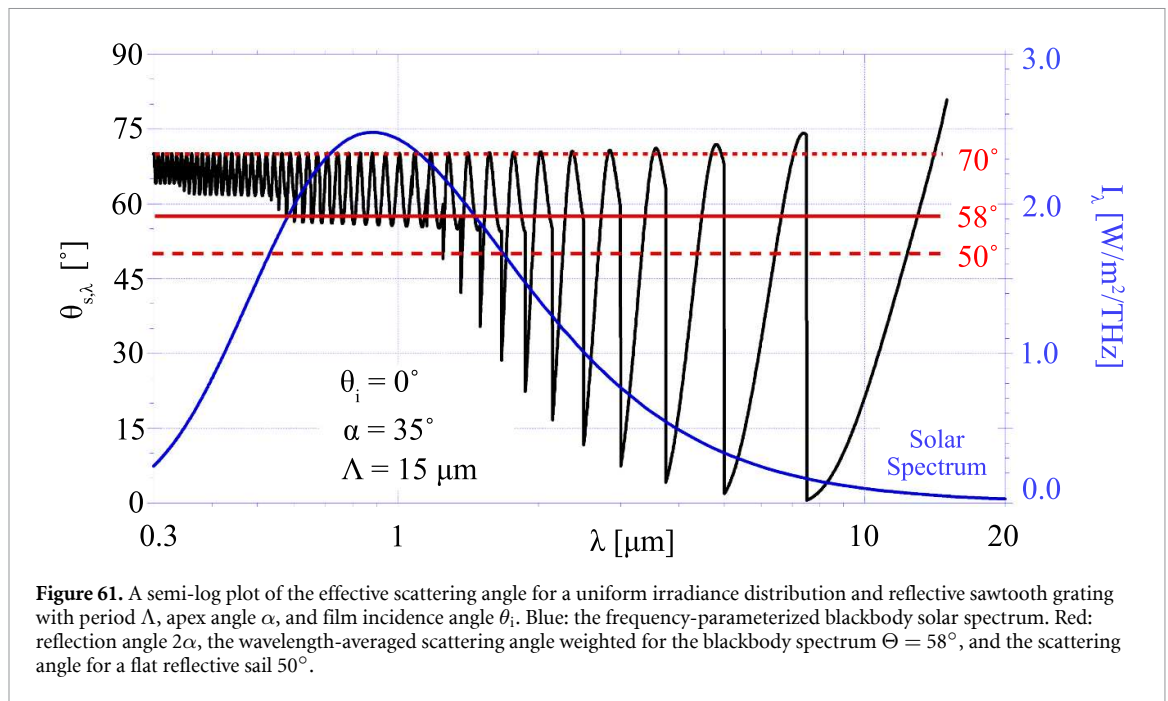
**Figure 60.** An artist's depiction of a constellation of diffractive light sails leaving Earth en route to the Sun (MacKenzi Martin, RIT, 2013).

### Advances in science and technology to meet challenges

A transmission or reflection function resembling  $f(x, \lambda) = \exp(2\pi i x \sin(\theta_s)/\lambda)$  is desired, where  $x$  is a coordinate that is perpendicular to the sunline, the wavelength  $\lambda$  ranges across the solar spectrum, and the scattering angle  $\theta_s$  is roughly  $90^\circ$ . While a prism can be made to satisfy these requirements, it would be too massive to function as a solar sail. A periodic sawtooth grating with a surface profile  $h(x) = h_0(1 - x/\Lambda)$  may also be used to create a tilted wavefront, where  $\Lambda$  is the period,  $h_0 = \Lambda \tan(\alpha)$  is the height above the surface, and  $\alpha$  is the apex angle. A short period grating has smaller mass than a long period grating with the same apex angle. However, a short period grating exhibits pronounced diffraction, producing a smaller equivalent scattering angle  $\Theta$  when averaged over the solar spectrum (figure 61). The FOM scales as  $\sin\Theta/M_{sc}$ . If the mass of the sail is a small fraction of the total sailcraft mass  $M_{sc}$ , then it is arguably desirable to first optimize the value of  $\Theta$ .

Advances in optical science in areas like space-variant polarization diffraction gratings [412, 413] and metasurfaces [414, 415] suggest paths for improving the FOM. Research is needed to design and fabricate reflective or transmissive elements that uniformly scatter light into a single direction or narrow cone with high efficiency. As depicted in figure 61, a simple sawtooth diffraction grating provides opportunities to achieve a larger equivalent scattering angle than a flat reflective sail ( $58^\circ$  vs  $50^\circ$ , representing a 10% increase in the FOM), but the  $\Theta \sim 90^\circ$  goal is yet beyond reach. At values of  $\lambda \sim \Lambda$ , the cumulative effect from multiple diffraction orders is to diminish the effective wavelength-dependent scattering angle,  $\theta_{s,\lambda}$  due to large modulations. The modulation is less pronounced at shorter wavelengths, resulting in a greater momentum transfer efficiency. Research on broadband engineered optical films that enables less wavelength-dependent modulation of the scattering angle may provide a path towards greater values of the FOM.

The ability to electro-optically switch the radiation pressure force on advanced diffractive elements (e.g. electro-optically or thermally) may provide significant opportunities to decrease the sailcraft mass, thereby affording greater acceleration. A key target for this is the attitude management system. Spacecraft often suffer a centre-of-mass/centre-of-pressure offset, resulting in a torque that must be countered to prevent spinning from the desired attitude. Gyroscopes may be used for this purpose; however, they contribute to system mass and they are prone to gimbal lock and failure. Radiation pressure on solar panels has been used in the past to



rescue missions from such failures; therefore, it is feasible that switchable diffractive elements could be integrated into a large solar sail to reduce both failure risk and sailcraft mass.

### Concluding remarks

Recent coalescing developments, including low-cost access to space, CubeSat and SmallSat technology, and the design and fabrication of engineered optical thin-film materials, are combining to provide opportunities to significantly enhance the in-space flight performance of solar sails. Besides the benefits afforded to the space science community and to the emerging space economy, the financial impact could amount to trillions of dollars of savings in the form of early warning systems to protect Earth from coronal mass ejections and other space hazards. Replacing a flat reflective solar sail with an advanced diffractive film may provide a  $\sim 30\%$  enhancement of the optical momentum transfer needed for spiral trajectory orbits, and furthermore, further FOM enhancements may be achieved by offsetting sailcraft mass with multifunctional sails. To achieve the required optical bandwidth (e.g. wavelengths ranging from roughly  $0.3\text{--}3\text{ }\mu\text{m}$ ) and high scattering efficiency at large angles, innovative ideas from the optical community are sought. Funding for material design, fabrication, and testing, as well as for validation experiments in low Earth orbit will be pivotal. The rapid advancement of aircraft design in the early 1900s serves as a historical guide, pointing towards an exciting future for solar sailing.

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### Data availability statement

No new data were created or analysed in this study.

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## References

- [1] Jones P H, Maragò O M and Volpe G 2015 *Optical Tweezers: Principles and Applications* (Cambridge: Cambridge University Press)
- [2] Kepler J 1619 *De Cometis libelli tres* (Augsburg: Avgvstae Vindelicorvm, A. Apergeri)
- [3] LeBlanc F 2011 *An Introduction to Stellar Astrophysics* (New York: Wiley)
- [4] Lebedev P 1901 Untersuchungen über die Druckkräfte des Lichtes *Ann. Phys.* **311** 433
- [5] Nichols E F and Hull G F 1901 A preliminary communication on the pressure of heat and light radiation *Phys. Rev.* **13** 307
- [6] Siegman A E 1986 *Lasers* (Mill Valley, CA: University Science Books)
- [7] Arthur Ashkin Nobel Lecture entitled Optical tweezers and their application to biological systems (Stockholm) (available at: [www.nobelprize.org/prizes/physics/2018/ashkin/lecture](http://www.nobelprize.org/prizes/physics/2018/ashkin/lecture)) (Accessed 8 December 2018)
- [8] Ashkin A 1970 Acceleration and trapping of particles by radiation pressure *Phys. Rev. Lett.* **24** 156–9
- [9] Ashkin A, Dziedzic J M, Bjorkholm J E and Chu S 1986 Observation of a single-beam gradient force optical trap for dielectric particles *Opt. Lett.* **11** 288–90
- [10] Ashkin A 1970 Atomic-beam deflection by resonance-radiation pressure *Phys. Rev. Lett.* **25** 1321
- [11] Chu S, Hollberg L, Bjorkholm J E, Cable A and Ashkin A 1985 Three-dimensional viscous confinement and cooling of atoms by resonance radiation pressure *Phys. Rev. Lett.* **55** 48
- [12] Chu S, Bjorkholm J E, Ashkin A and Cable A 1986 Experimental observation of optically trapped atoms *Phys. Rev. Lett.* **57** 314
- [13] Ashkin A, Dziedzic J M and Yamane T 1987 Optical trapping and manipulation of single cells using infrared laser beams *Nature* **330** 769–71
- [14] Ashkin A and Dziedzic J M 1987 Optical trapping and manipulation of viruses and bacteria *Science* **235** 1517
- [15] Pesce G, Giorgio Volpe O M, Maragó P H, Jones S G, Sasso A and Volpe G 2015 Step-by-step guide to the realization of advanced optical tweezers *J. Opt. Soc. Am. B* **32** B84–B98
- [16] Gieseler J et al 2021 Optical tweezers—from calibration to applications: a tutorial *Adv. Opt. Photonics* **13** 74–241



- [17] Favre-Bulle I A, Stilgoe A B, Scott E K and Rubinsztein-Dunlop H 2019 Optical trapping *in vivo*: theory, practice, and applications *Nanophotonics* **8** 1023–40
- [18] Kalantarifard F, Elahi P, Makey G, Maragò O M, Ilday F Ö and Volpe G 2019 Intracavity optical trapping of microscopic particles in a ring-cavity fiber laser *Nat. Commun.* **10** 2683
- [19] Li J, Chen Z, Liu Y, Kollipara P S, Feng Y, Zhang Z and Zheng Y 2021 Opto-refrigerative tweezers *Sci. Adv.* **7** eabhi1101
- [20] Markovich H, Shishkin I I, Hendler N and Ginzburg P 2018 Optical manipulation along an optical axis with a polarization sensitive meta-lens *Nano Lett.* **18** 5024–9
- [21] Shen K, Duan Y, Peng J, Zhujiang X, Chen X, Zhang L, Ahn J, Ni X and Li T 2021 On-chip optical levitation with a metalens in vacuum *Optica* **8** 1359–62
- [22] Grier D G 2003 A revolution in optical manipulation *Nature* **424** 810–6
- [23] Woerdemann M, Alpmann C, Esseling M and Denz C 2013 Advanced optical trapping by complex beam shaping *Laser Photonics Rev.* **7** 839–54
- [24] Aiello A, Banzer P, Neugebauer M and Leuchs G 2015 From transverse angular momentum to photonic wheels *Nat. Photon.* **9** 789–95
- [25] Nkosiphile Bhebhe P A, Williams C, Rosales-Guzmán C, Rodriguez-Fajardo V and Forbes A 2018 A vector holographic optical trap *Sci. Rep.* **8** 17387
- [26] Otte E and Denz C 2020 Optical trapping gets structure: structured light for advanced optical manipulation *Appl. Phys. Rev.* **7** 041308
- [27] Taylor M A, Waleed M, Stilgoe A B, Rubinsztein-Dunlop H and Bowen W P 2015 Enhanced optical trapping via structured scattering *Nat. Photon.* **9** 669–73
- [28] Shahabadi V, Madadi E and Abdollahpour D 2021 Optimized anti-reflection core-shell microspheres for enhanced optical trapping by structured light beams *Sci. Rep.* **11** 4996
- [29] Jannasch A, Demirörs A F, van Oostrum P D J, van Blaaderen A and Erik S 2012 Nanonewton optical force trap employing anti-reflection coated, high-refractive-index titania microspheres *Nat. Photon.* **6** 469–73
- [30] Horodynski M, Kühmayer M, Brandstötter A, Pichler K, Fyodorov Y V, Kuhl U and Stefan R 2019 Optimal wave fields for micromanipulation in complex scattering environments *Nat. Photon.* **14** 149–53
- [31] Ilic O and Atwater H A 2019 Self-stabilizing photonic levitation and propulsion of nanostructured macroscopic objects *Nat. Photon.* **13** 289–95
- [32] Delić U, Reisenbauer M, Dare K, Grass D, Vuletić V, Kiesel N and Aspelmeyer M 2020 Cooling of a levitated nanoparticle to the motional quantum ground state *Science* **367** 892–5
- [33] Magrini L, Rosenzweig P, Bach C, Deutschmann-Olek A, Hofer S G, Hong S, Kiesel N, Kugi A and Aspelmeyer M 2021 Real-time optimal quantum control of mechanical motion at room temperature *Nature* **595** 373–7
- [34] Madsen L S, Waleed M, Casacio C A, Terrasson A, Stilgoe A B, Taylor M A and Bowen W P 2021 Ultrafast viscosity measurement with ballistic optical tweezers *Nat. Photon.* **15** 386–92
- [35] Volpe G, Kurz L, Callegari A, Volpe G and Gigan S 2014 Speckle optical tweezers: micromanipulation with random light fields *Opt. Express* **22** 18159–67
- [36] Volpe G, Volpe G and Gigan S 2014 Brownian motion in a speckle light field: tunable anomalous diffusion and selective optical manipulation *Sci. Rep.* **4** 3936
- [37] Shvedov V G, Rode A V, Izdebskaya Y V, Desyatnikov A S, Krolikowski W and Kivshar Y S 2010 Selective trapping of multiple particles by volume speckle field *Opt. Express* **18** 3137–42
- [38] Horak P, Courtois J-Y and Grynberg G 1998 Atom cooling and trapping by disorder *Phys. Rev. A* **58** 3953–62
- [39] Hanes R D L, Dalle-Ferrier C, Schmiedeberg M, Jenkins M C and Egelhaaf S U 2012 Colloids in one dimensional random energy landscapes *Soft Matter* **8** 2714–23
- [40] Douglass K M, Sukhov S and Dogariu A 2012 Superdiffusion in optically controlled active media *Nat. Photon.* **6** 834–7
- [41] Bianchi S, Pruner R, Vizsnyiczai G, Maggi C and Di Leonardo R 2016 Active dynamics of colloidal particles in time-varying laser speckle patterns *Sci. Rep.* **6** 27681
- [42] Pastore R, Ciarlo A, Pesce G, Greco F and Sasso A 2021 Rapid Fickian yet non-Gaussian diffusion after subdiffusion *Phys. Rev. Lett.* **126** 158003
- [43] Brügger G, Froufe-Pérez L S, Scheffold F and Sáenz J J 2015 Controlling dispersion forces between small particles with artificially created random light fields *Nat. Commun.* **6** 7460
- [44] Nunes A S, Velu S K P, Kasianiuk I, Kasyanyuk D S, Callegari A, Volpe G, Telo da Gama M M, Volpe G and Araújo N A M 2020 Ordering of binary colloidal crystals by random potentials *Soft Matter* **16** 4267–73
- [45] Pinçe E, Velu S K P, Callegari A, Elahi P, Gigan S, Volpe G and Volpe G 2016 Disorder-mediated crowd control in an active matter system *Nat. Commun.* **7** 10907
- [46] Zunke C, Bewerunge J, Platten F, Egelhaaf S U and Godec A 2022 First-passage statistics of colloids on fractals: theory and experimental realization *Sci. Adv.* **8** eabk0627
- [47] Kang Z, Chen J, Wu S Y, Chen K, Kong S K, Yong K T and Ho H P 2015 Trapping and assembling of particles and live cells on large-scale random gold nano-island substrates *Sci. Rep.* **5** 9978
- [48] Tong L 2018 Micro/nanofibre optical sensors: challenges and prospects *Sensors* **18** 903
- [49] Brambilla G, Murugan G S, Wilkinson J S and Richardson D J 2007 Optical manipulation of microspheres along a subwavelength optical wire *Opt. Lett.* **32** 3041–3
- [50] Maimaiti A, Holzmann D, Truong V G, Ritsch H and Nic Chormaic S 2016 Nonlinear force dependence on optically bound micro-particle arrays in the evanescent fields of fundamental and higher order microfiber modes *Sci. Rep.* **6** 30131
- [51] Truong V G, Tkachenko G, Esporlas C L, Sanskriti I and Nic Chormaic S 2023 Evanescent field trapping and propulsion of Janus particles along optical nanofibers *Nat. Commun.*
- [52] Tkachenko G, Toftul I, Esporlas C, Maimaiti A, Le Kien F, Truong V G and Nic Chormaic S 2020 Light-induced rotation of dielectric microparticles around an optical nanofiber *Optica* **7** 59–62
- [53] Phelan C F, Hennessy T and Busch T 2013 Shaping the evanescent field of optical nanofibers for cold atom trapping *Opt. Express* **21** 27093–101
- [54] Romagnoli P, Maeda M, Ward J M, Truong V G and Nic Chormaic S 2020 Fabrication of optical nanofibre-based cavities using focussed ion-beam milling: a review *Appl. Phys. B* **126** 111
- [55] Morrissey M J, Deasy K, Frawley M, Kumar R, Prel E, Russell L, Truong V G and Nic Chormaic S 2013 Spectroscopy, manipulation and trapping of neutral atoms, molecules, and other particles using optical nanofibers: a review *Sensors* **13** 10449–81

- [56] Le Kien F, Balykin V I and Hakuta K 2004 Atom trap and waveguide using a two-color evanescent light field around a subwavelength-diameter optical fiber *Phys. Rev. A* **70** 063403
- [57] Bernien H et al 2017 Probing many-body dynamics on a 51-atom quantum simulator *Nature* **551** 579–84
- [58] Fatemi F K, Hoffman J E, Solano P, Fenton E F, Beadie G, Rolston S L and Orozco L A 2017 Modal interference in optical nanofibers for sub-angstrom radius sensitivity *Optica* **4** 157–62
- [59] Visscher K, Schnitzer M J and Block S M 1999 Single kinesin molecules studied with a molecular force clamp *Nature* **400** 184–9
- [60] Bustamante C J, Chemla Y R, Liu S and Wang M D 2021 Optical tweezers in single-molecule biophysics *Nat. Rev. Methods Primers* **1** 1–29
- [61] Wang Q, Goldsmith R H, Jiang Y, Bockenhauer S D and Moerner W E 2012 Probing single biomolecules in solution using the anti-Brownian electrokinetic (ABEL) trap *Acc. Chem. Res.* **45** 1955–64
- [62] Juan M L, Gordon R, Pang Y, Eftekhari F and Quidant R 2009 Self-induced back-action optical trapping of dielectric nanoparticles *Nat. Phys.* **5** 915–9
- [63] Kalantarifard F, Volpe G and Elahi P 2021 Self-adjusted counter-propagating intra cavity optical trapping *Proc. SPIE* **11798** 1179820
- [64] Kuang T, Liu Z, Xiong W, Han X, Xiao G, Chen X, Yang K and Luo H 2021 Dual-beam intracavity optical tweezers with all-optical independent axial and radial self-feedback control schemes *Opt. Express* **29** 29936–45
- [65] Pitzek M, Steiger R, Thalhammer G, Bernet S and Ritsch-Marte M 2009 Optical mirror trap with a large field of view *Opt. Express* **12** 19414–23
- [66] Woerdemann M, Berghoff K and Denz C 2010 Dynamic multiple-beam counter-propagating optical traps using optical phase-conjugation *Opt. Express* **18** 22348–57
- [67] Liu Z, Kuang T, Xiong W, Feng H, Chen X, Xiao G and Luo H 2021 Self-feedback induced bistability in dual-beam intracavity optical tweezers *Opt. Lett.* **45** 5328–31
- [68] Chen W T, Zhu A Y and Capasso F 2020 Flat optics with dispersion engineered-metasurfaces *Nat. Rev. Mater.* **5** 604–20
- [69] Khorasaninejad M and Capasso F 2017 Metalenses: versatile multifunctional photonics components *Science* **359** eaam8100
- [70] Tkachenko G, Stellinga D, Ruskuc A, Chen M, Dohlakia K and Krauss T F 2018 Optical trapping with planar silicon metalenses *Opt. Lett.* **43** 3224–7
- [71] Chantakit T, Schlickriede C, Sain B, Meyer F, Weiss T, Chattham N and Zentgraf T 2020 All-dielectric silicon metalens for two-dimensional particle manipulation in optical tweezers *Photon. Res.* **8** 1435
- [72] Andr  n D, Baranov D G, Jones S, Volpe G, Verre R and K  ll M 2021 Microscopic metavehicles powered and steered by embedded optical metasurfaces *Nat. Nanotechnol.* **16** 970–4
- [73] Plidschun M, Ren H, Kim J, F  rster R, Maier S A and Schmidt M A 2021 Ultrahigh numerical aperture meta-fibre for flexible optical trapping *Light Sci. Appl.* **10** 57
- [74] Ashkin A 1992 Forces of a single-beam gradient laser trap on a dielectric sphere in the ray optics regime *Biophys. J.* **61** 569–82
- [75] Ashkin A 1997 Optical trapping and manipulation of neutral particles using lasers *Proc. Natl Acad. Sci. USA* **94** 4853–60
- [76] Chang Y-R, Hsu L and Chi S 2006 Optical trapping of a spherically symmetric sphere in the ray-optics regime: a model for optical tweezers upon cells *Appl. Opt.* **45** 3885–92
- [77] Skelton S, Sergides M, Memoli G, Marag   O and Jones P 2012 Trapping and deformation of microbubbles in a dual-beam fibre-optic trap *J. Opt.* **14** 075706
- [78] Kajorndejnukul V, Ding W, Sukhov S, Qiu C-W and Dogariu A 2013 Linear momentum increase and negative optical forces at dielectric interface *Nat. Photon.* **7** 787–90
- [79] Catal   F, Mars   F, Arnau Farr   M-U M and Mart  n-Badosa E 2017 Extending calibration-free force measurements to optically-trapped rod-shaped samples *Sci. Rep.* **7** 42960
- [80] Sun B, Yang P, Kattawar G W and Zhang X 2017 Physical-geometric optics method for large size faceted particles *Opt. Express* **25** 24044–60
- [81] Masoumeh Mousavi S, Kasianiuk I, Denis Kasyanyuk S K, Velu P, Callegari A, Biancofiore L and Volpe G 2019 Clustering of Janus particles in an optical potential driven by hydrodynamic fluxes *Soft Matter* **15** 5748–59
- [82] Campos W H, Fonseca J M, Mendes J B S, Rocha M S and Moura-Melo W A 2018 How light absorption modifies the radiative force on a microparticle in optical tweezers *Appl. Opt.* **57** 7216–24
- [83] Park B J and Furst E M 2008 Optical trapping forces for colloids at the oil–water interface *Langmuir* **24** 13383–92
- [84] Muinonen K, Nousiainen T, Lindqvist H, Mu  oz O and Videen G 2009 Light scattering by Gaussian particles with internal inclusions and roughened surfaces using ray optics *J. Quant. Spectrosc. Radiat. Transfer* **110** 1628–39
- [85] Konoshonkin A V, Kustova N V and Borovoi A G 2015 Beam-splitting code for light scattering by ice crystal particles within geometric-optics approximation *J. Quant. Spectrosc. Radiat. Transfer* **164** 175–83
- [86] Callegari A, Mite Mijalkov A, G  k  z B and Volpe G 2015 Computational toolbox for optical tweezers in geometrical optics *J. Opt. Soc. Am. B* **32** B11–B19
- [87] Isaac C D, Lenton G V, Stilgoe A B, Nieminen T A and Rubinsztajn-Dunlop H 2020 Machine learning reveals complex behaviours in optically trapped particles *Mach. Learn.: Sci. Technol.* **1** 045009
- [88] Roichman Y, Sun B, Roichman Y, Amato-Grill J and Grier D G 2008 Optical forces arising from phase gradients *Phys. Rev. Lett.* **100** 013602
- [89] Albaladejo S, Marqu  s M I, Laroche M and S  enz J J 2009 Scattering forces from the curl of the spin angular momentum of a light field *Phys. Rev. Lett.* **102** 113602
- [90] Nieto-Vesperinas M, S  enz J J, G  mez-Medina R and Chantada L 2010 Optical forces on small magnetodielectric particles *Opt. Express* **18** 11428
- [91] Liu L, Di Donato A, Ginis V, Kheifets S, Amirzhan A and Capasso F 2018 Three-dimensional measurement of the helicity-dependent forces on a Mie particle *Phys. Rev. Lett.* **120** 223901
- [92] Jon  s A and Zem  nek P 2008 Light at work: the use of optical forces for particle manipulation, sorting, and analysis *Electrophoresis* **29** 4813
- [93] Tkachenko G and Brasselet E 2014 Optofluidic sorting of material chirality by chiral light *Nat. Commun.* **5** 3577
- [94] Albaladejo S, S  enz J J and Marqu  s M I 2011 Plasmonic nanoparticle chain in a light field: a resonant optical sail *Nanoletters* **11** 4597
- [95] Delgado-Buscalioni R, Mel  ndez M, Luis-Hita J, Marqu  s M I and S  enz J J 2018 Emergence of collective dynamics of gold nanoparticles in an optical vortex lattice *Phys. Rev. E* **98** 062614
- [96] Edelstein S, Garc  a-Mart  n A, Serena P A and Marqu  s M I 2021 Magneto-optical binding in the near field *Sci. Rep.* **11** 2820



- [97] Luis-Hita J, Marqués M I, Delgado-Buscalioni R, de Sousa N, Froufe-Pérez L S, Scheffold F and Sáenz J J 2019 Light induced inverse-square law interactions between nanoparticles: ‘Mock gravity’ at the nanoscale *Phys. Rev. Lett.* **123** 143201
- [98] Edelstein S, Abraham-Ekeröth R M, Serena P A, Sáenz J J, García-Martín A and Marqués M I 2019 Magneto-optical Stern–Gerlach forces and nonreciprocal torques on small particles *Phys. Rev. Res.* **1** 013005
- [99] Marqués M I, Edelstein S and Serena P A 2021 A proposal to measure Belinfante’s curl of the spin optical force based on the Kerker conditions *Eur. Phys. J. Plus* **136** 185
- [100] Gouesbet G and Gréhan G 2017 *Generalized Lorenz-Mie Theories* (Springer International Publishing)
- [101] Gouesbet G, Maheu B and Gréhan G 1988 Light scattering from a sphere arbitrarily located in a Gaussian beam, using a Bromwich formulation *J. Opt. Soc. Am. A* **5** 1427–43
- [102] Barton J P and Alexander D R 1989 Fifth-order corrected electromagnetic field components for a fundamental Gaussian beam *J. Appl. Phys.* **66** 2800–2
- [103] Simmons R, Finer J, Chu S and Spudis J 1996 Quantitative measurements of force and displacement using an optical trap *Biophys. J.* **70** 1813–22
- [104] Fontes A, Neves A A R, Moreira W L, de Thomaz A A, Barbosa L C, Cesar C L and de Paula A M 2005 Double optical tweezers for ultrasensitive force spectroscopy in microsphere Mie scattering *Appl. Phys. Lett.* **87** 221109
- [105] Neves A A R and Cesar C L 2019 Analytical calculation of optical forces on spherical particles in optical tweezers: tutorial *J. Opt. Soc. Am. B* **36** 1525–37
- [106] Moreira W L, Neves A A R, Garbos M K, Euser T G and Cesar C L 2016 Expansion of arbitrary electromagnetic fields in terms of vector spherical wave functions *Opt. Express* **24** 2370–82
- [107] Waterman P C 1971 Symmetry, unitarity, and geometry in electromagnetic scattering *Phys. Rev. D* **3** 825–39
- [108] Mishchenko M I 2020 Comprehensive thematic T-matrix reference database: a 2017–2019 update *J. Quant. Spectrosc. Radiat. Transfer* **242** 106692
- [109] Bui A A, Stilgoe A B, Lenton I C, Gibson L J, Kashchuk A V, Zhang S, Rubinshtein-Dunlop H and Nieminen T A 2017 Theory and practice of simulation of optical tweezers *J. Quant. Spectrosc. Radiat. Transfer* **195** 66–75
- [110] Polimeno P et al 2018 Optical tweezers and their applications *J. Quant. Spectrosc. Radiat. Transfer* **218** 131–50
- [111] Borghese F, Denti P and Saija R 2007 *Scattering from Model Nonspherical Particles. Theory and Applications to Environmental Physics* (Berlin: Springer)
- [112] Wolf E and Nieto-Vesperinas M 1985 Analyticity of the angular spectrum amplitude of scattered fields and some of its consequences *J. Opt. Soc. Am. A* **2** 886–90
- [113] Borghese F, Denti P, Saija R and Iati M A 2007 Optical trapping of nonspherical particles in the T-matrix formalism *Opt. Express* **15** 11984–98
- [114] Donato M G, Patti F, Saija R, Iati M A, Gucciardi P G, Pedaci F, Strangi G and Maragò O M 2021 Improved backscattering detection in photonic force microscopy near dielectric surfaces with cylindrical vector beams *J. Quant. Spectrosc. Radiat. Transfer* **258** 107381
- [115] Simpson S H and Hanna S 2009 Optical angular momentum transfer by Laguerre-Gaussian beams *J. Opt. Soc. Am. A* **26** 625–38
- [116] Capolino F 2017 *Theory and Phenomena of Metamaterials* (Boca Raton, FL: CRC Press)
- [117] Kiasat Y, Donato M G, Hinczewski M, ElKabbash M, Letsou T, Saija R, Maragò O M, Strangi G and Engheta N 2022 Epsilon-near-zero (ENZ)-based optomechanics (arXiv:2203.07525)
- [118] Patti F, Saija R, Denti P, Pellegrini G, Biagioni P, Iati M A and Maragò O M 2019 Chiral optical tweezers for optically active particles in the T-matrix formalism *Sci. Rep.* **9** 29
- [119] Polimeno P et al 2021 Optical tweezers in a dusty universe *Eur. Phys. J.* **136** 1–23
- [120] Poynting J H 1909 The wave motion of a revolving shaft, and a suggestion as to the angular momentum in a beam of circularly polarised light *Proc. R. Soc. A* **82** 560–7
- [121] Allen L, Beijersbergen M W, Spreeuw R and Woerdman J 1992 Orbital angular momentum of light and the transformation of Laguerre–Gaussian laser modes *Phys. Rev. A* **45** 8185
- [122] Friese M E, Nieminen T A, Heckenberg N R and Rubinshtein-Dunlop H 1998 Optical alignment and spinning of laser-trapped microscopic particles *Nature* **394** 348–50
- [123] Banzer P, Neugebauer M, Aiello A, Marquardt C, Lindlein N, Bauer T and Leuchs G 2013 The photonic wheel—demonstration of a state of light with purely transverse angular momentum *J. Eur. Opt. Soc.* **8** 13032
- [124] Bishop A I, Nieminen T A, Heckenberg N R and Rubinshtein-Dunlop H 2004 Optical microrheology using rotating laser-trapped particles *Phys. Rev. Lett.* **92** 198104
- [125] Richards B and Wolf E 1959 Electromagnetic diffraction in optical systems, ii. structure of the image field in an aplanatic system *Proc. R. Soc. A* **253** 358–79
- [126] Stilgoe A B, Nieminen T A and Rubinshtein-Dunlop H 2022 Controlled transfer of transverse optical angular momentum to optically trapped birefringent particles *Nat. Photon.* **16** 346–51
- [127] Neugebauer M, Bauer T, Aiello A and Banzer P 2015 Measuring the transverse spin density of light *Phys. Rev. Lett.* **114** 063901
- [128] Neugebauer M, Eismann J S, Bauer T and Banzer P 2018 Magnetic and electric transverse spin density of spatially confined light *Phys. Rev. X* **8** 021042
- [129] Malmqvist L and Hertz H M 1992 Trapped particle optical microscopy *Opt. Commun.* **94** 19–24
- [130] Ghislain L P and Webb W W 1993 Scanning-force microscope based on an optical trap *Opt. Lett.* **18** 1678–80
- [131] Kawata S, Inoué Y and Sugiura T 1994 Near-field scanning optical microscope with a laser trapped probe *Jpn. J. Appl. Phys.* **33** L1725
- [132] Maragò O M, Gucciardi P G and Jones P H 2010 Photonic force microscopy: from femtonewton force sensing to ultra-sensitive spectroscopy *Scanning Probe Microscopy in Nanoscience and Nanotechnology* (Berlin: Springer) pp 23–56
- [133] Florin E-L, Pralle A, Heinrich Hörber J K and Stelzer E H K 1997 Photonic force microscope based on optical tweezers and two-photon excitation for biological applications *J. Struct. Biol.* **119** 202–11
- [134] Bartsch T F, Kochanzyk M D, Lissek E N, Lange J R and Florin E-L 2016 Nanoscopic imaging of thick heterogeneous soft-matter structures in aqueous solution *Nat. Commun.* **7** 1–9
- [135] Friedrich L and Rohrbach A 2015 Surface imaging beyond the diffraction limit with optically trapped spheres *Nat. Nanotechnol.* **10** 1064–9
- [136] Nakayama Y, Pauzauksie P J, Radenovic A, Onorato R M, Saykally R J, Liphardt J and Yang P 2007 Tunable nanowire nonlinear optical probe *Nature* **447** 1098–101

- [137] Marago O M, Jones P H, Bonaccorso F, Scardaci V, Gucciardi P G, Rozhin A G and Ferrari A C 2008 Femtonewton force sensing with optically trapped nanotubes *Nano Lett.* **8** 3211–6
- [138] Phillips D B, Grieve J A, Olof S N, Kocher S J, Bowman R, Padgett M J, Miles M J and Carberry D M 2011 Surface imaging using holographic optical tweezers *Nanotechnology* **22** 285503
- [139] Phillips D B, Padgett M J, Hanna S, Ho Y-L D, Carberry D M, Miles M J and Simpson S H 2014 Shape-induced force fields in optical trapping *Nat. Photon.* **8** 400–5
- [140] Desgarceaux R, Santybayeva Z, Battistella E, Nord A L, Braun-Breton C, Abkarian M, Maragò O M, Charlot B and Pedaci F 2020 High-resolution photonic force microscopy based on sharp nanofabricated tips *Nano Lett.* **20** 4249–55
- [141] Ghosh S and Ghosh A 2019 All optical dynamic nanomanipulation with active colloidal tweezers *Nat. Commun.* **10** 1–8
- [142] Pedaci F, Huang Z, Maarten V O, Barland S and Dekker N H 2011 Excitable particles in an optical torque wrench *Nat. Phys.* **7** 259–64
- [143] Bennett J S, Gibson L J, Kelly R M, Brousse E, Baudisch B, Preece D, Nieminen T A, Nicholson T, Heckenberg N R and Rubinsztein-Dunlop H 2013 Spatially-resolved rotational microrheology with an optically-trapped sphere *Sci. Rep.* **3** 1–5
- [144] Capitanio M, Canepari M, Maffei M, Beneventi D, Monico C, Vanzi F, Bottinelli R and Pavone F S 2012 Ultrafast force-clamp spectroscopy of single molecules reveals load dependence of myosin working stroke *Nat. Methods* **9** 1013–9
- [145] Grimm M, Franosch T and Jeney S 2012 High resolution detection of Brownian motion for quantitative optical tweezers experiments *Phys. Rev. E* **86** 021912
- [146] Raizen M and Li T 2015 The measurement Einstein deemed impossible *Phys. Today* **68** 56
- [147] Chavez I, Huang R, Henderson K, Florin E-L and Raizen M G 2008 Development of a fast position-sensitive laser beam detector *Rev. Sci. Instrum.* **79** 105104
- [148] Kheifets S, Simha A, Melin K, Li T and Raizen M G 2014 Observation of Brownian motion in liquids at short times: instantaneous velocity and memory loss *Science* **343** 1493–6
- [149] Waitukaitis S R and Jaeger H M 2012 Impact-activated solidification of dense suspensions via dynamic jamming fronts *Nature* **487** 205–9
- [150] Taylor M A, Janousek J, Daria V, Knittel J, Hage B, Bachor H-A and Bowen W P 2013 Biological measurement beyond the quantum limit *Nat. Photon.* **7** 229–33
- [151] Casacio C A, Madsen L S, Terrasson A, Waleed M, Barnscheidt K, Hage B, Taylor M A and Bowen W P 2021 Quantum-enhanced nonlinear microscopy *Nature* **594** 201
- [152] La Porta A and Wang M D 2004 Optical torque wrench: angular trapping, rotation and torque detection of quartz microparticles *Phys. Rev. Lett.* **92** 190801
- [153] Deufel C, Forth S, Simmons C R, Dejgosha S and Wang M D 2007 Nanofabricated quartz cylinders for angular trapping: DNA supercoiling torque detection *Nat. Methods* **4** 223–5
- [154] Ramaiya A, Roy B, Bugiel M and Schaffer E 2017 Kinesin rotates unidirectionally and generates torque while walking on microtubules *Proc. Natl Acad. Sci. USA* **114** 10894–9
- [155] Vaipplully R, Ramanujan V, Gopalakrishnan M, Bajpai S and Roy B 2020 Detection of sub-degree angular fluctuations of the local cell membrane slope using optical tweezers *Soft Matter* **16** 7606–12
- [156] Bovyn M, Reddy B, Gross S and Allard J 2021 Diffusion of kinesin motors on cargo can enhance binding and run lengths during intracellular transport *Mol. Biol. Cell* **32** 984–94
- [157] Bang J, Sebersen T, Ju P, Ahn J, Xu Z, Gao X, Robicheaux F and Li T 2020 Five-dimensional cooling and nonlinear dynamics of an optically levitated nanodumbbell *Phys. Rev. Res.* **2** 043054
- [158] Roy B, Ramaiya A and Schaffer E 2018 Determination of pitch rotation in a spherical birefringent microparticle *J. Opt.* **20** 035603
- [159] Kumar S, Gunaseelan M, Vaipplully R, Kumar A, Ajith M, Vaidya G, Dutta S and Roy B 2020 Pitch-rotational manipulation of single cells and particles using single-beam thermo-optical tweezers *Biomed. Opt. Exp.* **11** 3555–66
- [160] Nalupurackal G et al 2022 Simultaneous optical trapping and magnetic micromanipulation of ferromagnetic iron-doped upconversion microparticles in six degrees of freedom (arXiv:2203.02152)
- [161] Lokesh M, Vaipplully R, Nalupurackal G, Roy S, Bhallamudi V P, Prabhakar A and Roy B 2021 Estimation of rolling work of adhesion at the nanoscale with soft probing using optical tweezers *RSC Adv.* **11** 34636
- [162] Lokesh M, Vaipplully R, Bhallamudi V P, Prabhakar A and Roy B 2021 Realization of pitch-rotational torque wrench in two-beam optical tweezers *J. Phys. Commun.* **5** 115016
- [163] Ghislain L P, Switz N A and Webb W W 1994 Measurement of small forces using an optical trap *Rev. Sci. Instrum.* **65** 2762–8
- [164] Simpson N, Dholakia K, Allen L and Padgett M 1997 Mechanical equivalence of spin and orbital angular momentum of light: an optical spanner *Opt. Lett.* **22** 52–54
- [165] Smith S B, Cui Y and Bustamante C 2003 Optical-trap force transducer that operates by direct measurement of light momentum *Methods in Enzymology* vol 361, ed G Marriott and I Parker (New York: Academic) pp 134–62
- [166] Farré A and Montes-Usategui M 2010 A force detection technique for single-beam optical traps based on direct measurement of light momentum changes *Opt. Express* **18** 11955
- [167] Thalhammer G, Obmascher L and Ritsch-Marte M 2015 Direct measurement of axial optical forces *Opt. Express* **23** 6112–29
- [168] Berg-Sørensen K and Flyvbjerg H 2004 Power spectrum analysis for optical tweezers *Rev. Sci. Instrum.* **75** 594–612
- [169] Strasser F, Moser S, Ritsch-Marte M and Thalhammer G 2021 Direct measurement of individual optical forces in ensembles of trapped particles *Optica* **8** 79–87
- [170] Strasser F, Barnett S M, Ritsch-Marte M and Thalhammer G 2022 Generally applicable holographic torque measurement for optically trapped particles *Phys. Rev. Lett.* **128** 213604
- [171] Tolic-Nørrelykke S F, Schäffer E, Howard J, Pavone F S, Jülicher F and Flyvbjerg H 2006 Calibration of optical tweezers with positional detection in the back focal plane *Rev. Sci. Instrum.* **77** 103101
- [172] Omori R, Kobayashi T and Suzuki A 1997 Observation of a single-beam gradient-force optical trap for dielectric particles in air *Opt. Lett.* **22** 816–8
- [173] Gieseler J, Deutsch B, Quidant R and Novotny L 2012 Subkelvin parametric feedback cooling of a laser-trapped nanoparticle *Phys. Rev. Lett.* **109** 103603
- [174] Risken H 1996 *The Fokker-Planck Equation* (Berlin: Springer)
- [175] Frishman A and Pierre R 2020 Learning force fields from stochastic trajectories *Phys. Rev. X* **10** 021009
- [176] Gavrilov M, Yonggun J and Bechhoefer J 2014 Real-time calibration of a feedback trap *Rev. Sci. Instrum.* **85** 095102
- [177] García L P, Pérez J D, Volpe G, Arzola A V and Volpe G 2018 High-performance reconstruction of microscopic force fields from Brownian trajectories *Nat. Commun.* **9** 1–9

- [178] Wu P, Huang R, Tischer C, Jonas A and Florin E-L 2009 Direct measurement of the nonconservative force field generated by optical tweezers *Phys. Rev. Lett.* **103** 108101
- [179] Huang R, Chavez I, Taute K M, Lukić B, Jeney S, Raizen M G and Florin E-L 2011 Direct observation of the full transition from ballistic to diffusive Brownian motion in a liquid *Nat. Phys.* **7** 576–80
- [180] Helgadottir S, Argun A and Volpe G 2019 Digital video microscopy enhanced by deep learning *Optica* **6** 506–13
- [181] Midtvedt B, Helgadottir S, Argun A, Pineda J, Midtvedt D and Volpe G 2021 Quantitative digital microscopy with deep learning *Appl. Phys. Rev.* **8** 011310
- [182] Argun A, Thalheim T, Bo S, Cichos F and Volpe G 2020 Enhanced force-field calibration via machine learning *Appl. Phys. Rev.* **7** 041404
- [183] Argun A, Volpe G and Bo S 2021 Classification, inference and segmentation of anomalous diffusion with recurrent neural networks *J. Phys. A: Math. Theor.* **54** 294003
- [184] Argun A, Thalheim T, Bo S, Cichos F and Volpe G 2020 *DeepCalib* (available at: <https://github.com/softmatterlab/DeepCalib>)
- [185] Muñoz-Gil G et al 2021 Objective comparison of methods to decode anomalous diffusion *Nat. Commun.* **12** 6253
- [186] Mizuno D, Tardin C, Schmidt C and Mackintosh F 2007 Nonequilibrium mechanics of active cytoskeletal networks *Science* **315** 370–3
- [187] Hurst S, Vos B E, Brandt M and Betz T 2021 Intracellular softening and increased viscoelastic fluidity during division *Nat. Phys.* **17** 1270–6
- [188] Mason T G and Weitz D A 1995 Optical measurements of frequency-dependent linear viscoelastic moduli of complex fluids *Phys. Rev. Lett.* **74** 1250–3
- [189] Turlier H and Betz T 2019 Unveiling the active nature of living-membrane fluctuations and mechanics *Annu. Rev. Condens. Matter Phys.* **10** 213–32
- [190] Guo M, Ehrlicher A, Jensen M, Renz M, Moore J, Goldman R, Lippincott-Schwartz J, Mackintosh F and Weitz D 2014 Probing the stochastic, motor-driven properties of the cytoplasm using force spectrum microscopy *Cell* **158** 822–32
- [191] Chapman C D and Robertson-Anderson R M 2014 Nonlinear microrheology reveals entanglement-driven molecular-level viscoelasticity of concentrated DNA *Phys. Rev. Lett.* **113** 098303
- [192] Haro-González P et al 2013 Quantum dot-based thermal spectroscopy and imaging of optically trapped microspheres and single cells *Small* **9** 2162–70
- [193] Turlier H, Fedosov D A, Audoly B, Auth T, Gov N S, Sykes C, Joanny J-F, Gompper G and Betz T 2016 Equilibrium physics breakdown reveals the active nature of red blood cell flickering *Nat. Phys.* **12** 513–9
- [194] Levine A J and Lubensky T C 2000 One- and two-particle microrheology *Phys. Rev. Lett.* **85** 1774–7
- [195] Waigh T A 2016 Advances in the microrheology of complex fluids *Rep. Prog. Phys.* **79** 074601
- [196] Preece D, Warren R, Evans R M L, Gibson G M, Padgett M J, Cooper J M and Tassieri M 2011 Optical tweezers: wideband microrheology *J. Opt.* **13** 044022
- [197] Minzioni P et al 2017 Roadmap for optofluidics *J. Opt.* **19** 093003
- [198] Yao A, Tassieri M, Padgett M and Cooper J 2009 Microrheology with optical tweezers *Lab Chip* **9** 2568–75
- [199] Yang T, Nava G, Vitali V, Bragheri F, Osellame R, Bellini T, Cristiani I and Minzioni P 2017 Integrated optofluidic chip for low-volume fluid viscosity measurement *Micromachines* **8** 65
- [200] Bellini N, Vishnubhatla K C, Bragheri F, Ferrara L, Minzioni P, Ramponi R, Cristiani I and Osellame R 2010 Femtosecond laser fabricated monolithic chip for optical trapping and stretching of single cells *Opt. Express* **18** 4679–88
- [201] Vitali V, Nava G, Zanchetta G, Bragheri F, Crespi A, Osellame R, Bellini T, Cristiani I and Minzioni P 2020 Integrated optofluidic chip for oscillatory microrheology *Sci. Rep.* **10** 5831
- [202] Nava G et al 2018 Newtonian to non-Newtonian fluid transition of a model transient network *Soft Matter* **14** 17
- [203] Vitali V 2021 Yield stress in a flash: investigation of nonlinearity and yielding in soft materials with an optofluidic microrheometer *Soft Matter* **17** 3105–12
- [204] Ferrara L, Baldini E, Minzioni P, Bragheri F, Liberale C, Fabrizio E D and Cristiani I 2011 Experimental study of the optical forces exerted by a Gaussian beam within the Rayleigh range *J. Opt.* **13** 075712
- [205] Svoboda K and Block S M 1994 Optical trapping of metallic Rayleigh particles *Opt. Lett.* **19** 930–2
- [206] Maragò O M, Jones P H, Gucciardi P G, Volpe G and Ferrari A C 2013 Optical trapping and manipulation of nanostructures *Nat. Nanotechnol.* **8** 807–19
- [207] Bendix P M, Reihani S N S and Oddershede L B 2010 Direct measurements of heating by electromagnetically trapped gold nanoparticles on supported lipid bilayers *ACS Nano* **4** 2256–62
- [208] Andres-Arroyo A, Gupta B, Wang F, Gooding J J and Reece P J 2016 Optical manipulation and spectroscopy of silicon nanoparticles exhibiting dielectric resonances *Nano Lett.* **16** 1903–10
- [209] Rodríguez-Sevilla P, Prorok K, Bednarkiewicz A, Marqués M I, García-Martín A, García Solé J, Haro-González P and Jaque D 2018 Optical forces at the nanoscale: size and electrostatic effects *Nano Lett.* **18** 602–9
- [210] Juan M L, Bradac C, Besga B, Johnsson M, Brennen G, Molina-Terriza G and Volz T 2017 Cooperatively enhanced dipole forces from artificial atoms in trapped nanodiamonds *Nat. Phys.* **13** 241–5
- [211] Shan X et al 2021 Optical tweezers beyond refractive index mismatch using highly doped upconversion nanoparticles *Nat. Nanotechnol.* **16** 531–7
- [212] Polimeno P, Patti F, Infusino M, Sánchez J, Iatì M A, Saija R, Volpe G, Maragò O M and Veltri A 2020 Gain-assisted optomechanical position locking of metal/dielectric nanoshells in optical potentials *ACS Photonics* **7** 1262–70
- [213] Ndukaife J C, Kildishev A V, Nnanna A G A, Shalae V M, Weryley S T and Boltasseva A 2016 Long-range and rapid transport of individual nano-objects by a hybrid electrothermoplasmonic nanotweezer *Nat. Nanotechnol.* **11** 53–59
- [214] Roder P B, Smith B E, Zhou X, Crane M J and Pauzauskie P J 2015 Laser refrigeration of hydrothermal nanocrystals in physiological media *Proc. Natl Acad. Sci.* **112** 15024–9
- [215] Juan M L, Righini M and Quidant R 2011 Plasmon nano-optical tweezers *Nat. Photon.* **5** 349–56
- [216] Xu Z, Song W and Crozier K B 2018 Optical trapping of nanoparticles using all-silicon nanoantennas *ACS Photonics* **5** 4993–5001
- [217] Chen Y-F, Serey X, Sarkar R, Chen P and Erickson D 2012 Controlled photonic manipulation of proteins and other nanomaterials *Nano Lett.* **12** 1633–7
- [218] Pang Y and Gordon R 2012 Optical trapping of a single protein *Nano Lett.* **12** 402–6
- [219] Mestres P, Berthelot J, Aćimović S S and Quidant R 2016 Unraveling the optomechanical nature of plasmonic trapping *Light Sci. Appl.* **5** e16092
- [220] Yang S, Hong C, Jiang Y and Ndukaife J C 2021 Nanoparticle trapping in a quasi-BIC system *ACS Photonics* **8** 1961–71

- [221] Hong C, Yang S and Ndukaife J C 2020 Stand-off trapping and manipulation of sub-10 nm objects and biomolecules using opto-thermo-electrohydrodynamic tweezers *Nat. Nanotechnol.* **15** 908–13
- [222] Kotnala A et al 2014 Double nanohole optical tweezers visualize protein p53 suppressing unzipping of single DNA-hairpins *Biomed. Opt. Express* **5** 1886–94
- [223] Geiselmann M, Marty R, Renger J, García De Abajo F J and Quidant R 2014 Deterministic optical-near-field-assisted positioning of nitrogen-vacancy centers *Nano Lett.* **14** 1520–5
- [224] Schirhagl R, Chang K, Loretz M and Degen C L 2014 Nitrogen-vacancy centers in diamond: nanoscale sensors for physics and biology *Annu. Rev. Phys. Chem.* **65** 83–105
- [225] Roberts R P 2018 Towards cooperatively enhanced resonant dipole forces in optical levitation, harnessing quantum emitters in diamonds *PhD Thesis* (available at: <http://hdl.handle.net/1959.14/1271361>)
- [226] Bradac C, Say J M, Rastogi I D, Cordina N M, Volz T and Brown L J 2016 Nano-assembly of nanodiamonds by conjugation to actin filaments *J. Biophoton.* **9** 296–304
- [227] Hoang T M, Ahn J, Bang J and Li T 2016 Electron spin control of optically levitated nanodiamonds in vacuum *Nat. Commun.* **7** 12250
- [228] Bose S, Mazumdar A, Morley G W, Ulbricht H, Toro's M, Paternostro M, Geraci A A, Barker P F, Kim M S and Milburn G 2017 Spin entanglement witness for quantum gravity *Phys. Rev. Lett.* **119** 240401
- [229] Frangeskou A C, Rahman A T M A, Gines L, Mandal S, Williams O A, Barker P F and Morley G W 2018 Pure nanodiamonds for levitated optomechanics in vacuum *New J. Phys.* **20** 043016
- [230] De Feudis M, Tallaire A, Nicolas L, Brinza O, Goldner P, Hetet G, Benedic F and Achard J 2020 Large-scale fabrication of highly emissive nanodiamonds by chemical vapor deposition with controlled doping by SiV and GeV centers from a solid source *Adv. Mater. Interfaces* **7** 1901408
- [231] Russell L W, Dossetor E C, Wood A A, Simpson D A and Reece P J 2021 Optimizing optical tweezers experiments for magnetic resonance sensing with nanodiamonds *ACS Photonics* **8** 1214–21
- [232] White J, Laplane C, Roberts R P, Brown L J, Volz T and Inglis D W 2020 Characterization of optofluidic devices for the sorting of sub-micrometer particles *Appl. Opt.* **59** 271–6
- [233] Chung H S, McHale K, Louis J M and Eaton W A 2012 Single-molecule fluorescence experiments determine protein folding transition path times *Science* **335** 981–4
- [234] Young G et al 2018 Quantitative mass imaging of single biological macromolecules *Science* **360** 423–7
- [235] Schmid S, Stömmmer P, Dietz H and Dekker C 2021 Nanopore electro-osmotic trap for the label-free study of single proteins and their conformations *Nat. Nanotechnol.* **16** 1244–50
- [236] Gordon R 2019 Biosensing with nanoaperture optical tweezers' *Opt. Laser Technol.* **109** 328–35
- [237] Verschueren D, Shi X and Dekker C 2019 Nano-optical tweezing of single proteins in plasmonic nanopores *Small Methods* **3** 1800465
- [238] Peri S S S, Sabnani M K, Raza M U, Ghaffari S, Gimlin S, Wawro D D, Lee J S, Kim M J, Weidanz J and Alexandrakis G 2020 Detection of specific antibody-ligand interactions with a self-induced back-action actuated nanopore electrophoresis sensor *Nanotechnology* **31** 085502
- [239] Peri S S S, Sabnani M K, Raza M U, Urquhart E L, Ghaffari S, Lee J S, Kim M J, Weidanz J and Alexandrakis G 2021 Quantification of low affinity binding interactions between natural killer cell inhibitory receptors and targeting ligands with a self-induced back-action actuated nanopore electrophoresis (SANE) sensor *Nanotechnology* **32** 045501
- [240] Gelfand R M, Wheaton S and Gordon R 2014 Cleaved fiber optic double nanohole optical tweezers for trapping nanoparticles *Opt. Lett.* **39** 6415
- [241] Novotny L, Bian R X and Xie X S 1997 Theory of nanometric optical tweezers *Phys. Rev. Lett.* **79** 645–8
- [242] Ashkin A and Dziedzic J M 1971 Optical levitation by radiation pressure *Appl. Phys. Lett.* **19** 283–5
- [243] Gong Z, Pan Y L, Videen G and Wang C 2018 Optical trapping and manipulation of single particles in air: principles, technical details, and applications *J. Quant. Spectrosc. Radiat. Transfer* **214** 94–119
- [244] Marmolejo J T, González M U, Isaksson O, Johansson A, Fragoso R M and Hanstorp D 2021 Visualizing the electron's quantization with a ruler *Sci. Rep.* **11** 1–5
- [245] Rondin L, Gieseler J, Ricci F, Quidant R, Dellago C and Novotny L 2017 Direct measurement of Kramers turnover with a levitated nanoparticle *Nat. Nanotechnol.* **12** 1130–3
- [246] Ward A D, Zhang M and Hunt O 2006 Broadband Mie scattering from optically levitated aerosol droplets using a white LED *Opt. Express* **16** 016390
- [247] Arita Y, Mazilu M and Dholakia K 2013 Laser-induced rotation and cooling of a trapped microgyroscope in vacuum *Nat. Commun.* **4** 2374
- [248] Kalume A, Wang C, Santarpia J and Pan Y-L 2018 Liquid-liquid phase separation and evaporation of a laser-trapped organic-organic airborne droplet using temporal spatial-resolved Raman spectroscopy *Phys. Chem. Chem. Phys.* **20** 19151–9
- [249] Diveky M E, Gleichweit M J, Roy S and Signorell R 2021 Shining new light on the kinetics of water uptake by organic aerosol particles *J. Phys. Chem. A* **125** 3528–48
- [250] Price C L, Bain A, Wallace B J, Preston T C and Davies J F 2020 Simultaneous retrieval of the size and refractive index of suspended droplets in a linear quadrupole electrodynamic balance *J. Phys. Chem. A* **124** 1811–20
- [251] Walker J S, Carruthers A E, Orr-Ewing A J and Reid J P 2013 Measurements of light extinction by single aerosol particles *J. Phys. Chem. Lett.* **4** 1748–52
- [252] Ahn J, Xu Z, Bang J, Deng Y-H, Hoang T M, Han Q, Ma R-M and Li T 2018 Optically levitated nanodumbbell torsion balance and GHz nanomechanical rotor *Phys. Rev. Lett.* **121** 033603
- [253] Kuhn S, Stickler B A, Kosloff A, Patolsky E, Hornberger K, Arndt M and Millen J 2017 Optically driven ultra-stable nanomechanical rotor *Nat. Commun.* **8** 1670
- [254] Ahn J, Xu Z, Bang J, Ju P, Gao X and Li T 2020 Ultrasensitive torque detection with an optically levitated nanorotor *Nat. Nanotechnol.* **15** 89–93
- [255] Stickler B A, Papendell B, Kuhn S, Schrinke B, Millen J, Arndt M and Hornberger K 2018 Probing macroscopic quantum superpositions with nanorotors *New J. Phys.* **20** 122001
- [256] Pendry J B 2010 Quantum friction—fact or fiction? *New J. Phys.* **12** 033028
- [257] Gooding C, Weinfurter S and Unruh W 2020 Reinventing the Zel'Dovich wheel *Phys. Rev. A* **101** 063819
- [258] Arita Y, Simpson S H, Zemánek P and Dholakia K 2020 Coherent oscillations of a levitated birefringent microsphere in vacuum driven by nonconservative rotation-translation coupling *Sci. Adv.* **6** aaz9858



- [259] Xu Z, Jacob Z and Li T 2021 Enhancement of rotational vacuum friction by surface photon tunneling *Nanophotonics* **10** 537
- [260] van der Laan F, Tebbenjohanns F, Reimann R, Vijayan J, Novotny L and Frimmer M 2021 Sub-Kelvin feedback cooling and heating dynamics of an optically levitated librator *Phys. Rev. Lett.* **127** 123605
- [261] Hoang T M, Ma Y, Ahn J, Bang J, Robicheaux F, Yin Z-Q and Li T 2016 Torsional optomechanics of a levitated nonspherical nanoparticle *Phys. Rev. Lett.* **117** 123604
- [262] Stickler B A, Hornberger K and Kim M S 2021 Quantum rotations of nanoparticles *Nat. Rev. Phys.* **3** 589–97
- [263] Reimann R, Doderer M, Hebestreit E, Diehl R, Frimmer M, Windey D, Tebbenjohanns F and Novotny L 2018 GHz rotation of an optically trapped nanoparticle in vacuum *Phys. Rev. Lett.* **121** 159901
- [264] Xu Z and Li T 2017 Detecting Casimir torque with an optically levitated nanorod *Phys. Rev. A* **96** 033843
- [265] Schäfer J, Rudolph H, Hornberger K and Stickler B A 2021 Cooling nanorotors by elliptic coherent scattering *Phys. Rev. Lett.* **126** 163603
- [266] Magrini L, Norte R A, Riedinger R, Marinković I, Grass D, Delić U, Gröblacher S, Hong S and Aspelmeyer M 2018 Near-field coupling of a levitated nanoparticle to a photonic crystal cavity *Optica* **5** 1597
- [267] Dholakia K and Zemánek P 2010 Grippled by light: optical binding *Rev. Mod. Phys.* **82** 1767–91
- [268] Brzobohatý O, Karásek V, Čížmár T and Zemánek P 2011 Dynamic size tuning of multidimensional optically bound matter *Appl. Phys. Lett.* **99** 101105
- [269] Brzobohatý O, Karásek V, Šiler M, Chvátal L, Čížmár T and Zemánek P 2013 Experimental demonstration of optical transport, sorting and self-arrangement using a tractor beam *Nat. Photon.* **7** 123–7
- [270] Brzobohatý O, Chvátal L, Jonáš A, Šiler M, Kaňka J, Ježek J and Zemánek P 2019 Tunable soft-matter optofluidic waveguides assembled by light *ACS Photonics* **6** 403–10
- [271] Donato M G, Brzobohatý O, Simpson S H, Irrera A, Leonardi A A, Lo Faro M J, Svak V, Maragò O M and Zemánek P 2019 Optical trapping, optical binding, and rotational dynamics of silicon nanowires in counter-propagating beams *Nano Lett.* **19** 342–52
- [272] Bykov D S, Xie S, Zeltner R, Machnev A, Wong G K L, Euser T G and Russell P S J 2018 Long-range optical trapping and binding of microparticles in hollow-core photonic crystal fibre *Light Sci. Appl.* **7** 22
- [273] Arita Y, Wright E M and Dholakia K 2018 Optical binding of two cooled micro-gyroscopes levitated in vacuum *Optica* **5** 910–7
- [274] Svak V, Flajšmanová J, Chvátal L, Šiler M, Jonáš A, Ježek J, Simpson S H, Zemánek P and Brzobohatý O 2021 Stochastic dynamics of optically bound matter levitated in vacuum *Optica* **8** 220–9
- [275] Rieser J, Ciampini M A, Rudolph H, Kiesel N, Hornberger K, Stickler B A, Aspelmeyer M and Delić U 2022 Observation of strong and tunable light-induced dipole-dipole interactions between optically levitated nanoparticles (arXiv:2203.04198)
- [276] England J L 2015 Dissipative adaptation in driven self-assembly *Nat. Nanotechnol.* **10** 919–23
- [277] Tebbenjohanns F, Mattana M L, Rossi M, Frimmer M and Novotny L 2021 Quantum control of a nanoparticle optically levitated in cryogenic free space *Nature* **595** 378–82
- [278] Ritort F 2019 The noisy and marvelous molecular world of biology *Inventions* **4** 24
- [279] Bustamante C, Liphardt J and Ritort F 2005 The nonequilibrium thermodynamics of small systems *Phys. Today* **58** 43–48
- [280] Seifert U 2012 Stochastic thermodynamics, fluctuation theorems and molecular machines *Rep. Prog. Phys.* **75** 126001
- [281] Ciliberto S 2017 Experiments in stochastic thermodynamics: short history and perspectives *Phys. Rev. X* **7** 021051
- [282] Rissone P, Bizarro C V and Ritort F 2022 Stem-loop formation drives RNA folding in mechanical unzipping experiments *Proc. Natl Acad. Sci. USA* **119** 3
- [283] Parrondo J M R, Horowitz J M and Sagawa T 2015 Thermodynamics of Information *Nat. Phys.* **11** 131
- [284] Horowitz J M and Gingrich T R 2020 Thermodynamic uncertainty relations constrain non-equilibrium fluctuations *Nat. Phys.* **16** 15–20
- [285] Santamaría-Holek I, López-Alamilla I N J, Hidalgo-Soria M and Pérez-Madrid A 2015 Nonlinear irreversible thermodynamics of single-molecule experiments *Phys. Rev. E* **91** 062714
- [286] Neupane K, Foster D, Dee D R, Yu H, Wang F and Woodside M T 2016 Direct observation of transition paths during the folding of proteins and nucleic acids *Science* **352** 239–42
- [287] Rico-Pasto M, Zaltron A, Davis S J, Frutos S and Ritort F 2022 Molten-globule like transition state of protein barnase measured with calorimetric force spectroscopy *Proc. Natl Acad. Sci. USA* **119** e2112382119
- [288] Keyser U F 2012 Optical tweezers for mechanical control over DNA in a nanopore *Nanopore-Based Technology* pp 115–34
- [289] Admon T, Rahav S and Roichman Y 2018 Experimental realization of an information machine with tunable temporal correlations *Phys. Rev. Lett.* **121** 180601
- [290] Flatt S, Busiello D M, Zamuner S and De Los Rios P 2021 ABC transporters are billion-year-old Maxwell demons *bioRxiv Preprint* (<https://doi.org/10.1101/2021.12.03.471046>) (posted online 3 December 2021)
- [291] Jacob F 1977 Evolution and tinkering *Science* **196** 1161
- [292] Mehl J, Blickle V, Seifert U and Bechinger C 2010 Experimental accessibility of generalized fluctuation-dissipation relations for nonequilibrium steady states *Phys. Rev. E* **82** 032401
- [293] Hoang T M, Pan R, Ahn J, Bang J, Quan H T and Li T 2018 Experimental test of the differential fluctuation theorem and a generalized Jarzynski equality for arbitrary initial states *Phys. Rev. Lett.* **120** 080602
- [294] Wang G M, Reid J C, Carberry D M, Williams D R M, Seveck E M and Evans D J 2005 Experimental study of the fluctuation theorem in a nonequilibrium steady state *Phys. Rev. E* **71** 046142
- [295] Ritort F, Bustamante C and Tinoco I 2002 A two-state kinetic model for the unfolding of single molecules by mechanical force *Proc. Natl Acad. Sci.* **99** 13544–8
- [296] Nagar H and Roichman Y 2014 Collective excitations of hydrodynamically coupled driven colloidal particles *Phys. Rev. E* **90** 042302
- [297] Tal-Friedman O, Pal A, Sekhon A, Reuveni S and Roichman Y 2020 Experimental realization of diffusion with stochastic resetting *J. Phys. Chem. Lett.* **11** 7350–5
- [298] Liu Y, Edmond K V, Curran A, Bryant C, Peng B, Aarts D G A L, Sacanna S and Dullens R P A 2016 Core-shell particles for simultaneous 3D imaging and optical tweezing in dense colloidal materials *Adv. Mater.* **28** 8001–6
- [299] Firth W J 1990 Spatial instabilities in a Kerr medium with single feedback mirror *J. Mod. Opt.* **37** 151–3
- [300] Fournier J-M et al 2005 Assembling mesoscopic particles by various optical schemes *Proc. SPIE* **5930** 59300Y
- [301] d'Alessandro G and Firth W J 1991 Spontaneous hexagon formation in a nonlinear optical medium with feedback mirror *Phys. Rev. Lett.* **66** 2597
- [302] Taturi J, Ma X, Stanton M M and Sánchez S 2017 Designing micro-and nanoswimmers for specific applications *Acc. Chem. Res.* **50** 2–11

- [303] Chen H, Zhao Q and Xuemin D 2018 Light-powered micro/nanomotors *Micromachines* **9** 41
- [304] Li T, Li J, Morozov K I, Wu Z, Xu T, Rozen I, Leshansky A M, Li L and Wang J 2017 Highly efficient freestyle magnetic nanoswimmer *Nano Lett.* **17** 5092–8
- [305] Rubinsztajn-Dunlop H et al 2016 Roadmap on structured light *J. Opt.* **19** 013001
- [306] Lin Z, Si T, Wu Z, Gao C, Lin X and He Q 2017 Light-activated active colloid ribbons *Angew. Chem.* **129** 13702–5
- [307] Búzás A, Kelemen L, Mathesz A, Orosz L, Vizsnyiczai G, Vicsek T and Ormos P 2012 Light sailboats: laser driven autonomous microrobots *Appl. Phys. Lett.* **101** 041111
- [308] Wittkowski R, Jeggle J and Denz C 2021 Photonically propelled nano- and microparticles: from single-particle motion to collective dynamics *Proc. SPIE* **11812** 1181205
- [309] Cichos F, Gustavsson K, Mehlig B and Volpe G 2020 Machine learning for active matter *Nat. Mach. Intell.* **2** 94–103
- [310] Patra P P, Chikkaraddy R, Tripathi R P N, Dasgupta A and Kumar G V P 2014 Plasmodifluidic single-molecule surface-enhanced Raman scattering from dynamic assembly of plasmonic nanoparticles *Nat. Commun.* **5** 4357
- [311] Le Ru E C and Etchegoin P G 2012 Single-molecule surface-enhanced Raman spectroscopy *Annu. Rev. Phys. Chem.* **63** 65–87
- [312] Tiwari S, Khandelwal U, Sharma V and Kumar G V P 2021 Single molecule surface enhanced Raman scattering in a single gold nanoparticle-driven thermoplasmonic tweezer *J. Phys. Chem. Lett.* **12** 11910–8
- [313] Sharma V, Tiwari S, Paul D, Sahu R, Chikkadi V and Kumar G V P 2021 Optothermal pulling, trapping, and assembly of colloids using nanowire plasmons *Soft Matter* **17** 10903–9
- [314] Wheaton S, Gelfand R M and Gordon R 2015 Probing the Raman-active acoustic vibrations of nanoparticles with extraordinary spectral resolution *Nat. Photon.* **9** 68–72
- [315] Tong L, Righini M, Ujue Gonzalez M, Quidant R and Käll M 2009 Optical aggregation of metal nanoparticles in a microfluidic channel for surface-enhanced Raman scattering analysis *Lab Chip* **9** 193–5
- [316] Fränzl M, Thalheim T, Adler J, Huster D, Posseckardt J, Mertig M and Cichos F 2019 Thermophoretic trap for single amyloid fibril and protein aggregation studies *Nat. Methods* **16** 611–4
- [317] Liu Y et al 2018 Nanoradiator-mediated deterministic opto-thermoelectric manipulation *ACS Nano* **12** 10383–92
- [318] Jiang Q, Roy P, Claude J-B and Wenger J 2021 Single photon source from a nanoantenna-trapped single quantum dot *Nano Lett.* **21** 7030–6
- [319] Gillibert R et al 2019 Raman tweezers for small microplastics and nanoplastics identification in seawater *Environ. Sci. Technol.* **53** 9003–13
- [320] Ajito K and Torimitsu K 2002 Single nanoparticle trapping using a Raman tweezers microscope *Appl. Spectrosc.* **56** 541–4
- [321] Schwaferts C, Sogne V, Welz R, Meier F, Klein T, Niessner R, Elsner M and Ivleva N P 2020 Nanoplastic analysis by online coupling of Raman microscopy and field-flow fractionation enabled by optical tweezers *Anal. Chem.* **92** 5813–20
- [322] Ripken C, Kotsifaki D G and Nic Chormaic S 2021 Analysis of small microplastics in coastal surface water samples of the subtropical island of Okinawa, Japan *Sci. Total Environ.* **760** 143927
- [323] Zhang S, Sun Y, Liu B and Li R 2020 Full size microplastics in crab and fish collected from the mangrove wetland of Beibu Gulf: evidences from Raman tweezers (1–20  $\mu\text{m}$ ) and spectroscopy (20–5000  $\mu\text{m}$ ) *Sci. Total Environ.* **759** 143504
- [324] Gigault J, Halle A T, Baudrimont M, Pascal P-Y, Gauffre F, Phi T-L, El Hadri H, Grassl B and Reynaud S 2018 Current opinion: what is a nanoplastic? *Environ. Pollut.* **235** 1030–4
- [325] Bergmann M, Mützel S, Primpke S, Tekman M B, Trachsel J and Gerdtts G 2019 White and wonderful? Microplastics prevail in snow from the Alps to the Arctic *Sci. Adv.* **5** eaax1157
- [326] Authority E F S 2021 EFSA scientific colloquium 25—A coordinated approach to assess the human health risks of micro- and nanoplastics in food *EFSA Support. Publ.* **18** 6815E
- [327] Ivleva N P 2021 Chemical analysis of microplastics and nanoplastics: challenges, advanced methods, and perspectives *Chem. Rev.* **121** 11886–936
- [328] Tinnefeld P, Eggeling C and Hell S W 2015 *Far-Field Optical Nanoscopy* (Berlin: Springer) (<https://doi.org/10.1007/978-3-662-45547-0>)
- [329] Erni-Cassola G, Gibson M I, Thompson R C and Christie-Oleza J A 2017 Lost, but found with Nile red: a novel method for detecting and quantifying small microplastics (1 mm to 20  $\mu\text{m}$ ) in environmental samples *Environ. Sci. Technol.* **51** 13641–8
- [330] Vidal C and Pasquini C 2021 A comprehensive and fast microplastics identification based on near-infrared hyperspectral imaging (HSI-NIR) and chemometrics *Environ. Pollut.* **285** 117251
- [331] Ren Y, Chen Q, He M, Zhang X, Qi H and Yan Y 2021 Plasmonic optical tweezers for particle manipulation: principles, methods, and applications *ACS Nano* **15** 6105–28
- [332] Reich O, David G, Esat K and Signorell R 2020 Weighing picogram aerosol droplets with an optical balance *Commun. Phys.* **3** 1–8
- [333] Abbondanzieri E A, Greenleaf W J, Shaevitz J W, Landick R and Block S M 2005 *Nature* **438** 460–5
- [334] Wen J-D, Lancaster L, Hodges C, Zeri A-C, Yoshimura S H, Noller H F, Bustamante C and Tinoco I 2008 *Nature* **452** 598–603
- [335] Sudhakar S, Abdosamadi M K, Jachowski T J, Bugiel M, Jannasch A and Schäffer E 2021 *Science* **371** eabd9944
- [336] Capitanio M and Pavone F S 2013 *Biophys. J.* **105** 1293–303
- [337] Dudko O K, Hummer G and Szabo A 2008 *Proc. Natl Acad. Sci. USA* **105** 15755–60
- [338] Ishijima A, Kojima H, Funatsu T, Tokunaga M, Higuchi H, Tanaka H and Yanagida T 1998 *Cell* **92** 161–71
- [339] Van Mameren J, Modesti M, Kanaar R, Wyman C, Peterman E J G and Wuite G J L 2009 *Nature* **457** 745–8
- [340] Comstock M J, Ha T and Chemla Y R 2011 *Nat. Methods* **8** 335–40
- [341] Desai V P, Frank F, Lee A, Righini M, Lancaster L, Noller H F, Tinoco I and Bustamante C 2019 *Mol. Cell* **75** 1007–1019.e5
- [342] Heller I, Sitters G, Broekmans O D, Farge G, Menges C, Wende W, Hell S W, Peterman E J G and Wuite G J L 2013 *Nat. Methods* **10** 910–6
- [343] Pertici I et al 2018 *Nat. Commun.* **9** 3532
- [344] Longyear T, Walcott S and Debold E P 2017 *Sci. Rep.* **7** 1822
- [345] Lombardo A T, Nelson S R, Kennedy G G, Trybus K M, Walcott S and Warshaw D M 2019 *Proc. Natl Acad. Sci. USA* **116** 8326–35
- [346] Arbore C, Perego L, Sergides M and Capitanio M 2019 *Biophys. Rev.* **11** 765–82
- [347] Freikamp A, Mehlich A, Klingner C and Grashoff C J 2017 *Struct. Biol.* **197** 37–42
- [348] Sergides M, Perego L, Galgani T, Arbore C, Pavone F S and Capitanio M 2021 *Eur. Phys. J. Plus* **136** 316
- [349] Agrawal R, Smart T J, Nobre-Cardoso J, Richards C J, Bhatnagar R, Tufail A, Shima D, Jones P H and Pavesio C 2016 Assessment of red blood cell deformability in type 2 diabetes mellitus and diabetic retinopathy by dual optical tweezers stretching technique *Sci. Rep.* **6** 15873



- [350] Guck J, Ananthakrishnan R, Mahmood H, Moon T J, Cunningham C C and Käs J 2001 The optical stretcher: a novel tool to micromanipulate cells *Biophys. J.* **81** 767–84
- [351] De Belly H, Stubb A, Yanagida A, Labouesse C, Jones P H, Paluch E K and Chalut K J 2021 Membrane tension gates ERK-mediated regulation of pluripotent cell fate *Cell Stem Cell* **28** 1–12
- [352] Bolognesi G, Friddin M S, Salehi-Reyhani A, Barlow N, Brooks N J, Ces O and Elani Y 2018 Sculpting and fusing biomimetic vesicle networks using optical tweezers *Nat. Commun.* **9** 1
- [353] Wang Y, Botvinick E L, Zhao Y, Berns M W, Usami S, Tsien R Y and Chien S 2005 Visualizing the mechanical activation of Src *Nature* **434** 1040–5
- [354] Feng Y, Reinherz E L and Lang M J 2018  $\alpha\beta$  T cell receptor mechanosensing forces out serial engagement *Trends Immunol.* **39** 596–609
- [355] Glass D G, McAlinden N, Millington O R, Wright A J and Frischknecht F 2017 A minimally invasive optical trapping system to understand cellular interactions at onset of an immune response *PLoS One* **12** e0188581
- [356] Matheson A B, Paterson L, Wright A J, Mendonca T, Tassieri M and Dalgarno P A 2021 Optical tweezers with integrated multiplane microscopy (OpTIMuM): a new tool for 3D microrheology *Sci. Rep.* **11** 5614
- [357] Selhuber-Unkel C, Yde P, Berg-Sørensen K and Oddershede L B 2009 Variety in intracellular diffusion during the cell cycle *Phys. Biol.* **6** 025015
- [358] Hendricks A, Holzbaur E and Goldman Y 2012 Force measurements on cargoes in living cells reveal collective dynamics of microtubule motors *Proc. Natl Acad. Sci. USA* **109** 18447–52
- [359] Mas J, Richardson A C, Reihani S N S, Oddershede L B and Berg-Sørensen K 2013 Quantitative determination of optical trapping strength and viscoelastic moduli inside living cells *Phys. Biol.* **10** 046006
- [360] Dzementsei A, Barooji Y F, Ober E A and Oddershede L B 2022 Foregut organ progenitors and their niche display distinct viscoelastic properties *in vivo* during early morphogenesis stages *Commun. Biol.* **5** 402
- [361] Chaubet L, Chaudhary A R, Heris H K, Ehrlicher A J and Hendricks A G 2020 Dynamic actin cross-linking governs the cytoplasm's transition to fluid-like behavior *Mol. Biol. Cell* **31** 1744–52
- [362] Borries M, Barooji Y F, Yennek S, Grapin-Botton A, Berg-Sørensen K and Oddershede L B 2020 Quantification of visco-elastic properties of a matrigel for organoid development as a function of polymer concentration *Front. Phys.* **8** 579168
- [363] Wullkopf L, West A-K V, Leijnse N, Cox T R, Madsen C D, Oddershede L B and Erler J T 2018 Cancer cell's ability to mechanically adjust to extracellular matrix stiffness correlates with their invasive potential *Mol. Biol. Cell* **29** 2378–85
- [364] Blazquez-Castro A 2019 Optical tweezers: phototoxicity and thermal stress in cells and biomolecules *Micromachines* **52** 507
- [365] Tahara T, Quan X, Otani R, Takaki Y and Matoba O 2018 Digital holography and its multidimensional imaging applications: a review *Microscopy* **67** 55–67
- [366] Pouladian P, Yamauchi T, Wakida N M, Gomez-Godinez V, Berns M W and Preece D 2021 Combining quantitative phase microscopy and laser-induced shockwave for the study of cell injury *Biomed. Opt. Express* **12** 4020–31
- [367] Dardikman G and Shaked N T 2018 Review on methods of solving the refractive index–thickness coupling problem in digital holographic microscopy of biological cells *Opt. Commun.* **422** 8–16
- [368] Park Y, Depeursinge C and Popescu G 2018 Quantitative phase imaging in biomedicine *Nat. Photon.* **12** 578–89
- [369] Marquet P, Depeursinge C and Magistretti P J 2014 Review of quantitative phase-digital holographic microscopy: promising novel imaging technique to resolve neuronal network activity and identify cellular biomarkers of psychiatric disorders *Neurophotonics* **1** 020901
- [370] Memmolo P, Miccio L, Merola F, Gennari O, Netti P A and Ferraro P 2014 3D morphometry of red blood cells by digital holography *Cytometry A* **85** 1030–6
- [371] Patel N, Rawat S, Joglekar M, Chhaniwal V, Dubey S K, O'Connor T, Javidi B and Anand A 2021 Compact and low-cost instrument for digital holographic microscopy of immobilized micro-particles *Opt. Lasers Eng.* **137** 106397
- [372] Merola F et al 2017 Tomographic flow cytometry by digital holography *Light Sci. Appl.* **6** e16241–e16241
- [373] Pouladian P, Perez N, Yamauchi T, Wakida N M, Berns M W and Preece D 2021 A method to study cellular injuries using optical trapping combined with laser-induced shockwaves under quantitative phase microscope *Proc. SPIE* **11798** 1179808
- [374] Thomas P 2019 Intrinsic and extrinsic noise of gene expression in lineage trees *Sci. Rep.* **9** 474
- [375] Creely C, Volpe G, Singh G, Soler M and Petrov D 2005 Raman imaging of floating cells *Opt. Express* **13** 6105–10
- [376] Xie C, Dinno M A and Li Y-Q 2002 Near-infrared Raman spectroscopy of single optically trapped biological cells *Opt. Lett.* **27** 249–51
- [377] Volpe G, Singh G P and Petrov D 2006 Dynamics of a growing cell in an optical trap *Appl. Phys. Lett.* **88** 231106
- [378] Singh G P, Volpe G, Creely C M, Grötsch H, Geli I M and Petrov D 2006 The lag phase and G1 phase of a single yeast cell monitored by Raman microspectroscopy *J. Raman Spectrosc.* **37** 858–64
- [379] Singh G P, Creely C M, Volpe G, Grötsch H and Petrov D 2005 Real-time detection of hyperosmotic stress response in optically trapped single yeast cells using Raman microspectroscopy *Anal. Chem.* **77** 2564–8
- [380] Blomqvist C H, Dinér P, Gröthli M, Goksör M and Adiels C B 2014 A single-cell study of a highly effective Hog1 inhibitor for *in situ* yeast cell manipulation *Micromachines* **5** 81–96
- [381] Babazadeh R, Adiels C B, Smedh M, Petelenz-Kurdiel E, Goksör M and Hohmann S 2013 Osmostress-induced cell volume loss delays yeast Hog1 signaling by limiting diffusion processes and by Hog1-specific effects *PLoS One* **8** e80901
- [382] Gustavsson A-K, van Niekerk D D, Adiels C B, Du Preez F B, Goksör M and Snoep J L 2012 Sustained glycolytic oscillations in individual isolated yeast cells *FEBS J.* **279** 2837–47
- [383] Bendrioua L, Smedh M, Almquist J, Cvijovic M, Jirstrand M, Goksör M, Adiels C B and Hohmann S 2014 Yeast AMP-activated protein kinase monitors glucose concentration changes and absolute glucose levels *J. Biol. Chem.* **289** 12863–75
- [384] Gustavsson A-K, Adiels C B, Mehlig B and Goksör M 2015 Entrainment of heterogeneous glycolytic oscillations in single cells *Sci. Rep.* **5** 9404
- [385] Wang X, Chen S, Kong M, Wang Z, Costa K D, Li R A and Sun D 2011 Enhanced cell sorting and manipulation with combined optical tweezer and microfluidic chip technologies *Lab Chip* **11** 3656–62
- [386] Pineda J, Midtvedt B, Bachimanchi H, Noé S, Midtvedt D, Volpe G and Manzo C 2022 Geometric deep learning reveals the spatiotemporal fingerprint of microscopic motion (arXiv:2202.06355)
- [387] Chapin S C, Germain V and Dufresne E R 2006 Automated trapping, assembly, and sorting with holographic optical tweezers *Opt. Express* **14** 13095–100
- [388] Managò S, Valente C, Mirabelli P, Circolo D, Basile F, Corda D and De Luca A C 2016 A reliable Raman-spectroscopy-based approach for diagnosis, classification and follow-up of B-cell acute lymphoblastic leukemia *Sci. Rep.* **6** 1–13

- [389] Pilát Z, Bernatová S, Ježek J, Kirchhoff J, Tannert A, Neugebauer U, Samek O and Zemánek P 2018 Microfluidic cultivation and laser tweezers Raman spectroscopy of *E. coli* under antibiotic stress *Sensors* **18** 1623
- [390] Chan J W, Esposito A P, Talley C E, Hollars C W, Lane S M and Huser T 2004 Reagentless identification of single bacterial spores in aqueous solution by confocal laser tweezers Raman spectroscopy *Anal. Chem.* **76** 599–603
- [391] De Luca A C, Rusciano G, Ciancia R, Martinelli V, Pesce G, Rotoli B, Selvaggi L and Sasso A 2008 Spectroscopical and mechanical characterization of normal and thalassemic red blood cells by Raman tweezers *Opt. Express* **16** 7943–57
- [392] Zhang Q, Zhang P, Gou H, Mou C, Huang W E, Yang M, Xu J and Ma B 2015 Towards high-throughput microfluidic Raman-activated cell sorting *Analyst* **140** 6758
- [393] Yan S, Qiu J, Guo L, Li D, Xu D and Liu Q 2021 Development overview of Raman-activated cell sorting devoted to bacterial detection at single-cell level *Appl. Microbiol. Biotechnol.* **105** 1315–31
- [394] Managò S, Tramontano C, Delle Cave D, Chianese G, Zito G, De Stefano L, Terracciano M, Lonardo E, De Luca A C and Rea I 2021 SERS quantification of galunisertib delivery in colorectal cancer cells by plasmonic-assisted diatomite nanoparticles *Small* **17** 2101711
- [395] Dochow S, Krafft C, Neugebauer U, Bocklitz T, Henkel T, Mayer G, Albert J and Popp J 2011 Tumour cell identification by means of Raman spectroscopy in combination with optical traps and microfluidic environments *Lab Chip* **11** 1484–90
- [396] Schie I W, Rüger J, Mondol A S, Ramoji A, Neugebauer U, Krafft C and Popp J 2018 High-throughput screening Raman spectroscopy platform for label-free cellomics *Anal. Chem.* **90** 2023–30
- [397] Williams D A and Cecchi-Pestellini C 2015 *The chemistry of cosmic dust* (London: Royal Society of Chemistry)
- [398] Alali H, Gong Z, Videen G, Pan Y-L, Muñoz O and Wang C 2020 Laser spectroscopic characterization of single extraterrestrial dust particles using optical trapping-cavity ringdown and Raman spectroscopy *J. Quant. Spectrosc. Radiat. Transfer* **255** 107249
- [399] Rietmeijer F J M, Della Corte V, Ferrari M, Rotundi A and Brunetto R 2016 Laboratory analyses of meteoric debris in the upper stratosphere from settling bolide dust clouds *Icarus* **266** 217–34
- [400] Cecchi-Pestellini C, Iati M A and Williams D A 2012 The nature of interstellar dust as revealed by light scattering *J. Quant. Spectrosc. Radiat. Transfer* **113** 2310–20
- [401] Zubko E, Muinonen K, Muñoz O, Nousiainen T, Shkuratov Y, Sun W and Videen G 2013 Light scattering by feldspar particles: comparison of model agglomerate debris particles with laboratory samples *J. Quant. Spectrosc. Radiat. Transfer* **131** 175–87
- [402] Shvedov V G, Rode A V, Izdebskaya Y V, Desyatnikov A S, Krolikowski W and Kivshar Y S 2010 Giant optical manipulation *Phys. Rev. Lett.* **105** 118103
- [403] Rudd D, Lopez-Mariscal C, Summers M, Shahvisi A, Gutiérrez-Vega J C and McGloin D 2008 Fiber based optical trapping of aerosols *Opt. Express* **16** 14550–60
- [404] Garces-Chavez V, Roskey D, Summers M D, Melville H, McGloin D, Wright E M and Dholakia K 2004 Optical levitation in a Bessel light beam *Appl. Phys. Lett.* **85** 4001–3
- [405] Pan Y L, Kalume A, Lenton I C, Nieminen T A, Stilgoe A B, Rubinsztein-Dunlop H, Beresnev L A, Wang C and Santarpia J L 2019 Optical-trapping of particles in air using parabolic reflectors and a hollow laser beam *Opt. Express* **27** 33061–9
- [406] Johnson L, Swartzlander G A Jr and Artusio-Glimpse A B 2014 An overview of solar sail propulsion within NASA *Advances in Solar Sailing* ed M Macdonald (Heidelberg: Springer Praxis) pp 15–23
- [407] Spencer D, Betts B, Bellardo J, Diaz A, Plante B and Mansell J 2020 The lightsail 2 solar sailing technology demonstration *Adv. Space Res.* **67** 2878–89
- [408] Atwater H A, Davoyan A R, Ilic O, Jariwala D, Sherrott M C, Went C M, Whitney W S and Wong J 2018 Materials challenges for the starshot lightsail *Nat. Mater.* **17** 861–7
- [409] Swartzlander G A Jr 2017 Radiation pressure on a diffractive sailcraft *J. Opt. Soc. Am. B* **34** C25–C30
- [410] McInnes C R 2004 *Solar Sailing: Technology, Dynamics and Mission Applications* (Berlin: Springer)
- [411] Dubill A L and Swartzlander G A Jr 2021 Circumnavigating the sun with diffractive solar sails *Acta Astronaut.* **187** 190–5
- [412] Nerisyan S R, Tabiryan N V, Steeves D M and Kimball B R 2009 Optical axis gratings in liquid crystals and their use for polarization insensitive optical switching *J. Nonlinear Opt. Phys. Mater.* **18** 1–47
- [413] Serak S V, Roberts D E, Hwang J-Y, Nersisyan S R, Tabiryan N V, Bunning T J, Steeves D M and Kimball B R 2017 Diffractive waveplate arrays *J. Opt. Soc. Am. B* **34** B56–B63
- [414] Yu N, Genevet P, Kats M A, Aieta F, Tetienne J-P, Capasso F and Gaburro Z 2011 Light propagation with phase discontinuities: generalized laws of reflection and refraction *Science* **334** 333–7
- [415] Wang P, Mohammad N and Menon R 2016 Chromatic-aberration-corrected diffractive lenses for ultra-broadband focusing *Sci. Rep.* **6** 21545